The development of a reference database with the Topcon 3D OCT-1 Maestro

Introduction

Since its introduction in 1991, optical coherence tomography (OCT) has become the reference standard imaging device for evaluating retinal and optic nerve disorders. It uses low-coherence interferometry to generate in vivo, cross-sectional images of ocular tissues. Over the last 2 decades, technology has evolved to produce the spectral domain OCT (SD-OCT) with rapid image acquisition rate and high-resolution axial images of the retina and optic nerve. Thus, SD-OCT is commonly used in the monitoring of glaucoma and diabetic macula edema.

Topcon 3D OCT-1 Maestro is a noncontact SD-OCT system introduced in 2013. The instrument operates a fully automated “alignment, focus and capture” procedure, and captures 50,000 axial scans per second. The device simultaneously captures the macula and incorporates the Creative Commons Attribution – Non Commercial (unported, v3.0) License (http://creativecommons.org/licenses/by-nc/3.0). By accessing the work you hereby accept the Terms. Non-commercial use of the work is permitted without any further permission from Dove Medical Press Limited, provided the work is properly attributed. For permission for commercial use of this work, please see paragraphs 42 and 5 of our Terms (https://www.dovepress.com/terms.php).
and optic nerve head areas, giving both a digital fundus image and a 12×9 mm automated segmentation OCT scan (“wide scan” setting). The device also has the option for separate 6×6 mm optic disc and macula scans. It produces a 20 μm lateral and 6 μm axial resolution (Topcon; http://www.topconmedical.com/products/3doct1maestro-literature.htm).

One of the goals of ophthalmic imaging is to assist clinicians to discriminate between normality and pathology. In order to provide quantitative metrics for clinicians to determine retinal pathologies, we conducted a multicenter prospective study within the USA (ClinicalTrial.gov Identifier: NCT02447120) to collect OCT data of healthy eyes for the estimations of normal variation limits for various retinal and optic disc measurements using the Topcon 3D OCT-1 Maestro. The reference limits were estimated using non-crossing quantile regressions and 1st, 5th, 50th, 95th, and 99th percentiles were reported.

**Methods**

The study was conducted at 7 investigational sites in the USA and was performed in accordance with Good Clinical Practices (as described by the International Conference on Harmonisation), the Code of Federal Regulations, the ethical principles in the Declaration of Helsinki, Health Insurance Portability and Accountability Act regulations, and other applicable local regulations. The study was registered at the US National Institutes of Health (ClinicalTrials.gov Identifier: NCT02447120). Between May and October 2015, 504 participants were enrolled. Institutional Review Board approval was provided by IntegReview IRB (Austin, TX, USA) for the following sites: Illinois College of Optometry, Marshall B. Ketchum University, State University of New York College of Optometry, Western University, and Valley Eye Care Center Medical Associates. Local IRB was used for the University of Alabama School of Optometry and New York Harbor Health Care System sites. All subjects, at all sites, provided written informed consent before the performance of any study procedure. Subjects were eligible for the study if both eyes were free of eye disease, with an intraocular pressure of ≤21 mmHg bilaterally and a best-corrected visual acuity of 20/40 or better in each eye. All subjects underwent Humphrey Field Analyzer (HFA; Carl Zeiss Meditech, Inc., Dublin, CA, USA) testing using the Swedish Interactive Threshold Algorithm (SITA) 24-2 test strategy. Subjects were excluded if they exhibited a field defect or if they had unreliable test result, (defined as fixation losses >20%, or false positives >33%, or false negatives >33%). Subjects were also excluded if they were unable to tolerate ophthalmic imaging; had media opacities that inhibited OCT imaging; showed the presence of any ocular pathology except for cataract; had narrow angles on gonioscopy; had a history of leukemia, dementia, or multiple sclerosis; or were concomitantly using hydroxychloroquine and chloroquine. All ocular examinations to determine participant eligibility were performed within 2 calendar months of the scan acquisitions, and where possible, all OCT scans were performed in a single session.

One eye of each study participant was randomly selected and scanned with the 3D OCT-1 Maestro (firmware version 1.27). A minimum of 9 scans were obtained under 3 different settings: 3 wide scans (12×9 mm), 3 disc scans (6×6 mm), and 3 macula scans (6×6 mm). Additional scans were taken at the operator’s discretion if image quality was unacceptable. All study scans that were deemed acceptable by the clinical site operator were saved.

