

Comparison of osteogenic differentiation induced by *siNoggin* and *pBMP-2* delivered by lipopolysaccharide-amine nanopolymersomes and underlying molecular mechanisms

This article was published in the following Dove Press journal:
International Journal of Nanomedicine

Mingdi Huang,^{1,*}
Xinchun Zhang,^{1,*} Jing Li,²
Yanshan Li,¹ Qinmei Wang,²
Wei Teng¹

¹Hospital of Stomatology, Guangdong Provincial Key Laboratory of Stomatology, Institute of Stomatological Research, Guanghua School of Stomatology, Sun Yat-sen University, Guangzhou, People's Republic of China;

²Laboratory of Biomaterials, Key Laboratory on Assisted Circulation, Ministry of Health, Cardiovascular Division, First Affiliated Hospital, Sun Yat-sen University, Guangzhou, People's Republic of China

*These authors contributed equally to this work

Correspondence: Wei Teng
Hospital of Stomatology, Guangdong Provincial Key Laboratory of Stomatology, Institute of Stomatological Research, Guanghua School of Stomatology, Sun Yat-sen University, 56 Linyuanxi Road, Guangzhou, Guangdong 510055, People's Republic of China
Tel +86 208 380 6601
Fax +86 208 733 0757
Email tengwei@mail.sysu.edu.cn

Qinmei Wang
Laboratory of Biomaterials, Key Laboratory on Assisted Circulation, Ministry of Health, Cardiovascular Division, First Affiliated Hospital, Sun Yat-sen University, 58 Zhongshan Road II, Guangzhou, Guangdong 510080, People's Republic of China
Tel +86 208 733 0757
Fax +86 208 733 0757
Email wangqinm@mail.sysu.edu.cn

Purpose: Gene therapies via *Noggin* small interfering (si)RNA (*siNoggin*) and bone morphogenetic protein (BMP)-2 plasmid DNA (*pBMP-2*) may be promising strategies for bone repair/regeneration, but their ideal delivery vectors, efficacy difference, and underlying mechanisms have not been explored, so these issues were probed here.

Methods: This study used lipopolysaccharide-amine nanopolymersomes (LNPs), an efficient cytosolic delivery vector developed by the research team, to mediate *siNoggin* and *pBMP-2* to transfect MC3T3-E1 cells, respectively. The cytotoxicity, cell uptake, and gene knockdown efficiency of *siNoggin*-loaded LNPs (LNPs/*siNoggin*) were studied, then the osteogenic-differentiation efficacy of MC3T3-E1 cells treated by LNPs/*pBMP-2* and LNPs/*siNoggin*, respectively, were compared by measuring the expression of osteogenesis-related genes and proteins, alkaline phosphatase (ALP) activity, and mineralization of the extracellular matrix at all osteogenic stages. Finally, the possible signaling pathways of the two treatments were explored.

Results: LNPs delivered *siNoggin* into cells efficiently to silence 50% of *Noggin* expression without obvious cytotoxicity. LNPs/*siNoggin* and LNPs/*pBMP-2* enhanced the osteogenic differentiation of MC3T3 E1 cells, but LNPs/*siNoggin* was better than LNPs/*pBMP-2*. BMP/Mothers against decapentaplegic homolog (Smad) and glycogen synthase kinase (GSK)-3 β / β -catenin signaling pathways appeared to be involved in osteogenic differentiation induced by LNPs/*siNoggin*, but GSK-3 β / β -catenin was not stimulated upon LNPs/*pBMP-2* treatment.

Conclusion: LNPs are safe and efficient delivery vectors for DNA and RNA, which may find wide applications in gene therapy. *siNoggin* treatment may be a more efficient strategy to enhance osteogenic differentiation than *pBMP-2* treatment. LNPs loaded with *siNoggin* and/or *pBMP-2* may provide new opportunities for the repair and regeneration of bone.

Keywords: gene delivery, nanopolymersomes, *Noggin*, small interfering RNA, bone morphogenetic proteins, osteogenesis

Introduction

Bone defects caused by trauma, tumor, inflammation, or other diseases are problems worldwide. They bring about not only suffering and inconvenience to patients, but also constitute a heavy financial burden to patients and society due to the huge expenditures from direct costs (medical treatments) and indirect costs (loss of productivity).^{1,2}

For example, after blood, bone is the second most common type of transplanted tissue. In the US, about 0.5–1.5 million cases of bone grafting per year are done, leading to a market for bone grafting of \$1.6–\$2.5 billion.¹ In Canada, the mean direct costs for established long-bone non-unions have been calculated to be CN\$11,800, and the indirect costs for a tibia fracture to be 67–79% of total costs.²

Bone tissue has intrinsic regenerative capacity, but satisfactory restoration in structure and function as well as the recovery time remain challenges due to the limited natural regeneration ability of bone, especially in patients with large defects, comorbidity, or biomechanical instability.^{1,3} Therefore, development of intervention strategies to promote the repair and regeneration of bone in terms of quality and speed is important.

Intervention strategies such as bone grafting as well as use of osteoinductive/osteoconductive matrices, stem cells, signaling molecules, and genes, alone or in combination, have been developed, and much progress has been made.^{1,3–8} Among these strategies, gene-based therapies via delivery of osteogenesis-related nucleic acids (eg, DNA, small interfering (si)RNA into target cells have been demonstrated to be promising due to their high specificity and low toxicity.^{1,5,6,8,9}

Bone morphogenetic protein (BMP) signaling has a pivotal role during osteogenesis. Increased expression of BMPs can enhance bone regeneration, which can be realized by “turning on” activator genes via DNA transfection, or by “turning off” inhibitor genes via siRNA transfection. Several genes can regulate BMP signaling, but BMP-2 has been used extensively due to its potent osteoinductive ability, and it is one of two proteins (the other one is BMP-7) approved for clinical use in bone defects in the US. Accordingly, *Noggin* (an antagonist of BMP), which can bind and inactivate BMP-2, -4, -5, -7, -13, and -14, has attracted much attention.^{10–12} Upregulating expression of *BMP-2* or downregulating expression of *Noggin* alone or in combination can promote osteogenic differentiation of several cell types and bone-tissue formation in vitro and in vivo.^{11–19} However, the difference in efficacy and the underlying molecular mechanisms between treatment of *BMP-2* and *Noggin* siRNA mediated by the same vector has not been reported.

Gene vectors are important factors for successful gene therapy. “Naked” genes must be transported to their action sites in cells by viral or nonviral vectors due to their nature, such as negative charge, susceptibility to

degradation, and large size. Usually, nonviral vectors have superior safety and lower cost, but limited transfection efficiency compared with those of viral vectors. To improve the transfection efficiency of nonviral vectors, numerous strategies have been developed to modify vectors to overcome the barriers in gene delivery, as reviewed thoroughly by Zhou et al.²⁰ However, the “ideal” vector has yet to be identified, and exploring safe and efficacious systems is a major concern for gene therapies for osteogenesis.

“Polymersomes” are vesicles self-assembled from amphiphilic copolymers. They consist of an aqueous core and enclosed hydrophobic membranes surrounded by hydrophilic coronas. As nonviral vectors, polymersomes have attracted considerable attention due to their controllable structure, nature (size, degradability, stability, and tailor-made surface chemistry for target delivery), and ability to load hydrophilic, hydrophobic, or amphiphilic compounds alone or in combination.^{21,22}

Zhong and colleagues synthesized chimeric polymersomes composed of polyethylene glycol (PEG), P(TMC-DTC) and polyethylenimine (PEI) blocks, and then decorated them with different peptides targeting brain and tumor cells, respectively.^{23,24} When using these functionalized polymersomes as vectors for anti-polo-like kinase 1 siRNA, they showed excellent packaging and protection of siRNA in their lumen while releasing “payloads” in a cytoplasmic reductive environment quickly. Such siRNA-loaded polymersomes could significantly boost targeted siRNA therapy against human lung cancer and glioblastoma in nude mice by prolonging the circulation time of siRNA, enhancing siRNA accumulation in cancer cells, silencing target genes, and suppressing the corresponding protein expression. Ge et al²⁵ used a PEG-PCL-DEX polymersome–protamine vector to mediate siRNA to transfect SMMC-7721 cells, and expression of the target gene could be reduced to 61.73%±6.25%.

Our research team has developed a nonviral vector of lipopolysaccharideamine nanopolymersomes (LNPs) for gene delivery.^{26–29} LNPs are prepared from a synthesized water soluble and degradable three-block-graft copolymer containing oxidized sodium alginate (OA; which forms the backbone), and cholesteryl-graft-polyethylenimine (Cho-PEI; 1.8 kDa of Mn_{PEI}; which forms the side chains). We have demonstrated that LNPs have low cytotoxicity, degradability, excellent abilities to enter cells, and to escape from lysosomes, as well as high stability against dilution, pH, heparin, salts, and serum.²⁹ LNPs have transfection efficiency >95% when delivering plasmids

encoding enhanced green fluorescent protein (*pEGFP*) into mesenchymal stem cells (MSCs)²⁶ and induce significant angiogenesis in zebrafish when delivering plasmids encoding vascular endothelial growth factor (*pVEGF*).²⁸ When using LNPs to deliver *pBMP-2* into MSCs, expression of BMP-2 protein in MSCs can be enhanced.²⁷

Based on the data mentioned above, to explore whether LNPs are good candidate vectors for siRNA delivery, we evaluated the knockdown efficiency of *Noggin* siRNA (*siNoggin*) mediated by LNPs. Meanwhile, we compared the osteogenic differentiation between LNPs/*pBMP-2* and LNPs/*siNoggin*, and then investigated the underlying molecular mechanisms. In this way, we hope that greater understanding of bone repair via siRNA or pDNA (or both) can be obtained and, thus, more choices provided for clinical treatment.

Materials and methods

Materials

LNPs were synthesized following our established method.²⁶ *siNoggin* (catalog numbers Line 1-10620318 and Line 2-10620319), Alexa Fluor[®]555 siRNA, Stealth[™] RNAi Negative Control Duplexes (ctrRNA), lipofectamine3000 (lipo) (catalog number L3000015), Opti-MEM[™] I Reduced Serum Media, trypsin, TRIzol[®] Reagent, α -minimum essential medium (MEM), fetal bovine serum (FBS) and Penicillin/Streptomycin were purchased from Thermo Scientific (Waltham, MA, USA). *pBMP-2* (vector ID: VB160930-1048bkg), osteogenic medium, and Alizarin Red were obtained from Cyagen Biosciences. (Guangzhou, China). Cell Counting Kit-8 (CCK-8) was supplied by Dojindo (Tokyo, Japan). A bicinchoninic acid (BCA) assay kit was ordered from CWBIO (Beijing, China). An alkaline phosphatase (ALP) kit was supplied by Nanjing Jiancheng Bioengineering Institute (Nanjing, China). Cetylpyridinium chloride was purchased from Sigma-Aldrich (Saint Louis, MO, USA). A Prime-Script[™] Real Time (RT) reverse transcription kit was obtained from Takara Biotechnology (Shiga, Japan). LightCycler[®]480 SYBR[®] Green I Master was supplied by Roche Molecular Systems (Basel, Switzerland).

