

Nanomedicine applications in women's health: state of the art

Oliver Lloyd-Parry
Charlotte Downing
Eisa Aleisaei
Celine Jones
Kevin Coward

Nuffield Department of Obstetrics
and Gynaecology, University of
Oxford, John Radcliffe Hospital,
Headington, Oxford, UK

Abstract: State-of-the-art applications of nanomedicine have the potential to revolutionize the diagnosis, prevention, and treatment of a range of conditions and diseases affecting women's health. In this review, we provide a synopsis of potential applications of nanomedicine in some of the most dominant fields of women's health: mental health, sexual health, reproductive medicine, oncology, menopause-related conditions and dementia. We explore published studies arising from in vitro and in vivo experiments, and clinical trials where available, to reveal novel and highly promising therapeutic applications of nanomedicine in these fields. For the first time, we summarize the growing body of evidence relating to the use of nanomaterials as experimental tools for the detection, prevention, and treatment of significant diseases and conditions across the life course of a cisgender woman, from puberty to menopause; revealing the far-reaching and desirable theoretical impact of nanomedicine across different medical disciplines. We also present an overview of potential concerns regarding the therapeutic applications of nanomedicine and the factors currently restricting the growth of applied nanomedicine.

Keywords: nanomedicine, mental health, sexual health, reproductive medicine, oncology, menopause, dementia

Introduction

Nanomedicine is the application of nanotechnology in the field of medicine with a view to enhancing the diagnosis and treatment of various diseases. Nanotechnology is already involved in a range of biomedical applications including drug and vaccine delivery, diagnostic imaging, nanosensor diagnostics, nano-enabled therapies, and tissue engineering.¹⁻³ Across the UK and the European Union, a growing recognition of the specific health care requirements of women has resulted in the proposed organizational changes in the provision of health care, focusing predominantly on a life course approach to women's health care.⁴⁻⁷ However, the predictable long-term health care needs of women demand greater biomedical and translational research to develop the diagnostic tools and treatments necessary to improve the care and well-being of women. Although cancer has been the predominant focus of research in the field of nanomedicine,⁸ there is an increasing awareness and exploration of the potential application of nanomedicine to noncancerous pathologies. As our understanding of the benefits of nanomaterial-based agents and diagnostics continues to grow in terms of selectivity, sensitivity, affinity, and detection limits, there is a widespread anticipation that nanotechnology will play an increasing role in women's health.^{1,9-18} This review explores the selection of potential nanomedicine applications in women's health, from puberty to menopause in cisgender women, including mental, sexual, reproductive, cancer, and menopause-related health care (Figure 1; Tables 1 and 2). We also address

Correspondence: Kevin Coward
Nuffield Department of Women's
and Reproductive Health, Level 3,
Women's Centre, John Radcliffe Hospital,
Headington, Oxford OX3 9DU, UK
Tel +44 1865 951 030
Email kevin.coward@obs-gyn.ox.ac.uk

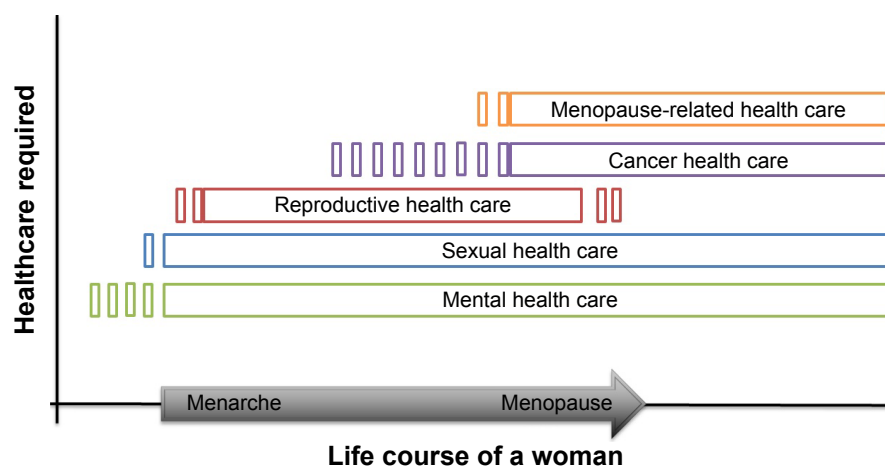


Figure 1 A representative graph showing the significant and predictable health care needs across the life course of a woman.

how this exciting technology might be deployed in early-onset dementia health care. These disciplines align directly to the key components of the World Health Organization's "Top Ten Issues for Women's Health." Specifically, we highlight the potential of nanomedicine to revolutionize health care throughout the life course of women and discuss the challenges that might restrict the widespread application of these nanotechnologies to clinical medicine.