Clinical sites were also allowed to make manual adjustments to correct automatic segmentation errors such as grid locations, boundary segmentations, and/or disc margin with Fastmap (version 8.27). Such modifications were performed only at the clinical sites by qualified investigators within the purview of typical clinical use. All manual adjustments were electronically documented. The fovea modification corresponded to relocation of the Early Treatment Diabetic Retinopathy Study (ETDRS) and Macula 6 grid center location, while the disc margin and disc center modifications corresponded to adjustments of the disc outline and location, respectively. The remaining modifications involved segmentation adjustments between boundaries. The scan adjustment rates were between 1% and 8%. The scan adjustment rates with respect to macula measurements ranged between 1% and 3%, and the adjustment rates with respect to optic disc and circum-papillary measurements fell within the 6%–8% range.

OCT data were then exported to Topcon Reading Center (Oakland, NJ, USA), where image quality was checked by individuals with experience in OCT imaging. Scan exclusion criteria included image quality score, presence of eye blinks, eye motion, clipping, local weak signal, and feature centration. All scan exclusions were documented. No manual adjustments were made in the Topcon Reading Center. Approximately 1,200 scans were captured per scan mode (all subjects combined). Scan exclusion rates were 3% for wide scans, 3% for disc scans, and 2% for macula scans. All scans deemed acceptable by Topcon Reading Center qualified for data analysis.

**Measurement endpoints**

Measurement endpoints by scan patterns are listed below:

Macular full retinal thickness (FRT, Figure 1): ETDRS grid was placed automatically at the foveal center and sectors...
measured as per ETDRS chart specifications;\textsuperscript{11} central fovea, superior, nasal, inferior, and temporal inner quadrants (parafoveal); superior, nasal, inferior, and temporal outer quadrants (peri-foveal), measured with 12×9 wide and 6×6 macula modes; FRT consisted the distance between the inner limiting membrane (ILM) and the outer segments/retinal pigment epithelium junction boundary (Figure 1), the 2 green boundaries. An average value over the entire sector was reported.

Macular ganglion cell + inner plexiform layer thickness (GCL + IPL, Figure 1): The Macula 6 sector circle was placed automatically at the foveal center (Figure 1). The center 1 mm region was excluded from measurement. Superior, superior nasal, superior temporal, inferior, inferior nasal, inferior temporal, and average thickness were measured with 12×9 wide and 6×6 macula modes; GCL + IPL thickness included the distance labeled in Figure 1 (regions between 2 green boundaries). An average value of the entire sector was reported.

Macular ganglion cell complex (GCC, Figure 1): GCC measurement was performed with the same Macula 6 sector circle as GCL + IPL measurements. Superior, superior nasal, superior temporal, inferior, inferior nasal, inferior temporal, and average thickness were measured with 12×9 wide and 6×6 macula modes; GCC thickness consisted of the regions labeled in Figure 1, which consisted of regions between the ILM (blue) and the green boundary vitreal to inner nuclear layer. An average value of the entire sector was reported.

Circumpapillary retinal nerve fiber layer (cpRNFL) thickness: 3.4 mm diameter temporal-superior-nasal-inferior-temporal (TSNIT) circle was placed automatically at the optic disc center (Figure 1). Average RNFL thickness over TSNIT circle; 4 quadrants and 12 clock-hour sectors around TSNIT circle; measured with 12×9 wide and 6×6 disc modes; RNFL thickness consisted of regions labeled in Figure 1 (between 2 green boundaries). Average values of each sector (excluding the optic disc contour and cyan circle) were reported.

Optic disc measurements: Optic disc contour was automatically detected (Figure 1, cyan circle). Disc area, cup area, rim area, cup/disc (C/D) vertical diameter, C/D area, cup volume and rim volume were measured with 12×9 wide and 6×6 disc modes. Optic disc measurements were based on optic disc contour; an example is shown in Figure 1.

Data analysis
For each scan mode, the first acceptable scan by chronological order from each subject and scan mode was included in the analysis. The 99 percentiles (the 1st to the 99th) of each parameter were estimated by a simultaneous estimation of 99 non-crossing quantile regressions.\textsuperscript{12} Age was the regression covariate used in reference limits estimation for macula FRT, GCL + IPL, and GCC, whereas age and disc area were used as the regression covariates for RNFL thickness and
optic disc parameters.\textsuperscript{13–17} Estimation of the non-crossing quantile regressions was performed using an R program provided by Bondell (available at http://www4.stat.ncsu.edu/~bondell/Software/NoCross/NoCrossQuant.R). The 1st, 5th, 50th (median), 95th, and 99th percentile results were reported.