Antibodies against mouse *Noggin* were purchased from Novus Biologicals (Centennial, CO, USA). Antibodies against mouse *BMP-2*, osteopontin (OPN), and Mothers against decapentaplegic homolog (Smad)/1/5/9 were supplied by Abcam (Cambridge, UK). Antibodies against mouse β -catenin, Runt-related transcription factor (Runx)

2, phosphorylated (p)-Smad/1/5/9, glycogen synthase kinase (GSK)-3 β , p-GSK-3 β (Ser⁹), and glyceraldehyde 3-phosphate dehydrogenase (GAPDH) were obtained from Cell Signaling Technology (Danvers, MA, USA). The secondary antibody was anti-rabbit immunoglobulin G, horseradish peroxidase-linked antibody (catalog number 7074S), which was purchased from Cell Signaling Technology. The MC3T3-E1 cell line was obtained from the Cell Bank of the Chinese Academy of Sciences (Shanghai, China) (catalog number CRL-2593). Detailed information on other reagents can be found in the Supplementary Materials.

Complexation of siRNA or pDNA with vectors

First, stock solutions of LNPs (0.67 mg/mL) and siRNA (20 μ M) in nuclease-free sterile water were prepared and stored at 4°C until further use. Before use, the two stock solutions were diluted separately with culture medium to a certain concentration. Then, equal volumes of the two diluted solutions were mixed thoroughly and incubated at room temperature for 10 minutes to allow formation of LNPs/*siNoggin* complexes. Complexes of LNPs/ctrRNA, which were used as controls to clarify the *Noggin*-targeted specificity of *siNoggin*, were prepared by the same method. Likewise, complexes of lipo/*siNoggin* and lipo/ctrRNA were prepared, whereby the lipo concentration followed manufacturer suggestions. In addition, 50 nM of siRNA (final concentration in the culture medium) was used for cell transfection according to manufacturer instructions and our preliminary results (data not shown). Complexes of LNPs/*pBMP-2* (molar ratio of the amino groups in LNPs to the phosphate groups in *pBMP-2* was 60) with optimal transfection were prepared according to a method reported by our research team.^{26,27} All complex solutions were used immediately after preparation.

Cell culture and osteoblast differentiation

MC3T3-E1 cells were cultured in basal growth medium (α -MEM, 10% FBS, 1% Penicillin/Streptomycin) at 37°C with 5% carbon dioxide. To induce osteogenic differentiation, cells were first cultured in basal growth medium until 60–70% confluence, and then transferred to osteogenic medium containing 0.1 μ M of dexamethasone, 50 μ g/mL of ascorbic acid, and 10 mM of β -glycerol phosphate.

Cytotoxicity

Toxicity of LNPs to MC3T3-E1 cells was evaluated using a CCK-8 kit, and lipo was used as a control. Briefly, cells were seeded in 96-well plates (10^4 cells/well). After overnight incubation, medium was replaced by 100 μ L of fresh basal growth medium with different concentrations of LNPs and lipo. According to our preliminary data, optimal transfections could be achieved for LNPs/*siNoggin* with 3.35 μ g/mL of LNPs and 50 nM of siRNA and for lipo/*siNoggin* with 2.5 μ L/mL of lipo and 50 nM of siRNA, so the concentrations of LNPs were set as 0, 1.675, 3.35, 5.025, 6.70, 10.05, and 13.40 μ g/mL, and the concentrations of lipo were set as 1.25, 2.50, 3.75, 5.00, 6.25, and 7.50 μ L/mL, respectively. After 4 hours of incubation, the medium was replaced with fresh growth medium. Cells were cultured continuously for 48 hours, then 10 μ L CCK-8 was added to each well for an additional 2 hours of incubation, and their absorbance was measured at 450 nm using a microplate reader (Infinite200; Tecan, Männedorf, Switzerland).

Cell uptake of siRNA

In this experiment, Alexa Fluor 555-labeled siRNA was used to prepare complexes of LNPs/siRNA and lipo/siRNA. The efficiency of cell uptake efficiency was defined as the percentage of cells with red fluorescence. MC3T3-E1 cells were seeded in six-well plates (10^6 cells/well) and cultured until 60% confluence. Complexes of vector/siRNA with different concentrations were added to culture medium, and cells were incubated for 4 hours. Then, medium was replaced with new growth medium, and cells were cultured continuously for 24 hours. Thereafter, some cells were observed under an automatic inverted fluorescence microscope (DMI8; Leica, Wetzlar, Germany), and the other cells were cultured continuously and harvested at 48 hours for measurement of cell-uptake efficiency with a flow cytometer (FC500MPL; Beckman Coulter, Fullerton, CA, USA), as described previously.²⁶ Combining the results from cytotoxicity studies and this experiment, the final concentration of vectors in the culture medium for optimal transfection (maximal efficiency of cells with minimal cytotoxicity) were determined to be 3.35 μ g/mL LNPs for LNPs/siRNA and 2.50 μ L/mL lipo for lipo/siRNA, respectively, and they were used for subsequent experiments unless specified otherwise.

Cell proliferation assay

The effects of transfection upon cell proliferation were determined using a CCK-8 kit as described for the

cytotoxicity test with some changes. That is, in the cell-proliferation test, cells were treated with LNPs/*siNoggin* instead of LNPs, and MC3T3-E1 cells were cultured continuously for 7 days after transfection, the absorbance of which was measured on days 1, 3, 5, and 7, respectively.

ALP activity in transfected cells

MC3T3-E1 cells were seeded in 6-well plates (1×10^6 cells/well) and cultured until 60% confluence. Then cells were treated with LNPs/*siNoggin* for 4 hours, followed by incubation in osteogenic medium for 7 days or 14 days. During this period, osteogenic medium was exchanged every 3 days. At predetermined time points, cells were lysed for assays of total-protein concentration and ALP activity. The protein concentration was detected by a BCA assay kit following manufacturer protocols. ALP activity was measured by an ALP kit according to manufacturer instructions.

Mineralization of the extracellular matrix (ECM)

Mineralization in MC3T3-E1 cells was determined by Alizarin Red staining.³⁰ MC3T3-E1 cells were cultured and treated as described for the ALP-activity test. After 28 days of culture in osteogenic medium, cells were washed with phosphate-buffered saline (PBS), fixed in 4% paraformaldehyde for 30 minutes, rinsed with PBS, and stained in 2% Alizarin Red solution for 15 minutes at room temperature, followed by thorough washing with PBS. Thereafter, some stained cells were observed under an inverted microscope (Axio Observer Z1; Zeiss, Oberkochen, Germany) to evaluate the formation of calcified nodules. To quantify mineralization, the other stained cells were incubated in 10% cetylpyridinium chloride for 30 minutes to dissolve calcified nodules, and their absorbance at 562 nm was measured.

Real-time polymerase chain reaction (RT-PCR) quantification of *Noggin* mRNA and *Runx2* mRNA

MC3T3-E1 cells were cultured and treated as described for the ALP-activity test. We undertook RT-PCR according to a reported method.^{6,8,30} Briefly, after culture in osteogenic medium for 2, 7, and 14 days, total RNA in cells was extracted using TRIzol Reagent. Then, 0.5 μ g of total RNA was reverse-transcribed to cDNA using a Prime-Script RT kit according to manufacturer instructions. RT-PCR was carried

out a RT-PCR instrument (LightCycler 480 SYBR Green I Master). Expression of target genes was calculated by the $2^{-Ct\Delta\Delta}$ method using expression of the housekeeping gene (GAPDH) as a control. The target primer sequences are listed in the Supplementary Materials.

Western blotting

Western blotting was done using a standard method. Briefly, MC3T3-E1 cells were cultured and treated as described above in the ALP-activity test. After culture in osteogenic medium for a predetermined time, cells were lysed for extraction of total protein. The concentration of total protein was determined with a BCA assay kit according to supplier protocols. Then, the proteins were separated by sodium dodecyl sulfate-polyacrylamide gel electrophoresis using 8% gels and transferred to polyvinylidene difluoride (PVDF) membranes. After blockade, PVDF membranes were incubated overnight using antibodies against mouse *Noggin*, *BMP-2*, *OPN*, β -catenin, *Runx2*, *Smad1/5/9*, *p-Smad1/5/9*, *GSK-3 β* , *p-GSK-3 β* (Ser⁹), and *GAPDH*. All antibodies were diluted to 1:1,000. Finally, the PVDF membranes were incubated with secondary antibody (1:2,000 dilution) for 1 hour at room temperature. Western-blotting signals were detected using ECL Plus (Millipore, Billerica, MA, USA).

Statistical analyses

Data are the mean \pm standard deviation (n=3). Statistical tests were undertaken using one-way analysis of variance by Prism 6.0 (GraphPad, La Jolla, CA, USA) or SPSS v-20.0 (IBM, Armonk, NY, USA). $P<0.05$ was considered significant.

Results

Toxicity of Inps to MC3T3-E1 cells

Safety is the most important parameter for a gene-delivery vector, and cytotoxicity is the basic mode of evaluation. The cytotoxicity of LNPs was measured by cell viability using the CCK-8 assay. Lipo3000, a commercially available transfection reagent, was used as a control, and MC3T3-E1 cells were used as “model” cells. In the concentration range tested, 48 hours after transfection, in the LNPs group, cell viability was ~20% higher than that in untreated cells (Figure 1), which could be ascribed to the rapid proliferation of untreated MC3T3-E1 cells. At 48 hours after transfection (at ~60 hours after seeding), untreated cells were crowded, and their metabolic activity

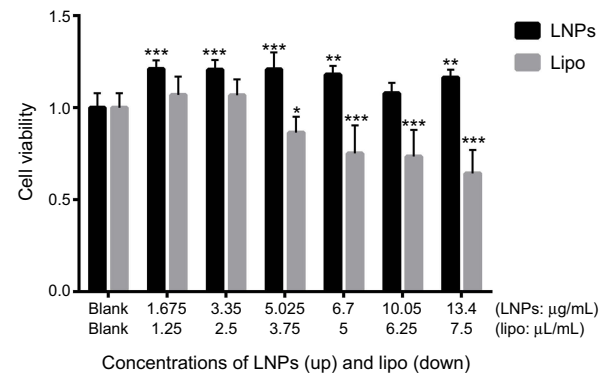


Figure 1 Cell viability 48 hours after transfection.

Notes: * $P<0.05$, ** $P<0.01$ and *** $P<0.001$ vs the blank group. The error bars represent the mean \pm SD (n=3).

Abbreviations: LNPs, lipopolymer-amine nanopolymerosomes; lipo, lipofectamine3000.

decreased due to contact inhibition; whereas, after adaptation to transfection, the transfected cells had high metabolic activity. In the lipo group, cell viability was comparable with that of untreated cells at ≤ 2.5 μ L/mL, but further increases in concentration (≥ 3.75 μ L/mL) decreased cell viability. Cells treated with 3.35 μ g/mL of LNPs (the concentration for optimal transfection) showed high viability, which was slightly higher than that for cells treated by 2.5 μ L/mL of lipo, but the difference was not significant. The low cytotoxicity of LNPs was consistent with previous data from our research team, in which the viability of transfected MSCs was ~88% at 25 μ g/mL of LNPs for 48 hours of incubation.²⁶ However, in the present study, we used a lower concentration (the upper concentration of LNPs was 13.4 μ g/mL) and, thus, cells showed higher viability.