Table 1 The applications of nanoparticles in women's health care: mental health and sexual health care trials and clinical studies

Sector	Specialty	Application	References
Mental health care	Therapeutics	Enhanced drug delivery and release mechanisms	Ashok et al, ⁴⁰ Leyva-Gómez et al, ⁴¹ Kim et al, ⁴² Jana et al, ⁴³ Zhou et al, ⁴⁷ Shah et al ⁴⁸
		Increasing bioavailability of drugs	Gao et al, ⁵² Yan et al ⁵³
Sexual health care	Fertility	Alternative drug delivery systems	Huang et al, ⁵⁷ Wei et al, ⁵⁸ Grabrucker et al ⁵⁹
		Nanoparticles with antifertility capability	Gaurav et al, ⁶¹ Liu et al, ⁶² Jha et al, ⁶⁶ Marfatia et al ⁷⁰
	Sexually transmitted diseases	Prevention of infection	Fayaz et al, ⁷¹ Caron et al, ⁸¹ Kovarova et al ⁸²
		Detection of infection	Lee et al, ⁸³ Singh et al, ⁹⁵ Singh et al, ⁹⁶ Yang et al, ¹⁰⁵ Tang et al, ¹⁰⁶ Beeghly-Fadiel et al ¹¹⁹
		Treatment of infection	Rauta et al, ⁹⁷ Mishra et al, ¹⁰¹
		Vaccination/immunity against infection	Fairley et al, ⁹⁸ Dixit et al, ⁹⁹ Cambridge et al, ¹⁰⁰ Yilma et al, ¹⁰² Liu et al, ⁹⁴ Villa et al ⁸⁷

Table 2 The applications of nanoparticles in women's health care: reproductive health care, cancer, and menopause care trials and clinical studies

Sector	Specialty	Application	References
Reproductive health care	Endometriosis	Imaging of endometriosis	Hue et al, ¹¹⁰ Zhang et al ¹¹¹
		Delivering gene therapies to target tissues	Zhao et al, ¹¹² Chaudhury et al ¹¹³
		Uterine fibroids	Targeting delivery of antitumor drugs
Cancer health care	Tumor imaging	Magnetic resonance imaging (MRI)	Zhang et al, ¹²⁵ Yang et al ²¹³
		Computed tomography (CT)	Zhou et al ¹²⁶
	Cancer screening	Detection of malignant cells in tissue samples	Liu et al, ¹³⁰ Jo et al, ¹³² Palantavida et al ¹²⁹
Menopause-related health care	Therapeutics	Receptor specific targeting	Zhang et al, ¹⁴² Yu et al, ¹⁵⁶ Yang et al ¹⁵⁰
		Sensitization of malignant cells	Yang et al, ¹²¹ Liang et al ¹⁴³
			Manipulation of cellular pathways
	Overcoming drug resistance	Peetla et al, ¹⁴⁶ Roberts et al, ¹⁴⁷ Wang and Jia ¹⁴⁹	
		Declining estrogen	Improvements for hormone therapy
	Osteoporosis	Manipulation of osteogenesis activity	Hwang et al, ¹⁷⁸ Psarros et al ¹⁷⁹
		Bone-specific drug delivery	Khajuria et al ¹⁷⁶
Cardiovascular disease		Reduction of LDL levels	Xiao et al ¹⁸³
		Targeting atherosclerotic growth/inflammation	Chono et al, ¹⁸¹ Chnari et al, ¹⁸² Winter et al ¹⁸⁴

Mental health care

Mental health is a significant and growing issue in women's health. Analysis of the four Adult Psychiatric Morbidity Surveys published since 1993 has demonstrated the growing burden of common mental health disorders in women's health care and revealed a gender gap in common mental health disorders.¹⁹ Analysis of these surveys indicated that in England, 20.7% of women had a common mental health disorder, a figure which was 7.5% higher than that in men. Furthermore, since 2000, the prevalence of common mental health disorders in women has continued to increase, yet has remained stable, for the most part, in men. Although women are found to be more likely to receive treatment than men, the antidepressants commonly used in the treatment of common mental health disorders such as anxiety and depression are not consistently efficacious.

An individual's gender has been identified as a factor affecting treatment response.²⁰ Studies in mice have shown that greater neuronal activation arises in response to an acute citalopram injection in male mice, than in female mice or gonadectomized male mice, suggesting the possible influence of gonadal hormones upon the complex interactions between serotonin and neural circuits that mediate the hypothalamic–pituitary–adrenal stress axis.²¹ It was proposed that the regulation of androgens might dampen and modulate the activation of the stress pathway, which could contribute to the greater vulnerability of women to stress-related affective disorders. In light of the possible inherent gender gap in common mental health disorders, it is vital that efforts are made to increase the efficacy of the existing pharmacological treatments to improve the well-being of women. Both pharmacological and neurobiological factors have been implicated in antidepressant resistance.²²

The function of the blood–brain barrier is believed to be a significant factor affecting antidepressant resistance.²³ The blood–brain barrier contributes to brain homeostasis and features drug efflux transporters of the ATP-binding cassette gene family including P-glycoprotein (P-gp).²⁴ Many antidepressants are substrates of P-gp and therefore exhibit reduced penetration into the brain.²² Although not all antidepressants are subject to the same degree of limitation to brain penetration by P-gp *in vivo*,^{25–28} several single-nucleotide polymorphisms of the *ABCB1* gene have been linked to reduced levels of clinical response to antidepressants,^{29–33} and a poorer tolerance profile.^{34–36} However, several studies have failed to reproduce these results.^{37–39} The proposed involvement of P-gp in antidepressant resistance indicates

that P-gp may be systematically targeted and inhibited by particular drug delivery systems, enabling more of the drug to cross the blood–brain barrier, thus establishing greater concentrations at the site of action.¹⁴

