Carbon Ion Radiotherapy in the Management of Hepatocellular Carcinoma

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Abstract: Localized hepatocellular carcinoma (HCC) that is unresectable and non-transplantable can be treated by several liver-directed therapies. External beam radiation therapy (EBRT) is an increasingly accepted and widely utilized treatment modality in this setting. Accelerated charged particles such as proton beam therapy (PBT) and carbon ion radiation therapy (CIRT) offer technological advancements over conventional photon radiotherapy. In this review, we summarize the distinct advantages of CIRT use for HCC treatment, focusing on physical and biological attributes, and outline dosimetric and treatment planning caveats. Based on these considerations, we posit that HCC may be among the best indications for use of CIRT, as it allows for maximizing tumoricidal doses to the target volume while minimizing the dose to the organs at risk.

Keywords: carbon ion therapy, hepatocellular carcinoma, hypofractionation

Introduction

Hepatocellular carcinoma (HCC) ranks seventh worldwide among the highest frequently diagnosed cancers and ranks second in cancer-related deaths. It is predominantly prevalent in Asia and Africa, accounting for more than 70% of the disease burden worldwide.¹ There were nearly 900,000 people diagnosed with HCC and over 800,000 deaths from HCC globally in 2020. Despite novel therapeutic advances, 10–15% of HCC patients could achieve 5-year overall survival (OS).² Likely reflecting the widespread use of preventative hepatitis B virus (HBV) vaccinations, the prevalence of hepatitis B and C induced HCC is decreasing in high socio-economic index nations. However, HCC associated with long standing alcoholic cirrhosis and non-alcoholic fatty liver disease has been rising steadily in Western nations over the last decade.³

Surgical resection, thermal ablation, and liver transplant remain the gold standard treatments for primary HCC and may yield favorable clinical outcomes. Unfortunately, no more than 30% of localized HCC patients could be eligible for surgical treatment due to underlying liver dysfunction, or deteriorating performance status or medical comorbidities.⁴ Local tumor control while preserving liver function can potentially decrease HCC-related mortality and improve OS.⁵ Minimally invasive techniques can be applied as an alternative treatment option for those who are not surgically eligible. These include transcatheter arterial chemoembolization (TACE), during which chemotherapeutics are infused selectively to the tumor through the feeding blood vessel, yttrium-90 transarterial radioembolization (TARE), wherein the feeding vessel is embolized with radiolabeled beads, and radiofrequency ablation.⁶

Radiotherapy was evaluated as a potential non-invasive treatment for HCC in different stages. HCC is a radiosensitive tumor occurring in a radiosensitive organ that is often diseased and chronically inflamed. Radiotherapy has historically been underutilized for HCC due to concerns regarding the risk of normal liver toxicity. Nevertheless, pioneering research in the arena of partial liver radiation in the 1980s and 1990s in addition to TARE in the past two decades set the stage for delivering ablative doses to the area of interest while at the same time reducing the dose to the adjacent areas. By using highly conformal techniques including stereotactic ablative body radiotherapy and intensity modulated radiation therapy (IMRT), tumor-directed but uninvolved liver sparing therapy has become easier to administer, resulting in a resurgence of interest in the use of this non-invasive modality to treat HCC. Several trials have proven the efficacy and tolerability of different photon-based techniques of EBRT, particularly in complex cases involving large lesions, vascular invasion, and recurrent disease. In early stage inoperable HCC, radiation therapy has also been used to bridge patients to liver transplant.⁷ Photon-based radiotherapy for HCC is constrained by the possibility of triggering radiation-induced liver disease (RILD) and bowel toxicity, uncertainties posed by organ motion, and the difficulty of achieving an effective dose within the tumor while maintaining the mean dose to uninvolved liver as low as possible.⁸ Achieving a low mean liver dose is particularly important in X-ray based therapies given the extensive low dose bath associated with photon therapy. However, this may be less of a concern when utilizing high linear energy transfer (LET) radiation therapy which has no low dose bath and deposits a high dose within the target.⁹

Although not widespread, accelerated particle therapies such as PBT and CIRT have been investigated in selected centers for the management of HCC since the 1980s, and early reports regarding the efficiency of proton therapy in HCC were published in the 1990s.¹⁰ Since then, charged particle therapies have become more widely adopted in the treatment of HCC, as these modalities allow for the delivery of highly localized tumor-targeted radiation to enhance tumor control, while maximally sparing the normal liver via increased dose conformality to the tumor and the absence of an exit dose beyond the tumor along the beam path.¹¹ This review seeks to provide a general overview of CIRT, as well as explore the advantages and pitfalls associated with its use in the management of HCC.

