The effect of implant placement torque on crestal bone remodeling after 1 year of loading

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Purpose: The aim of this study was to evaluate and compare crestal bone levels (CBLs) after 1 year of loading of self-tapping bone condensing implants placed with high insertion torque (IT) compared to those placed with lower IT.

Materials and methods: A retrospective chart review of 66 consecutive patients who received at least one self-tapping bone condensing implant and were in function for at least 1 year was conducted. On the basis of intrasurgical notes documenting the implant IT, the patient population was divided into group A (implant IT, >55 Ncm) and group B (IT, <55 Ncm). Radiographs taken immediately after insertion and during annual follow-up appointments were evaluated for detecting crestal bone loss. The relationship between IT and crestal bone loss, bone density, and jaw location were analyzed, and a P-value of 0.05 was considered to be statistically significant.

Results: A total of 113 self-tapping bone condensing NobelActive™ implants were placed. The average follow-up period from the placement of the implant restoration was 12.87 (±4.83) months. Six implants were classified as failures resulting in overall survival rate of 94.6%.

Implants in group A had a mean IT of 67.35 ± 4.0 Ncm, whereas implants in the group B had a mean IT of 37.9 ± 12.6 Ncm. Implants in group A had statistically significant crestal bone loss compared to implants in group B (0.95 ± 1.60 and 0.18 ± 0.68 mm, respectively). Group A implants placed in the mandible showed significantly more pronounced crestal bone loss (2.12 ± 1.99 mm) compared to those placed in the maxilla (0.25 ± 0.65 mm; P<0.05); however, this was not the case in group B implants.

Conclusion: Implants inserted with high IT (>55 Ncm) showed more peri-implant bone remodeling than implants inserted with a less assertive IT (<55 Ncm). Bone density and jaw location affect IT and CBLs.

Keywords: dental implant, nobelactive, insertion torque, torque, crestal bone level, marginal bone level

Introduction

Implant primary stability (PS) is defined as “the stability of the implant immediately post insertion”.¹ As it is related to implant micro motion, PS has been considered in the past to be an important prognostic factor for osseointegration and implant success.²

Implant insertion torque (IT) is frequently used as an indication of implant PS, and, although there is no consensus on what is considered the minimal torque needed for an implant to be successful, clinicians frequently use a torque value in the range of 20–40 Ncm.²³ Many factors can affect implant IT, for example, initial implant bone contact, bone quality at the osteotomy site,⁴ osteotomy preparation technique, and implant geometry/morphology.⁵

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The NobelActive™ Implant (Nobel Biocare USA, LLC, Yorba Linda, CA, USA) features a tapered body and a variable thread design with a high pitch and long wings that permit the implant to condense the surrounding bone during insertion. This potentially improves the implant stability and allows for higher IT to be reached. An average IT of 50 Ncm has been reported in the literature when the NobelActive system is used. This feature makes it ideal to use in the areas where implant stability can be challenging. The higher PS is especially beneficial when it is placed immediately in fresh extraction sockets or in the areas of soft (type IV) bone. Due to its bone condensing ability, the system seems to have an advantage in thin ridges where it minimizes the need for bone grafting.The ability to reach high IT makes it a suitable system for immediate or early loading protocols. However, some risks are involved when attempting to reach high IT as jaw fracture has been reported in dense (type I) bone or in thin ridges.

The effect of high IT on osseointegration and crestal bone levels (CBLs) has been a controversial dispute in the literature. Historically, excessive IT (>50 Ncm) has been assumed to compress the surrounding bone and reduce microcirculation. This may induce bone necrosis and therefore negatively affect the implant osseointegration. However, this concept has been challenged. Animal studies did not show a negative effect on osseointegration in high IT group (up to 150 Ncm), whereas human studies showed controversial results. A recent systematic review indicated that there is no significant difference in bone resorption and implant failure rate between implants placed with high IT (up to 176 Ncm) and low (30 Ncm). However, the authors reported that most studies have a high risk of bias. Recently, significant marginal bone loss and buccal soft tissue recession were reported in implants placed with high IT (>50 Ncm) compared to those placed with regular IT (<50 Ncm) at 1- and 3-year post-loading follow-up.

