Comparison of Hemodialysis Using a Medium Cutoff Dialyzer versus Hemodiafiltration: A Controlled Cross-Over Study

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Purpose: Conventional hemodialysis (HD) treatment has an acceptable removal of small uremic molecules, but so-called “middle molecules” in the range of 0.5–60 kDa are poorly cleared with HD compared to a native kidney, which may contribute to morbidity in the dialysis population. Hemodiafiltration (HDF) has a better removal of middle molecules compared to HD but is technically demanding and requires well-functioning dialysis access. The newly introduced medium cutoff (MCO) filters have been developed to enhance middle molecule clearance in HD-mode. The aim of this study was to compare reduction ratios (RRs) of molecules with different molecular weights (0.06–150 kDa) during dialysis with MCO dialyzer (used in HD-mode) compared to online-hemodiafiltration (ol-HDF) treatment with a conventional high-flux dialyzer.

Patients and Methods: This is a prospective controlled single-center cross-over study, including 16 patients in Malmö, Sweden. All patients had ongoing post-dilution ol-HDF treatment before the study. The study compared reduction ratios of small-, middle-, and large-sized molecules during a single 4h dialysis treatment with post-dilution ol-HDF (Polyflux 210H) to a 4h dialysis treatment with MCO dialyzer (Theranova 500) in HD-mode. Between treatments, the patients had a washout period of at least two weeks of their ordinary HDF treatment to reach their ordinary steady state.

Results: ol-HDF had significantly higher RR for cystatin C (13 kDa), compared to MCO (RR 68.1 vs 65.8, p<0.003), during a 4h dialysis treatment (mean convection volume of 24.5 L for HDF, and mean Qₜ of 324 mL/min for HDF and 323 mL/min for MCO). There was no significant difference in the RR for other middle molecules, or for smaller or larger molecules.

Conclusion: Overall, the RRs were comparable for ol-HDF and MCO-HD. There was a slightly higher RR of cystatin C (a small middle molecule) for HDF compared to MCO but no difference in other measured molecules.

Keywords: chronic hemodialysis, dialysis, hemodiafiltration, hemodialysis, MCO, uremic toxins

Introduction
Conventional hemodialysis (HD) treatment has an acceptable removal of small (<0.5 kDa) uremic molecules like urea, but so-called “middle molecules” in the range of 0.5–60 kDa¹ are poorly cleared with HD compared to a native kidney. It has been hypothesized that increased middle molecule clearance could lead to better survival/health. Hemodiafiltration (HDF) was invented to improve middle molecule clearance, since larger molecules have slow removal by diffusion compared to...
small molecules, and are more dependent on convective transport for removal. There is some weak evidence that HDF with high convection volumes (above 17–23 L) lowers cardiovascular mortality compared to HD. However, since middle molecule clearance is still inferior with HDF compared to a native kidney, new dialysis technology aims to further improve middle molecule removal.5

Removal of middle molecules is highly dependent on convective volume, but also on the pore size of the dialysis membrane, i.e., the sieving coefficient must be high enough for the molecule to pass through the dialysis membrane. The total convective transport is a product of convection volume times the sieving coefficient (K = Q_m x S). High cutoff (HCO) membranes with a higher pore size (high sieving coefficient) were introduced to the market, but due to unacceptably large albumin (67 kDa) losses, they are unsuitable for long-term use.7 The large albumin loss is due to a large variability in pore size; high average mean pore size gives a few pores that are too large. Recent technology has allowed production of dialyzers with more uniformly distributed pores, and the newly introduced medium cutoff (MCO) dialyzer has, despite comparable average pore size, much less albumin leak due to more uniform pores. The sieving coefficient for albumin is 0.008 for the new MCO dialyzers, to be compared with 0.2 for HCO-dialyzers, and <0.01 for high-flux membranes.7 A recent safety study did not find any significant albumin decrease during 6 months use of MCO filters.8

The MCO dialyzers, which are used in HD-mode, achieve convective transport by internal convection, by varying the pressure gradient over the dialysis membrane to create a very high amount of backfiltration (approximately 7.6 L with Q_s 300 mL/min, and 12.7 L with Q_s 400 mL/min).9 This internal convection thus gives a moderate convection volume despite no substitution fluid. Despite a lower convection volume than HDF (which often gives convection volumes >23 L), the combination of a moderately high internal convection volume with a higher sieving coefficient gives better performance on clearing middle molecules, compared to standard HD, and under some circumstances also better clearance than HDF.

