Enhanced antibiotic activity of ampicillin conjugated to gold nanoparticles on PEGylated rosette nanotubes

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Purpose: This work presents the preparation of a nanocomposite of ampicillin-conjugated gold nanoparticles (AuNPs) and self-assembled rosette nanotubes (RNTs), and evaluates its antibacterial properties against two strains of drug-resistant bacteria (*Staphylococcus aureus* [*S. aureus*], methicillin-resistant *S. aureus* [MRSA]).

Materials and methods: Small, nearly monodisperse AuNPs (1.43±0.5 nm in diameter) nucleated on the surface of polyethylene glycol-functionalized RNTs in a one-pot reaction. Upon conjugation with ampicillin, their diameter increased to 1.86±0.32 nm. The antibacterial activity of the nanocomposite against *S. aureus* and MRSA was tested using different concentrations of ampicillin. The cytocompatibility of the nanocomposite was also tested against human dermal fibroblasts.

Results: Based on bacterial inhibition studies, the nanocomposite demonstrated enhanced antibiotic activity against both bacterial strains. The minimum inhibitory concentration (MIC) of the nanocomposite against *S. aureus* was found to be 0.58 µg/mL, which was 18% lower than ampicillin alone. The nanocomposite also exhibited a 20 hrs MIC of 4 µg/mL against MRSA, approximately 10–20 times lower than previously reported values for ampicillin alone. In addition, at concentrations of 4 µg/mL of ampicillin (70 µg/mL of AuNPs), the nanocomposite showed negligible cytotoxic effects.

Conclusion: Our findings offer a new approach for the treatment of drug-resistant bacteria by potentiating inhibitory effects of existing antibiotics, and delivering them using a non-toxic formulation.

Keywords: ampicillin, rosette nanotubes, gold nanoparticles, *S. aureus*, methicillin-resistant *S. aureus*

Introduction

Resistance to β-lactam antibiotics appeared alongside the first use of penicillin in the 1940s. Bacteria strains, such as *Staphylococcus aureus* (*S. aureus*), rapidly evolved to produce enzymes that deactivate the antibiotic. Shortly after, the penicillin derivative methicillin was introduced due to its proved resistance to bacterial enzymes. However, resistance to methicillin developed with the growth of a bacterial isolate of *S. aureus* called methicillin-resistant *S. aureus* (MRSA).^{1,2}

Regardless of the influence of risk factors and country variability, the increasing prevalence of *S. aureus* and MRSA infections necessitates the need for new antibiotics and/or therapeutic formulations. For instance, the β-lactam antibiotic ampicillin, an extended spectrum penicillin, was developed to extend the antibacterial activity of

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penicillins.³ While ampicillin was once used to treat a number of bacterial infections with particularly high efficiency, its widespread use has also triggered the growth of drug-resistant bacterial isolates.^{4,5} The recurring growth of bacterial isolates has consequently prompted research for new antibiotic treatments. With the emergence of nanoscience and nanotechnology in the field of drug delivery, several reports have found that the bactericidal efficacy of ampicillin can be improved when conjugated to gold nanoparticles (AuNPs).⁵⁻⁷

AuNPs are an ideal drug delivery vehicle due to their low-toxicity, biocompatibility, high chemical stability, and ease of synthesis.^{8,9} Furthermore, antibiotics could be conjugated to AuNPs in one simple step.¹⁰ Surface functionalization of AuNPs with antibiotics occurs because the drugs can coordinate to the surface of the AuNPs via their carboxylic acid, hydroxyl, thiol, or amine functional groups.¹¹ The resulting functionalization imparts antibacterial properties to the AuNPs that consequently result in bacteria degradation and death.¹²

In an effort to improve the efficacy and biocompatibility of antibiotic-conjugated AuNPs, our group has been concerned with the use of ultra-small AuNPs (ie, high surface area) grown on the surface of a new class of self-assembled nanotubes, rosette nanotubes (RNTs). RNTs are obtained through the self-assembly of a synthetic DNA base analog, the G $\wedge$ C motif.¹³⁻¹⁶ Intermolecular hydrogen bonding allows six G $\wedge$ C bases to form a supermacrocycle (rosette) maintained by 18 hydrogen bonds, which then self-organize to produce a tubular stack with tunable dimensions and surface chemistry (Figure 1).¹⁷