The Relevance of Physical Properties of CIRT in the Treatment of HCC

The elastic and inelastic collisions of charged particles with the atomic nuclei and electrons of tissues allow for the release of its energy in the tissues while heavy ions transverse through tissues and eventually grind to a halt. At the very end of its range, they deposit most of their energy over a short distance, creating the characteristic Bragg peak. In addition to the interaction with electrons, the Coulomb field of charged particles is also repulsed by the electric field of the nucleus of atoms within tissues, causing deflections in its path. Multiple Coulomb scattering events result in lateral beam scattering, explaining the penumbra of a charged particle beam. This penumbra is smaller for heavier particles. Another interaction is the inelastic collision with atomic nuclei wherein the heavy ion is fragmented into multiple lighter ions that travel in the same general direction as the incident ion to create the characteristic fragmentation tail that persists beyond the Bragg peak¹² (Figure 1).

It is important to note that although CIRT and PBT are often thought to be similar, their physical and biological properties differ significantly. Compared to PBT, CIRT has a narrower lateral penumbra, as noted above.¹¹ CIRT is also different from PBT in the creation of the characteristic fragmentation tail. Although the tail constitutes a small fraction of overall dose, the high LET of these light ions can contribute considerably to their biological dose. And compared to PBT where there is no measurable distal dose beyond the Bragg peak, the physical dose profile of CIRT is distinctly altered by the presence of this fragmentation tail. Similar to passively scattered PBT, ridge filters are used to widen the narrow Bragg peak and encompass the tumor volume within the spread out Bragg peak (SOBP). Raster-scanning technology facilitates modulating the intensity of CIRT beam energy to achieve higher conformality of dose to the tumor.^{12–15} Most published data for CIRT of HCCs utilized passive scattering methods. Yet, the promising results reported suggest that in settings of large tumor size and considerable organ motion, a passively scattered beam may be sufficient. Nonetheless, the optimal field formation technique (passive scattering versus spot scanning) for the treatment of HCC warrants further investigation.¹⁶

The treatment of HCC requires the delivery of highly targeted radiation therapy to a large mass while limiting

Figure 1 Percentage depth dose curves for carbon, proton, and photon beams.

radiation dose to the surrounding normal liver and nearby GI tract. The unique physical features of carbon ions including their Bragg peak characteristics, narrow lateral penumbra, and steep dose gradients may serve as ideal attributes for HCC treatment wherein sparing even a low dose bath to the uninvolved liver could be advantageous when there is underlying liver dysfunction.¹⁵ Similar conformality achieved with ablative TARE or “radiation segmentectomy” has demonstrated increased pathologic necrosis rates,^{17–19} providing further justification for employing CIRT as a means to achieve conformality, high radiation doses to the tumor, and efficient sparing of the uninvolved liver. Hypothesizing that an increased tumor dose will translate into improved LC and, in turn, improved OS, one could conjecture that CIRT tumor control is superior to that of the photon and PBT. However, there is no conclusive evidence that this is indeed true. Clearly, randomized data is not available currently and non-randomized comparisons are fraught with biases. The closest data that we are aware of is a report from the Massachusetts General Hospital where retrospective analysis of HCC treatment concluded that proton therapy resulted in better OS compared to photon therapy (median OS was 31 months versus 14 months, $p=0.008$). This was not attributed to a decrease in locoregional recurrence but reduced the risk of non-classic RILD (odds ratio=0.2; 95% CI=0.08–0.8; $p=0.03$). The ongoing prospective randomized NRG study comparing protons to photons may

answer this question and by extension shed light on the potential benefit of CIRT.²⁰

