Daunorubicin-loaded magnetic nanoparticles of Fe₃O₄ overcome multidrug resistance and induce apoptosis of K562-n/VCR cells in vivo

Abstract: Multidrug resistance (MDR) is a major obstacle to cancer chemotherapy. We evaluated the effect of daunorubicin (DNR)-loaded magnetic nanoparticles of Fe₃O₄ (MNPs-Fe₃O₄) on K562-n/VCR cells in vivo. K562-n and its MDR counterpart K562-n/VCR cell were inoculated into nude mice subcutaneously. The mice were randomly divided into four groups: group A received normal saline, group B received DNR, group C received MNPs-Fe₃O₄, and group D received DNR-loaded MNPs-Fe₃O₄. For K562-n/VCR tumor, the weight was markedly lower in group D than that in groups A, B, and C. The transcriptions of Mdr-1 and Bcl-2 gene were significantly lower in group D than those in groups A, B, and C. The expression of Bcl-2 was lower in group D than those in groups A, B, and C, but there was no difference in the expression of P-glycoprotein. The transcriptions and expressions of Bax and caspase-3 in group D were increased significantly when compared with groups A, B, and C. In conclusion, DNR-loaded MNPs-Fe₃O₄ can overcome MDR in vivo.

Keywords: multidrug-resistance reversal, leukemia, magnetic nanoparticles of Fe₃O₄, in vivo

Introduction

The development of new cytotoxic drugs and treatment strategies has resulted in improved response rates for patients with hematological malignancies. However, multidrug resistance (MDR) is the primary cause for almost 90% of cancer treatment failures.¹,² Cancer cells are becoming resistant to the cytotoxic effects of a wide range of structurally and mechanistically unrelated anticancer drugs. It has been proved that various molecular mechanisms,³ including the activation of detoxifying systems of the glutathione-S-transferase gene, DNA repair, and alteration in drug-induced apoptosis of genes in the Bcl-2 pathway, contribute to the complex story of cancer drug resistance. However, the most commonly encountered effect of MDR in the laboratory is the decreased intracellular drug accumulation caused by enhanced drug efflux from tumor cells.⁴ This is related to the overexpression of a family of energy-dependent transporters,¹ known as ATP-binding cassette (ABC) transporters such as P-glycoprotein (P-gp) and MDR-associated protein.⁵ Among these ABC transporters, P-gp confers cancer cells the strongest resistance to the widest variety of compounds. P-gp, a 170-kDa membrane-associated glycoprotein, transports a broad class of hydrophobic cytotoxic drugs that are central to most chemotherapeutic regimens from cell cytoplasm to outside the plasma membrane.⁶ Despite the wealth of information collected about the biochemistry and substrate specificity of P-gp and other types of ABC transporters, translation of this knowledge from the bench to the bedside has proved to be unexpectedly difficult. Because cytotoxic drugs typically

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carry numerous dose-limiting normal tissue side effects, it is generally impractical to overcome this form of drug resistance simply by increasing the drug dose. Extensive efforts have been made to design P-gp modulators (chemosensitizers). Unfortunately, modulation of P-gp activity by current chemosensitizers to inhibit ABC transporters is limited for several reasons, such as low efficiency, strong adverse effects, and pharmacokinetic interactions that limit anticancer drug clearance and metabolism.

Nanotechnology is no stranger to oncology. A wide variety of nanovectors have been used for the delivery of anticancer drugs to overcome drug resistance as well as to improve the effectiveness and safety of cancer chemotherapy, such as the use of drug-loaded liposomes, stealth liposomes, polymeric nanospheres with equivalent stealth properties, polymeric nanocapsules, and solid lipid nanoparticles. The major advantages sought by the use of nanovectors over simple drugs are as follow: the specific delivery of large amounts of therapeutic agents using biorecognition targets; protection of the drug from premature degradation and interaction with the biological environment; enhanced absorption of the drugs into a selected tissue through enhanced permeability and retention (EPR) effect; controlling the pharmacokinetic and drug tissue distribution profile; and improvement of intracellular penetration, which ameliorates the therapeutic index.