Clinical studies have confirmed better reduction rate (RR) and clearance for middle molecules with MCO compared to high-flux HD.10-12 Comparisons between MCO and HDF have shown more mixed results. MCO has been superior to HDF in two studies, Kirsch et al10,11 (HDF convection volume 24 L), and Reque et al13 (HDF convection volume 23.5 L), but in two studies not, Maduell et al14 (convection volumes ~ 33–35 L), and Garcia Prieto et al12 (convection volume 28 L), and in vitro study by Voigt et al15 (convection volume 24 L), showed no difference in loss of coagulation factors. The conflicting results on middle molecule removal by MCO compared to HDF may at least partly be explained by different convection volumes used for the HDF, where MCO has not been superior to HDF with very high convection volumes. An observational long-term study comparing MCO and HDF (24.4 L mean convection volume) showed no difference between treatments.16 Some authors also make a distinction between smaller middle molecules (0.5–15 kDa) and larger middle molecules (15–60 kDa), where theoretically, MCO dialyzers should be superior especially for the larger middle molecules.17

Large molecules >60 kDa should be minimally filtered through dialysis filters (since they are designed to avoid albumin (67 kDa) leakage). However, large molecules can also be removed in dialysis by adsorption onto the dialyzer membrane.18 Albumin, transferrin and IgG have been shown to be major components of the protein coating on dialyzer membranes.19

We wanted to compare the RR for small (<500 Da), middle (500–60,000 Da) and large molecules (>60,000 Da), during a single dialysis of MCO vs standard HDF treatments.

Patients and Methods
Study Design
This is a prospective controlled, non-randomized, single-center cross-over study, including 16 patients at the Department of Nephrology, Skåne University Hospital, Malmö, Sweden. Eighteen patients were originally enrolled, but one was lost to follow-up due to transfer to another dialysis center and one died of causes unrelated to the dialysis. The study was designed to compare Reduction Ratios (RRs) during a single 4h-dialysis treatment with post-dilution ol-HDF (conventional high-flux filter) compared to MCO dialyzer in HD-mode. All included patients had ongoing maintenance with post-dilution hemodiafiltration (HDF) as standard treatment. We aimed for a washout period of at least two weeks between treatments. The study was initially randomized, but due to practical considerations of the dialysis nurses, the order of the measurements (MCO first or HDF first) was finally non-randomly assigned to provide equal
number in both cross-over groups. We compared TheraNova 500 (MCO) dialyzer (Baxter Inc, Lund, Sweden), in HD-mode, vs Polyflux 210H (Baxter Inc, Lund, Sweden), using online HDF (ol-HDF). Dialysis monitors were Baxter, Artis Physio (Baxter Inc, Lund, Sweden).

The study was not blinded, neither to the patient, physicians, nurse or data analyst.

**Inclusion Criteria and Ethical Permission**

The patients included were stable dialysis patients at Skåne University Hospital, Malmö, Sweden, with ongoing treatment with ol-HDF (post-dilution). The patients had (at study inclusion) CRP ≤30 mg/L, and no myocardial infarction within 3 months. This study was approved by the Lund University Ethical Committee (registration no. 2017/830) and followed the Helsinki declaration. Written informed consent was obtained from all patients in the study.

The study has been registered in Clinicaltrials.gov, NCT03437538.

