The digital aqueous humor outflow meter: an alternative tool for screening of the human eye outflow facility

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Purpose: To develop, characterize, and validate a prototype digital aqueous humor outflow tonographer (DAHOM).

Material and methods: The DAHOM was developed, characterized, and validated in three phases. Phase 1 involved construction of the sensor. This was broadly based on the fundamental design of a typical Schiotz tonographer with a series of improvements, including corneal indentation, which was converted to an electrical signal via a linear variable differential transducer, an analog signal which was converted to digital via ADC circuitry, and digital data acquisition and processing which was made possible by a serial port interface. Phase 2 comprised development of software for automated assessment of the outflow facility. Automated outflow facility assessment incorporated a series of fundamental improvements in comparison with traditional techniques, including software-based filtering of ripple noise and extreme variations, rigidity impact analysis, and evaluation of the impact of patient age, central corneal thickness, and ocular axial length. Phase 3 comprised characterization and validation of DAHOM, for which we developed an experimental setup using porcine cadaver eyes. DAHOM’s repeatability was evaluated by means of Cronbach’s alpha and intraclass correlation coefficient. The level of agreement with a standard Schiotz tonographer was evaluated by means of paired t-tests and Bland-Altman analysis in human eyes.

Results: The experimental setup provided the necessary data for the characterization of DAHOM. A fourth order polynomial equation provided excellent fit (R square $>0.999$). DAHOM demonstrated high repeatability (Cronbach’s alpha $>0.997$; intraclass correlation coefficient $>0.987$) and an adequate level of agreement with a standard Schiotz tonographer.

Conclusions: This study presents the development, characterization, and validation of a prototype digital tonographer. DAHOM demonstrates high repeatability and a sufficient level of agreement with a typical Schiotz tonographer, while its digital design remedies known vulnerabilities of conventional tonographers.

Keywords: glaucoma, tonography, pressure, outflow facility, aqueous humor

Introduction

The importance of aqueous humor tonography in research settings has been highlighted over many years. Tonography outcomes provide essential information for a series of ophthalmic diseases, eg, the glaucomas, and facilitate exploration of the ocular manifestations of systemic diseases. However, tonography in daily clinical settings has yet to be applied, mainly due to time constraints in hospital departments. Moreover, prevalent tonographic settings suffer from poor repeatability which limits their clinical usefulness. Among the primary causes of variability is the fact that reliable measurements require continuous eye alignment, which is...
difficult to achieve in practice. On the other hand, data collection and processing using traditional tonographers is difficult, because they do not provide digital output, automated assessment of the outflow facility, or evaluation of the impact of a series of known modifiers of the outflow facility. Within this context, we demonstrate here the development, characterization, and validation of a novel digital aqueous humor outflow topographer (DAHOM) that addresses the series of vulnerabilities of traditional tonographers.

**Materials and methods**

**Setting**
The study adhered to the tenets of the Declaration of Helsinki and written informed consent was given by all participants. This was a prospective study conducted in the Department of Ophthalmology at the University Hospital of Alexandroupolis in Greece between 2004 and 2007.

**Development of DAHOM**
The digital outflow meter was designed at the Eye Institute of Thrace, in collaboration with the Electrical Engineering Department of the Technical University of Thrace. The development of the system was done in three phases.

**Phase 1**
Phase 1 included construction of the electromechanical system with the sensor and the electronic circuitry (Figure 1). The sensor design was broadly based on the fundamental design of a typical Schiotz tonographer. The sensor converted corneal indentation to electrical signal with high sensitivity (1.719 mV/volt/0.0254 mm) using a linear variable differential transducer. All elements were connected to an aluminum alloy frame capable of retraction and sterilization. Analog to digital signal conversion was accomplished using ADC electronic circuitry providing interface via a serial port (RS232, Figure 2).

**Figure 1** Digital outflow meter, including linear variable differential transducer and signal conditioner circuit.

The digital outflow transducer with the contact tip (indentation piston), the base (center), and the linear variable differential transducer sensor (right). Connector cables are used for power supply and data transfer to the DAQ board. The signal conditioning board is responsible for sinusoidal wave generation, signal rectification, and phase-sensitive demodulation processing.
Phase 2

Phase 2 involved development of the software and the conversion algorithm for the evaluation of the outflow facility. A software-based percentile filter was used to cut out ripple noise and random measurement variations (Figure 3). Observed differences in intraocular pressure (IOP) measurements between the DAHOM and Goldmann applanation tonometer (GAT) were used for assessment of ocular rigidity.