Serotonin–norepinephrine reuptake inhibitors (SNRIs) and selective serotonin reuptake inhibitors (SSRIs), in addition to the other commonly prescribed benzodiazepine class of anxiolytics, are orally administered in the majority of cases of common mental health disorders. Therefore, these drugs are also limited by factors such as low drug aqueous solubility, food–drug interactions, high hepatic first-pass metabolism effects, and short half-lives. In addition, poor compliance is a common cause of anxiolytic resistance in all three classes. Promising *in vitro* and *in vivo* studies offer the hope that nanomedicine could overcome many of these causes of low bioavailability and drug resistance.¹⁴

The initial studies involving benzodiazepine drug nanocarriers have been positive. Lipid-based micelles have proved to be successful at improving the aqueous solubility of diazepam *in vitro* by 2.3- to 6-fold. Furthermore, solid lipid nanoparticles (NPs) carrying clonazepam demonstrate enhanced blood–brain barrier permeability and efficacy at lower doses than required by the pure form of the drug revealing their potential as oral delivery systems for drugs with poor water solubility.^{14,40,41} In addition, *in vivo*, clonazepam-loaded polymeric NPs demonstrated sustained drug release exceeding 80 hours in the presence of the enzyme dextranase, subject to the pH of the release medium being appropriate, and alprazolam-loaded polymeric NPs have also demonstrated sustained drug release over a 24-hour period *in vitro*.^{42,43} Moreover, liposomes have been utilized *in vivo* to encapsulate midazolam, successfully increasing the oral bioavailability of the drug by 3.6-fold relative to the pure form of the drug.^{14,44} These examples provide clear evidence of the potential of nanoscale drug delivery systems to improve the physicochemical properties of benzodiazepine drugs, ultimately increasing the fraction of the orally administered drugs that reach the systemic circulation. They also suggest the possibility of benzodiazepine depots, which could maintain a constant drug concentration for a prolonged and predetermined period of time with minimum side effects, offering hope for the safer prescription of drugs with improved patient compliance.

Other studies that have been conducted in nanocarriers loaded with SNRIs and SSRIs have proved similarly promising results. Solid lipid NPs carrying duloxetine HCl have demonstrated excellent stability in acidic media and enhanced

pharmacodynamic properties *in vivo*. Likewise, duloxetine HCl-loaded mesoporous silica NPs exhibited sustained drug release during *in vitro* studies.^{45,46} Furthermore, solid lipid NPs carrying venlafaxine showed a 1.45-fold increase in oral bioavailability relative to the pure drug. The drug concentrations in the brain were also increased significantly when administered through the solid lipid nanocarrier, suggesting a reduction in P-gp-mediated efflux of the drug.^{14,47} Moreover, venlafaxine hydrochloride (VHL)-loaded chitosan NPs have shown steady release *in vitro*, and VHL-loaded dendrimers demonstrated sustained drug release *in vitro*.^{48,49} Studies of fluoxetine HCl cocrystals, fluoxetine HCl with benzoic, succinic, and fumaric acid cocrystal formers in the same crystal lattice, further revealed that the solubility of the cocrystal formers determined the aqueous solubility of the cocrystals. This has the potential to inform the development of optimal cocrystal engineering for maximal bioavailability in future.^{14,50} As with the benzodiazepine class of drugs described in the preceding paragraph, this initial preclinical evidence indicates that SNRIs and SSRIs may benefit from nanoscale drug delivery systems that can provide opportunities for enhanced oral bioavailability and the development of drug depots. In addition, these studies demonstrate that greater concentrations of SSRIs and SNRIs may be established in the brain by reducing P-gp-mediated efflux and by preventing the upregulation of P-gp expression through the use of drug delivery systems.

Nanomedicine also offers significant potential to improve the efficacy of alternative and novel therapies, administration techniques, and augmentation strategies. For example, solid lipid NPs were successfully demonstrated to increase the bioavailability of buspirone HCl by 2.35-fold. This phenomenon was attributed to reduced hepatic first-pass metabolism, which may ultimately enhance the efficacy and diminish the inter-individual variability associated with this novel anxiolytic which is sometimes used to augment antidepressants.^{14,51} In addition, *in vitro* studies of amitriptyline HCl nanocrystals suggested that the development of nanocrystals may offer a means to increase the rate and extent of drug dissolution.^{14,52} Although tricyclic antidepressants such as amitriptyline HCl have been largely superseded by SNRIs and SSRIs, this study demonstrated the potential of nanocrystals to enhance the physiochemical properties of the drug for application in suitable, antidepressant-resistant, patients. Furthermore, agomelatine cocrystals enhanced aqueous solubility by up to 4.7-fold relative to the pure form of the drug, which is a novel melatonergic antidepressant with a favorable side effect profile relative to the more commonly used antidepressants.^{14,53}

A study conducted on the antidepressant effects of the curcumin/solid lipid NP dexanabinol (Cur/SLNs-HU-211) dual-drug NPs for the treatment of major depression utilized corticosterone-induced cellular and animal models of major depression.⁵⁴ Cur/SLNs-HU-211 showed superior antidepressant activity compared to HU-211, Cur, and Cur/SLNs *in vitro* and *in vivo*.⁵⁴ Although curcumin remains a controversial and poorly researched alternative form of therapy, this study is suggestive of the potential of nanomedicine to overcome pitfalls that can curtail experimental leads for novel antidepressants; in the case of curcumin, potentially improving the normally unstable, reactive, and non-bioavailable compound. A superior antidepressant-like effect of trefoil factor 3 (TFF3) loaded into negatively charged liposomes was observed in animal models of depression. These findings indicated the potential of developing TFF3 liposomes as a potential antidepressant drug for acute systemic administration. In this way, the neuropeptide TFF3 may be enhanced by nanomedicine to potentially improve the efficacy of clinically used antidepressants.⁵⁵ Moreover, cRGD-modified liposomes produced a heightened antidepressant response of TFF3 by increasing the brain distribution of TFF3. It is now necessary to conduct further research on the efficacy and safety of using cyclic Arg-Gly-Asp (cRGD) coupled with liposomes as a drug delivery system targeted at the brain. This may enable exploration of the potential use of cRGDL-TFF3 for the treatment of common mental health disorders.⁵⁶

