

# Analysis of the Sagittal Motion Posture of the Acromioclavicular Joint Using Image Registration and Axial Angle Representation

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**Objective:** This study aimed to directly and accurately measure the range of motion of the acromioclavicular joint through 3D reconstruction and image registration.

**Methods:** Thirteen healthy volunteers participated in the study. Computerized tomography (CT) was used to measure the acromioclavicular joint in four different motion poses. The images were integrated using reconstruction and registration technology, and the rotation angle range of the acromioclavicular joint was measured using 3D reconstruction. The measurements were expressed by axial angle representation. The dominant and the non-dominant sides were compared, and the difference in the axial angle of the acromioclavicular joint was compared in different postures.

**Results:** The difference between the dominant and non-dominant sides in acromioclavicular motion was not significant. In the sagittal motion of the upper limb, the rotation angle of the acromioclavicular joint was greatest in a resting horizontal position, with an average of 26.1°. In this position, 34.6% of flexion and extension movements of the upper limb were completed by the acromioclavicular joint, which was the highest level of engagement. The rotation angle was lowest in the resting posteroinferior position, with an average of 8.2°. In this position, 24.9% of the flexion and extension movements of the upper limb were completed by the acromioclavicular joint.

**Conclusion:** Combining 3D reconstruction and image registration is a direct and accurate method of measuring the motion of the acromioclavicular joint. The rotational motions of the acromioclavicular joint are bilaterally symmetrical and can be used as a reference for comparative study. The maximum range of motion of the acromioclavicular joint during rotation was found in the resting horizontal position. The clinical examination and post-treatment evaluation of the acromioclavicular joint's rotation function can therefore be targeted in this range.

**Keywords:** image registration, axial angle representation, acromioclavicular joints

## Introduction

The acromioclavicular joint connects the clavicle with the scapula and forms a combined motion with the sternoclavicular joint and glenohumeral joint to complete the function of the shoulder girdle.<sup>1</sup> It allows the scapula additional range of rotation on the thorax. The acromioclavicular joint is therefore an important part of synchronous combined motions. However, it is difficult to measure the joint's range of motion because it is affected by both clavicle and glenohumeral joint movements.

For anatomical reasons, the acromioclavicular joint has two forms of rotation and displacement. Codman and Rockwood<sup>1,2</sup> both identified synchronous

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movements of the clavicle and scapula and found that the motion of the acromioclavicular joint is only 5–8° when the shoulder is raised. A study by Inman<sup>3</sup> revealed that full shoulder elevation includes clavicle axial rotation of 40–50°, elevation of 11–15°, and rear extension of 15–30°. Sahara<sup>4</sup> found that, during the coracoid, the scapula usually rotates around a specific screw axis via the acromioclavicular ligament and the coracoclavicular ligament, with an average rotation of 34.9°.

In 2015, the International Society of Biomechanics (ISB)<sup>5</sup> recommended using a joint coordinate system, bone marker points, and Euler angles to represent joint rotation. However, the clinical definition of Euler angles is not consistent in 3D. Lawrence<sup>6</sup> found that the rotation of the scapula is defined by three rotations of Euler angles. Her results showed that the motions of the acromioclavicular joint include an internal rotation of 60.0–62.3°, an upper rotation of 2.5–2.9°, and a forward inclination of 8.2–8.4°. The joint motion described by the ISB defines a rotation sequence (such as the Y-Z-Y of the Euler angle) so that the angle is as close to the clinical definition of joints and segmental motions as possible. However, the Euler angle cannot easily be used to describe the motion of the acromioclavicular joint, especially when the description of the joint's rotation does not follow clinical terminology.<sup>7</sup>

Following the standardized protocol for the recording of shoulder movement proposed by van der Helm,<sup>13</sup> a 3D video (VICON and Optotrack, etc.) of the chest and humerus is usually recorded. However, clavicle and scapular movements cannot be recorded using external markers due to significant bone and skin displacements. Anglin<sup>7</sup> stated that the rotations of the scapula and clavicle are difficult to track with external markers because of the large amount of movement under the skin. It is the most authentic and accurate way of measuring the angle between bones directly *in vivo*.