This study was conducted to evaluate and compare CBLs after 1 year of loading of self-tapping bone condensing NobelActive implants placed with high IT compared to those placed with lower IT. The null hypothesis is that IT does not affect the CBL at short-term follow-up.

Materials and methods

Study design

This study is a retrospective chart review of consecutive patients who received at least one NobelActive implant and treated by one of two experienced periodontists in a private practice setting. Human ethics approval was attained from the Clinical Research Ethics Board, University of British Columbia, Office of Research Services. All patients provided a written informed consent to review their medical records as per University of British Columbia policy. The inclusion criteria for the study were as follows: patients who received at least one NobelActive implant that had been in function for an average post-loading period of 12 months and availability of post-loading radiographic and clinical follow-up assessments with radiographs depicting implants in their entirety with clearly discernible threads, thus making them radiographically diagnostic.

The implants were placed in partially dentate and edentulous sites of the maxilla and mandible, in either native bone or at sites augmented previously or simultaneously with bone grafting. Implants were immediately placed in fresh extraction sockets or in native bone and were restored with immediate or delayed loading protocols.

Surgical protocol

All procedures were done under local anesthesia. All surgeries were done under antibiotic prophylaxis with 2 g amoxicillin (or 600 mg clindamycin in penicillin-allergic patients). Postoperatively, patients took 500 mg amoxicillin (or 300 mg clindamycin) three times daily for 7 days. Patients were asked to rinse with 0.2% chlorhexidine gluconate mouthwash for 1 minute pre-operatively and then twice a day for up to 2 weeks post-operatively. Appropriate pain medication was prescribed after the implant installation surgery. All procedures were done following the NobelActive original procedural protocol, which advocated the placement to 70 Ncm. A surgical guide was used to prosthetically determine the implant position. Patients were seen at 10–14 days post-operatively for a follow-up and suture removal. All patients were referred to the restorative dentist for final restoration(s), unless immediate loading was performed in which case the restorative clinician was present during the surgery. Patients were recalled at regular intervals for periodontal and implant maintenance.

Data collection

Patient charts were audited for patients’ demographic data and smoking and medical history. Intra-surgical notes documenting implant width, length, location, IT, and bone density were recorded. The IT was measured using the NobelActive hand torque wrench instrument from the NobelActive surgery kit (Figure 1). Implants were divided into two groups based on the IT value: group A with IT >55 Ncm and group B with IT ≤55 Ncm. Bone density was recorded as soft, medium, and
dense. Dense bone corresponded to type I bone and soft bone correspond to type IV. Medium bone density corresponded to type II and III, which are difficult to differentiate clinically.7

Procedural information regarding the timing of implant placement (in extraction socket or healed ridges), the need for bone augmentation (simultaneous with implant placement or staged), and loading protocol (immediate loading or delayed) were collected.

Intraoral radiographs taken at implant placement and during follow-up appointments were scanned and measured by Romexis 2.2.7R Software System (Planmeca, Helsinki, Finland). The coronal margin of the implant collar and the most coronal aspect of the bone-to-implant contact were used as reference points for the linear measurements of marginal bone loss. Known implant lengths were used for the calibration of the measurements. Measurements of the mesial and distal CBLs adjacent to each implant were performed. The amount of true bone resorption and the difference between the initial bone level and the bone level at follow-up examinations were calculated (Figure 2). For those implants placed intentionally in a supra-crestal position, the height of the implant collar above the alveolar crest during placement was subtracted from follow-up radiographs. The mesial, distal, average, and worst marginal bone loss values were recorded for each implant. One examiner who was not involved in the treatment of patients evaluated all intraoral radiographs. Intra-examiner reliability was assessed in the sample of 25 randomly selected periapical radiographs that were measured twice, once at baseline and again after 4 months. The two recordings were highly correlated with a Pearson correlation coefficient of 0.981 (P = 0.000) and 0.994 (P = 0.000) at the mesial and distal measurements, respectively.