In our previous research, we have developed tetraheptylammonium-capped MNPs-Fe$_3$O$_4$, which could facilitate the drug accumulation of daunorubicin (DNR) inside MDR leukemia K562/A02 cells and enhance the response of DNR in MDR leukemia K562/A02 cells in vitro. It has been demonstrated that DNR polymerized with MNPs-Fe$_3$O$_4$ have shown more chemosensitizing activities than those of DNR alone. The cytotoxicity test in vitro revealed that MNPs-Fe$_3$O$_4$ exhibit excellent biocompatibility. Furthermore, no carcinogenic effects have been observed for MNPs-Fe$_3$O$_4$. Its effect on MDR leukemic cells in vivo remains unknown. In this work, we demonstrate that DNR-loaded MNPs-Fe$_3$O$_4$ are able to reverse MDR leukemic K562-n/VCR cells in vivo by inducing apoptosis. However, DNR-loaded MNPs-Fe$_3$O$_4$ fails to enhance cytotoxicity response in sensitive leukemic K562-n cells in vivo.

**Materials and methods**

**Preparation of DNR-loaded MNPs-Fe$_3$O$_4$**

MNPs-Fe$_3$O$_4$ were produced by electrochemical deposition under oxidizing conditions in a 0.1 mol/L tetraheptylammonium 2-propanol solution, where the magnetization and the size of MNPs-Fe$_3$O$_4$ was found to be 25.6 \times 10^{-3} $\text{emu/mg}$ and 30 nm, respectively. The deposited clusters were capped with tetraheptylammonium, which acts as a stabilizer of the colloidal nanocrystallites. Before being applied in this experiment, the magnetized nanoparticles of Fe$_3$O$_4$ were well distributed in 0.9% NaCl solution by using ultrasound treatment in order to obtain colloidal suspension of MNPs-Fe$_3$O$_4$. 0.2 g/L DNR (Sigma Aldrich, St. Louis, MO, USA) conjugated with 0.116 g/L MNPs-Fe$_3$O$_4$ were prepared by mechanical absorption polymerization as previously reported.

**Cell lines and cell culture**

K562-n, a cell strain with high tumorigenicity in nude mice, was derived from K562 cells, which were cloned from human chronic myelogenous leukemia by repeated passage in nude mice and in culture alternatively. MDR leukemia cell K562-n/VCR, which expresses MDR gene (mdr-1), was established by a long-term, intermittent, low-dose, and gradually escalated vincristine (VCR) added into the culture medium. K562-n/VCR has been proved to be resistant to some extent to many cytotoxins including VCR, DNR, and has high tumorigenicity in nude mice. It has been proved that K562-n/VCR cells in the xenograft model had a comparatively stable MDR phenotype to the corresponding cells. K562-n and K562-n/VCR cells (gifted from the department of hematology, Shanghai Hospital, Second Military Medical University, Shanghai, China) were maintained in RPMI 1640 medium (Gibco, Carlsbad, CA, USA) with 10% fetal bovine serum (Sijiqing, Hang Zhou, China), penicillin G (100 IU/mL), streptomycin (100 μg/mL), and streptomycin (100 μg/mL) at 37 °C in a humidified 5% CO$_2$ atmosphere. 0.64 μg/ml VCR was added regularly in K562-n/VCR culture medium to maintain drug resistance. K562-n/VCR cells were incubated in VCR-free medium for over two weeks before the planned experiment.