The outflow facility was calculated according to the following formula:

\[
C_{\text{out}} = \frac{\Delta V}{\left(\frac{P_{t0} + P_{t4}}{2} - P_{\text{applanation}} - \Delta P_{\text{indentation}}\right) \cdot 4}
\]

\[
= \frac{(V_{c4} - V_{c9}) + \left(\frac{1}{K} \log \left(\frac{P_{t0}}{P_{t4}}\right)\right)}{\left(\frac{P_{t0} + P_{t4}}{2} - P_{\text{applanation}} - \Delta P_{\text{indentation}}\right) \cdot 4}
\]

where \(V_{c4} - V_{c9}\) is the corneal volume displacement during the tonography study, \(K\) is the sclera rigidity factor or ocular rigidity factor, \(P_{t0}/P_{t4}\) is the hydrostatic pressure difference between the points of flow resistance, \(P_{\text{applanation}}\) is the IOP measured by GAT, \(\Delta P\) is the mechanical increase of IOP from the weight of the tonographer, and 4 is duration of the study in minutes.4

A software program was developed in Java language, capable of calculating the outflow facility (Figure 4). Rigidity impact analysis was incorporated in the software algorithm using GAT IOP measurement, as suggested by Friedenwald.4

The following formula was used to calculate rigidity:

\[
\text{Rigidity} = 4.5282E^{-3} + 6.7443E^{-4}X + 6.165E^{+6}X^2
\]

\[
- 2.18104E^{-1}X^3 - 2.07212E^{-8}X^4 + 2.7598E^{+9}X^5
\]

\[
- 1.1391E^{-10}X^6 + 2.26627E^{-12}X^7
\]

\[
- 2.20326E^{-14}X^8 + 8.45107E^{+7}X^9
\]

where \(X\) is the mathematical arc tangent operator of the difference between the applanation and the indentation IOP, while the following three formulas (F1–F3) were used to define the indentational versus IOP measurement for 5.5, 7.5, and 10 g weight of the digital outflow meter:

\[
\text{IOP}_{\text{indent}}^{5.5g} = 51.081 - 5.887x + 0.479x^2
\]

\[
- 0.0215x^3 + 3.832E^{-4}x^4
\]  

(F1)
where \( x \) is the magnitude of indentation for the digital tonographer in mm.

A series of optional parameters were also incorporated in the algorithm in order to correct the rigidity measurements based on the influence of several biomechanical factors, including central cornea thickness, age of patient, and ocular axial length (Figure 4). These formulae were derived from previously published studies on ocular rigidity variation.\(^{5,6}\)

\[
IOP_{\text{Indent}}^{7.5\%} = 69.668 - 8.045x + 0.655x^2 - 0.029x^3 + 5.204E^{-4}x^4 \quad (F2)
\]

\[
IOP_{\text{Indent}}^{10\%} = 92.89 - 10.717x + 0.872x^2 - 0.039x^3 + 6.937E^{-4}x^4 \quad (F3)
\]

\[
K_{\text{age}} = 0.00526 + 1.09285E^{-4} \times \text{Age}
\]

\[
K_{\text{cct}} = -0.02055 + 6.33781E^{-5} \cdot \text{CCT}
\]

\[
K_{\text{refraction}} = 0.02056 + 6.6158E^{-4}L + 2.0559E^{-5}L^2 + 9.70044E^{-7}L^3 + 1.6981E^{-8}L^4
\]
where $K_{\text{age}}$ is the rigidity variation based on the age of the patient; $K_{\text{CCT}}$ is the rigidity variation based on central cornea thickness; $K_{\text{refraction}}$ is the rigidity variation based on the ocular axial length; age is patient age in years; CCT is the central corneal thickness (µm); and L is the ocular axial length (mm).

**Phase 3**
Phase 3 involved characterization and validation of the DAHOM. Characterization of the tonometer was accomplished using porcine cadaver eyes according to the following procedure. A microelectronic pressure sensor was implanted into the anterior chamber using a fine needle. A second needle was injected into the eye, connecting a water tank of balanced solution for IOP regulation, which was accomplished by altering the water tank height and thus affecting the hydrostatic pressure difference in the eye (Figures 5 and 6). Experimental IOP measurements were obtained in the range 5–90 mmHg, with a 1 mmHg increment.

Validation of the system was accomplished by comparing the measurement outcomes of the DAHOM with the corresponding ones of a Schiotz tonographer in a population of 30 volunteers according to the following procedure. Outflow facility measurements were obtained in one eye using a Schiotz tonographer and in the fellow eye by the DAHOM. Within one week, the procedure was repeated in a crossover manner. All tonography measurements were obtained by the same experienced operator (NF) who ensured proper eye fixation. Before each measurement, the Schiotz tonographer was calibrated according to the manufacturer’s instructions. GAT IOP measurements determined the indentation weight for both systems. For IOPs less than 30 mmHg, a 5.5 g weight was used, while a 7.5 g weight was used for IOP between 30 and 45 mmHg. For IOPs higher than 45 mmHg, a 10 g weight was used. The level of agreement between the two systems was evaluated by means of paired $t$-test and by Bland-Altman analysis. DAHOM repeatability was evaluated.