Nanomedicine may also contribute to improving alternative drug administration methods. An animal study highlighted the potential of micro-emulsions to be utilized as a drug delivery system for the transdermal administration of citalopram. This study indicated that a formulation, containing 3% citalopram within an application area of 3.46 cm², was capable of reaching the minimum effective therapeutic concentration with no significant local side effects.⁵⁷ In addition, curcumin didecanoate CurDD nanosuspensions have been proposed as an alternative long-acting intramuscular injectable antidepressant through the sustained delivery of curcumin.⁵⁸

In another study, novel biodegradable NPs, composed of poly-lactide-co-glycolide (PLGA) conjugated with glycopeptides, were shown to be capable of crossing the blood-brain barrier and were able to deliver Zn²⁺ ions, which may permit their application in the augmentation of antidepressant treatments.⁵⁹

In summary, the clinical application of nanocarrier systems in mental health remains a speculative, but tantalizing, possibility at this time. The studies presented here illustrate the

positive theoretical impact of their translation into clinical medicine. Nanomedicine may offer the potential to improve the efficacy of conventional pharmaceuticals that are currently limited by antidepressant resistance, by enhancing the bioavailability and pharmacokinetics, as well as facilitating antidepressant augmentation. Furthermore, it may facilitate the development of novel therapies for use in the treatment of common mental health disorders. In addition, it may improve the range of drug administration methods available to clinicians and enable the implementation of long-acting drug depots to reduce patient noncompliance. Further investigation is required before clinical investigation and translation is possible, but this may ultimately prove to be productive in addressing the significant burden of mental health.

Sexual health care

Statistics on Sexual and Reproductive Health (SRH) services in England (2015/2016) revealed that 7% of the resident population of women aged between 13 and 54 years had contacted the SRH services at least once. Furthermore, 19% of women aged between 18 and 19 years had accessed the SRH service at least once.⁶⁰ This seems to indicate that effective SRH services might have a significant impact on their health care experience.

Nanomedicine has the potential to offer improvements in reproductive choice and contraceptive safety, and thus provide additional benefit to the well-being of women. For example, copper–curcumin– β -cyclodextrin (Cu–Cur)CD nano-inclusion complexes have demonstrated significant spermicidal effects *in vitro*. Safety and toxicity results were also favorable, suggesting that this complex could be potentially used as a topical vaginal contraceptive.⁶¹ This type of topical vaginal contraceptive could be implemented as a short-term, nonsteroidal contraceptive measure. However, initial investigations into the potential application of nanomedicine in long-acting reversible birth control are arguably more exciting.

Copper/low-density polyethylene nanocomposite has been shown to have potential for use in intrauterine devices with antifertility effectiveness demonstrated in rats, together with high contraceptive efficacy and fewer clinical side effects compared to other copper intrauterine devices in humans.^{62,63} In addition to improving the existing contraceptive measures such as intrauterine devices, nanomedicine may also enable the development of novel longer-acting contraceptive options. For example, a polymeric NP formulation of follicle-stimulating hormone (FSH)-receptor binding inhibitor-8, purified from human ovarian follicular fluid,

has demonstrated antifertility activity when studied *in vivo* in marmosets. *In vitro*, sustained release of FSH-receptor binding inhibitor-8 was exhibited for 21 days.⁶⁴

Reversible sterilization is an attractive long-term contraceptive option, and early developments have been significantly aided by the use of nanomedicine. Gonadotropin-releasing hormone (GnRH)-conjugated chitosan may represent a promising carrier for the targeted delivery of DNA to GnRH-expressing cells, which could be used to implement noninvasive sterilization by means of gene silencing.⁶⁵ Another means of reversible sterilization, smart reversible inhibition of sperm under guidance (Smart RISUG) utilizes nano- to micro-sized magnetic particles in the iron oxide–copper–styrene maleic anhydride–dimethyl sulfoxide contraceptive drug. Drug–sperm interactions are mediated by the presence of a pulsed magnetic field to facilitate better spermicidal action and control of distribution inside either male or female reproductive tubes. Smart RISUG is of significant interest because it is long acting, yet readily reversible.⁶⁶ The application of RISUG in men offers the hope of greater shared contraceptive responsibility. RISUG is a promising male contraceptive and has already reached Phase III clinical trial stage.^{67–69}

Using nanotechnology to improve and redevelop the existing barrier contraceptives, such as condoms, could have a positive impact on efficacy. For example, graphene and nano-lubricated condoms could offer greater protection for sexual partners.⁷⁰ The inactivation of microbial infectiousness by silver NP-coated polyurethane condoms has also been demonstrated.⁷¹

Although RISUG and nanotechnology-enhanced condoms can provide some level of antimicrobial protection, additional vaccinations, diagnostic tests, and antimicrobial drugs are necessary to prevent and treat sexually transmitted infections.^{70–72}