Axial angle representation is a method of describing joint rotation in 3D space. It defines the rotation of an object in 3D space with an axis or a straight line, describing the amount of rotation around the axis using an angle, thereby achieving a definition of the action that corresponds to a rotation axis and a rotation motion. This avoids the three rotation order problems of Euler angles. Because there is only one rotation, the interaction problem of subsequent rotation is also effectively avoided. In 1989, Sangeorzan<sup>8</sup> stated that axial angle representation (rotation vector) was an intuitive way of describing rotation in 3D space and that it was suitable for clinical operation in the design of orthopedic surgery. Wu<sup>9</sup> also used axial angle

representation when studying the computer-aided design of orthopedic devices in 2014.

There are many ways to detect the movements between the 4 different positions and postures of the boom sections,<sup>7</sup> including electromagnetic and sonic sensors, passive and active optical markers, an electric goniometer, a potentiometer-based beat-frequency detector, X-ray stereogrammetry, and magnetic resonance imaging (MRI). A significant problem with these methods, however, is the interference of respiratory movement and sternal position changes on measurements. Image registration solves this problem. The main principle of image registration is the correlation of spatial transformation between images, transforming the problem from a registration problem into a mathematical parameter optimization problem.

It is often necessary to convert images registered in different modes into images<sup>10</sup> with the same mode. Lawrence's contrastive study<sup>11</sup> revealed that a single-plane perspective and 2D/3D shape matching can accurately quantify the complex kinematics of a shoulder in a resting position, thereby proving that image registration technology can achieve the accuracy of a single-plane perspective. Seo<sup>12</sup> studied the motion of the acromioclavicular joint in different movements between the 4 different positions and the changes in ligament length and tension using a 3D registration technique based on computerized tomography (CT) images.

In the present study, in order to find a way to directly and accurately measure the range of motion of the acromioclavicular joint through 3D reconstruction and image registration, a 3D rotation of the scapula relative to the clavicle was used as a study object.

## Methods

### Study Subjects

A total of 13 healthy adults with no history of shoulder trauma or chronic pain were enrolled in this study. The sample was made up of 7 men and 6 women, with ages ranging from 22 to 42 and a mean age of 26.5 years. Their BMI scores were between 18.9 and 39.2, with a mean of 24.2. The dominant shoulder of 2 of the participants was their left, while for the other 11 it was their right.

This study was conducted with approval from the Ethics Committee of Beijing Shijingshan Hospital (2019–13). This study was conducted in accordance with the declaration of Helsinki. Written informed consent was obtained from all participants.

## Image Acquisition

CT scan (Discovery CT750HD, GE). Parameter settings—Slice thickness: 0.625 mm; layer distance: 0.625 mm. Shooting position—(a) Supine and resting position (the baseline position which the three other movements were compared to); (b) supine position with forward extension of the elbow joint, horizontal position of upper limb; (c) prone position with excessive posterosuperior extension of the elbow joint, posterosuperior position of upper limb; (d) prone position with back extension of the elbow joint, posteroinferior position of upper limb. Shooting range—From 2 cm below the sternal angle plane to the extremitas acromialis clavicularae, including the proximal humerus above the deltoid tuberosity. See [Figure 1](#). In this experiment, healthy volunteers were examined by CT for four times, and the cumulative radiation dose was as follows: Minimum value: 570.15 Maximum value: 1950.84 Mean  $1231.5777 \pm 449.96090$  DLP(MGY-CM).

## Image Registration

Raw image data were imported into MIMICS 21 software to form a 3D image complex with four postures containing the sternum, clavicle, and humerus. In accordance with ISB recommendations, a thoracic reference coordinate system

and bone reference points were adopted. The motion of the acromioclavicular joint was considered the rotation of the scapula relative to the clavicle represented by axial angle. The 3D images of the sternum in a supine and resting position were used as registration objects to register the 3D image complex in other poses. Finally, the images of the clavicle in four different postures were overlapped, and the 3D images of the scapula and humerus were registered in different poses. See [Figure 2](#) and [Supplemental Figure 1](#).