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**Figure 5** Laboratory setup for the characterization of the digital outflow meter. Laboratory setup for the calibration of the system. The balanced solution (BSS) container is used for intracameral pressure regulation, the micropressure sensor is used for intracameral real-time intraocular pressure measurements, while the digital outflow meter performs tonography. All data are collected by the PC and analyzed.
by both Cronbach’s alpha test and the intraclass correlation coefficient (ICC) from three consecutive measurements prior to the tonography study.

Statistical analysis
Results were analyzed with the SPSS Version 17.0 (Statistical Package for the Social Sciences Inc., Chicago, IL). The normality of continuous variables was assessed using the Kolmogorov-Smirnov test. Quantitative variables expressed as mean ± standard deviation (SD) and qualitative variables were expressed as frequencies and percentages. The Mann-Whitney test was used to assess outflow facility variations between the Schiotz and digital outflow meters. All tests were two-tailed, and statistical significance was considered as $P < 0.05$. Intrasection repeatability was tested using Cronbach’s alpha test and the ICC. Agreement of the outflow facility measurements between the digital and Schiotz outflow meters was assessed with Bland-Altman plots and 95% limits of agreement. MedCalc version 9.0 software was used for the Bland-Altman plots.

Results
The experimental setup with the porcine eyes provided the necessary data for the characterization of the system’s response, according to the following formulae:

\[ IOP_{MEMS} = 51.081 - 117.735x + 191.649x^2 - 171.753x^3 + 61.131x^4 \]  
(F4)

\[ IOP_{MEMS} = 69.668 - 160.908x + 262.05x^2 - 234.266x^3 + 83.266x^4 \]  
(F5)

\[ IOP_{MEMS} = 92.89 - 214.339x + 348.911x^2 - 312.038x^3 + 111x^4 \]  
(F6)

where $x$ is the magnitude of indentation for the DAHOM in mm.

In fact, the characterization of the DAHOM was accomplished using a fourth order polynomial equation (adjusted R-square >0.999 in all polynomial fittings, Figure 7). Three different polynomial equations were derived, each one
corresponding to a different plunger weight. Systems transfer functions are shown below. Equation F7 was used for a 5.5 g plunger weight, F8 for 7.5 g, and F9 for 10 g:

\[
y(x) = 51.081 - 117.735x + 191.649x^2 - 171.753x^3 + 61.131x^4 \quad (F7)
\]

\[
y(x) = 69.668 - 160.908x + 262.05x^2 - 234.266x^3 + 83.266x^4 \quad (F8)
\]

\[
y(x) = 92.89 - 214.339x + 348.911x^2 - 312.0.8x^3 + 111x^4 \quad (F9)
\]

It should be mentioned that all polynomials were derived by assessment of the best fitting of the experimental results in a Cartesian plot, with one axis representing the experimental measurements of interest and the second axis representing the values obtained by the DAHOM. The order of polynomial fitting was selected in a way to provide R-Square adjustment higher than 0.98, ensuring minimum calculation error.

DAHOM demonstrated a sufficient level of agreement with the Schiotz tonographer. Specifically, the results for DAHOM were: \( C_{\text{Digital}} \pm SD_{\text{Digital}} = 0.168 \pm 0.08 \mu \text{L} \times \text{min}^{-1} \times \text{mmHg}^{-1} \) and for the Schiotz tonometer were: \( C_{\text{Schiotz}} \pm SD_{\text{Schiotz}} = 0.163 \pm 0.09 \mu \text{L} \times \text{min}^{-1} \times \text{mmHg}^{-1} \); Paired sample \( t \)-test validated measurements conformity \((P > 0.12)\). Sufficient level of agreement was also confirmed by Bland-Altman analysis. According to the plot in Figure 8, with the exception of two outlying values, the plot points are distributed in a symmetric manner about the “zero difference” line.

Regarding DAHOM’s measurement repeatability, the Cronbach’s alpha was 0.997 and the ICC was 0.987, both tests suggesting high intrasession reliability.

**Discussion**

The objective of this study was to develop a digital aqueous humor tonographer that could provide valid information about the outflow facility and address a series of technical and design limitations of the conventional tonographers.

Various tonographers have been introduced during the past 60 years. First, Schiotz, then Bock et al and others introduced tonographers for measuring the outflow coefficient, and in 1951, Gant reported the use of an electronic tonographer connected to a paper strip.
studies that used different tonographers.\textsuperscript{14–20} Regarding outflow facility, the series of rigidity impact algorithms (which is not the case however, the outcomes of the DAHOM are corrected by a implementation of the DAHOM project.\textsuperscript{13} Specifically, the ocular rigidity assessment rather than to the design and/or vulnerabilities of the traditional tonographers. Addressing these vulnerabilities will allow the implementation of future relevant studies with high clinical significance in diseases with disrupted aqueous humor outflow, eg, the glaucomas. Among them are the qualitative outflow profile analysis that could provide detail information of the dynamic regulation of the outflow facility,\textsuperscript{23–26} and the development of a glaucoma risk assessment algorithm, capable of identifying preclinical patterns of glaucoma development.

**Disclosure**

The authors report no conflict of interest in this work.

**References**