In 2016, women represented 32% of patients receiving care for human immunodeficiency virus (HIV) in England, thus demonstrating the significant impact of HIV on women's health.⁷³ Although combination antiretroviral therapy has helped to improve the morbidity and mortality of patients infected with this virus, the presence of the virus persists in reservoir organs and treatment remains limited by drug–drug interactions, side effects, and noncompliance.⁷⁴ Nanomedicine can aid the provision of such treatment by capitalizing on the ability of nanomedicines to overcome anatomical barriers and to partake in active cell targeting and controlled release.⁷⁵ In fact, a Phase I clinical trial has already been underway to compare the relative bioavailability of different

MK-1439 experimental nanoformulations (NFs) with that of a MK-1439 film-coated tablet.⁷⁶ In addition, a Phase I clinical trial investigating the pharmacokinetics of the antiretroviral agents efavirenz and lopinavir, administered as NFs in healthy volunteers, is due to begin, pending the acquisition of appropriate funding.⁷⁷ Furthermore, nanosuspensions of the non-nucleoside reverse-transcriptase inhibitor TMC278-LA⁷⁸ and the integrase inhibitor GSK1265744⁷⁹ are examples of antiretroviral NFs that have been tested in Phase II clinical trials for HIV. Polyethylenimine mannose NPs that carry the HIV antigen-coding DNA plasmid DermaVir Patch vaccine have also reached this phase of development.⁸⁰ The potential of vaginally administered agents to target HIV has also been explored. Lecithin/cholesterol-based liposomes that carry MC1220⁸¹ and PLGA NPs which carry rilpivirine are among several NFs to reach the in vivo study stage of development.⁸² Proposed methods of nanotechnology-enhanced HIV-1 detection include surface-enhanced Raman spectroscopy using plasmonic NPs; electrochemical detection based on direct electron transfer in the virus; optical detection systems based on localized surface plasmon resonance; and vertically configured electrical detection based on scanning tunneling microscopy.⁸³

The proportion of cervical cancers in women which are attributable to human papillomavirus (HPV) infection is in excess of 99%, of which over 75% are attributable to HPV16 and/or 18.^{84,85} Phase III clinical trials have shown that the quadrivalent Gardasil vaccine is effective against HPV type 6, 11, 16, and 18 and that the bivalent Cervarix vaccine is effective against HPV type 16 and 18.^{86–89} These vaccines consist of virus-like particles that are constructed from L1 capsid monomer protein of the respective HPV types.⁹⁰ Biphasic vesicles used for topical delivery of interferon alpha have brought about marked therapeutic effects in patients.⁹¹ The use of biosensors may aid the development of rapid, cost-effective, and accurate diagnostic tests with appropriate sensitivities and detection limits.⁹²

The second largest proportional increase in sexually transmitted disease diagnosis in England between 2014 and 2015 was reported for gonorrhea (11%).⁹³ Nanomedicine may provide a novel means to treat antibiotic-resistant gonorrhea, therefore helping to prevent sequela such as pelvic inflammatory disease. One study showed that nanoencapsulation technology had the potential to enhance adaptive immunity to *Neisseria gonorrhoea* when combined with the intravaginal administration of microencapsulated interleukin-12 (IL-12) in mice. Treated mice responded faster to antibiotics and were significantly less likely to be re-infected than controls,

due to the adjunct effects of the IL-12, essentially converting the infection into a live vaccine.⁹⁴ A nanobiocomposite platform based on polyaniline-iron oxide-carbon nanotubes (PANI-nFe₃O₄-CNT) has also been used to fabricate a genosensor for *N. gonorrhoeae* and proven to be effective.⁹⁵ A bioelectrode using chitosan-iron oxide nanocomposite also demonstrated a high degree of accuracy for the detection of *N. gonorrhoeae* nucleic acid.⁹⁶

Research has shown that chlamydia detection rates are 1.7–2.2 times higher in women than men, thus reflecting higher testing rates in women.⁹³ One study demonstrated that when the antibiotic clindamycin hydrochloride, effective against chlamydia, was encapsulated in a poly-lactic acid (PLA)/PLGA-based NP system for oral delivery, enhanced efficacy was noted, as a result of improved bioavailability and drug action.⁹⁷ *Chlamydia trachomatis* recombinant major outer membrane protein (MOMP) encapsulated in PLGA NPs has also been shown to trigger primarily T helper 1 (Th1) cells and enhancement of T- and B-cell-mediated immunity in mice and to confer protective immunity against *C. trachomatis*.⁹⁸ Furthermore, PLA-poly(ethylene glycol) NPs have been shown to provide sustained delivery of a *C. trachomatis* recombinant MOMP peptide and to potentiate systemic adaptive immune responses in vivo.⁹⁹ Encapsulating recombinant MOMP *C. trachomatis* DNA vaccine in biodegradable chitosan NPs facilitates stability and protection from enzymatic digestion, while also enhancing delivery and expression of MOMP DNA in vitro and in mice.¹⁰⁰ Neutral generation-4 polyamidoamine (PAMAM) dendrimer – azithromycin conjugate nanodevices have displayed an ability to deliver drugs efficiently to growing intracellular *C. trachomatis* in vitro.¹⁰¹ Other studies have demonstrated similarly encouraging findings. Silver-polyvinyl pyrrolidone NPs in mouse macrophages infected in vitro with live *C. trachomatis* exhibit anti-inflammatory effects, possibly due to the regulation of various upstream surface receptors and downstream inflammatory pathway genes.¹⁰² Furthermore, charge-switching synthetic adjuvant particle-based mucosal vaccination elicited protective immune responses in mice.¹⁰³ Gold NPs and silver enhancement have been used to enable rapid, simultaneous detection of *Ureaplasma parvum* and *C. trachomatis* antigens by using a method based on visual protein microarray. This may have clinical applications for the simultaneous clinical diagnosis of *U. parvum* and *C. trachomatis*.¹⁰⁴