## Data Acquisition and Processing

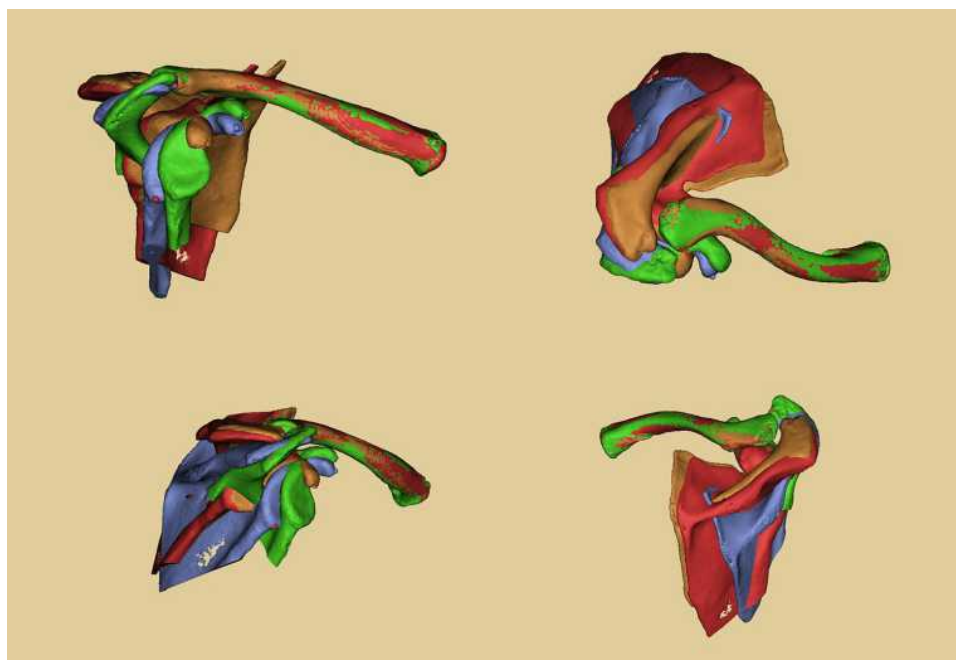
The participants were divided into two groups according to their dominant shoulders, then into three groups according to posture changes (resting horizontal, horizontal posterosuperior, and resting posteroinferior). Using the baseline 3D image complex of the clavicle, scapula, and humerus in a supine and resting position, the rotation angle of the acromioclavicular joint in different postures was measured and expressed as an axial angle. The corresponding flexion and extension angle of the humerus was measured.

## Statistical Methods

An independent sample *t*-test was used to compare the data of the two groups (left-side dominant and right-side



**Figure 1** Image shooting movements between the 4 different positions: 1) resting position, 2) 90° of anterior flexion, 3) complete anterior flexion, and 4) complete posterior extension of the shoulder.



**Figure 2** 3D images after registration: front view, vertical view, side view, and rear view.

dominant) in three different posture angles.  $P < 0.05$  was considered statistically significant.

The three groups of data from the humerus and acromioclavicular joint in three different postures were processed to calculate the axial angles of the acromioclavicular joint in different poses. Grouping was then carried out based on posture. Statistical analysis was conducted using analysis of variance (ANOVA).  $P < 0.05$  was considered statistically significant. The contribution of the acromioclavicular joint's angle of motion to brachial axillary joint motion range was grouped into different poses (acromioclavicular joints/thoracohumeral joints), and statistical analysis was carried out using a chi-squared test. SPSS 19 software was used for statistical analysis.

## Results

### Comparison of the Acromioclavicular Joint Angle and Humeral Angle in Different Postures Between Dominant and Non-Dominant Sides in Sagittal Motion (n=13)

The axial angle of the acromioclavicular joint, humeral flexion, and extension angle in different postures in the dominant and non-dominant sides were compared. See Table 1.