Statistical analysis was completed using the PASW statistics program (version 18.0, PASW, Chicago, IL, USA). Descriptive statistics were used for all evaluated parameters, and baseline patient and implant characteristics were summarized in terms of frequencies and percentages. Implant taper and crestal bone remodeling

Figure 1 The NobelActive™ implant features tapered body and accentuated threads/wings.

Notes: (A) The osteotomy site is slightly underprepared, which allows for the surrounding bone to be compressed laterally during implant insertion. (B) The manual torque wrench for NobelActive system allows controlled measurement of insertion torque up to 70 Ncm.

Figure 2 Example of measurements taken to estimate the crestal bone level.

Notes: The coronal margin of the implant collar and the most coronal aspect of the bone-to-implant contact were used as reference points for the linear measurements of crestal bone loss. The known implant length was used to compensate for radiograph magnification or angulation. Measurements were done on the mesial and distal aspects.
IT, jaw location, and CBL were compared by independent t-test. One-way ANOVA was used to compare bone density, implant IT, and CBL. The P-value of 0.05 was considered to be statistically significant.

## Results

A total of 66 patients (31 females and 35 males) were included in the study. The average age of patients at the time of implant placement was 56.31 (±16.20) years. A total of 10 subjects reported to be smokers. The demographic data are shown in Table 1.

Most subjects (62%) received one implant; 21% received two implants, 9% received three implants, and 6% received more than three implants. A total of 113 NobleActive implants were placed. Group A had 51 implants, whereas group B had 62 implants.

Guided bone regeneration (GBR) or sinus augmentation was performed prior to the placement of 12 implants (10.6%). Average healing period of sites was 7.2 months (5–9 months) prior to implant placement. Simultaneous GBR or sinus augmentation was performed in 45 of the 113 implants (39.8%). The most common bone graft material used was Bio-Oss® (Geistlich Pharma North America Inc., Princeton, NJ, USA), which is used in 41% (n = 23) of sites, followed by Puros® Allograft (Zimmer Biomet, Warsaw, IN, USA) in 30% (n = 17) of the sites and DynaBlast™ (Citagenix, Laval, QC, Canada) in 10.7% of sites (n = 6).

A one-stage implant protocol was employed for 63.7% (n = 72) of implants and a two-stage protocol for 36.3% (n = 41) of the implants. Of the evaluated implants, 34.5% were placed immediately into extraction sockets, while implants that were immediately loaded had a mean IT of 54.4 ± 14.2 Ncm. Implants that were both immediately placed and loaded had a mean IT of 58.3 ± 13.5 Ncm. (Table 1)

### Implant survival rates

A total of 113 implants were placed. Six implants were classified as failures (5.4%) due to implant mobility, progressive bone loss, or infection. The overall survival rate was 94.6%.

Two failures in group A occurred after 3 and 5 months of implant placement. The four failures in group B occurred between 1 and 11 months after implant placement. None of the subjects who experienced failure were smokers. Five of the six failures occurred prior to implant restoration and one failure occurred 11 months after immediate loading. Description of failures is presented in Table 2. This resulted in survival rates of 96% and 93.5% in group A and group B, respectively.

<table>
<thead>
<tr>
<th>Site</th>
<th>Torque (Ncm)</th>
<th>Smoking status</th>
<th>Time from placement to removal (months)</th>
<th>Bone augmentation</th>
<th>Placement</th>
<th>Immediate loading</th>
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<td>Simultaneous with implant placement</td>
<td>Conventional</td>
<td>Conventional</td>
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<tr>
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<td>Conventional</td>
</tr>
<tr>
<td>#25</td>
<td>20</td>
<td>No</td>
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<td>Simultaneous with implant placement</td>
<td>Immediate</td>
<td>Conventional</td>
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<tr>
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<td>Prior to implant placement</td>
<td>Conventional</td>
<td>Conventional</td>
</tr>
<tr>
<td>#44</td>
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<td>No</td>
<td>11</td>
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</tr>
<tr>
<td>#22</td>
<td>40</td>
<td>No</td>
<td>5</td>
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</table>
Mean crestal bone loss
The average follow-up period from the placement of the implant restoration was 12.87 (±4.83) months with the range of 4–27 months.