**Animals and establishment of the xenograft leukemia model in nude mice**

Female BALB/c-nu/nu mice were purchased from Beijing National Center for Laboratory Animals, the Chinese Academy of Medical Sciences, and were four weeks old at the beginning of our experiments. They were maintained in specific pathogen-free (SPF) facilities in our college and fed with irradiated chow. The two subclones of cells, K562-n and K562-n/VCR, were inoculated subcutaneously into each side of the back of athymic nude mice (5 × 10$^6$ cells each) simultaneously, resulting in the formation of two tumors per mouse. The mice were assigned randomly to five groups.
after inoculation for 10 days when both tumors formed. Mice in the control group were treated with normal saline 0.2 ml (group A). Nude mice in group B were treated with MNPs-Fe$_3$O$_4$ (0.58 mg/kg). Group C were treated with DNR (1 mg/kg). Group D were treated with MNPs-Fe$_3$O$_4$ (0.58 mg/kg) loaded with DNR (1 mg/kg) every other day for 20 days by vena caudalis injection, respectively.

Tumor assessment
After the planned treatment all animals were killed with ether anesthesia. Tumors were isolated for weight detection and then for quantitative real-time reverse transcription–polymerase chain reaction and western blotting.

Quantitative real-time reverse transcription–polymerase chain reaction
A total RNA of K562-n/VCR tumors from all groups and K562-n tumor of group A were isolated by using Trizol reagent (Invitrogen Life Technologies, Carlsbad, CA, USA) according to the manufacturer’s protocol. One microgram of total RNA was used to generate cDNA by using SuperScript II Reverse Transcriptase (Invitrogen Life Technologies). PCR primers were designed to amplify products within target and control sequences (primer sequences for Mdr-1 (427 bp) and reverse, 5'-TGTTGAGTGACAGATGTTGGG-3' and reverse, 5'-AGATCGAGGAAAAGCAGCACCATA-3'; Bcl-2 (452bp) forward, 5'-GGGAGAACAGGGTACGATTAA-3' and reverse, 5'-CCACCGAACTCAAAGAAGG-3'; Bax (114bp) forward, 5'-TTTTGCTTCAGGTTTTTATC-3' and reverse, 5'-GACACTGCTCAAGCTTCTTG-3'; caspase-3 (445 bp) forward, 5'-CACAATAGCACCACCCCG-3' and reverse, 5'-GGGACATCGTCTCATTCA-3'; GAPDH (205bp) forward, 5'-CGGATTTGTGCTGTAGTG-3' and reverse, 5'-GAAGATGGGTATGGGAT-3'). Quantitative PCR was performed by monitoring in real-time the increase in fluorescence of SYBR green I dye (Takara, Shiga, Japan) with Rotor-Gene 3000 (Corbett Research, Sydney, Australia). Each experiment was undertaken in triplicate. The relative gene copy number was calculated by the concentration-CT standard curve method and normalized using the average expression of GAPDH.

Western blot analysis
Western blotting was used for the detection of P-gp. After treatment for 20 days, 0.1 g K562-n/VCR tumor tissue was collected from each mouse and homogenized for P-gp detection, tumor tissue from K562n is used as negative control. Tissues were extracted with 1 g/L Triton X-100 and protein concentration was determined with a Bio-Rad protein assay kit (Bio-Rad Laboratories, Hercules, CA, USA) and standardized with bovinersum albumin. A 50 μg sample of protein was separated on electrophoresed SDS-PAGE and electroblotted onto PVDF membrane (BioRad Laboratories). The membrane was blocked with buffer containing 10% fat free dry milk. Mouse anti-Bcl-2 antibody (1:500), mouse anti-Bax antibody (1:500), mouse anti-Caspase-3 antibody (1:500), mouse anti-P-gp antibody (1:500) and mouse anti-β-actin antibody (1:1000) were used respectively as the primary antibody. Horseradish peroxidase-conjugated anti-rabbit antibody (1:1000) was the secondary antibody. The band was detected by using an enhanced chemiluminescence (ECL) detection system.

Statistical analysis
For tumor diameter assessment and pathological examinations, experiments were repeated at least three times and evaluated by two independent researchers when indicated. Reported values represent the means ± SD. The significance of differences between experimental variables was determined using parametric Student’s t-test.

Results
DNR-loaded MNPs-Fe$_3$O$_4$ could greatly suppress the growth of K562n/VCR tumor, but failed to further inhibit the proliferation of sensitive K562-n tumor in vivo.