**Dialysis Session**

Blood samples were taken during a 4h dialysis session, at time point 0, 30, 60, 120, 240, and 243 minutes after treatment start, at blood inlet (arterial port, A), and at 30, 60, 120, and 240 min at blood outlet (venous port, V). The last sample in the blood inlet (arterial port) at time 243 was performed using the low-flow method to avoid the impact of potential access recirculation (waiting 30 seconds after reducing the blood flow to 75 mL/min and stopping the infusion pump). Dialysis flow was set to 550 mL/min and blood flow was set to 325 mL/min. Convection volume goal was >23 L. Ultrafiltration was performed according to the need of the patient. Low molecular weight heparin (LMWH) was used according to individual usual prescription. All dialysis patients had a dialysis regimen between 3–5 times a week.

**Laboratory Measures**

We measured the following molecules at each time point: Small molecules: urea (0.06 kDa), creatinine (0.113 kDa), phosphate (0.095 kDa).

Middle molecules: β2-microglobulin (11 kDa), cystatin C (13 kDa), myoglobin (18 kDa), beta-trace-protein (25 kDa), troponin T (35 kDa).

Large/mixed molecules: albumin (67 kDa), transferrin (80 kDa), IgG (150 kDa). Additionally, we measured hematocrit (EVF), plasma-protein (total), and transthyretin (prealbumin).

All blood samples were immediately sent to the chemical laboratory at Skane University Hospital, Malmö, Sweden, and analyzed according to routine methodology. β2-microglobulin, beta-trace-protein and transthyretin were analyzed on a BNII ProSpec-system (Siemens) according to the manufacturer’s instructions. Cystatin C, myoglobin, troponin T, albumin (immunochemical), transferrin and IgG were analysed on a Cobas system (ROCHE) according to the manufacturer’s instructions.

**Statistical Analysis**

All statistical analyses were done using R, version 3.5.1. An unpaired t-test was used for comparison of intraindividual differences in RR, since a paired t-test is unsuitable in absence of carry-over effects. Testing for carry-over effects was performed as recommended by Welke and Blettner. An overall significance level of α=0.05 was used. A Bonferroni-corrected threshold for multiple outcomes, based on 14 outcomes: p=(α/14)=0.0036, was used as significance threshold for the individual outcomes.

**Calculations**

Reduction ratio (RR) = ((pre-dialysis-concentration[A0]–post-dialysis-concentration[A240])/ pre-dialysis-concentration[A0]) X 100%.

The RRs are based on concentrations in the arterial port (blood inlet) blood samples. One patient received a shorter dialysis and RRs for this patient is calculated based on the observations at 2 hours (which were available for both HDF and MCO treatment for the patient). This patient was excluded from the descriptive plots of convection volume in relation to RR (since the dialysis time affects not only convection volume but also diffusion).

The post-dialysis concentrations of middle molecules and large molecules were adjusted for hematocrit according to Schneditz et al.

\[
P_{\text{corrected}} = P/h_p \\
h_p = H1(100-H_0)/H_0(100-H_1)
\]

where P is the measured plasma concentration, H is hematocrit, and indices 0 and 1 are before and after dialysis (A0 and A240, respectively).

The study originally intended to calculate clearance based on arteriovenous difference at time points 30, 60, 120 and 240 min. However, the blood samples taken in the
venous port had a high variability (indicating non-reliability) and had to be discarded.

Missing data: albumin was missing at A240 for 1 patient, IgG at A0 for 1 patient, and total protein at A240 for 2 patients. RRs and mean values pre- and post-dialysis are calculated based on patients with no missing measurements for the analyzed molecule (n=15 for albumin and IgG, n=14 for total protein, n=16 for all other molecules).

Dialysis vintage time was only approximately calculated. Year of dialysis start was known for all patients, but month of dialysis start (or month of dialysis restart after transplantation) was missing for 5 patients. For these, the start date was approximated to be in the middle of the year of dialysis start (1st of July).

Results
Descriptive results can be seen in Tables 1 and 2. The treatments had a mean convection volume of 24.5 L (for HDF), mean blood flow of 324 mL/min for HDF and 323 mL/min for MCO, and a dialysis flow of 550 mL/min for all patients except one patient which had a dialysis flow of 500 mL/min during the MCO-treatment. No carry-over effects were seen between treatments.