Cell uptake

siRNAs must enter cells to exert their functions. Therefore, we measured the cellular uptake of LNPs/si*Noggin* labeled by Alexa Fluor 555 by fluorescence and flow cytometry. When the concentration of LNPs was ≤ 5.025 μ g/mL, cells treated by LNPs/si*Noggin* emitted strong red fluorescence 24 hours after transfection (Figure 2A), suggesting successful uptake of LNPs/si*Noggin*. In addition, cells (bright-field images) exhibited a fusiform appearance with ~95% confluence, which was similar to that of blank (untreated) cells, indicating that the cells were healthy. These data further confirmed the low cytotoxicity of LNPs because cell morphology is a visual indicator of cytotoxicity. Upon increasing the concentration of LNPs to 6.7 μ g/mL, strong red fluorescence remained, but cells shrank and decreased in number,

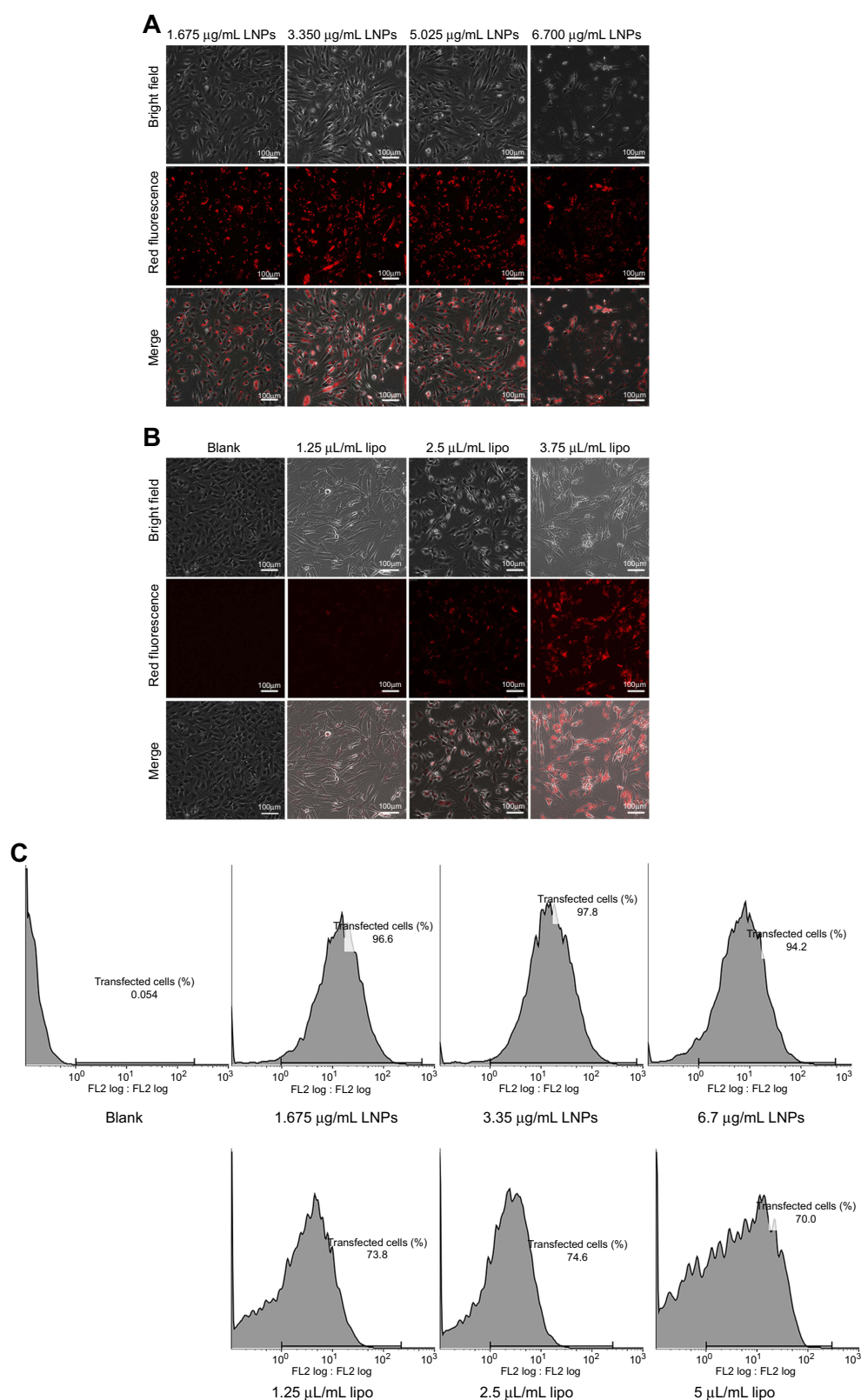


Figure 2 (A and B) Images of MC3T3-E1 cells treated by different concentrations of LNPs/siRNA or lipo/siRNA 24 hours after transfection treatment. **(C)** Efficiency of cell uptake quantified by flow cytometry 48 hours after transfection.

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

and a few extracellular fragments could be seen, suggesting that use of this concentration may be slightly harmful to cells. When the concentration of lipo was ≤ 2.5 $\mu\text{L/mL}$, cells treated by lipo/*siNoggin* were healthy, with $\sim 50\%$ confluence (Figure 2B), which suggested the low toxicity of reagents. Also, the distribution of red fluorescence became denser with an increase in concentration, suggesting an increase in the cell-uptake efficiency of lipo/*siNoggin*; when the concentration of lipo increased to 3.75 $\mu\text{L/mL}$, the health of cells deteriorated obviously.

Figure 2C shows the cell uptake efficiency of LNPs/*siNoggin* and lipo/*siNoggin* 48 hours after transfection. The maximal cell-uptake efficiency was 97.8% for LNPs/*siNoggin* at 3.35 $\mu\text{g/mL}$ of LNPs, and 74.6% for lipo/*siNoggin* at 2.5 $\mu\text{L/mL}$ of lipo. From the results of cytotoxicity and cell uptake, we concluded that 3.35 $\mu\text{g/mL}$ of LNPs for LNPs/*siNoggin* and 2.5 $\mu\text{L/mL}$ of lipo for LNPs/*siNoggin* were the concentrations for optimal transfection (the concentration at which the gene-delivery systems showed maximal efficiency of cell uptake with minimal cytotoxicity).

Knockdown of *Noggin* by LNPs/*siNoggin*

To evaluate gene-knockdown efficiency via LNPs/*siNoggin*, *Noggin* expression in transfected MC3T3-E1 cells was tested by RT-PCR (Figure 3A). To clarify the specificity of siRNA on target genes, we undertook transfection using *Noggin*-targeted siRNA (*siNoggin*) and non-targeted siRNA (ctrRNA). *siNoggin* treatment led to much lower expression of *Noggin* and *Noggin* protein in cells than ctrRNA treatment using the same vector. For example, compared with LNPs/ctrRNA treatment, LNPs/*siNoggin* treatment decreased expression of *Noggin* and *Noggin* protein by 40% and 35%, respectively. Compared with the blank, 2 days after transfection, the LNPs/*siNoggin* group had a knockdown efficiency for *Noggin* of 50%, but that of lipo/*siNoggin* was 25%. Then, to further verify gene suppression, expression of *Noggin* protein in transfected MC3T3-E1 cells was detected by Western blotting 3 days after transfection (Figures 3B and C). Expression of *Noggin* protein decreased by 40% in the LNPs/*siNoggin* group and 20% in the lipo/*siNoggin* group. These results of *Noggin*-protein expression were consistent with *Noggin* knockdown, and showed that LNPs could deliver *siNoggin* into cells to suppress *noggin* expression; were a more efficient gene delivery vector than lipo; and could induce two-fold higher gene-knockdown efficiency than that induced by lipo.

Effects of transfection via different delivery systems upon cell proliferation

The effects of transfection via LNPs/*siNoggin* and LNPs/*pBMP-2* upon cell proliferation were examined using the CCK-8 assay. During days 1–7 of culture after transfection, MC3T3-E1 cells proliferated with time in all groups (Figure 4). This finding is consistent with the reported developmental sequence of MC3T3-E1 cells, which replicate actively during the initial developmental phase (days 1–9 of culture), as evidenced by a progressive increase in cell number.³¹ As expected, cells treated by LNPs/(ctrRNA or *siNoggin* or *pBMP-2*) exhibited higher proliferation than cells untreated or treated by lipo/(ctrRNA or *siNoggin*), indicating that LNPs/(*siNoggin* or *pBMP-2*) could enhance proliferation of MC3T3-E1 cells. On day-7, the proliferation in LNPs/*pBMP-2* is higher than that in LNPs/*siNoggin*, whereas no obvious difference was observed between them before day 7. Based on the results from experiments on the viability, morphology, and proliferation of cells, we concluded that LNPs and LNPs/(*siNoggin* or *pBMP-2*) did not show obvious toxicity, and could enhance proliferation within 7 days.

ALP activity of MC3T3-E1 cells treated by LNPs/*siNoggin*

ALP activity was measured to assess the effects of LNPs/*siNoggin* treatment on osteogenesis of MC3T3-E1 cells (Figure 5A). ALP activity increased with culture time in all groups, and vector/*siNoggin* treatment led to higher ALP activity than that observed with vector/ctrRNA treatment. Compared with untreated cells, treatment with LNPs/*siNoggin*, LNPs/*pBMP-2*, or lipo/*siNoggin* enhanced ALP activity in cells by approximately 1.98-, 1.45-, and 1.28-fold on day 7, and by 1.56-, 1.42-, and 0.98-fold on day 14, respectively, suggesting that the ability of complexes for promoting ALP activity was in the order LNPs/*siNoggin* > LNPs/*pBMP-2* > lipo/*siNoggin*.