All models of nude mice with transplanted leukemic K562-n cell and its MDR counterpart K562n/VCR were established after subcutaneous injection for 10 days, with an average volume of 100 mm$^3$. The rate of subcutaneous tumor formation was 100%. For MDR-bearing K562-n/VCR tumors, there was no significant difference in the average tumor weight between groups A and B, the average tumor volume of group C seemed smaller but without statistic difference. The average tumor weight was less in group D than that in groups A, B, and C ($P < 0.05$) (Figure 1A). For sensitive K562-n tumors, there was no significant difference in the average tumor weight between groups A and B. The average tumor weight was less in groups C and D than that in groups A and B ($P < 0.05$). But the average tumor weight showed no difference in groups C and D (Figure 1B).

Transcription of Mdr-1, Bcl-2, Bax, and caspase-3 in K562-n/VCR tumor by RT-PCR
The transcription of Mdr-1 and Bcl-2 gene was significantly lower in group D than those in groups A, B, and C (group D vs groups A, B, or C; $P < 0.05$). The transcription of Bax and caspase-3
with DNR alone according to the average tumor weight ($P < 0.05$), while MNPs-$\text{Fe}_3\text{O}_4$ didn’t show any antitumor activity without DNR.

Many chemotherapeutic agents target intracellular organelles or molecules to achieve their anticancer activities.\textsuperscript{29} Effective chemotherapy thus requires an effectively high level of drug molecules to accumulate within the cancer cells. In addition, the effectiveness of chemotherapy is also correlated with drug exposure time.\textsuperscript{30} In P-gp overexpressing cells, it becomes a difficult task to maintain a high intracellular drug level for a reasonable length of time. Experimental studies have shown that the main antitumor effect of anthracyclines is correlated to the induction of apoptotic cells.\textsuperscript{31} Escape from apoptotic signals often accompanies MDR and tumor progression.\textsuperscript{32,33} In general, apoptosis may occur through specific apoptosis signaling pathways such as death receptors and mitochondria. However, the mitochondrial pathway plays a crucial role in anthracycline-related apoptosis,\textsuperscript{34} which is regulated by the Bcl-2 protein family.\textsuperscript{35} Bcl-2 family proteins consist of antiapoptotic and pro-apoptotic members.\textsuperscript{36} Previous reports have also documented that the ratio of antiapoptotic Bcl-2 to proapoptotic Bax protein determined, at least in part, the susceptibility of cells to a death signal,\textsuperscript{37} and are used as a predictive marker for therapeutic response to radiotherapy.\textsuperscript{38} It is well known that caspase-3 plays the central role in the initiation of apoptosis.\textsuperscript{39} Our study showed that DNR-loaded MNPs-$\text{Fe}_3\text{O}_4$ could decrease the expression of Bcl-2 and increase the expression of Bax and caspase-3 in K562-n/VCR tumors ($P < 0.05$), indicating that this therapy can overturn poor response and induce apoptosis of MDR K562-n/VCR cells to anticancer drugs \textit{in vivo}. Our outcomes clearly indicate that a MNPs-$\text{Fe}_3\text{O}_4$ drug delivery system can facilitate DNR accumulation in MDR cells and enhance apoptosis in MDR cells.