We have previously shown the nucleation, growth, and morphogenesis of nearly monodisperse AuNPs (1.4 nm $\pm$ 0.2 nm)¹⁷ on self-assembled RNTs using a one-pot reaction process. We have also developed a new synthetic strategy to prepare PEGylated RNTs (Figure 1) using G $\wedge$ C motifs covalently grafted with polyethylene glycol (PEG). PEGylated biomaterials have been shown in different studies to possess advantages for drug delivery, including reduced immunogenicity, improved pharmacokinetics, biodistribution, and biocompatibility.¹⁸⁻²⁰ In addition, the RNTs were previously shown to be non-toxic²¹⁻²³ and biocompatible with bone,²⁴⁻³² cartilage,^{33,34} heart,³⁵ skin,³⁶ endothelial,³⁷ and nerve cells functions.³⁸

Based on these studies, here we present the preparation of a new nanocomposite material of ampicillin-conjugated AuNPs nucleated on PEGylated RNTs (Amp-AuNPs-PEG-RNT) and

Figure 1 PEG-functionalized G $\wedge$ C base (A) self assembles into a rosette (B), which in turn self-assembles into a PEG-RNT via stacking interactions (C).

Abbreviations: RNT, rosette nanotube; PEG, polyethylene glycol.

an evaluation of its antibacterial properties against *S. aureus* and MRSA. Finally, we tested the cytocompatibility of this nanomaterial against human dermal fibroblasts (HDF) in vitro.

Materials and methods

Synthesis of AuNPs on PEGylated RNTs

The formation of AuNPs on PEGylated RNTs was studied in a systematic fashion by altering the ratios of reactants used (Table 1). The PEGylated RNTs used in the synthesis method were prepared using a strategy previously developed by the authors.^{13–17} A solution of PEGylated RNTs was treated with potassium tetrachloroaurate (KAuCl₄, Sigma) solution. The resulting solution was aged in the dark at room temperature for 24 hrs then treated with hydrazine hydrate (Acros Organics). The final solution was stored in the dark at room temperature for an additional 4 days.

Synthesis of ampicillin-conjugated AuNPs on PEGylated RNTs

Amp-AuNPs-PEG-RNT nanocomposite was prepared using a one-pot reaction. Ampicillin solution (Fisher, 4 µL, 1% w/w) was added to a solution of prepared AuNPs-PEG-RNTs (1 mL, Au-PEG-RNT-2, 2 days aging). The mixture was then aged in the dark at room temperature for 4 days. All the concentrations noted refer to the total ampicillin concentration in solution.

Electron microscopy

Transmission electron microscopy (TEM) and scanning electron microscopy (SEM) were used to image the formation of AuNPs on the RNTs. Samples were prepared according to our previously reported protocol. Briefly, carbon-coated 300-mesh copper grids (CF300-Cu from EM Sciences) were floated on droplets of AuNP solutions. After 1 min, the grids were blotted with filter paper and air-dried for 24 hrs. TEM images were recorded on JEOL JEM-1010 instrument at 80 kV and SEM images were

recorded on a Hitachi S 4800 at 3 kV with *ca.* 3 mm working distance.

Bacterial assays

The bacterial growth curve is a typical method for quantifying the number of bacteria in a sample over a period of time. As the OD of bacterial solution increases with bacteria multiplication, a growth curve is obtained. In this study, OD values were continuously recorded at 600 nm on SpectraMax Paradigm (Molecular Devices, Sunnyvale, CA) for up to 24 hrs at 37°C.

Bacteria colonies of *S. aureus* (*Staphylococcus aureus* subsp. *aureus*, ATCC[®] 12600[™]) and MRSA (*Staphylococcus aureus* subsp. *aureus*, ATCC[®] 43300[™]) were suspended in tryptic soy broth (TSB, 30 g/L, 5 mL) and solutions were propagated for 16 hrs in a shaking incubator at 37°C. The solutions were diluted with TSB to a concentration of 10⁹ bacteria/mL, where the bacterial density was determined by measuring OD values at 600 nm. Further dilution with TSB was made until a final concentration of 10⁶ bacteria/mL was achieved. The resulting bacterial solution was then transferred into a 96-well plate with a volume of 100 µL per well. The bacteria were then treated with Amp-AuNPs-PEG-RNT (10 µL, various concentrations). The final concentrations of ampicillin were 1.2, 0.86, 0.58, 0.29, 0.23, and 0.12 µg/mL. Negative control wells received 10 µL of TSB only. For the treatment of MRSA, the final concentration of ampicillin in each well was 4, 3.2, 2 µg/mL, 1, and 0.8 µg/mL.