The largest proportional increase in sexually transmitted disease diagnosis in England between 2014 and 2015 was reported for syphilis,⁹³ highlighting the imperative need to

address this issue. A novel quantum dot (QD)-based point of care test for syphilis has been developed.¹⁰⁵ The potential application of Goldmag immune probes, as part of a NP-based colorimetric assay for the detection of syphilis, has also been indicated.¹⁰⁶ In addition, polyelectrolyte-coated gold magnetic NPs have been proven to be sensitive and selective when used in a syphilis immunoassay, suggesting a possible use in point of care diagnostics for syphilis screening.¹⁰⁷

Consequently, it is already evident that nanomedicine may benefit the health of women by minimizing the side effects of contraceptives. Nanomedicine may also enhance contraceptive efficacy, enabling the refinement of planned pregnancy. Furthermore, it may enable the development of reversible long-term contraceptives suitable for all genders, with the possibility of promoting equality and shared contraceptive responsibility between partners. In addition to contraception, nanomedicine may significantly improve the prevention, diagnosis, and treatment of sexually transmitted diseases which currently pose a significant challenge to women's health. As the diagnosis of bacterial infections increases, it is crucial that an effective arsenal of antibacterial agents is made available to treat such infections and reduce the incidence of serious clinical sequelae. However, with antibacterial resistance making many existing therapeutics redundant, novel treatments may become increasingly important. In addition, viral infections such as HIV and HPV are preventable infections; however, they are also attributable to the development of devastating conditions, namely, acquired immune deficiency syndrome and cervical cancer, respectively. Thus, it is crucial that viral infections are prevented, where possible, with optimized vaccines and barrier contraceptives; diagnosed as early as possible using highly sensitive diagnostic tools and treated before the development of secondary conditions. It is imperative that innovative research into theoretical nanomedicine applications in sexual health is translated into the clinic, to meet the expectations of increasingly scientifically literate patients who deserve the best care with minimal side effects.

Reproductive health care

Research is now underway to allow the field of reproductive science to benefit from the advancements in nanotechnology, by the application of NPs to diagnose and treat common conditions that affect many women of reproductive age, including endometriosis and uterine fibroids.

Endometriosis, which affects 2%–10% of women of reproductive age, involves the development of endometrial-like tissues outside of the uterine cavity¹⁰⁸ and is prevalent in

25%–30% of women suffering from infertility.¹⁰⁹ Conventional imaging of the affected tissues yields limited results, and currently, there is no suitable sensitive serum biomarker for endometriosis. Therefore, development in this field is pressing. NPs may provide the solution for this problem as these engineered particles possess a novel ability to provide excellent contrast enhancements for specific markers. One study demonstrated the production of an enhanced magnetic resonance imaging (MRI) contrast of ectopic uterine tissues in a rat model. The NPs involved were ultra-small superparamagnetic iron oxide NPs (IONPs), achieved through the high affinity of the NPs toward macrophages.¹¹⁰ Alternatively, magnetic oxide NPs, which had been modified with hyaluronic acid (HA-Fe₃O₄ NPs), have shown potential in detecting lesions.¹¹¹ Investigations into the treatment of endometriosis have used the therapeutic gene, pigment epithelium-derived factor (PEDF), which has both antitumor and antiangiogenic properties. Lipid-grafted chitosan micelles were loaded with PEDF and intravenously injected into rats with surgically induced endometriosis.¹¹² Following treatment, there were significant reductions in ectopic lesion volume. Growth inhibition of endometrioid cysts was also observed. Another study demonstrated that nanoceria (cerium oxide NPs) caused a reduction in the levels of reactive oxygen species (ROS) and angiogenic factors in endometriosis. Regression of endometriosis is also associated with the reduced density of endometrial glands and microvessels.¹¹³

Uterine fibroids (leiomyomas) are the most common type of pelvic tumor in women of reproductive age, often requiring invasive treatment. NPs have the potential to provide less intrusive treatment options. Cryosurgery offers potential treatment for these tumors. However, recurrence is a common drawback. Therefore, one previous study used nanogold particles conjugated with tumor necrosis factor alpha (TNF- α) as a cryo-adjuvant during cryosurgery and demonstrated significant reduction in tumor growth.¹¹⁴ Another research group investigated an alternative to hysterectomy by using poly L-lysine-PLGA NPs to deliver an antitumor and antiangiogenic biologically active metabolite of estradiol (2-methoxyoestradiol) into a human leiomyoma cell line (huLM).¹¹⁵ Both of these studies provided evidence of improved activity of the drug compared to the free molecule controls, as typically expected due to NP targeting capabilities. The use of adenovirus as a gene delivery vector to modify diseased cells has also been enhanced by conjugating the virus with magnetic NPs. With the appropriate magnetic field, the group demonstrated a statistically significant suppression of proliferation, and induced apoptosis, in both the cell types.¹¹⁶

The emerging evidence described herein suggests promising avenues for the clinical translation of nanomedicine in reproductive health. From imaging to diagnostics and therapeutics, nanomedicine already shows potential to enhance the care available for women of reproductive age with conditions such as endometriosis and uterine fibroids.