Effects of LNPs/*siNoggin* on expression of *Runx2* mRNA

Runx2 is a major transcription gene that regulates osteogenic differentiation. *Runx2* expression in MC3T3-E1 cells was examined by RT-PCR on days 7 and 14. Expression of *Runx2* mRNA increased on days 7 and 14 in all groups compared with that in the blank (untreated) cells (Figure 5B). Compared with untreated cells, on day-7, *Runx2* expression increased to 1.75-, 1.50-, and 1.50-fold in LNPs/*siNoggin*, LNPs/*pBMP-2*, and lipo/*siNoggin* groups, respectively;

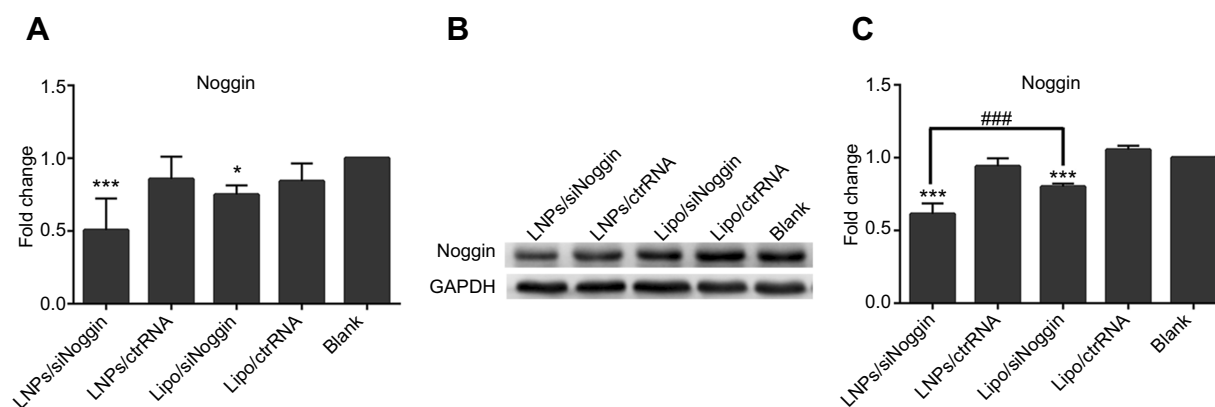


Figure 3 Expression of *Noggin* and *Noggin* protein in MC3T3-E1 cells transfected with different siRNA delivery systems. **(A)** Expression of *Noggin* on day-2 (PCR data). **(B)** Expression of *Noggin* protein on day-3 (data from Western blotting). **(C)** Semiquantitation of *Noggin* protein from Western blotting images analyzed by ImageJ software. **Notes:** * $P < 0.05$ and *** $P < 0.001$ vs the blank group. ### $P < 0.001$. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

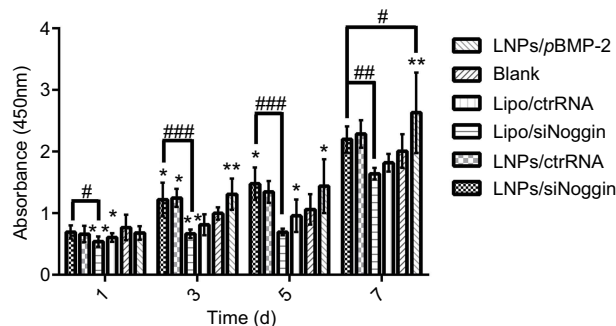


Figure 4 Effects of transfection via different systems on proliferation of MC3T3-E1 cells on days 1, 3, 5, and 7. The error bars represent the mean \pm SD ($n = 3$).

Notes: * $P < 0.05$ and ** $P < 0.01$ vs the blank group. # $P < 0.05$, ## $P < 0.01$ and ### $P < 0.001$. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

on day-14, the corresponding value was 1.22-, 1.14-, and 1.18-fold, respectively, but a significant difference was not found between groups at this time. Based on these results, we concluded that LNPs/siNoggin could contribute more to improving expression of *Runx2* mRNA in MC3T3-E1 cells than LNPs/pBMP-2 and lipo/siNoggin.

ECM mineralization

Late-stage osteogenesis was characterized further by examining ECM mineralization through Alizarin Red staining on day-28. Compared with the blank, all transfection groups had significantly enhanced formation of calcified nodules (stained red) in MC3T3-E1 cells (Figure 6A). The mineralization level in the LNPs/siNoggin group was ~1.2-fold higher than that in the LNPs/pBMP-2 group, and was comparable between the groups of LNPs/pBMP-2 and lipo/siNoggin (Figure 6B), indicating that promotion of mineralization regulated via LNPs/siNoggin was more

powerful than that via LNPs/pBMP-2 at the late stage of osteogenesis.

Effects of gene transfection on expression of osteogenic proteins

After assessing the effect of gene transfection on osteogenic differentiation via measuring expression of related genes, we further assessed this effect by determining the expression of related proteins in transfected MC3T3-E1 cells at different osteogenesis stages using Western blotting.

At the early stage of osteogenesis (1–7 days of culture), compared with untreated cells, transfection increased protein expression of BMP-2, OPN, Runx2, and β -catenin in cells. However, expression of OPN protein in the lipo/siNoggin group and β -catenin protein in the LNPs/pBMP-2 group on day-3 was not significantly different from that of blank (untreated) cells. The same was true for expression of OPN and Runx2 proteins in the lipo/siNoggin group and BMP-2 and Runx2 proteins in the LNPs/pBMP-2 group on day-7 (Figure 7). LNPs/siNoggin led to higher expression of protein than that elicited by LNPs/pBMP-2 or lipo/siNoggin treatment. For example, compared with the LNPs/pBMP-2 group, on day-3, protein expression of BMP-2, OPN, Runx2 and β -catenin in the LNPs/siNoggin group increased by 1.57-, 1.66-, 1.64-, and 1.43-fold (Figures 7A and B) and on day 7, it increased by 1.48-, 1.19-, 1.50-, and 1.28-fold, respectively (Figures 7C and D).

At the intermediate stage of osteogenesis (8–14 days of culture), on day-14, protein expression of β -catenin

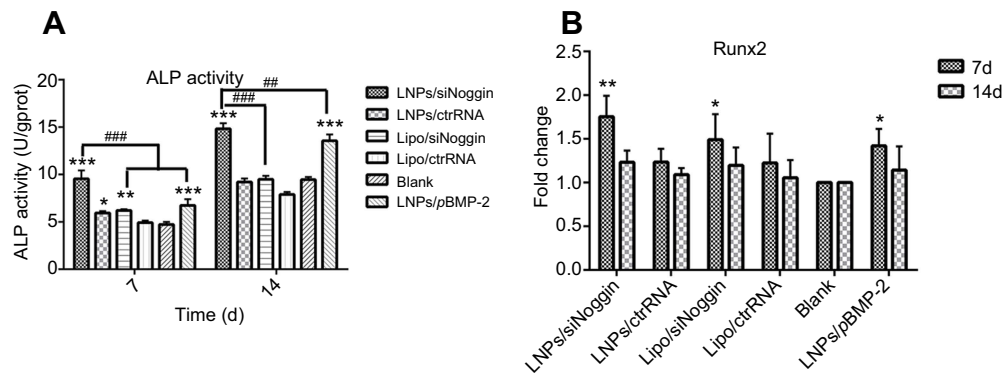


Figure 5 ALP activity (A) and relative expression of *Runx2* mRNA determined by RT-PCR (B) in transfected MC3T3-E1 cells after 7 days and 14 days of culture in osteogenic medium.

Notes: * $P < 0.05$, ** $P < 0.01$ and *** $P < 0.001$ vs the blank group. ### $P < 0.01$ and #### $P < 0.001$. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000; ALP, alkaline phosphatase.

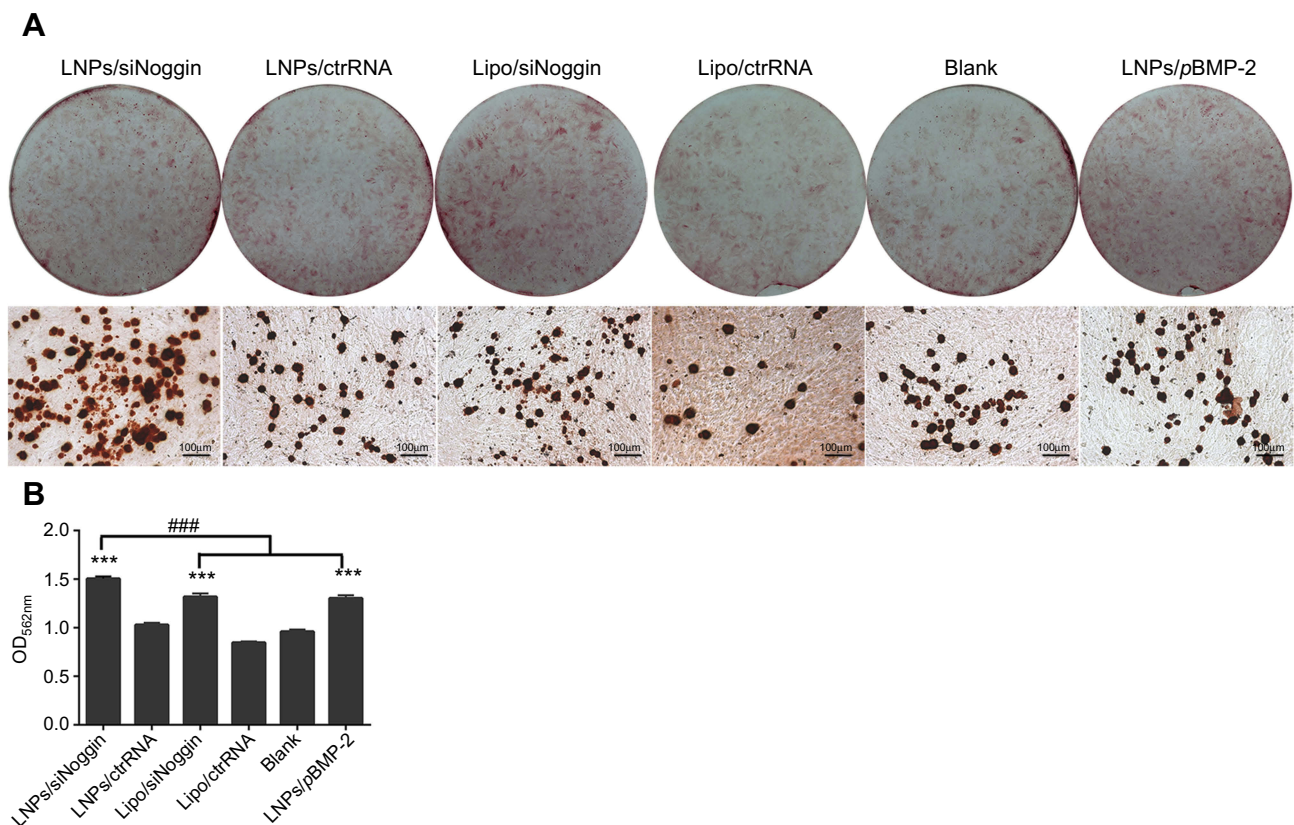


Figure 6 Mineralization of transfected MC3T3-E1 cells on day 28. (A) Alizarin Red staining. Photos (upper) and microscopic images (lower) show formation of calcified nodules (stained red). (B) Quantification of calcified nodules dissolved by 10% cetylpyridinium chloride solution.

Notes: *** $P < 0.001$ vs the blank group. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

and *Runx2* was enhanced significantly in cells treated by LNPs/*siNoggin* or lipo/*siNoggin* compared with that in untreated cells, but there was no significant difference in protein expression between cells untreated and cells treated by LNPs/*pBMP-2* (Figures 8A and B). In addition, LNPs/*siNoggin* treatment led to higher expression of β -

catenin protein and *Runx2* protein than that by lipo/*siNoggin* treatment.