Small Molecules
No difference was seen between the reduction ratios for MCO and HDF for small molecules (Table 3).

Table 1 Description of the Patients (n=16)

<table>
<thead>
<tr>
<th>Cause of CKD (Chronic Kidney Disease)</th>
<th>N (%)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Diabetes Polycystic kidney disease</td>
<td>7 (44%)</td>
</tr>
<tr>
<td>Other</td>
<td>2 (12.5%)</td>
</tr>
<tr>
<td></td>
<td>7 (44%)</td>
</tr>
<tr>
<td>Vascular access</td>
<td></td>
</tr>
<tr>
<td>AV-fistula Central venous dialysis catheter</td>
<td>15 (94%)</td>
</tr>
<tr>
<td></td>
<td>1 (6%)</td>
</tr>
<tr>
<td>Urine production</td>
<td></td>
</tr>
<tr>
<td>Anuric 700–3000 mL</td>
<td>11 (69%)</td>
</tr>
<tr>
<td></td>
<td>5 (31%)</td>
</tr>
<tr>
<td></td>
<td>Mean ± SD (range)</td>
</tr>
<tr>
<td></td>
<td>59.6±12.9 (34–81)</td>
</tr>
<tr>
<td></td>
<td></td>
</tr>
<tr>
<td>Dialysis vintage (years)*</td>
<td>4.9±4 (1–13)</td>
</tr>
</tbody>
</table>

Note: *Dialysis vintage is only approximate.

Table 2 Description of the Renal Replacement Therapy (n=16)

<table>
<thead>
<tr>
<th></th>
<th>ol-HDF</th>
<th>MCO-HD</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood flow mL/min (at 30 min)</td>
<td>324±9.6</td>
<td>323±10.8</td>
</tr>
<tr>
<td>Dialysate flow mL/min</td>
<td>550±0</td>
<td>547±12.5</td>
</tr>
<tr>
<td>UF rate (L/h)</td>
<td>0.62±0.29</td>
<td>0.64±0.34</td>
</tr>
<tr>
<td>Convection volume</td>
<td>24.5±3.5 range: (16.9–30.6)</td>
<td>-</td>
</tr>
<tr>
<td>Hematocrit initial, A0</td>
<td>0.333±0.046</td>
<td>0.329±0.046</td>
</tr>
<tr>
<td>Dialyzer</td>
<td>Polyflux 210H</td>
<td>Theranova 500</td>
</tr>
</tbody>
</table>

Middle Molecules
HDF treatment gave a significantly higher RR for cystatin C (Table 3). The reduction ratio was also higher with HDF for β2-microglobulin, myoglobin, and beta-trace-protein, but this did not reach statistical significance.

Large/Mixed Molecules
No significant difference was seen between treatments for any of the large molecules (Table 3). All large molecules generally showed negative RRs (ie, the concentrations increased during dialysis).

Adverse Effects
Adverse effects were only recorded during the dialysis sessions. No adverse effects were seen during these treatments.

Descriptive Analysis of RR in Relation to Convection Volume
A plot of the relation between convection volume and RR for the HDF treatment is displayed in Figure 1. A plot of convection volume during HDF against the difference in RR (ΔRR) is displayed in Figure 2.

Discussion
ol-HDF treatment with Polyflux 210H had significantly higher RR for cystatin C compared to MCO treatment with a Theranova 500-dialyzer, during a 4h dialysis treatment, with a mean convection volume of 24.5 L for the HDF, and a mean Q_b of 324 mL/min. There was no difference in the RR for smaller or larger molecules.