Cancer health care

Cancer located in the breasts, uterus, ovaries, and cervix are the first, fourth, sixth, and seventh most common cancers among women in the UK (2015), respectively.¹¹⁷ There is a growing body of evidence in support for the use of NPs to enable the early and accurate diagnosis of cancer and promote the efficacious treatment of cancers in women. With some new methodologies reaching the clinical trial phase of development, in time, nanomedicine may provide significant, state-of-the-art treatment options for women, subject to further investigation.

Currently, the imaging of cancer tissues by methods such as MRI, computed tomography (CT), and positron emission tomography is restricted by the use of nonspecific contrast agents, which only provide limited morphological information. The properties of NPs, such as paramagnetic particles, can be applied to provide a tissue-specific contrast for imaging and therefore provide a much more detailed image for diagnostic purposes.¹¹⁸

The principle of conjugating ligands targeting cancer-specific receptors with paramagnetic NPs is available for some time. For example, in ~20%–30% of breast cancers, the tyrosine kinase human epidermal growth factor receptor 2 (HER2)/neu receptor is overexpressed.¹¹⁹ In 2003, a study demonstrated how IONPs conjugated with molecules that targeted this receptor could be manipulated to improve MRI contrasts.¹²⁰ A more recent study showed how NPs coated in biocompatible material could be used to increase lifespan in the circulation. In this study, iron paramagnetic NPs were coated with HER2/neu antibody-conjugated poly(amino acid) derivatives (PAION-Ab)¹²¹ and showed specific targeting to SKBR-3 cells, which overexpressed the receptor and thus possess the potential to be a good MR contrast agent. This principle, however, is yet to be tested in vivo. Another study demonstrated promising in vivo results for targeting HER2- or epidermal growth factor receptor (EGFR)-positive breast cancer cells, by using conjugated IONPs with a block copolymer PEO-*b*-PyMPS to reduce the nonspecific uptake of the NPs by macrophages.¹²² This increases the availability of the circulating NPs to the cancer cells and therefore has the potential to increase tissue-specific uptake and subsequently signal intensity under MRI.

Regarding ovarian cancer, current imaging methods are incapable of detecting tumors <0.5 cm;¹²³ this must be improved for both detection and treatment purposes. It has been reported that 90% of solid ovarian cancer tumors overexpress the folate receptor alpha; therefore, NPs targeting this receptor offer potential benefits.^{123,124} Folic acid (FA)-targeted IONPs have been developed as a T2-negative contrast agent for MRI. It has been demonstrated in a xenograft tumor mouse model that FA-targeted IONPs specifically targeted the Skov-3 cells (with overexpressed FA receptors). Therefore, there is a potential to specifically localize carcinoma tissues, using the NPs as a negative contrast.¹²⁵ Another group used polyethylenimine-entrapped gold NPs, which were modified with a FA-linked polyethylene glycol (PEG) to form (FA-Au PENPs), to be used as a nanoprobe for CT imaging of cells which overexpressed the FA receptor.¹²⁶

MRI/CT imaging can leave much to be desired in terms of the resolution of tumor images, especially with tumors of small diameter. Therefore, one group by using a combination of photo acoustic tomography which has good resolution and imaging depth and fluorescence molecular tomography which provides 3D optical imaging used an NP contrast to provide images of ovarian cancers.¹²⁷ HER2/neu-specific affibody conjugation to imaging and quantification of IONPs was labeled at the cysteine residue of the affibody with near-infrared dye (NIR-830 dye). This proposed method provides a more advanced imaging prospect, specifically for ovarian cancer, and thus has promising clinical implications.

Cervical cancer screening is an important aspect of women's care, identifying women at risk of developing or who have developed cervical cancer. Initially, QDs conjugated to anti-EGFR antibodies were studied for the replacement of the organic dyes used in histological analyses.¹²⁸ However, it was found that ultra-bright fluorescent mesoporous silica NPs, functionalized with FA, exhibit greater fluorescence and have thus been developed to distinguish precancerous and cancerous cervical epithelial cells.¹²⁹ These NPs significantly increased the sensitivity of testing compared with currently available tests such as HPV-DNA and pathology tests.

A metastasizing cancer will often release cancer cells into the blood stream, and it could therefore be possible to detect these cells in a blood sample. However, the concentration of cancer cells can be very small and therefore difficult to identify. Serum detection for ovarian cancer is limited, but NPs may offer new techniques. One research group has developed a technique to separate and detect ovarian cancer cells from female whole blood using FA-conjugated

magnetic IONPs.¹³⁰ Unlike the previously discussed FA imaging methods, these NPs aim to mechanically separate cancer cells from other blood cells and are able to bind with metastasized cells overexpressing the FA receptor in a sample of whole blood. The sample is placed on a magnetic separator, and the pellet containing the IO–FA NP captured cells can be examined. This provides a method of identifying minute quantities of circulating ovarian cancer cells and could thus provide a means of early detection to enhance treatment options.