At the late stage of osteogenesis (15–21 days of culture), on day 21 (Figures 8C and D), LNPs/*siNoggin* treatment enhanced expression of β -catenin protein and *Runx2* protein significantly to 1.40- and

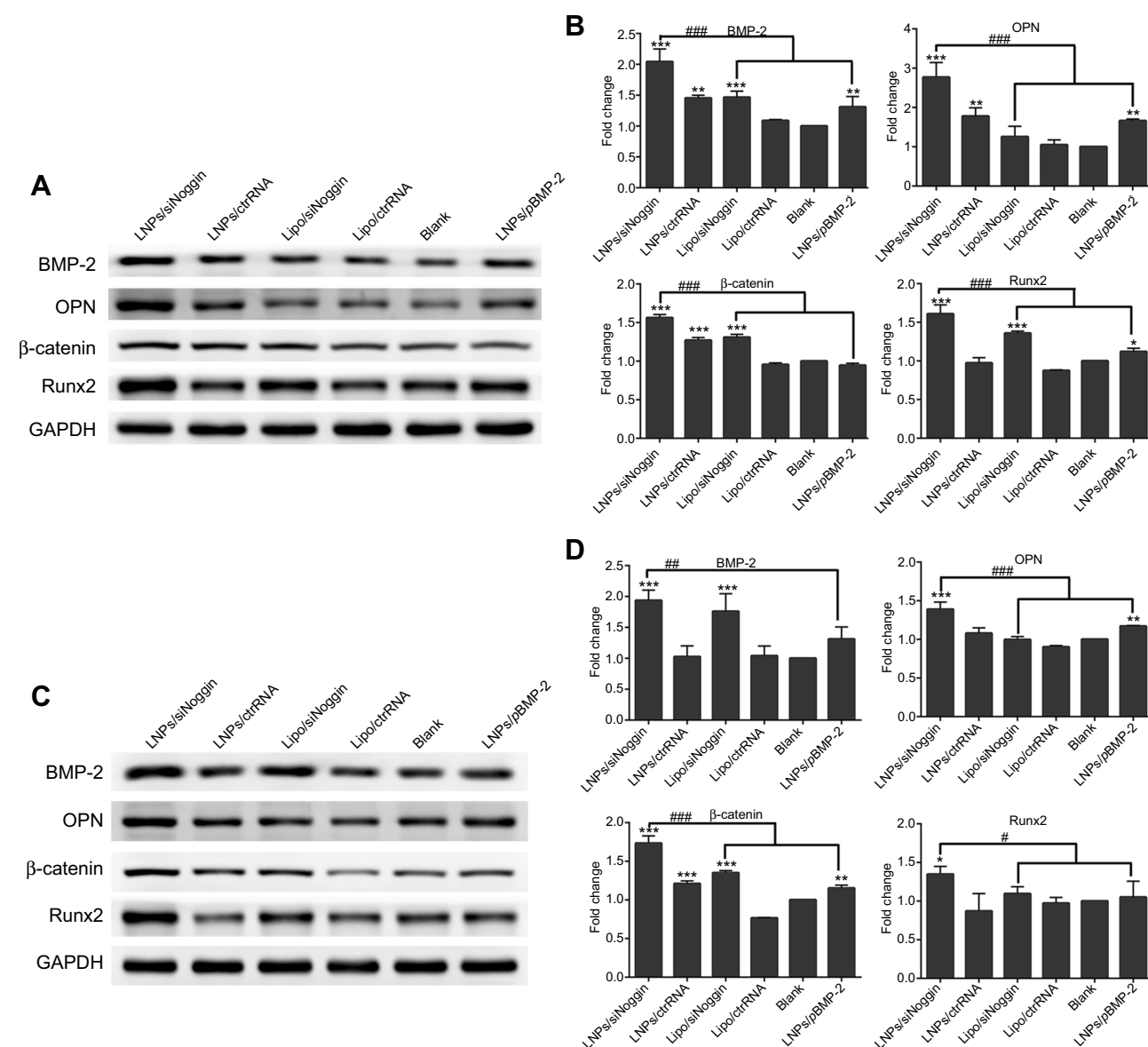


Figure 7 Effects of siNoggin and pBMP-2 treatment on expression of osteogenic-related proteins on day 3 (A, B) and 7 (C, D). (A, C) Representative Western blots of each protein. (B, D) Semiquantitative expression of BMP-2, OPN, β -catenin, and Runx2 proteins by ImageJ software.

Notes: * $P < 0.05$, ** $P < 0.01$ and *** $P < 0.001$ vs the blank group. # $P < 0.05$, ## $P < 0.01$ and ### $P < 0.001$. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

1.34-fold compared with that in untreated cells, but expression of these two proteins in LNPs/pBMP-2 and lipo/siNoggin groups was almost identical to that in untreated cells.

Taken together, during all stages of osteogenesis, in the case of osteogenesis-related protein expression, LNPs/siNoggin exhibited the strongest ability to promote osteogenic differentiation of MC3T3-E1 cells among LNPs/siNoggin, LNPs/pBMP-2, and lipo/siNoggin. At early and intermediate stages, lipo/siNoggin showed a stronger ability to promote

osteogenic differentiation than that by LNPs/pBMP-2. At the late stage of osteogenesis, lipo/siNoggin or LNPs/pBMP-2 contributed little to osteogenic differentiation, and their osteogenesis-related protein expression was almost identical to that in untreated cells. Therefore, we may conclude that LNPs are more efficient gene-delivery vectors compared with lipo, and that the negative regulation of suppressors via LNPs/siNoggin may be better in osteogenic differentiation than positive regulation of promoters via LNPs/pBMP-2.

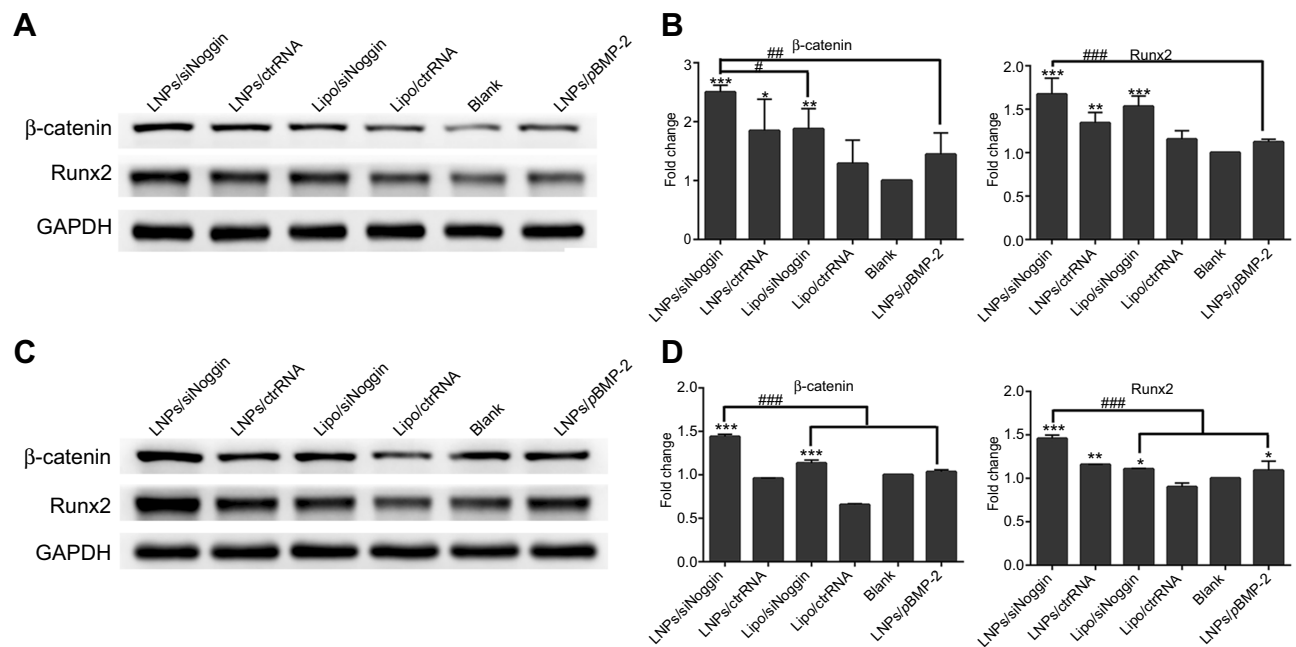


Figure 8 Effects of *siNoggin* and *pBMP-2* treatment on expression of osteogenic-related proteins on days 14 (**A, B**) and 21 (**C, D**). (**A, C**) Representative Western blots of each protein. (**B, D**) Semi-quantitative expression of β -catenin protein and Runx2 protein by ImageJ software. The error bars represent the mean \pm SD (n=3).

Notes: * $P < 0.05$, ** $P < 0.01$ and *** $P < 0.001$ vs the blank group. # $P < 0.05$, ## $P < 0.01$ and ### $P < 0.001$. The error bars represent the mean \pm SD (n=3).

Abbreviations: LNPs, lipopolymer-amine nanopolymerosomes; lipo, lipofectamine 3000.

Effects of LNPs/*siNoggin* on BMP/Smad and GSK-3 β / β -catenin signaling pathways

Noggin is an antagonist of BMP-2/4/5/6/7/13/14. BMP-2/4/6/7/14 has been demonstrated to enhance osteogenic differentiation and bone formation. Binding of *Noggin* to BMP-2/4/7/14 inhibits signaling pathways induced by BMPs through blockade of binding sites for the type-I and type-II receptors of BMPs.^{8,10,30,32} It is clear that the BMP/Smad signaling pathway is involved in osteogenic differentiation and bone formation upon *siNoggin* treatment, but whether other signaling pathways are involved is not clear.

Among signals stimulating bone formation, BMP/Smad and GSK-3 β / β -catenin signaling pathways are two of the most critical. In the BMP/Smad signaling pathway, BMPs bind to and activate receptors to phosphorylate Smad1/5/9 proteins, which further drives osteogenic differentiation. In the GSK-3 β / β -catenin signaling pathway, inhibition of GSK-3 β activity is a key step that protects β -catenin from degradation and leads to its accumulation in cytoplasm, and then β -catenin translocates to the nucleus to drive osteogenic differentiation.^{33,34} GSK-3 is a widely expressed and highly conserved serine/threonine protein kinase. It is encoded by two genes that generate two related proteins (GSK-3 α and GSK-3 β) and acts downstream of several essential osteogenesis-related signaling

pathways such as phosphatidylinositol 3' kinase (PI3K), Wnt/ β -catenin, Hedgehog, and Notch pathways. The mechanism of GSK-3 regulation is not fully understood, but it has been demonstrated that GSK-3 activity can be suppressed by: phosphorylation of GSK-3 β (p-GSK-3 β) induced by agonists (eg, neurotrophins, growth factors); formation of protein complexes of GSK-3 β induced by Wnt ligands; intracellular localization.³³

Therefore, we tested if LNPs/*siNoggin* treatment activated BMP/Smad and GSK-3 β / β -catenin signaling pathways by measuring their respective protein expression of Smad1/5/9 and p-Smad1/5/9, GSK-3 β , and p-GSK-3 β (Ser⁹) and β -catenin by Western blotting.