The Relevance of Biological Properties of CIRT in the Treatment of HCC

The high ionization density along the carbon ion beam track result in greater LET, and, in turn, a higher likelihood of complex and clustered DNA damage. These DNA lesions arise along a single track of ionizing radiation and are comprised of two or more distinct lesions within 1–2 helical turns (~10–20 base pairs) of DNA. Individual lesions may be abasic sites, base damage, or single or double strand DNA breaks. The complexity of such multiply damaged DNA sites contributes to the difficulty with repairing them and therefore the persistence of unrepaired DNA damage, readily visualized as widespread γ H2AX foci on 3D structured illumination microscopy following CIRT.²¹ Often the damage is so catastrophic that it results in chromothripsis or chromosome shattering where genome rearrangements and chromosome translocations can contribute to immense genome instability. Both homologous and non-homologous end joining DNA repair pathways are significantly impaired by high LET irradiation, rendering typically radioresistant cells more sensitive to radiotherapy. CIRT has been shown to cause a higher proportion

of damage left unrepaired by homologous recombination mechanisms, because it creates short DNA fragments that remain unbound to the Ku70/Ku80 heterodimer.²² Consequent to this increased DNA damage, CIRT has a higher relative biological effectiveness (RBE) compared to PBT (2–4 vs 1.1).²³ RBE correlates with the dose per fraction with a higher dose per fraction resulting in a lower RBE. Another factor affecting the value of RBE is the repair capacity of tissues after radiation; tissues with a higher repair capacity show lower RBE and tissues with a higher α/β ratio show lower RBE. One of the most important factors determining the radiosensitivity of tissues to low LET radiation is the oxygenation status where hypoxic tissue are known to be more radioresistant, but in CIRT hypoxic tissues are not significantly more resistant to treatment than normoxic tissue. Lastly, CIRT results in greater cell cycle delays in the G2 phase and its efficacy is less cell cycle dependent.²⁴

The intent of treatment is to achieve maximum RBE within the tumor while limiting impact within the normal liver. CIRT can be delivered in ultra-hypofractionated regimens which allow for decreasing RBE, particularly in normal liver tissues, which may ultimately limit the risk of RILD. These distinctive biological properties of carbon ions, particularly their ability to achieve a high RBE in tumor while allowing for a favorable dosimetric profile within normal tissues, present significant advantages over alternative forms of radiation therapy in the treatment of HCC. LET and RBE of various radiation modalities is shown in Table 1.

Table 1 LET and RBE of Various Radiation Modalities

Radiation Modality	Linear Energy Transfer (keV/ μ m)	Relative Biological Effectiveness
Linear accelerator X-rays (6–15 MeV)	0.3	~0.8
Linear accelerator electrons (1 MeV)	0.3	0.9
Cobalt-60 gamma rays	0.2	0.8–0.9
250 kVp X-rays	2	1.0
150 MeV PBT	0.5	~1.1
Neutrons	0.5–100	1–2
Alpha particles	50–200	5–10
CIRT	40–90	2–5

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Dose Prescription for CIRT

Scaling of physical CIRT dose along a beam to biological dose requires careful benchmarking and indexing since the RBE along this path can vary as much as 2–4-fold. This is more complex than proton RBE calculations because an arbitrary value of 1.1 works fairly well for most portions of the Bragg curve besides the very distal portion. However, with CIRT the RBE varies considerably across a long segment of the beam path and cannot be arbitrarily assigned a uniform value. To account for this, Japanese investigators performed CIRT irradiation experiments with human salivary gland cells, as representative of early responding tissues, placed along different points along an SOBP and scaled each voxel of an SOBP using relative cellular cytotoxicity of treatment at that depth. This allowed a downward slanting physical dose profile of CIRT SOBP to result in a flat RBE profile across a tumor. To then generate absolute RBE values, the classical mixed-effects (or Kanai) model used a scaling factor that assigned a value of 3 for a LET of 80 keV/ μ m. This assumption was predicted on an appreciation of biological equivalence of this LET to that of 16 fast neutron treatments of 0.9 Gy. This served the clinical practice well for many years until the advent of intensity modulated CIRT both in Japan and Europe. Here, the models diverged and were refined using slightly different assumptions and mathematical formalisms, although both recognize that ionization density at a microscopic scale defines spatial dose deposition. The Japanese developed the microdosimetric kinetic model (MKM) where RBE was defined within each microscopic spatial “domain” as a function of α and β parameters of the linear quadratic model, with α being proportional to LET and β being independent of LET.¹⁵ The α and β parameters were derived from human salivary gland cell line irradiation experiments to generate relative RBE values. Absolute RBE values were generated by cross-referencing prior RBEs within the middle of a 6 cm SOBP from a 350 MeV/nucleon carbon ion beam. The German local effects model (LEM) indexed RBE to in vitro survival data from neuronal cells (late responding normal tissue with an α/β ratio of 2) in an effort to account for normal tissue complications more so than tumor control. The LEM model has been refined and modified (LEM I–IV) over the years and are increasingly complex, often resulting in simple versus complex breaks in both DNA strands with euchromatin versus heterochromatin, etc. Naturally, the biological or