HDF viability assay

HDF (Lonza, CC-2509) were cultured in filter-sterilized (0.22 µm, Corning) DMEM (Corning 10013CV) supplemented with 10% FBS (ATCC SCRR-30-2020[™]) and 1% penicillin-streptomycin (P/S, Sigma-Aldrich) under standard culturing condition (37°C, humidified, 5% CO₂/95% air). Cells at passage number of 4–6 were used in the experiments. To determine cell viability, HDF cells were seeded in a 96-well plate at a density of 20,000 cells per cm² and subsequently dosed with 10 µL Amp-AuNPs-PEG-RNT (10 µL,

Table 1 Concentration of PEG-RNTs, KAuCl₄, (NH₂)₂-H₂O, and the ratios of PEG-RNTs/KAuCl₄/(NH₂)₂-H₂O used for gold deposition studies

Sample	PEG-RNTs	KAuCl ₄ Solution	(NH ₂) ₂ -H ₂ O
Au-PEG-RNT-1	1 mg/mL, 930 µM, 1 mL	3.77 mg/mL, 10 mM, 9.3 µL, 1 eq	32.1 µg/mL, 1 mM, 9.3 µL, 0.1 eq
Au-PEG-RNT-2	1 mg/mL, 930 µM, 1 mL	3.77 mg/mL, 10 mM, 18.6 µL, 2 eq	32.1 µg/mL, 1 mM, 18.6 µL, 0.2 eq
Au-PEG-RNT-3	1 mg/mL, 930 µM, 1 mL	3.77 mg/mL, 10 mM, 37.2 µL, 4 eq	32.1 µg/mL, 1 mM, 37.2 µL, 4 eq
Au-PEG-RNT-4	1 mg/mL, 930 µM, 1 mL	3.77 mg/mL, 10 mM, 74.4 µL, 8 eq	32.1 µg/mL, 1 mM, 74.4 µL, 8 eq

various concentrations) in 100 μL DMEM. The final concentrations of ampicillin were 0.8, 1, 2, 3.2, and 4 $\mu\text{g/mL}$. The cells were incubated under standard culturing conditions for 24 hrs. Negative control group contained DMEM only.

MTS assay

Antibacterial drugs and 20,000 cells/ cm^2 were seeded in 96-well plates with a final volume of 100 μL /well. An additional set of wells was added (medium only) for background subtraction. The mixtures were incubated for 24 hrs, after which the solutions were gently removed from the wells. To each well, 20 μL MTS ((3-(4,5-dimethylthiazol-2-yl)-5-(3-carboxymethoxyphenyl)-2-(4-sulfophenyl)-2H-tetrazolium), Promega medicine) solution and 100 μL DMEM were added and the resulting solutions were incubated for 3 hrs under standard cell culture condition (37°C, humidified, 5% CO_2 /95% air). The OD values at 490 nm against background were then recorded.

Minimum inhibitory concentration (MIC) values were determined using Prism 7 (GraphPad software) to fit concentration data based on a modified Gompertz function.³⁹ All cell and bacterial experiments were run in triplicate and repeated at least three times. One-tailed Student's *t*-tests were used to estimate the significant differences, with a *p*-value ≤ 0.05 .

Results

Amp-AuNPs-PEG RNT nanocomposites

TEM imaging was used to assess the nucleation and size of AuNPs on PEGylated RNTs (Figure 2). The presence of the RNTs is an indication that they did not disassemble

under the conditions tested. It is apparent from the images that at high KAuCl_4 /PEG-RNTs ratios, small and nearly monodisperse AuNPs were obtained. Statistical analysis of the particle diameter revealed an average diameter of 1.43 ± 0.5 nm. However, at low concentration of KAuCl_4 relative to PEG-RNTs (eg, 1:1 and 2:1), larger polydisperse AuNPs were observed (Figure S1).