A total of 79.6% of the implants placed during the study period had crestal bone loss of <1.0 mm, 2.65% had crestal bone loss of 1–2 mm, 8% had crestal bone loss of 2–4 mm, and 4.4% had crestal bone loss of >4 mm.

The mean mesial crestal bone loss (±SD) was 0.52 (±1.28) mm with a minimum of 0 mm and a maximum of 6.1 mm. The mean distal crestal bone loss (±SD) was 0.54 (±1.33) mm with a minimum of 0 mm and a maximum of 5.2 mm. Since the mean mesial and distal crestal bone loss measurements were highly correlated (Pearson correlation coefficient = 0.643, P = 0.000), the average mean crestal bone loss (0.53 ± 1.25 mm) was used for subsequent statistical analysis (minimum, 0 mm; maximum, 5.6 mm; Figures 3 and 4).

IT and bone loss
Implants in group A had an average crestal bone loss of 0.95 ± 1.60 mm, whereas implants in group B had an average bone loss of 0.18 ± 0.68 mm. A statistically significant impact of torque on crestal bone loss was observed (P = 0.001).

IT was highly correlated with bone density (P = 0.000). The mean torque was 65.0 ± 9.7 Ncm in dense bone, 47.8 ± 16.6 Ncm in medium bone, and 47.9 ± 19.6 Ncm in soft bone. More specifically, an analysis with multiple comparisons revealed a significant difference in torque values between dense and medium bone (P = 0.000) and dense and soft bone (P = 0.007).

Mean marginal bone loss (±SD) was 1.25 (±1.70) mm for dense bone, 0.44 (±1.12) mm for medium bone, and 0.86 (±0.65) mm for soft bone. There was a statistically significant effect of bone density on mean marginal bone loss (P = 0.004). Post-hoc Tukey honest significant difference test showed a statistically significant difference between dense bone and medium bone (P = 0.01) and between dense bone and soft bone (P = 0.004). However, the difference between medium and soft bone was not statistically significant (P = 0.45).

Group A included 32 (62.7%) implants placed in the maxilla and 19 implants (37%) placed in the mandible. Group B included 53 implants (85%) that were placed in the maxilla, while the remaining implants (n = 9) were inserted in the mandible.

In group A, the average IT was 66 and 70 Ncm in the maxilla and mandible, respectively. The average bone loss was 0.25 (±0.68) mm in the maxilla and 2.12 (±1.99) mm in the mandible. Greater bone loss was present in the mandible than in the maxilla, and this finding was statistically significant (P = 0.00).

In group B, the average IT was 36 and 47 Ncm in the maxilla and mandible, respectively. The average bone loss was 0.19 (±0.65) mm in the maxilla and 0.15 (±0.82) mm in the mandible. However, this difference was not statistically significant (P = 0.10).
Discussion
This study compared the changes in CBL of self-tapping bone condensing implants placed with high IT (>55 Ncm) and regular IT (<55 Ncm) after 1 year of function. Moreover, the effect of bone quality and jaw location on IT and crestal bone loss was assessed.

The cumulative survival rate of the implants in this study was 94.6% with an average mean bone loss after 1 year of function of 0.53 ± 1.25 mm. This is comparable to marginal bone loss measurements reported by short-term reports. Also, the average marginal bone loss reported in this study was within the acceptable threshold recommended by Albrektsson and Zarb for rough surface implants.