RBE-weighted dose (denoted as Gy(RBE)), used for prescribing CIRT treatment in Japan and Europe, are slightly different; yet, the mathematical formulas have been relatively robust at modeling a complex problem of variable LET along a carbon beam path.^{26,27}

Advantages of CIRT in the Management of HCC

Hypofractionation and Dose Escalation in HCC

There have been limited studies regarding the use of CIRT in HCC. Below, a comprehensive review of available studies reporting the use of CIRT in this disease cohort is provided.

The National Institute of Radiological Sciences (NIRS) has carried out several clinical studies since the 1990s using five different fractionation schedules in order to establish the optimal dose of CIRT in a series of dose escalation studies. The first study, Phase I/II trial, used a 15-fraction regimen with doses ranging from 49.5 to 79.5 Gy (RBE), delivered over 5 weeks in 24 patients (10 stage II, 6 stage III, and 8 stage IVA). After a median follow-up of 71 months, the study showed nearly no adverse effects and demonstrated a complete response in 41.7% of patients, a partial response in 29.2%, stable disease in 12.5%, and progression in 16.7% of patients.²⁸ The subsequent Phase I/II study used a 2-fraction regimen with doses ranging from 32–37 Gy(RBE). The preliminary findings of this study indicated an overall tumor response rate of 96% at 6 months after CIRT with no adverse effects observed at 1 year.²⁹

These preliminary NIRS studies established that hypofractionated CIRT was safe and effective in the treatment of HCC. Nonetheless, many patients experienced both in-field and out-of-field disease recurrence on long-term follow-up, though treatment was well tolerated. Further dose escalation was evaluated by Yasuda et al²⁶ in 57 patients with localized HCC (72% newly diagnosed, 28% persistent after prior TACE or RFA treatment or recurrent) receiving 45 Gy(RBE) delivered in 2 days. One-, 3-, and 5-year local control (LC) rates were 98%, 91%, and 91%, respectively, even after failure of prior TACE or RFA treatment. Consistent with these results but with a slightly more fractionated course of radiation, Shibuya et al³⁰ analyzed outcomes of 21 patients (11 with tumors measuring >5 cm and 10 measuring <5 cm, Child-Pugh A or B, without major vascular invasion or extrahepatic metastases) treated between 2012 and 2016 to a dose of 60 Gy(RBE) in four

fractions. Progression-free survival rates were 100% and 92.3% at 1- and 2-years, respectively. No patient experienced acute grade 3/4 toxicities, but three experienced late grade 3 toxicities; Child–Pugh score worsened in two patients at 3months. Similarly, Kasuya et al³¹ performed two trials, a phase I/II trial (protocol 9603) and a Phase II trial (protocol 0004). The initial trial used doses of 69.6 Gy(RBE), 58.0 Gy(RBE), and 52.8 Gy(RBE) delivered in progressive hypofractionation schedules from 12 to four fractions. The recommended phase II dose was four fractions of 13.2 Gy(RBE) each and was utilized for an expansion cohort of 124 patients. In-field and out-of-field tumor recurrence rates were 2.2%, 4.5%, and 8.4% at 1, 3, and 5 years, respectively.