Our results were in line with some previous studies reporting superior RR for HDF compared to MCO for
**Table 3** Description of Pre- and Post-Dialysis Concentrations, and Reduction Ratios During Dialysis with MCO-HD (Theranova) vs HDF (Polyflux 210H)

<table>
<thead>
<tr>
<th></th>
<th>Pre-Dialysis Concentration</th>
<th>Post-Dialysis Concentration</th>
<th>Reduction Ratio</th>
</tr>
</thead>
<tbody>
<tr>
<td></td>
<td>Mean [A0]</td>
<td>Mean [A240]</td>
<td>RR, Mean ± SD</td>
</tr>
<tr>
<td>Small</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Urea (mmol/L)</td>
<td>18.9</td>
<td>18.6</td>
<td>HDF</td>
</tr>
<tr>
<td>Creatinine (µmol/L)</td>
<td>791</td>
<td>794</td>
<td>5.51</td>
</tr>
<tr>
<td>Phosphate (mmol/L)</td>
<td>1.57</td>
<td>1.49</td>
<td>0.667</td>
</tr>
<tr>
<td>Middle</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>β2-microglobulin (mg/L)</td>
<td>24.8</td>
<td>25.6</td>
<td>7.25</td>
</tr>
<tr>
<td>Cystatin C (mg/L)</td>
<td>6.94</td>
<td>7.02</td>
<td>2.21</td>
</tr>
<tr>
<td>Myoglobin (µg/L)</td>
<td>209</td>
<td>203</td>
<td>91.1</td>
</tr>
<tr>
<td>Beta-Trace (mg/L)</td>
<td>7.72</td>
<td>7.79</td>
<td>4.69</td>
</tr>
<tr>
<td>Tropinon T (ng/L)</td>
<td>79.9</td>
<td>79.4</td>
<td>53.7</td>
</tr>
<tr>
<td>Large/mixed</td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>Albumin (g/L)</td>
<td>34.8</td>
<td>34.2</td>
<td>36.2</td>
</tr>
<tr>
<td>Transferrin (g/L)</td>
<td>1.56</td>
<td>1.56</td>
<td>1.63</td>
</tr>
<tr>
<td>IgG (g/L)</td>
<td>10.7</td>
<td>10.4</td>
<td>11.0</td>
</tr>
<tr>
<td>Transhytrem (Prealbumin) (g/L)</td>
<td>0.316</td>
<td>0.320</td>
<td>0.337</td>
</tr>
<tr>
<td>Total protein (g/L)</td>
<td>63.6</td>
<td>63.1</td>
<td>65.3</td>
</tr>
<tr>
<td>EVF</td>
<td>0.333</td>
<td>0.329</td>
<td>0.349</td>
</tr>
</tbody>
</table>

**Notes:** [A0] = Concentrations at the dialysis inlet, at time 0. [A240] = Concentrations at the dialysis inlet, at time 240. *Post-dialysis concentrations of middle and large molecules are adjusted for hematocrit according to Schneiditz et al. **Difference between RRs (HDF-MCO). ***Significant using the Bonferroni-corrected threshold for 14 outcomes, p=0.0036.

Small middle molecules (such as β2-microglobulin), but not for larger middle molecules. 10,12,14,26 Although our study only showed significantly higher RR with HDF for Cystatin C (13 kDa), the RR was slightly lower also for β2-microglobulin (11 kDa), although this was not statistically significant. Comparing our study to two studies with similar convection volumes to our study, which could be expected to show similar results, the study by Kirsch et al showed that HDF had higher RR for β2-microglobulin, although MCO was superior for larger middle molecules. 10 In the study by Reque et al, however, MCO was superior for both β2-microglobulin and larger middle molecules, although the difference was only statistically significant for the larger middle molecules. 13

A difference compared to these studies was the lower Qb in our study (Qb 324 mL/min, compared to Qb 400 mL/min for Kirsch, 10 and Qb 350 mL/min for Reque 13), which decreases the internal convection volume for MCO, while not affecting the HDF if assuming a fixed convection volume (although the maximal capacity for HDF convection volume is decreased). The convection volume is also dependent on factors such as hematocrit (determining the effective Qb), and protein oncotic pressure, and such factors might differ between the studies, not only depending on dialysis mode and dialyzer type, but also in analytical adjustments done to account for changes in blood viscosity during dialysis. One semi-empirical study has suggested that diffusion, not convection, of middle molecules is actually the main mechanism of removal with MCO dialyzers also for middle molecules. 23 Potential dialyzer differences in diffusion capacity may therefore also complicate comparisons between studies when different dialyzers have been used for HDF. Dialyzer type for HDF was Polyflux 210H for both our study and the study by Reque, 13 while Kirsch et al 10 compared with FX CorDiax (Freensius).