The main outcomes of this study showed that NobelActive implants placed with high IT had an average crestal bone loss of 0.95 ± 1.60 mm, and this was significantly more pronounced when compared to crestal bone loss of implants placed with regular IT (0.18 ± 0.68 mm). Frequently, implants placed in the mandible have a higher IT compared to the maxilla (70 vs 66 Ncm in group A and 47 vs 36 Ncm in group B). The 1-year follow-up showed significantly increased crestal bone loss in implants placed in the mandible in group A (high IT) compared to the implants placed in the maxilla. This difference was not detected between the mandible and maxilla in group B (regular IT) implants. High IT was consistently achieved in dense bone compared to soft or medium bone, and subsequently, more pronounced crestal bone loss was detected in implants placed in dense bone.

Those results are consistent with the recent work of Marconcini et al in which implants placed with high IT (>50 Ncm) exhibited invariably significant crestal bone loss and soft tissue recession compared to implants placed with regular IT at 3-year follow-up. A similar trend was detected in the earlier follow-up of the same group of implants at 1 and 2 years. Similar to our findings, more crestal bone loss was detected in implants placed in the mandible compared to the maxilla with the average mandibular crestal bone loss in the high IT group being 1.23 ± 0.36 mm compared to 0.88 ± 0.43 mm in the maxilla. It is interesting that in our study, the difference between jaw location was not detected in group B (regular IT). This could be attributed to the small number of mandibular implants in this group. It could also indicate that lower IT values do not lead to the pronounced crestal bone loss in a dense bone environment (typical for the mandible).

A recent systematic review concluded that IT does not have a detrimental effect on crestal bone loss or implant failure. The review included only four human studies that specifically addressed CBL changes in relation to IT. Two of the studies included did not have a proper randomization to their subjects and therefore selection bias could affect their results. In addition, the studies had a wide range of IT (25–176 Ncm), and there was no consensus on what was considered a high IT. Therefore, no agreement was reached on what is considered a proper IT value or on the threshold of IT that could eventually lead to bone resorption.

Many studies confirmed the relationship between bone quality and IT. In our study, there was a consistently high IT in dense bone compared to soft bone. This was reflected in CBL changes as implants placed in dense bone had significant crestal bone loss compared to those placed in medium or soft bone.

NobelActive implants have a geometrical structure that allows them to achieve a higher IT and PS. IT s of >40 Ncm have routinely been reported in the literature with this system, which is advantageous in areas where implant stability is challenging. In comparison with other implants systems, NobelActive drilling protocol creates an osteotomy site that is slightly underprepared, ie, smaller than the planned implant size. This allows the bone to be compressed laterally during implant insertion and therefore generates a higher IT. This is a similar concept to the use of osteotome to condense bone suggested by Summers. Another feature of this implant system is its ability to reach a higher IT without the risk of damaging the internal hex connection or inducing pressure necrosis. However, insertion of the implant should be performed slowly especially in the areas of dense bone, with frequent reversing to allow the cutting of bone trabeculae and reducing the insertion pressure to avoid surgical complication like bone fracture or crestal bone loss.

There are several limitations to this study. The retrospective nature affects the homogeneity of the sample, and every effort was done to keep the procedure and the documentation consistent, but there was no calibration among the surgeons, and clinical judgment was used for the best of the patient, which may affect the results. Other limitations include the small population, lack of comparison group, and the short-term follow-up, which make the detection of correlations between contributing factors and failure rates difficult. More studies with larger sample size and longer follow-up are needed.

Conclusion
The findings of this study showed that the self-tapping bone condensing NobelActive implants inserted with high IT (>55 Ncm) result in statistically significant more crestal bone loss after 1 year of loading compared to those inserted with a lower IT. Moreover, more pronounced bone loss was detected in the
mandible when the IT was high. Although clinical outcomes for the NobelActive implant system are favorable compared to other clinically validated implant systems, clinical judgment is still needed to prevent overcompression of the surrounding bone especially in the areas of high bone density to avoid short-term unfavorable effects on CBLs.

**Author contributions**

SA: data acquisition, analysis and interpretation, manuscript writing, and available literature review. AD: data acquisition and analysis. TI: study design and revising the manuscript critically for important intellectual content. All authors contributed toward data analysis, drafting and revising the paper and agree to be accountable for all aspects of the work.

**Disclosure**

The authors report no conflicts of interest in this work.

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