In a multicentric retrospective study of 174 previously treated patients who received <5 fractions of CIRT between 2005 and 2014, LC rates were 94.6%, 87.7%, and 81.0% at 1, 2, and 3 years, respectively. Only 10 patients experienced grade 3/4 toxicities and a mere 1.7% of patients developed RILD.³² The results of the PROMETHEUS clinical trial are awaited as they investigated the feasibility of escalating the dose of CIRT from 40 to 56 Gy(RBE) in four fractions using active raster scanning.³³

In a retrospective comparison of PBT and CIRT done by Komatsu et al,³⁴ 343 patients who had 386 tumors were studied and they concluded that the rate of LC was 90.8% and the average OS rate was 38.2% at 5 years for both groups, with those numbers being 90% and 38%, respectively, for those receiving PBT and 93% and 36.3% for those undergoing CIRT.

Selected clinical studies regarding the use of CIRT in HCC are documented in Table 2.

Treatment Planning Considerations for CIRT in HCC

CIRT affords excellent dose conformality, sharp penumbra, and steep dose gradients around the target volume to allow (i) the delivery of ablative doses to the tumor, ie, a higher tumor control probability and (ii) lower dose to surrounding liver tissue (mean liver dose and V5–V20) and organs at risk, ie, lower probability of RILD. Another advantage of CIRT that adds to the better conformality of CIRT is the usage of the least number of fields and low exit dosage in comparison to the multiple fixed beams or arcs used in IMRT or SBRT. CIRT and SBRT plans were compared in 10 respiratory gated HCC patients, the ability

Table 2 Literature Review of Studies Reporting Outcomes After CIRT for Hepatocellular Carcinoma

Author, Year, Center	No. of Pts	Total Dose and/or Range, Gy(RBE)	Total Fractions	Median Follow-Up, Mos (Range)	Local Control			PFS			Overall Survival			Grade 3+ Acute or Late Toxicities or Other Endpoint
					1 Yr	3 Yr	5 Yr	1 Yr	3 Yr	5 Yr	1 Yr	3 Yr	5 Yr	
Prospective Phase I/2 Trials														
Shibuya et al 2019 ³⁰ Gunma	21	60 (RBE)	4	24.2 (6.3–43.7)	100%	92.3% (2yr)	NIR	81.0%	50.0% (2 yr)	NIR	90.5%	80.0% (2 yr)	NIR	Acute: None Late: gr 3 cholecystitis and encephalopathy, 2 pts; gr 3 other toxicity (not specified), 1 pt
Kasuya et al 2017 ³¹ NIRS	127	69.6, 58.0, and 52.8 (RBE)	4, 8, or 12	27.1 (0.9–154.8)	94.7%	91.4%	90.0%	NIR			90.3%	50.0%	25.0%	Acute: gr 3 skin toxicity, 3 pts Late: gr 3 skin, 3 pts; gr 3 pleural effusion, 1 pt
Kato et al 2004 ²⁸ NIRS	24	49.5–79.5 (RBE)	15	71 (63–83)	92%	81%	81%	NIR	NIR	NIR	92%	50%	25%	Acute: gr 3 skin toxicity, 1 pt; gr 3 leucopenia and thrombocytopenia, 5 pts Late: gr 3 thrombocytopenia, 3 pts (one died of variceal bleed and hepatic failure)
Retrospective Studies														
Shibuya et al 2018 Japan Carbon Ion Radiation Oncology Study Group ³²	174	48, 52.8, or 60 (RBE)	2, 4 or 4	20.3 (2.9–103.5)	95.4%	82.5%	73.3%	NIR	NIR	NIR	94.6%	81.0%	NIR	Acute: gr 3 dermatitis, 2 pts; gr 3 elevation of AST (alanine aminotransferase), 1 pt Late: gr 3 dermatitis, 4 pts; gr 3 myopathy, 1 pt; gr 3 rib fracture, 1 pt; gr 4 dermatitis, 1 pt