Compared with untreated cells, treatment of LNPs/*siNoggin*, lipo/*siNoggin*, or LNPs/*pBMP-2* up-regulated protein expression of p-Smad1/5/9 by 2.38-, 1.52-, and 1.05-fold, and of p-GSK-3 β (Ser⁹) by 2.53-, 2.26-, and 1.61-fold, respectively (Figure 9). Up-regulation of p-GSK-3 β further increased expression of β -catenin protein by 1.61-, 1.32-, and 0.95-fold in LNPs/*siNoggin*, lipo/*siNoggin*, and LNPs/*pBMP-2* groups, respectively (Figure 7). Finally, the osteogenic differentiation marked by ALP activity, mineralization, and the genes and proteins of osteogenic markers was enhanced (Figures 5–7). These results suggested that: *Noggin* suppression from

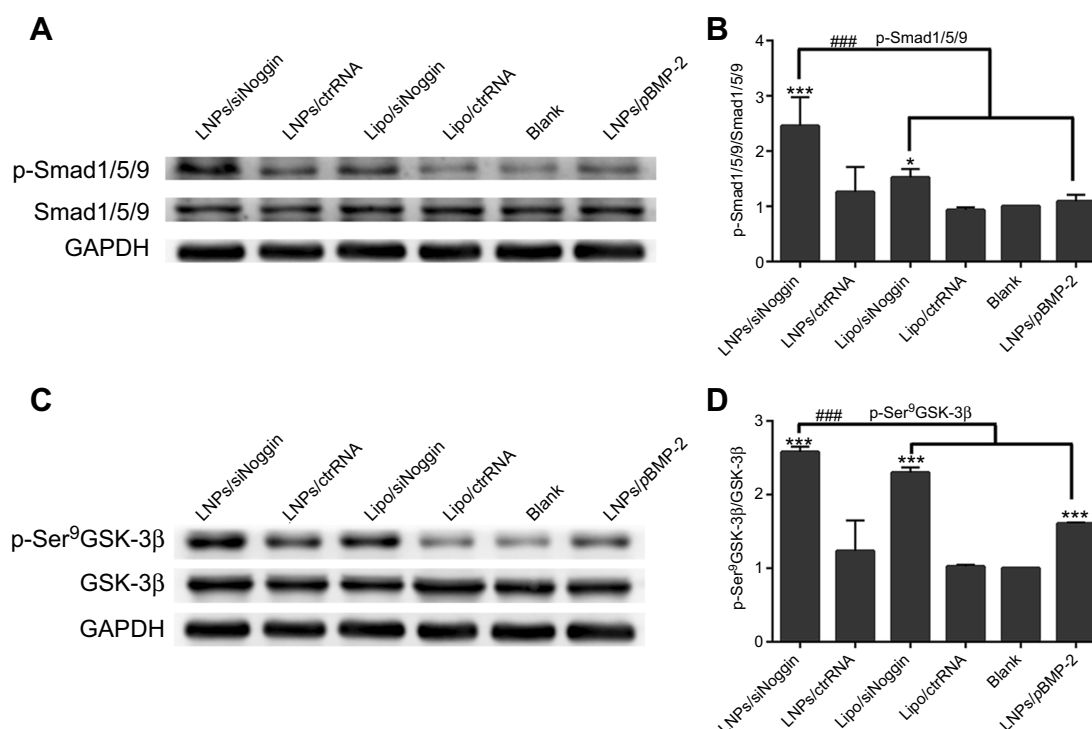


Figure 9 LNP/siNoggin promotes osteogenesis differentiation by activating BMP/Smad and GSK-3 β / β -catenin signaling pathways in MC3T3-E1 cells on day-3. **(A)** Effects on the expression of phosphor-Smad/1/5/9 proteins. **(C)** Effects on the expression of phosphor-GSK-3 β (Ser⁹) proteins by ImageJ software.

Notes: * $P < 0.05$, ** $P < 0.01$ and *** $P < 0.001$ vs the blank group. The error bars represent the mean \pm SD ($n = 3$).

Abbreviations: LNPs, lipopolymer-saccharide-amine nanopolymerosomes; lipo, lipofectamine3000.

siNoggin treatment promoted osteogenesis differentiation possibly by the BMP/Smad and GSK-3 β / β -catenin signaling pathways; LNPs may be more efficient gene-delivery vectors than lipo; *siNoggin* treatment may be more efficient for stimulating osteogenic differentiation than *pBMP-2* treatment via delivery of nonviral vectors. We obtained some evidence that *siNoggin* treatment affects the GSK-3 β / β -catenin signaling pathway. However, the detailed underlying molecular mechanisms (how the regulation of GSK-3 β activity is triggered, the ratio of phosphorylated and unphosphorylated β -catenin, and the concentration of unphosphorylated β -catenin in nuclei) were not revealed, but merit detailed study.

Discussion

Gene therapy based on RNA or DNA can offer a new, efficacious option for treatment of bone defects. Theoretically, osteogenesis can be enhanced through downregulation of negative (eg, by gene silencing) or upregulation of the positive (eg, by gene expression) regulators of osteogenic signaling. In osteogenic gene therapy, *BMP-2* (DNA) and *siNoggin* (siRNA) are used extensively alone or in combination, and have been

demonstrated to be potent in promoting osteogenesis in vitro or in vivo.^{1,5,6,8,16,20,35} The safety and efficacy of gene therapy are dependent largely on gene-delivery vectors, and an ideal gene-delivery vector has not been identified.

Therefore, the first goal of our work was to explore whether the LNPs, which were developed by our research team and have been shown to mediate the transient transfection of pDNA,^{26–29} were also good candidates for siRNA delivery. MC3T3-E1 cells were chosen as target cells for the study of transfection and osteogenic differentiation. MC3T3-E1 cells are clonal osteoblast-like cells from murine calvaria with distinct proliferative and differentiated stages in culture. They are a recognized in vitro model of osteoblast development due to their convenience and a developmental sequence similar to osteoblasts in bone tissue.³¹ Hence, MC3T3-E1 cells are used widely in the study of osteogenic differentiation.^{6,31,36,37}

LNPs could deliver *siNoggin* into MC3T3-E1 cells in the present study. Optimal transfection could be achieved at 3.35 μ g/mL of LNPs and 50 nM of siRNA with uptake efficiency of $\sim 98\%$ and minimal cytotoxicity. The latter was evidenced by the higher viability, similar morphology,

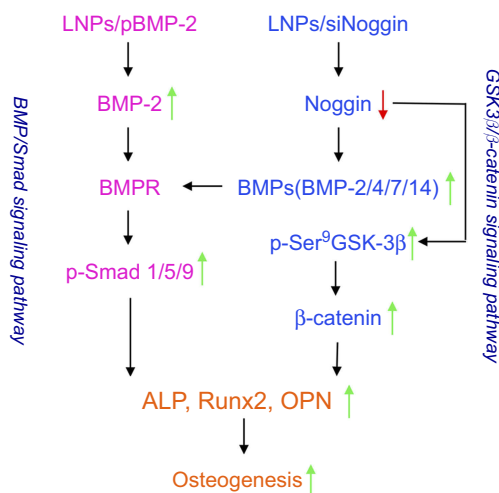
and enhanced proliferation of cells compared with those of the untreated cells (Figures 1 and 2). At this condition, delivery of LNPs/*siNoggin* into MC3T3-E1 cells led to a silencing efficiency of *Noggin* of 50% (Figure 3A). This value is not the highest among reported nonviral vectors, but is attractive because it is relatively higher than that for most reported nonviral vector systems and close to the viral vector system for *siNoggin* delivery. For example, for a viral vector delivery system, about 30–70% of gene knockdown can be achieved using lentiviral particles containing shRNA targeting *Noggin* to transduce adipose-derived mesenchymal stem cells (ASCs).^{30,38} For nonviral vector/*siNoggin* systems, the efficiency of gene knockdown is about 45–50% in ASCs using a vector of cationic sterosomes of stearylamine/cholesterol vesicles,¹⁷ ~25% in ASCs when using a vector of commercially available lipo 2000,¹⁷ ~25% in MC3T3-E1 cells when using a vector of lipo in the present study (Figure 3A), and <20% in human MSCs when using a vector of PEI.¹⁵ Recently, 68% of *Noggin* knockdown has been reported using a supramolecular vector comprising anionic fusogenic peptides and biocleavable cationic polyrotaxanes (GALA/DMAE-SS-PRX) to transfect MC3T3-E1 cells.⁶ Such high knockdown efficiency is attributed to the improved escape of siRNA polyplexes from endosomes/lysosomes whose membranes are destabilized by the protonation of fusogenic peptides at acidic pH. Also, in vitro osteogenic differentiation at intermediate and late development stages and in vivo efficacy of bone formation mediated by this vector have been postulated.

LNPs/siRNA had higher transfection efficiency compared with lipo/siRNA, which may be ascribed to their different delivery mechanisms. Lipo is thought to facilitate transfection in the early stages by mediating nucleic-acid condensation and nucleic acid-cell interactions (<https://www.thermofisher.com/cn/zh/home/references/gibco-cell-culture-basics/transfection-basics/gene-delivery-technologies/cationic-lipid-mediated-delivery/how-cationic-lipid-mediated-transfection-works.html>). With regard to LNPs, the natural merits of three blocks (PEI 1.8k, cholesteryl, OA) and the newly acquired properties of lipopolysaccharide-amine copolymer and formation of polymersomes overcome the barriers in different steps during cytosolic delivery, which has been explained in detail in our previous publications.^{26,28} For example, LNPs/siRNA can efficiently enter cells, which is attributed to synergistic facilitation of endocytosis via ionic attraction from cationic PEI blocks and a receptor-mediated

cholesterol-uptake pathway from the cholesteryl block. Then, LNPs/siRNA can escape efficiently from endosomes/lysosomes, which is ascribed to an increased membrane-disrupting ability of LNPs at an acidic pH of endosomes/lysosomes. That is, at an acidic pH, PEI and OA are protonated sufficiently, which induces a “proton sponge effect” (from PEI protonation) and enhances interactions between LNPs and endosomes/lysosomes membranes due to the increases in positive charge density (PEI protonation) and hydrophobicity (OA protonation).

Comparing vectors is difficult due to differences in the: cell types and their culture conditions, concentrations of nucleic acid and vectors; transfection timing; characterization methods; and way data are presented. For example, protein expression can be an absolute value from enzyme-linked immunosorbent assays or fold-change compared with the control from Western blots. Therefore, setting standards for evaluation of nucleic acid-based delivery therapy is important. Controllable expression of *Noggin* in a reasonable range is necessary for a good vector, and the final efficacy is the only “gold standard”. As such, for appropriate and controlled regeneration of bone, optimal expression of *Noggin* should be explored in efficacy experiments.