Typically, conjugation of antibiotics with AuNPs requires chemical functionalization of the AuNPs.⁴⁰ However, these subsequent steps could affect the efficacy of the antibiotics.^{41,42} In this study, we used a one-pot synthesis method to conjugate ampicillin to AuNPs on PEG-RNTs without further modification of the surface of the AuNPs or the antibiotic.

An earlier report by Brown et al showed that ampicillin can be conjugated to AuNPs via the thioether moiety on ampicillin.⁵ We anticipate a similar type of coordination in this study as depicted in Figure 3. As a result, the TEM images of Amp-AuNPs-PEG-RNTs show that the average diameter of the AuNPs increased to 1.86 ± 0.32 nm suggesting that ampicillin is effectively coordinated to the surface of the AuNPs.

Bacterial inhibition

The antibacterial activity of ampicillin conjugated to AuNPs on PEG-RNTs was compared to ampicillin alone against *S. aureus* (Figures S2 and S3). The results showed that bacteria growth treated with Amp-AuNPs-PEG-RNT at concentrations higher than 0.58 $\mu\text{g/mL}$ was inhibited for 24 hrs (MIC=0.58 $\mu\text{g/mL}$, Figure 4). The free ampicillin solutions were less effective at inhibiting bacteria growth than Amp-AuNPs-PEG-RNT (MIC=0.71 $\mu\text{g/mL}$) (Figure S2).

Figure 2 TEM images of (A) PEG-RNTs, (B) AuNP/PEG-RNT nanocomposite and (C) model of the nanocomposite. Black arrows in (B) point at AuNPs grown on PEG-RNT surface.

Abbreviations: RNT, rosette nanotube; PEG, polyethylene glycol; TEM, transmission electron microscopy; AuNP, gold nanoparticle.

Figure 3 TEM image AuNPs-PEG-RNT functionalized with ampicillin (A), and schematic representation of ampicillin coordination to AuNPs (B). Black arrows point at AuNPs on PEG-RNT surface.

Abbreviations: RNT, rosette nanotube; PEG, polyethylene glycol; TEM, transmission electron microscopy; AuNPs, gold nanoparticles.

The antibacterial activity of Amp-AuNPs-PEG-RNT was also evaluated against MRSA. Unlike *S. aureus*, MRSA required a higher concentration of Amp-AuNPs-PEG-RNT (2–4 $\mu\text{g/mL}$) to exert an antibacterial effect (Figure 5). This higher concentration is likely due to the acquired gene in MRSA (*mecA*) that encodes for the penicillin-binding protein PBP2a.^{43,44} In contrast, the MRSA grew rapidly when treated with ampicillin alone,

suggesting that Amp-AuNPs-PEG-RNT is effective at delivering ampicillin.

Based on the results from Figure 5, the MIC value of Amp-AuNPs-PEG-RNT against MRSA was estimated to be 4 $\mu\text{g/mL}$. Earlier reports have shown that ampicillin alone has MIC values ranging from 32 to 50 $\mu\text{g/mL}$ against MRSA.^{45–47} Therefore, the MIC of the nanocomposite against MRSA in this study is at least ten times lower than ampicillin alone.

To test the cytocompatibility of Amp-AuNPs-PEG-RNT an MTS assay was carried out using HDF cells. The cells treated with 0–4 $\mu\text{g/mL}$ of ampicillin (70 $\mu\text{g/mL}$ of AuNPs) exhibited viability similar to control groups after 24 hrs exposure (Figure 6).

Discussion

We have shown that the nanocomposite, Amp-AuNPs-PEG-RNT, has greater antibacterial activity (18% lower MIC) than the antibiotic ampicillin alone against *S. aureus*. While there are many MRSA strains, *Staphylococcus aureus* subsp. *aureus*, ATCC[®] 43300[™] exhibits methicillin resistance and expresses *mecA* to produce PBP2a.⁴⁸ Therefore, for this MRSA strain, the ampicillin-loaded nanocomposite was 10–20 times lower than ampicillin alone, suggesting significantly enhanced antibacterial properties. This could result from three possible mechanisms operating at the same time, with possible synergistic effects among the three: 1) electrostatic interaction between the cationic nanocomposite

Figure 4 Bacterial growth inhibition curve for *S. aureus* up to 24 hrs against Amp-AuNPs-PEG-RNT with different ampicillin concentrations and medium-only (negative control). Values are mean $\pm$ SD, N=3.