Komatsu et al 2011 HIBM ³⁴	101	52.8, 52.8, 66, or 76 (RBE)	4, 8, 10, 20	31	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	36.3%	Acute: None Late: gr 3 Elevation of transaminase level, 3 pts; gr 3 subcutaneous panniculitis, 1 pt
Shiba et al 2018 Gunma ⁵¹	68	52.8 or 60.0 (RBE)	4	33.5 (3.9–83.1)	NR	81%	NR	NR	46%	NR	NR	NR	66%	NR	NR	NR	NR	NR	Acute: None Late: gr 3 encephalopathy, 2 pts
Yasuda et al 2019 NIRS ²⁶	57	45 (RBE)	2	54 (7–103)	98%	91%	91%	NR	NR	NR	97%	67%	45%	NR	NR	NR	NR	45%	Acute: gr 3 skin toxicity, 2 pts Late: None
Shiba et al 2020 Gunma ⁵²	11	52.8 or 60.0 (RBE)	4 or 12	36.4 (4.3–86.2)	NR	78%	NR	NR	18%	NR	NR	64%	NR	NR	NR	NR	NR	NR	Acute: None Late: Grade 3 bone fracture, 1
Shiba et al 2017 ⁴⁹ and 2019 ⁵³ Gunma	31	52.8 or 60.0 (RBE)	4 or 12	43 (4–84)	89.2% (2 yrs)	80%	NR	51.3% (2 yrs)	51%	NR	82.3% (2 yrs)	88%	NR	NR	NR	NR	NR	NR	Acute: None Late: Encephalopathy, 3 pts CIRT demonstrated better clinical outcomes when compared to TACE for monofocal HCC.
Imada et al 2010 NIRS ⁵⁴	43	48.0–79.5 (RBE)	4–15	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	48.9% (≥50 cm ³) 29.4% (< 50cm ³)	Patients who showed compensatory enlargement of the liver within 1 year of treatment had higher reserve of liver function.
Habermehl et al 2013 HIT ⁵⁵	6	40 (RBE)	4	11 (3.4–12.7)	11.3 (2.7–11.9) mo	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	NR	Acute: None Late: None

Abbreviations: gr, grade; mos, months; Gunma, Gunma University Heavy Ion Medical Center (Japan); HIBM, Hyogo Ion Beam Medical Center (Japan); NIRS, National Institute of Radiological Sciences (Japan); NR, not reported; pts, patients; yrs, years.

to cover the PTV with 90% of the prescribed dose was found to be higher in CIRT [59.6 ± 0.2 Gy(RBE)] versus SBRT groups [56.6 Gy] ($p < 0.05$).³⁵ The CIRT group also showed a better homogeneity index and a better conformity index, and the maximal dose to the gastrointestinal tract was lower for CIRT than SBRT (8.4 ± 4.3 Gy(RBE) versus 17.4 ± 7.1 Gy).³⁵ A multitude of photon and radio-embolization trials demonstrated that LC was enhanced with the escalation of dose delivered to tumor and a similar correlation between RILD and mean radiation dose to “normal” liver.^{17–19,26,36–38}

Design and delivery of treatment fields for HCC CIRT require careful consideration of some practical issues. The exquisite sensitivity of the range of carbon beams to changes in Hounsfield units along their path mandates that planning be performed on non-contrast scans that mimic the tissue configurations at the time of treatment. Similarly, it is customary to minimize beams traversing through the lungs or bowel and terminating in critical normal organs like the bowel, spinal cord, and central biliary structures, since slight changes in air content of these structures may significantly change penetrance of the beam. Likewise, metal fiducials have the potential to shield dose downstream of them and create unwanted cold spots in the dose distributions; carbon and polymer fiducials are preferable and create fewer artifacts. The sharp penumbra of carbon ion beams may under-treat tumors with ill-defined infiltrative margins. Lastly, respiratory motion management is critical since the range of uncertainty of carbon ions is exacerbated when tissue planes and densities vary over the time frame that the beam is on.³⁹

HCC CIRT in Special Scenarios

As a consequence of better dose conformity and maximal sparing of normal liver tissue, CIRT may be especially well suited for salvaging patients who recur locally following prior high-dose radiotherapy; the higher RBE within the tumor and the high dose-conformality sparing “normal” liver may both be advantageous. Reirradiation using CIRT has been reported in recurrent head and neck cancers, base of skull chordomas, pancreatic cancers, and rectal cancers.^{40–43} Although no such HCC reirradiation series has been reported, in a report of 57 patients who received CIRT, four developed local failure and one was salvaged with another four fractions of 13.2 Gy(RBE) of CIRT and no treatment-related adverse events reported at 5 years.²⁶