### Statistical Description of the Axial Angle of the Acromioclavicular Joint, Humeral Flexion, and Extension Angle in Different Postures in Sagittal Motion in 13 Patients (Table 2)

The results of the chi-squared test, showing the contribution of the acromioclavicular joint (axial angle of acromioclavicular angle/humeral flexion and extension angle) are shown in Table 3.

Analysis of results: In the sagittal motion of the upper limb, the rotation angle of the acromioclavicular joint is greatest in a resting horizontal position, with an average of  $26.1^\circ$ . In this position, 34.6% of the flexion and extension motions of the upper limb are completed by the acromioclavicular joint, accounting for the greatest proportion of motions. The rotation angle is smallest in a resting posteroinferior position, with an average of  $8.2^\circ$ . In this position, 24.9% of the flexion and extension motions of the upper limb are completed by the acromioclavicular joint.

## Discussion

### The Advantage of 3D Image Registration Techniques

Although Seo<sup>12</sup> conducted studies using image registration techniques, no 3D image registration techniques were

**Table 1** Comparison of Axial Angle of Acromioclavicular Joints and Humeral Flexion and Extension Angle Between the Dominant Side and Non-Dominant Side Under Different Postures

	Postures		Mean $\pm$ SD	T-value	Sig
Axial angle of acromioclavicular joints	Resting - horizontal	Non-dominant sides	25.9208 $\pm$ 7.97070	2.6	0.7
		Dominant sides	26.2008 $\pm$ 5.4603	0.06	0.8
	Horizontal-posterosuperior	Non-dominant sides	19.5392 $\pm$ 6.6448	0.5	0.5
		Dominant sides	18.8462 $\pm$ 6.7171		
	Resting- posteroinferior	Non-dominant sides	8.7331 $\pm$ 3.8766		
		Dominant sides	7.7038 $\pm$ 4.4141		
Humeral flexion and extension angle	Resting - horizontal	Non-dominant sides	83.4705 $\pm$ 13.9086	0.3	0.6
		Dominant sides	81.3761 $\pm$ 12.7083	0.2	0.7
	Horizontal-posterosuperior	Non-dominant sides	96.2585 $\pm$ 13.8511	0.2	0.7
		Dominant sides	99.2588 $\pm$ 16.4926		
	Resting- posteroinferior	Non-dominant sides	47.4823 $\pm$ 11.5488		
		Dominant sides	48.2270 $\pm$ 10.1962		

**Table 2** Statistical Description of Axial Angle of Acromioclavicular Joints/Humeral Flexion and Extension Angle Under Different Postures

Postures	Axial Angle of Acromioclavicular Joints	ANOVA		Humeral Flexion and Extension Angle	ANOVA	
	Mean $\pm$ SD	F	Sig	Mean $\pm$ SD	F	Sig
1:Resting - horizontal	26.0 $\pm$ 6.7	60.4	0.000	82.4 $\pm$ 13.1	99.8	0.000
2:Horizontal-posterosuperior	19.2 $\pm$ 6.6			97.8 $\pm$ 15.0		
3:Resting- posteroinferior	8.2 $\pm$ 4.1			47.8 $\pm$ 10.7		

**Abbreviation:** ANOVA, analysis of variance.

**Table 3** Chi-Square Test for Axial Angle of Acromioclavicular Joints/Humeral Flexion and Extension Angle Under Different Postures

Postures	Mean $\pm$ SD	$\chi^2$	Sig
1:Resting - horizontal	34.6 $\pm$ 9.0	234.7	0.000
2:Horizontal-posterosuperior	22.7 $\pm$ 7.6		
3:Resting- posteroinferior	24.9 $\pm$ 11.6		

used. In the present study, the acromioclavicular joints of a healthy person were photographed via CT, and the 3D images were reconstructed by computer. In the virtual 3D space, the acromioclavicular joints in different postures were uniformly registered to the sternum in a resting position, and the angle change of the acromioclavicular joints in different postures were measured directly in the 3D space. The advantage of this image registration technique is that it can effectively eliminate the interference of acromioclavicular motion, respiratory motion, and sternal motion, making the measurements more reliable. The changes in the angles of the acromioclavicular joints

were also measured directly in the virtual 3D space using the 3D reconstruction technology of CT, which is more accurate and objective.