Based on the concepts mentioned above, after probing the knockdown efficiency of LNPs/*siNoggin*, we investigated the effects of LNPs/*siNoggin* on the expression of *Noggin* protein and osteogenic differentiation of MC3T3-E1 cells at different development stages. Suppression of *Noggin* led to reduced expression of *Noggin* protein. In the LNPs/*siNoggin* group, the expression of *Noggin* protein decreased by 40% compared with that in the blank, which was significantly lower than that in the lipo/*siNoggin* group (decreased by 20%) (Figure 3). Scholars have shown that a decrease in levels of endogenous *Noggin* up-regulates BMP activity and thereby affects BMP-driven actions such as osteogenic differentiation,^{8,15,17,18,30,39} and our results are consistent with those studies. In detail, LNPs/*siNoggin* stimulated ALP activity, increased expression of *Runx2* mRNA, and BMP-2 protein at an early stage, and enhanced expression of osteogenic proteins and mineralization of MC3T3-E1 cells significantly at the medium and late stages of cell differentiation (Figures 5–9). Taken together, these results suggest that LNPs are good nonviral vectors for *siNoggin* delivery, and that LNPs/*siNoggin* can promote osteogenic differentiation of MC3T3-E1 cells, thereby indicating their promising future in bone repair and regeneration.



Scheme 1 Possible signaling pathways and roles of LNPs/siNoggin and LNPs/pBMP-2 for osteogenesis.

After confirming that LNPs/siNoggin can promote osteogenic differentiation, we further tested the possible signaling pathways involved in siNoggin and pBMP-2 treatment (our second goal) (Scheme 1). For siNoggin treatment, it has been shown that the BMP/Smad signaling pathway is involved in osteogenic differentiation.^{10,11,30,32,38} However, other signaling pathways might be involved, and this hypothesis was confirmed by our results.

First, after LNPs/siNoggin treatment, expression of BMP-2 protein and phosphorylated Smad1/5/9 protein increased significantly (Figures 7–9) which, in turn, promoted the expression of Runx2 and protein (Figures 5, 7, and 8), key osteogenic transcription factors, and, finally, improved the osteogenic differentiation of MC3T3-E1 cells (as evidenced by an increase in ECM mineralization) (Figure 6). These results confirmed that the BMP/Smad signaling pathway played an important part in the osteogenic differentiation of LNPs/siNoggin-treated MC3T3-E1 cells. Second, LNPs/siNoggin treatment up-regulated protein expression of β-catenin, which can drive osteogenic differentiation, and β-catenin is also the key component in the canonical Wnt signaling pathway. In general, β-catenin

in expression can be regulated by GSK-3β in the cytoplasm. Hence, GSK-3β can drive the phosphorylation and degradation of β-catenin, and, conversely, suppression of GSK-3β activity leads to the β-catenin stabilization, and induces its accumulation in cytoplasm and translocation to the nucleus to drive osteogenic differentiation.³³ GSK-3β activity can be inhibited through phosphorylation induced by agonists (eg, neurotrophins, growth factors) or complex formation induced by Wnt ligands (canonical Wnt/β-

catenin signaling pathway). LNPs/siNoggin treatment enhanced phosphorylation of GSK-3β at Ser⁹ (Figure 9), and promoted intracellular accumulation of β-catenin (Figures 7, 8). However, β-catenin accumulation might have been caused by canonical Wnt pathways or other pathways, which merits further investigation. Taken together, LNPs/siNoggin promoted osteogenic differentiation, possibly by activating BMP/Smad and GSK-3β/β-catenin signaling pathways, but the detailed molecular mechanisms must be studied further. With respect to pBMP-2 treatment, the BMP/Smad signaling pathway has been demonstrated to be involved in osteogenic differentiation.¹² Our results are consistent with this observation, whereby LNPs/pBMP-2 treatment increased expression of pSmad1/5/9 and Runx2 slightly, but could not increase protein expression of β-catenin (0.946-fold, compared with untreated cells).

Our third goal was to compare the in vitro efficacy of pBMP-2 and siNoggin delivered by LNPs. BMP-2 is considered to be a powerful osteoinductive factor, and is approved for clinical application for bone-defect treatment. Noggin is a potent extracellular antagonist of BMPs encoded by *NOG*. Noggin is a secreted homodimeric glycoprotein with a molecular mass of 64 kDa. Through specific binding with BMPs to shield the binding sites for BMP receptors on cell surfaces, Noggin inhibits the action mediated by BMP-2, -4, -5, -7, -13, and -14, such as osteoblast differentiation.¹⁰ BMP-2 and siNoggin have been used extensively alone or in combination in large studies, but few scholars have compared their efficacy.

Clinical treatments must be safe and efficacious. Hence, comparison of the efficacy of BMP-2 and siNoggin delivered by nonviral vectors is needed to provide evidence for treating physicians and patients to make choices in bone-defect treatments. As expected, LNPs/siNoggin and LNPs/pBMP-2 enhanced osteogenic differentiation by increasing ALP activity, expression of osteogenesis-related gene/proteins, and ECM mineralization, but LNPs/siNoggin was more powerful than LNPs/pBMP-2 and, at a late stage of cell differentiation, LNPs/pBMP-2 could not enhance expression of Runx2 protein or β-catenin. These data suggest that regulation via LNPs/siNoggin may be a more effective way to enhance osteogenic differentiation than that via LNPs/pBMP-2.

Despite the fact that few studies have assessed the difference in the osteogenic efficacy between pBMP-2 and siNoggin delivered by the same nonviral vector, we found some clues to support this conjecture. For

example, Ramasubramanian et al¹⁹ reported that delivery of *pBMP-2* alone upregulated expression of osteogenic markers slightly in hADSCs, whereas co-delivery of *siNoggin* and *pBMP-2* (cells first treated by *siNoggin*/lipid and then *pBMP-2*/PBAE C32-122 polymer) accelerated their osteogenic differentiation significantly with a marked increase in bone-marker expression and ECM mineralization. The first reason for this difference in efficacy may be because *Noggin* binds and inactivates BMP-2/4/5/7/13/14.^{10–12} BMP-2/4/7/14 have been reported to induce osteogenic differentiation of MSCs, ADSCs, and MC3T3-E1 cells in vitro and in vivo.^{11,12,16} As a result, *Noggin* silencing leads to activation of other downstream pathways besides *BMP-2*, and their synergistic actions may be more beneficial to osteogenesis than the activation of *BMP-2* signaling alone induced by LNPs/*pBMP-2*. Protein expression of p-Smad1/5/9, p-GSK-3 β , Runx2 and β -catenin provide evidence of this hypothesis (Figure 9), which suggests that LNPs/*pBMP-2* treatment causes activation of the BMP/Smad signaling pathway, but LNPs/*siNoggin* treatment may (at least) activate BMP/Smad and GSK-3 β / β -catenin signaling pathways. The second reason may be the different mechanisms of action of siRNA and pDNA. pDNA delivery undergoes a longer path with more barriers than that of siRNA because the action site is in the cell nucleus for DNA and in the cytoplasm for siRNA. Also, production of the target protein via pDNA delivery can occur only in dividing cells, but suppression of the target protein via siRNA delivery can occur in dividing and non-dividing cells. In addition, unwanted genetic changes may occur due to integration of exogenous DNA sequences into host DNA.⁸ Also, *Noggin* knockdown can increase angiogenesis, which will further facilitate bone formation.⁴⁰

Collectively, for biomaterial-mediated delivery of nucleic acids, *siNoggin* therapy may be a more efficacious, safer, and easier alternative technology than *pBMP-2* therapy to regulate expression of the target protein for tissue regeneration. Further (especially efficacy verification in vivo) studies will be undertaken in the future.

Conclusions

We demonstrated that LNPs can deliver *siNoggin* into MC3T3-E1 cells efficiently to knock down *Noggin* in MC3T3-E1 cells with minimal cytotoxicity. This action significantly enhanced the expression of osteogenic markers and in vitro osteogenic differentiation, possibly through the

BMP/Smad and GSK-3 β / β -catenin signaling pathways. Compared with LNPs/*pBMP-2*, LNPs/*siNoggin* had better efficacy for osteogenic differentiation of MC3T3-E1 cells. Our results suggest that LNPs are efficient vectors for delivery of nucleic acids such as pDNA and siRNA. *siNoggin* delivery via nonviral vectors may be a more effective and alternative way to promote osteogenic differentiation than *pBMP-2* delivery. LNPs/*siNoggin* alone or in combination with other stimulators may have great potential in the repair and regeneration of bone.

Acknowledgments

This work was supported by the National Natural Science Foundation of China (No. 81571015 and No. 81371665), the Guangdong Science and Technology Project (2016A050502012), the Natural Science Foundation of Guangdong Province (2015A030313087), and the Guangzhou Science and Technology Plan Project (201707010011 and 201803010102).

Disclosure

The authors report no conflicts of interest in this work.

References

1. Kowalczycki CJ, Saul JM. Biomaterials for the delivery of growth factors and other therapeutic agents in tissue engineering approaches to bone regeneration. *Front Pharmacol*. 2018;9:513. doi:10.3389/fphar.2018.00513
2. Hak DJ, Fitzpatrick D, Bishop JA, et al. Delayed union and nonunions: epidemiology, clinical issues, and financial aspects. *Injury*. 2014;45 (Suppl 2):S3–S7. doi:10.1016/j.injury.2014.04.002
3. Haumer A, Bourguin PE, Occhetta P, et al. Delivery of cellular factors to regulate bone healing. *Adv Drug Deliv Rev*. 2018;129:285–294. doi:10.1016/j.addr.2018.01.010
4. Bai X, Gao M, Syed S, et al. Bioactive hydrogels for bone regeneration. *Bioact Mater*. 2018;3(4):401–417. doi:10.1016/j.bioactmat.2018.05.006
5. Hasan A, Byambaa B, Morshed M, et al. Advances in osteobiologic materials for bone substitutes. *J Tissue Eng Regen Med*. 2018;12 (6):1448–1468. doi:10.1002/term.2677
6. Inada T, Tamura A, Terauchi M, Yamaguchi S, Yui N. A silencing-mediated enhancement of osteogenic differentiation by supramolecular ternary siRNA polyplexes comprising biocleavable cationic polyrotaxanes and anionic fusogenic peptides. *Biomater Sci*. 2018;6(2):440–450. doi:10.1039/c8bm00675j
7. Liu H, Li D, Zhang Y, Li M. Inflammation, mesenchymal stem cells and bone regeneration. *Histochem Cell Biol*. 2018;149(4):393–404. doi:10.1007/s00418-018-1643-3
8. Nguyen MK, Jeon O, Dang PN, et al. RNA interfering molecule delivery from in situ forming biodegradable hydrogels for enhancement of bone formation in rat calvarial bone defects. *Acta Biomater*. 2018;75:105–114. doi:10.1016/j.actbio.2018.06.007
9. Tatiparti K, Sau S, Kashaw SK, Iyer AK. siRNA delivery strategies: a comprehensive review of recent developments. *Nanomaterials (Basel)*. 2017;7(4). doi:10.3390/nano7120458