Tumor size is an independent predictor of objective response rates, LC rates, in-field recurrence-free rates, and OS rates in photon radiotherapy of HCC.^{44–46} In a representative retrospective study, 141 patients underwent SBRT and they were grouped in accordance with the longest diameter of the lesion into small (<4 cm), intermediate (4–10 cm), and large (>10 cm) and had objective response rates of 96.15%, 90.90%, and 76.47%, respectively ($p \leq 0.0001$). The 3 year LC rates of 97%, 72%, and 82%, respectively, were significantly different ($p = 0.0035$), but the 3 year OS difference was not significant.⁴⁴ In dosimetric comparisons of protons versus IMRT, proton treatments achieve better sparing of the liver and gastrointestinal tract than photons. This benefit was more evident for larger tumors, with tumors larger than 6.3 cm having an estimated risk of RILD of 94.5% with photons compared to 6.2% with PBT.⁴⁷ PBT was also effective in controlling larger (>5 cm) HCCs with PVTT, achieving 66% OS at 2 years.⁴⁸ By extrapolation, it seems reasonable to assume that CIRT would be beneficial for patients with larger tumors since the volume of “normal” liver to spare is smaller and the lack of a low dose radiation bath could minimize the risk of RILD and permit greater dose escalation to the tumor itself. There are, however, no published reports with objective data confirming this assumption.

Even among elderly patients with limited capacity of liver function recovery, the use of short course CIRT has been shown to be safe. For instance, in an analysis of 31 patients over the age of 80 treated with CIRT, only one patient progressed from Child-Pugh A to Child-Pugh B within the first 3 months of CIRT.⁴⁹

Radiation Induced Liver Disease

As a major adverse effect of liver irradiation is the development of RILD, most CIRT studies have quantified and reported results that include this information. Yet, the majority of these studies were retrospective, and they reported hepatotoxicity in different ways with no unified criteria for the severity of the hepatotoxicity. This makes the comparison between studies highly challenging. Nonetheless, there are some unmistakable trends that are seen. For instance, despite 45 Gy(RBE) being delivered in 2 consecutive days, one CIRT study noted no acute or late RILD (considered when the Child-Pugh score increases by ≥ 2 after a median follow-up of 51 months).²⁶ In a combined analysis of two prospective trials involving hypofractionated CIRT, 29% of patients

experienced an increase in Child-Pugh score ≥ 1 at 3 months, but this declined to 22% at 6 months, indicating that acute liver injury from CIRT may be transient and can recover over time. An increase by ≥ 2 in Child-Pugh was only reported in 3% at 3 months and 5% at 6 months.³¹

Limitations of CIRT in HCC

The greatest impediment to widespread adoption of CIRT for HCC is the high cost of construction and operation of treatment facilities; this is compounded by the lack of FDA approval, approved billing codes, and insurance coverage in the US. Another limitation is the lack of consensus in RBE modeling or objective liver or gastrointestinal tract specific preclinical data to build these models on. As noted previously, the lack of a low dose bath is especially useful for tumors where the remaining liver tissue represents the dose limiting structure. However, when the dose-limiting normal structure is the gastrointestinal tract, the benefit of CIRT may be less evident since point dose or focal high dose (especially distal to the Bragg peak if the beam exits into this mucosa) dictates toxicity.⁵⁰

Conclusions

The incidence of HCC is growing globally, with the majority of patients in populations without active screening protocols presenting with advanced tumors, oftentimes with associated portal vein thrombosis within a background of considerable liver dysfunction. Given the complexity of HCC treatments and the need to achieve a delicate balance between disease control and limiting toxicity, there is a critical need for therapies which achieve adequate LC with minimal impact on the surrounding liver. Due to the associated low dose radiation bath, traditional photon radiotherapy may not adequately spare non-tumor-bearing liver; CIRT offers an alternative form of radiotherapy that delivers highly conformal high-LET radiation to tumors. Through our comprehensive review of physical and biological properties of CIRT, associated dosimetric and treatment planning concerns, and available clinical data to date, we posit that CIRT is well tolerated and leads to excellent disease control in HCC with minimal impact on normal liver function. CIRT might have a unique and distinct niche in the treatment of HCC with liver-directed therapies that will need to be defined in the coming years.

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