The sample size was based on the nonparametric 95% CI for the percentiles of the scan parameters without any covariate adjustments. The goal was to find a minimum sample size such that the nonparametric 95% CI for the 1st and the 5th percentiles did not overlap. For a sample size of 315 eyes, the nonparametric 95% CI values are \((X_{.01}, X_{.05})\) and \((X_{.95}, X_{.99})\) for the 1st and the 5th percentiles, respectively, where \(X_k\) is the \(k\)th smallest value in a sample of 315 measurements without ties.\textsuperscript{18} Therefore, at least 315 evaluable eyes were needed to achieve the sample size goal. A study eye was evaluable if the subject met all eligibility criteria and had at least 1 acceptable scan. The final sample size was increased by about 10\% of the minimum number of evaluable eyes to 350 evaluable eyes to ensure that all scan parameters would have at least 315 eyes for analysis. Assuming 30\% of the subjects would not meet eligibility criteria, the study planned to enroll 500 subjects.

**Results**

Five hundred and four subjects were screened for the study. One hundred and two did not meet the eligibility criteria and were excluded from imaging. Reasons for screen failure included visual fields with an apparent defect or artifact per study criteria \((n=26)\), unreliable HFA visual field \((n=26)\), and other ocular pathology/presence of eye disease \((n=33)\). Some subjects failed multiple eligibility criteria. Two subjects who met the eligibility criteria did not have acceptable scans and 1 subject with unknown eligibility status did not have any scans. Therefore, 399 eyes of the 504 enrolled subjects were included in the analysis.

The mean (SD) age was 46.3 (16.3) years (ranged 18–88 years). The most prominent age group was 18–30 years (22\%) followed by 51–60 years (20\%). Fifty-seven percent \((n=226)\) of the subjects were female and 18\% \((n=71)\) of the subjects were Hispanic or Latino. Fifty-nine percent of the subject were Caucasians, followed by Black/African American (20\%), Asian (13\%), Native American/Pacific Islander (2\%), and American Indian/Alaskan Native (1\%); 6\% reported their race as “other”.

The study eyes had a mean sphere of \(-1.441\) diopters \((D)\) \pm 2.537 \((ranged -12.5D to 4.0D), a cylinder of 0.565D \pm 0.691 \((ranged 0–5.0D), and a manifest refractive spherical equivalent of \(-1.159\)D \pm 2.418 \((ranged -11.00 to 4.50D).

Subjects had at least 3 acceptable scans per scan mode. Images were reviewed for acceptability prior to calculating results. The first accepted scan of each scan parameter in each scan mode from each eligible subject was included in the analysis. Scan rejection rates ranged from 2\% to 5\%. Specifically, the scan rejection rates were 2\%–4\% with respect to macula measurements and 4\%–5\% with respect to optic disc and circumpapillary measurements.

**Macular FRT**

Summary statistic of foveal FRT measured with 2 scan modes are shown in Table 1. Four patients were excluded from this analysis, as all their macula scans were determined to be unacceptable; thus, 395 of 399 subjects were included. The 1st, 5th, 50th, 95th, and 99th percentiles of foveal FRT by age are shown in Figure 2. The median intercepts and
coefficients were highly similar between 12×9 wide and 6×6 macula scan modes. Overall, there was a reduction in FRT with age in the outer ETDRS quadrants.

**GCL + IPL thickness**

The 1st, 5th, 95th, and 99th percentiles of average macula GCL + IPL thickness are shown in Figure 2. The median intercepts and coefficients were highly similar between 12×9 wide and 6×6 macula scan modes, and overall, there was a reduction in GCL + IPL thickness with age.

**GCC thickness**

Summary statistics of average GCC thickness with 2 scan modes are shown in Table 1. The disc areas ranged from 1.25 to 3.97 mm² (2.26±0.41 mm², mean±SD) for 12×9 wide scan and 1.03–3.85 mm² (2.10±0.41 mm²) for 6×6 disc scan. The median intercepts and slopes were highly similar between 12×9 wide and 6×6 disc scan modes. Age had little or no effect, whereas disc area showed large degree of influence on the cpRNFL thickness (Figure 3A). Reference limits of the circle profile around the perimeter of the 3.4 mm TNSIT circle is shown in Figure 3B.

**Optic disc parameters**

Summary statistics of disc area, cup area, rim area, cup volume, and rim volume with both 12×9 wide and 6×6 disc scan modes are reported in Table 1. Age and disc area were the covariates used in the quartile regression analyses. Overall, optic disc parameters increased with disc area, except rim volume, and the effect of aging was not significant.