In the studies with very high convection volumes (Garcia-Preto et al 12 and Maudell et al 14), there was a tendency towards higher RRs for small middle molecules (but not for the largest middle molecules), for HDF compared to MCO, although the differences were large between the 8 different dialysis dialyzer types used for HDF in the study by Maudell, and significantly higher for both β2-microglobulin and myoglobin only for the dialyzer Elisio19H. 14 Although the previously cited studies used post-dilutional HDF, a recent study comparing HDF in pre-dilution mode (convection volume 49.91, blood flow 250 mL/min) also found HDF to be superior for
β2-microglobulin (11 kDa) but MCO superior for λ free light chains (45 kDa). 

Even if large molecules theoretically should not pass the dialysis membrane in significant amounts, protein adsorption on the dialyzer membrane is also a potential mechanism for removal. In vitro studies of MCO dialyzers have shown that protein fouling greatly decreases the permeability of the dialysis membrane during the first 40 minutes of blood contact. Also, studies in vitro of HDF-dialyzer (Revaclear) have shown the sieving coefficient for myoglobin to be reduced from 79% at 15 min to 67% at 60 min. This may be important especially for consideration of alternative dialysis treatments, such as short daily dialysis.

Our study was underpowered for the comparison of the RR of large molecules, but the results are of descriptive interest. Despite hemoconcentration adjustment, there were negative RRs seen for some of the larger molecules (ie, that the concentrations are slightly higher at the end than the beginning of the dialysis session, probably reflecting hemoconcentration), something which suggests that the RR in this range is strongly dependent on very adequate hemoconcentration adjustments. Such analytical method choices, which differ between studies, are important to consider in future comparisons and reviews of study results, especially for the large molecules and the larger middle molecules.

The study was non-randomized, but the potential risk for bias due to this is limited (although not eliminated) in the present study because of two study design features; 1) The cross-over design where people acted as their own controls minimizes bias due to different patient characteristics. 2) It was a controlled study with equal number performing the dialysis treatments in both sequences of intervention, which limits potential period effects.

The study was also non-blinded, a limitation that could be a concern especially for the reporting of adverse effects, but no adverse effects were seen during either treatment.
Since many factors may influence the dialysis efficiency in addition to the main type of dialysis mode/filter (HDF with conventional high-flux filter vs MCO-HD), it is important with replication of studies across different dialysis settings. We believe our study contributes to the evidence from previous studies comparing HDF with MCO in a dialysis population with well-functioning vascular access (mean convection volume of 24.5 L for HDF, and mean Q_b of 324 mL/min for HDF). Under these conditions, HDF and MCO overall gave comparable RRs, although HDF slightly outperformed MCO for a small middle molecule. A weakness of our study, however, was that we had no middle molecules in the upper middle molecular range (between 40–60 kDa), where theoretically the MCO membrane should be more permeable.\(^\text{17}\)

**Conclusion**

Overall, the RRs were comparable for ol-HDF and MCO-HD. The study found a slightly higher RR of cystatin C (a small middle molecule) for HDF compared to MCO, but no difference in other measured molecules. Whether HDF or MCO is superior for smaller middle molecules is likely to be influenced by the exact blood flows/convection volumes used during the dialysis treatment.

**Data Sharing Statement**

Study data will not be publicly archived since ethical permission for this has not been obtained.

**Ethics Approval and Informed Consent**

This study was approved by the Lund University Ethical Committee (registration no. 2017/830) and followed the Helsinki declaration. Written informed consent was obtained from all patients in the study.
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Disclosure
The authors report no conflicts of interest in this work.

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