## Euler Angle Representation and Axis Angle Representation

Euler angle representation and axis angle representation are effective ways of describing the rotation of objects in 3D space. However, there are two problems in the description of Euler angles:<sup>14</sup> order and interaction. The rotation order of Euler angles is defined by the individual, and each rotation order will have different angles. Hence, the ISB has suggested that the order of rotation is limited if Euler angles are used to represent rotation. Moreover, the Euler angle divides a motion into three rotating movements in different coaxial directions, which is inconsistent with the characteristics of human joint motions. Anglin<sup>7</sup> stated that there are many different terms because these rotations do not follow clinical linguistics. For example, the elevation plane may not be the plane on which the action takes place, but merely the mathematical rotation



required to define a particular resting position. Matsuki<sup>15</sup> used the Euler angle to describe the comparison between rotations in the dominant shoulder and non-dominant shoulder. The study found differences in two of the three rotations. Lawrence<sup>6</sup> stated that the clinical significance of using the Euler angle to describe the rotation of different movements of the same joint is also difficult to understand.

Axial angle representation is a way of expressing rotations in 3D space, and is more accurate than description on a 2D plane. Compared with Euler angles, axial angle representation simplifies the description of joint rotations and makes them more intuitive and easier to compare. Jehee<sup>16</sup> showed that there is no singularity in 3D space and that axis angle representation (rotation vector) can parameterize rotations. Therefore, it is suggested that rotation should be represented by rotation vector. A description of the rotation of an independent joint in a composite motion is especially suitable for the shoulders.

Axial angle representation also effectively avoids the order problem and mutual interference problem of acromioclavicular joints described by Euler angles. In human multi-joint composite motions, each joint motion tries to complete a certain action as simply as possible (with minimum energy consumption). Axis angle representation expresses the position change through one rotation, while Euler angle representation expresses the position change through three rotations. Therefore, axial angle representation is more in line with the movement characteristics of human anatomy and more closely reflects the characteristics of joint movement. As such, it is more useful as a guide for clinical practice.

## Sagittal Motion of the Upper Limb

The results of this study show that differences between dominant and non-dominant sides in the 3D rotation angles of the acromioclavicular joint in the sagittal motion of the upper limb are not significant. The rotational motions of the acromioclavicular joint could be bilaterally symmetrical and may be used as a reference for comparative study. This provides a theoretical basis for clinical examination and post-treatment evaluation.

In the sagittal motion of the upper limb, the acromioclavicular joint has the greatest rotation angle and participation in the resting horizontal position; it has the smallest rotation angle in the resting posteroinferior position. This shows that the maximum action range of the acromioclavicular joint rotation is the resting horizontal position, and the clinical examination and post-treatment evaluation of the rotation

function of the acromioclavicular joint can be targeted in this range.

## Conclusion

The combination of 3D reconstruction and image registration can effectively reduce the interference of respiratory and sternal motion on measurements. It is a direct and accurate method for the measurement of acromioclavicular joint motions. Axial angle representation also simplifies the presentation of joint rotation, which makes it more intuitive, easier to compare, and more in line with the movement characteristics of human anatomy; therefore, it more closely reflects the characteristics of joint movement and is useful for the instruction of clinical practice. The rotational motions of the acromioclavicular joint are bilaterally symmetrical and can be used as a reference for comparative study. The maximum range of rotational motion of the acromioclavicular joint is in the resting horizontal position.

The study has two limitations: firstly, the sample size was small; secondly, radiographic tests were used, although the radiation dose is not very large. Further supplementary experiments can be carried out by increasing the sample size. Also, we did not measure the “in between” instant; we measured 4 positions, not a continuum.

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## Disclosure

The authors declare that they have no competing interests.

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