10. Krause C, Guzman A, Knaus P, Noggin. *Int J Biochem Cell Biol*. 2011;43(4):478–481. doi:10.1016/j.biocel.2010.11.015
11. Pensak MJ, Lieberman JR. Gene therapy for bone regeneration. *Curr Pharm Des*. 2013;19(19):3466–3473. doi:10.2174/1381612811319190012
12. Zhang X, Guo J, Zhou Y, Wu G. The roles of bone morphogenetic proteins and their signaling in the osteogenesis of adipose-derived stem cells. *Tissue Eng Part B Rev*. 2014;20(1):84–92. doi:10.1089/ten.teb.2013.0204
13. Wagner DO, Sieber C, Bhushan R, et al. BMPs: from bone to body morphogenetic proteins. *Sci Signal*. 2010;3(107):mr1.
14. Molina CS, Stinner DJ, Obrensky WT. Treatment of traumatic segmental long-bone defects: a critical analysis review. *JBJS Rev*. 2014;2(4). doi:10.2106/JBJS.RVW.M.00062
15. Nguyen MK, Jeon O, Krebs MD, Schapira D, Alsberg E. Sustained localized presentation of RNA interfering molecules from in situ forming hydrogels to guide stem cell osteogenic differentiation. *Biomaterials*. 2014;35(24):6278–6286. doi:10.1016/j.biomaterials.2014.01.026
16. Carreira AC, Zambuzzi WF, Rossi MC, et al. Bone morphogenetic proteins: promising molecules for bone healing, bioengineering, and regenerative medicine. *Vitam Horm*. 2015;99:293–322.
17. Cui ZK, Fan J, Kim S, et al. Delivery of siRNA via cationic Sterosomes to enhance osteogenic differentiation of mesenchymal stem cells. *J Control Release*. 2015;217:42–52. doi:10.1016/j.jconrel.2015.08.031
18. Orciani M, Fini M, Di Primio R, Mattioli-Belmonte M. Biofabrication and bone tissue regeneration: cell source, approaches, and challenges. *Front Bioeng Biotechnol*. 2017;5:17. doi:10.3389/fbioe.2017.00017
19. Ramasubramanian A, Shiigi S, Lee GK, Yang F. Non-viral delivery of inductive and suppressive genes to adipose-derived stem cells for osteogenic differentiation. *Pharm Res*. 2011;28(6):1328–1337. doi:10.1007/s11095-011-0406-9
20. Zhou Z, Liu X, Zhu D, et al. Nonviral cancer gene therapy: delivery cascade and vector nanoproperty integration. *Adv Drug Deliv Rev*. 2017;115:115–154. doi:10.1016/j.addr.2017.07.021
21. Leong J, Teo JY, Aakalu VK, Yang YY, Kong H. Engineering polymersomes for diagnostics and therapy. *Adv Healthc Mater*. 2018;7(8):e1701276. doi:10.1002/adhm.201701276
22. Chidanguro T, Ghimire E, Liu CH, Simon YC. Polymersomes: breaking the glass ceiling? *Small*. 2018;14(46):e1802734. doi:10.1002/sml.v14.46
23. Shi Y, Jiang Y, Cao J, et al. Boosting RNAi therapy for orthotopic glioblastoma with nontoxic brain-targeting chimaeric polymersomes. *J Control Release*. 2018;292:163–171. doi:10.1016/j.jconrel.2018.10.034
24. Zou Y, Zheng M, Yang W, et al. Virus-mimicking chimaeric polymersomes boost targeted cancer siRNA therapy in vivo. *Adv Mater*. 2017;29(42). doi:10.1002/adma.201700681
25. Ge X, Zhang Q, Cai Y, et al. PEG-PCL-DEX polymersome-protamine vector as an efficient gene delivery system via PEG-guided self-assembly. *Nanomedicine (Lond)*. 2014;9(8):1193–1207. doi:10.2217/nnm.13.83
26. Huang Z, Teng W, Liu L, et al. Efficient cytosolic delivery mediated by polymersomes facilely prepared from a degradable, amphiphilic, and amphoteric copolymer. *Nanotechnology*. 2013;24(26):265104. doi:10.1088/0957-4484/24/26/265104
27. Guan Y, Wang Q, Cheng Y, Teng W, Huang H. Study on gene transfection in bone marrow mesenchymal stem cells mediated by plasmid of bone morphogenetic protein 2 loaded lipopolymer-saccharide-amine nanopolymerosomes. *Zhongguo Xiu Fu Chong Jian Wai Ke Za Zhi*. 2014;28(10):1292–1297.
28. Teng W, Huang Z, Chen Y, et al. pVEGF-loaded lipopolymer-saccharide-amine nanopolymerosomes for therapeutic angiogenesis. *Nanotechnology*. 2014;25(6):065702. doi:10.1088/0957-4484/25/6/065702
29. Wang Q, Chen Y, Wang L, et al. Stability and toxicity of empty or gene-loaded lipopolymer-saccharide-amine nanopolymerosomes. *Int J Nanomedicine*. 2015;10:597–608. doi:10.2147/IJN.S74156
30. Fan J, Im CS, Guo M, et al. Enhanced osteogenic differentiation of adipose-derived stem cells by regulating bone morphogenetic protein signaling antagonists and agonists. *Stem Cells Transl Med*. 2016;5(4):539–551. doi:10.5966/sctm.2015-0249
31. Quarles LD, Yohay DA, Lever LW, Caton R, Wenstrup RJ. Distinct proliferative and differentiated stages of murine MC3T3-E1 cells in culture: an in vitro model of osteoblast development. *J Bone Mineral Res*. 1992;7(6):683–692. doi:10.1002/jbmr.5650070613
32. Groppe J, Greenwald J, Wiater E, et al. Structural basis of BMP signalling inhibition by the cystine knot protein Noggin. *Nature*. 2002;420(6916):636–642. doi:10.1038/nature01131
33. Kaidanovich-Beilin O, Woodgett JR. GSK-3: functional insights from cell biology and animal models. *Front Mol Neurosci*. 2011;4:40. doi:10.3389/fnmol.2011.00040
34. Lin FX, Zheng GZ, Chang B, et al. Connexin 43 modulates osteogenic differentiation of bone marrow stromal cells through GSK-3 β /catenin signaling pathways. *Cell Physiol Biochem*. 2018;47(1):161–175. doi:10.1159/000491620
35. Shapiro G, Lieber R, Gazit D, Pelled G. Recent advances and future of gene therapy for bone regeneration. *Curr Osteoporos Rep*. 2018;16:504–511. doi:10.1007/s11914-018-0459-3
36. Casati L, Pagani F, Fibiani M, Lo Scalzo R, Sibilio V. Potential of delphinidin-3-rutinoside extracted from *Solanum melongena* L. as promoter of osteoblastic MC3T3-E1 function and antagonist of oxidative damage. *Eur J Nutr*. 2018. doi:10.1007/s00394-018-1618-0
37. Qing T, Mahmood M, Zheng Y, et al. A genomic characterization of the influence of silver nanoparticles on bone differentiation in MC3T3-E1 cells. *J Appl Toxicol*. 2018;38(2):172–179. doi:10.1002/jat.3528
38. Fan J, Park H, Tan S, Lee M. Enhanced osteogenesis of adipose derived stem cells with Noggin suppression and delivery of BMP-2. *PLoS One*. 2013;8(8):e72474. doi:10.1371/journal.pone.0072474
39. Fan J, Park H, Lee MK, et al. Adipose-derived stem cells and BMP-2 delivery in chitosan-based 3D constructs to enhance bone regeneration in a rat mandibular defect model. *Tissue Eng Part A*. 2014;20(15–16):2169–2179. doi:10.1089/ten.tea.2013.0523
40. Levi B, Nelson ER, Hyun JS, et al. Enhancement of human adipose-derived stromal cell angiogenesis through knockdown of a BMP-2 inhibitor. *Plast Reconstr Surg*. 2012;129(1):53–66. doi:10.1097/PRS.0b013e3182361ff5

Supplementary materials

Table S1 Primer sequences

Gene	5'-3' Sequence
<i>Noggin</i>	Forward-TGCTGTACGCGTGGAATGA Reverse-TGAGGTGCACAGACTTGGATG
<i>Runx2</i>	Forward-AAGTGTCTGTGGTCTCTGAGTTGA Reverse-GCTGTATGGTGAGGCTGGTAGG
<i>GAPDH</i>	Forward-AAGAAGGTGGTGAAGCAGG Reverse-GAAGGTGGAAGAGTGGGAGT

Cat No. of materials

MC3T3-E1 cell line (Cat No. CRL-2593)

Noggin siRNA (*siNoggin*) (Line 1 - Cat No. 10620318;
Line 2 - Cat No. 10620319)

Alexa Fluor[®] 555 siRNA (Cat No. 14750100)

Stealth[™] RNAi Negative Control Duplexes (ctrRNA)
(Cat No. 12935400)

lipofectamine3000 (lipo) (Cat No. L3000015)

Opti-MEM[™] I Reduced Serum Media (Cat No.
31985062)

trypsin (Cat No. 15050065)

Trizol (Cat No. 15596-026)

α -MEM (Cat No. C12571500bt)

Fetal Bovine Serum (FBS) (Cat No. 10099141)

Penicillin/Streptomycin (Cat No. 15140122)

pBMP-2 (Vector ID: VB160930-1048bkg)

osteogenic medium (Cat No. MUBMX-90021)

Alizarin Red (Cat No. Alizarin Red S)

Cell Counting Kit-8 (CCK-8) (Cat No. ck04)

BCA assay kit (Cat No. CW0014S)

alkaline phosphatase kit (Cat No. A059-2)

Cetylpyridinium chloride (Cat No. C9002-100G)

Prime Script[™] RT transcription kit (Cat No. RR036A)

LightCycler[®]480 SYBR Green I Master (Cat No.
4887352001-1)

Antibodies against mouse noggin (Cat No. NB110-
40413)

Antibodies against mouse BMP-2 (Cat No. ab214821),
OPN (Cat No. ab8448), Smad1/5/9 (Cat No. ab66737)

Antibodies against mouse β -catenin (Cat No. 8480),
Runx2 (Cat No. 12556), p-Smad1/5/9 (Cat No. 13820),
GSK-3 β (Cat No. 12456S), p-GSK-3 β (Ser⁹) (Cat No.
5558S) and GAPDH (Cat No. 2118)

The secondary antibody is Anti-rabbit IgG, HRP-linked
Antibody (Cat No. 7074S)

International Journal of Nanomedicine

Dovepress

Publish your work in this journal

The International Journal of Nanomedicine is an international, peer-reviewed journal focusing on the application of nanotechnology in diagnostics, therapeutics, and drug delivery systems throughout the biomedical field. This journal is indexed on PubMed Central, MedLine, CAS, SciSearch[®], Current Contents[®]/Clinical Medicine,

Journal Citation Reports/Science Edition, EMBASE, Scopus and the Elsevier Bibliographic databases. The manuscript management system is completely online and includes a very quick and fair peer-review system, which is all easy to use. Visit <http://www.dovepress.com/testimonials.php> to read real quotes from published authors.

Submit your manuscript here: <https://www.dovepress.com/international-journal-of-nanomedicine-journal>