It has been reported that DNR can interact with DNA in the presence of Fe (III) ions which hampers the recognition of DNA by transcription factors and then inhibits transcription.\textsuperscript{40} We also found that DNR-loaded MNPs-$\text{Fe}_3\text{O}_4$ could downregulate the transcription of mdr-1 gene. The downregulation of the transcription of mdr-1 gene may attribute to the relatively high DNR concentration in K562-n/VCR, since MNPs-$\text{Fe}_3\text{O}_4$ alone is not able to inhibit the mdr-1 gene transcription. On the contrary, there is no difference in the quantity of P-gp on K562-n/VCR tumors among the four groups. Therefore functionalized MNPs-$\text{Fe}_3\text{O}_4$ can enhance DNR accumulation inside MDR cells without interfering with the quantity of P-gp, a mechanism which differs from many types of P-gp modulators such as tetrandrine, PC833,
Proper interaction of these two ATP-binding sites is crucial for the proper functioning of P-gp. Therefore, the structural perturbations in the lipid membranes induced by MNPs-Fe$_3$O$_4$ may decrease the affinity of ATP to its binding site and interfere with the ATPase activity. Not only have MNPs-Fe$_3$O$_4$ the ability to block P-gp function, but they also have the potential for aggregation and drug capsulation. Nanoparticles loaded with anticancer drugs could readily approach the cell membrane, leading to drug concentrations at the cell surface higher than those obtained with the same amount of free drug solution, which leads in turn to higher intracellular drug concentrations. It has been reported that it is more difficult for P-gp to remove the drug molecules from the cells when these molecules are associated with nanoparticles. DNR-loaded MNPs-Fe$_3$O$_4$ complexes are likely to be too large to be handled by P-gp and are consequently “trapped” within the cancer cells once they gain entrance into the targeted cells. This is another possible mechanism responsible for enhanced cellular drug retention. These mechanisms may be the reason that MNPs-Fe$_3$O$_4$, which has no cytotoxicity to cells, is able to reverse MDR. Another important observation of the present work is that DNR-loaded MNPs-Fe$_3$O$_4$ fail to further suppress the growth of K562-n tumor cells. The advantages of nanoparticles over solution appear to be augmented by the increases in P-gp levels of the treated cells. This phenomenon is consistent with recent studies of polymer-lipid hybrid nanoparticle systems and Pluronic block copolymers. However, these mechanisms are not able to explain the remarkable selectivity of DNR-loaded MNPs-Fe$_3$O$_4$ complexes with respect to MDR cells. Since MNPs-Fe$_3$O$_4$ may not completely inhibit the P-gp function, DNR-loaded MNPs-Fe$_3$O$_4$ complexes are able to enhance...
the DNR accumulation in P-gp negative cells at the same time as the MDR counterpart. It has been demonstrated that DNR–nanoparticle conjugates are transported via a different mechanism than the free drug. The conjugate is most likely to be transported in the cells via endocytosis, which represents a P-gp-independent pathway, whereas the free drug is transported via membrane diffusion, a pathway affected by efflux pumps. It also has been reported that endocytosis, secretion, and some other processes related to phase transitions in the plasma membrane are more active in MDR cells than in sensitive ones due to the higher membrane fluidity of the former. This suggests that the increase in the drug uptake observed in MDR cells in the presence of DNR–Fe₃O₄ was conditioned by the higher flexibility of their membranes. P-gp is normally expressed in the transport epithelium of the liver, kidney, and gastrointestinal tract, at pharmacological barrier sites, in adult stem cells, and in assorted cells of the immune system. A wide variety of substrates are translocated by P-gp transporters, ranging from chemotherapeutic drugs to naturally occurring biological compounds. It is becoming increasingly evident that P-gp has a pivotal role in host detoxification and protection of the body against xenobiotics. We wonder if the abrogation of P-gp by tetraheptylammonium-capped MNPs-Fe₃O₄ would result in systemic toxicity. It has been reported that mdr-1a/1b double knockout mice are viable and fertile and are almost indistinguishable from their wild-type littermates, which suggests that pharmacological modulation of human P-gp could represent a safe and effective strategy to thwart MDR cancers. Our histological data show that the application of MNPs-Fe₃O₄ was well tolerated by nude mice.

In conclusion, our results support the proposition that MNPs-Fe₃O₄ offers an attractive means of delivering DNR into MDR tumor cells and enhances apoptosis in the MDR cells without reducing P-gp protein in the cell membrane. DNR-loaded MNPs-Fe₃O₄ complex is insensitive to P-gp-mediated drug efflux and is more effective than free DNR in MDR cells. In any case, the DNR-loaded MNPs-Fe₃O₄ complex may target the Achilles’ heel of MDR cells.

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