Abbreviations: RNT, rosette nanotube; PEG, polyethylene glycol; AuNPs, gold nanoparticles.

Figure 5 Bacterial growth inhibition graph for MRSA up to 24 hrs against Amp-AuNPs-PEG-RNT with different concentrations of ampicillin and medium-only (negative control). Values are mean $\pm$ SD, N=3, $p^{***}<0.001$ when compared to medium-only.

Abbreviations: MRSA, methicillin-resistant *S. aureus*; RNT, rosette nanotube; PEG, polyethylene glycol; AuNPs, gold nanoparticles.

Figure 6 HDF cell viability after 1-day exposure to Amp-AuNPs-PEG-RNT with total ampicillin concentrations varying from 0 to 4 µg/mL. Values are mean $\pm$ SD, N=3.

Abbreviations: RNT, rosette nanotube; PEG, polyethylene glycol; AuNPs, gold nanoparticles; HDF, human dermal fibroblasts.

and negatively charged bacterial surface, 2) AuNP bacterial membrane disruption, and 3) ampicillin mode of action.

The cationic nature of the nanocomposite^{13–17} suggests a possible mechanism that could help deliver the antibiotic to the target bacteria. Previous authors have reported influences of cell-surface charge against different cationic antimicrobial agents.^{45,49,50} These studies have detected electrostatic attractions between the antimicrobial agents and negatively charged bacterial surfaces which consequently induce a binding effect. Therefore, the electrostatic

attraction seems to play an important role in potentially binding the nanocomposite to the bacteria surface, which thereby increases the likelihood of delivery of the ampicillin.

In addition to the overall surface charge of the nanocomposite, the AuNPs of the nanocomposite could disrupt the bacterial membrane thereby contributing to bacteria death. For example, Cui et al have shown that AuNPs exert their therapeutic effects by interfering with bacterial metabolism, notably by collapsing the membrane

potential, limiting ATP synthase activity and inhibiting tRNA binding to the ribosomes.⁵¹ These effects induced by the AuNPs offer a possible secondary mechanism for the enhanced antibiotic activity of the nanocomposite against the two strains of bacteria.

Finally, a third possible mechanism for the observed enhanced antibacterial activity is the mode of action of ampicillin. It is well understood that the β -lactam antibiotics, such as ampicillin, target penicillin-binding proteins required for bacterial peptidoglycan (the polymer of amino acids that make up the bacterial cell wall) synthesis, thereby resulting in bacterial lysis.⁵² Therefore, this mechanism may have been retained in the inhibition of the bacteria with the nanocomposite alongside the two mechanisms discussed above.

In another experiment, we tested the cytocompatibility in vitro of the nanocomposite against HDF cells using different concentrations of ampicillin. Under 4 $\mu\text{g/mL}$ of ampicillin (equivalent to 70 $\mu\text{g/mL}$ of AuNPs) and 24 hrs exposure, HDF cells exhibited viability similar to control groups. Earlier reports suggest that charges on the surfaces of AuNPs are the primary factor contributing to their cytotoxicity at concentrations as low as 10 $\mu\text{g/mL}$. Charged AuNPs decrease the membrane potential and intracellular Ca^{2+} levels, resulting in up- or downregulated gene expression,⁵³ whereas neutral AuNPs do not.^{54,55} Our results show that our nanocomposite formulation containing 70 $\mu\text{g/mL}$ of AuNPs was negligible confirming that the AuNPs are bound to the RNTs and may be released in a controlled manner.

Conclusion

We have presented the formation of a new nanocomposite composed of ampicillin-conjugated AuNPs on the surface of PEGylated RNTs to inhibit the bacterial growth of *S. aureus* and MRSA. The nanocomposite displayed significantly higher antibacterial activity against *S. aureus* than ampicillin alone. At higher concentration of AuNPs, we have also shown that the nanocomposite inhibits MRSA growth. Taken together, these results establish the enhanced potential of antibiotics such as ampicillin when combined with the AuNPs-PEG-RNTs and lay a foundation for future research of this biomaterial against antibiotic-resistant bacteria.

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Disclosure

The authors report no conflicts of interest in this work.

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