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**Figure 2** Quantile regression fits of various macula measurements from 12×9 wide and 6×6 macula scans are shown.

**Notes:** Age did not have a significant effect on FRT near the foveal center (top row). There were negative associations of age with macula GCL + IPL thickness and GCC thickness (middle and bottom rows). The 1st (red line), 5th (green line), 50th (yellow line), 95th (blue line), and 99th (cyan line) percentiles were estimated by non-crossing quantile regressions based on the data displayed in the scatter plots.

**Abbreviations:** FRT, full retinal thickness; GCC, ganglion cell complex; GCL, ganglion cell; IPL, inner plexiform layer.
Discussion

The purpose of this paper was to report the normal reference limits for macula, optic nerve, and nerve fiber layer thickness measurements from Topcon 3D OCT-1 Maestro. The measurements included various parameters of full retinal thickness, RNFL thickness, ganglion cell layer plus the IPL layer thickness, ganglion cell complex, and the optic disc for healthy eyes. Across all parameters, the measurements obtained by the 12×9 wide, the 6×6 macula, and 6×6 disc scan modes were generally similar.

FRT measurements were consistent with reported OCT measured thickness ranges for healthy eyes.19–21 We found a negative association between peri-foveal (outer retinal) thickness with age, but there were no significant age associations with central foveal or inner ETDRS quadrants. There are conflicting reports in the literature regarding whether retinal thickness, as measured with digital imaging techniques, decreases with age. Some authors found no association between overall macula thickness and age.19–21 However, like us, others have found a decreased FRT in both the inner and outer quadrants with age.23–26 Histological studies suggest that retinal thickness reduces with age, but that the changes in the foveal region are much less than those in the outer retinal areas.27 As with others’ reports, we recommend that due to differences in image acquisition and processing methods, imaging devices should not be interchanged when evaluating retinal thickness measurements.21–28
Our reported reference values for ganglion cell and inner limiting plexiform layer thickness were thinner than those reported by others using the Cirrus SD-OCT, but similar to measurements found using swept source OCT. Furthermore, we found a thicker GCC average measurement than previous reports. Differences may be primarily due to size and location of grid sectors used by the different devices, and add further evidence that imaging devices should not be interchanged when monitoring ophthalmic disease in an individual. We found that both the GCL + IPL thickness and GCC thickness decreased with advancing age, which is consistent with some published data, but not with other published data. An age-related reduction in the ganglion cell layer has been noted in histological studies; thus, it might be expected that in vivo imaging of the area in a wide age range would show similar findings. In addition to age-related trends in loss of tissue, individual variation in the location of the major RNFL arcuates (since the GCC includes the nerve fiber layer, the ganglion cell layer, and the inner plexiform layer) is also likely factoring in our results.

cpRNFL thickness parameters included average, superior quadrant, nasal quadrant, inferior quadrant, temporal quadrant, and 12 clock-hour sections around the TSNIT circle. Overall, the measurements were consistent with those in the literature, although there is some variation in the values reported by different devices. Some sectors showed the trend of cpRNFL thickness decreasing with age, which can be explained by 2 competing factors: a neuronal tissue loss and a non-neuronal tissue gain that typically occurs to a smaller extent. However, our data showed that disc area had a more profound effect on cpRNFL thickness. This is mainly due to the following reasons:

1. The measurement region was a circle with a fixed diameter of 3.4 mm centering at the geographical center of the optic disc. As it has been proposed in previous studies, there could be greater amount of retinal neural fibers present with eyes having large optic disc, or it could be an artifact with fixed diameter scans.

2. Individual variation in the location of blood vessels and RNFL arcuates could contribute to variations in RNFL layer segmentations. To encompasses individual variations, the 3D OCT-1 Maestro’s cpRNFL reference variation limits were estimated based on the influence of both age and disc area.

In summary, the measurements and trends observed for the various parameters were largely consistent with those in the literature. Thus, the measurements presented in this report can be considered as a reference database for the measurements of healthy eyes. This study collected measurements of healthy eyes for full retinal thickness, RNFL thickness, ganglion cell layer plus the IPL layer thickness, GCC, and the optic disc in addition to small and large super pixel grid and TSNIT circle profile measurements. The reference limits at the 1st, 5th, 95th, and 99th percentile points establish thresholds to provide for the quantitative comparison of the RNFL, optic nerve head, and the macula in the human retina to a database of known healthy eyes. Consistent with the device’s proposed indications for use, this quantitative comparison can aid in the diagnosis, documentation, and management of ocular health and diseases in the adult population.

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Disclosure

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References