The detection of circulating breast cancer cells has been explored using a nanostructure-based platform for rare cell capture; this technique relies upon the platform's increased surface area. The streptavidin-conjugated silicon nanowire was shown to identify 16.2 ± 5.5 cells per 0.5 mL of whole blood.¹³¹ Dual aptamer-modified silica NPs have also been developed which target two cell lines, mucin 1 and human epidermal growth factor receptor 2 (EGFR2). This system will allow for the identification of two different types of breast cancer cells, thus enabling a broader range of diagnosis. Moreover bespoke NPs (dye-doped), in which dye molecules are directly incorporated in the NPs, lead to the creation of highly fluorescent NPs. This technique boasts a 1 cell/100 μ L detection limit, which is much better than that reported in previous studies.¹³²

Sentinel lymph nodes are the lymph nodes in which cancer tissues drain. Thus, if a cancer has metastasized, there will often be cancer cell parents in these lymph nodes. While operating to remove breast tumors, surgeons must identify the sentinel lymph nodes to allow for a biopsy of these lymph nodes to be taken as these can be histologically analyzed to confirm whether the cancer has metastasized. Current techniques include radiocolloid tracer, isosulfan blue dye, and indocyanine green (ICG).¹³³ These either require specialist gamma tracing equipment or, in the case of isosulfan blue dye, cause anaphylactic shock in 1.1% of patients.¹³⁴ Carbon NPs have been proposed to replace these techniques as the black appearance of the NPs can be detected by the operating surgeon to identify the correct lymph nodes to biopsy. Injection of 1 mL of carbon NP suspension leads to a significantly increased identification rate and also reduced false negative compared with blue dye (carbon NP versus blue dye: identification rate 100% versus 88%, false negative 11.1% versus 15.8%).¹³⁵ Due to their 150 nm diameter, carbon NPs are unable to enter the circulation, thus providing a distinct advantage (Figures 2 and 3).

Progression in the field of NPs has recently shifted toward sugar-based NPs. Some cancer cells are preprogrammed to

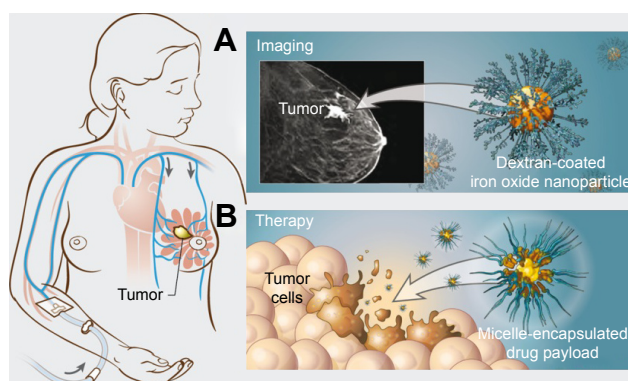


Figure 2 Nanoparticles in cancer management.

Notes: Nanoparticle accumulation at the tumor site can be used to deliver (A) contrast agents such as dextran-coated iron oxide nanoparticles for magnetic resonance imaging (MRI) or (B) chemotherapeutic drugs encapsulated in nanomaterials such as micelles. Reproduced with permission of Annual Review of, Volume 14 © by Annual Reviews, <http://www.annualreviews.org>. Albanese A, Tang PS, Chan WCW. The effect of nanoparticle size, shape, and surface chemistry on biological systems. In: Yarmush ML, editor. Palo Alto, CA: *Annual Review of Biomedical Engineering*. Vol 14. 2012:1–16.³

internalize sugar-based molecules at a faster rate than normal cells as some have an increased expression of glucose transporters (GLUT), described by the Warburg effect.¹³⁶ The fluorescent dye, ICG, was combined with NPs by encapsulation in levan NPs via self-assembly to demonstrate the effectiveness of sugar-based NPs. Without encapsulation, ICG has a very short half-life in the human environment, and so encapsulation helps to stabilize the dye, and the activity is preserved. These NPs were shown to successfully accumulate in breast cancer cells due to the increased expression of GLUT. Levan, in particular, has fructose moieties that interact with GLUT5 and pose new avenues for the exploration of drug delivery and imaging.¹³⁶

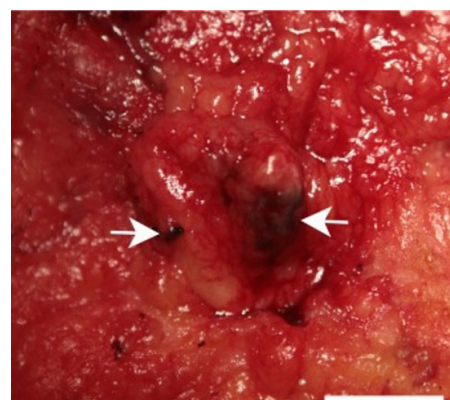


Figure 3 A photograph demonstrating the black-dyed lymph nodes (shown by the white arrows) in breast tissue 1 day postinjection of nanoparticle carbon suspension.

Notes: Scale bar is 1 cm. Reprinted from *Diagn Microbiol Infect Dis*, 67(2), Tang JF, Xu ZH, Zhou L, Qin H, Wang YF, Wang HH, Rapid and simultaneous detection of *Ureaplasma parvum* and *Chlamydia trachomatis* antibodies based on visual protein microarray using gold nanoparticles and silver enhancement, 122–128, Copyright (2010), with permission from Elsevier.¹⁰⁴

Treatment of cancer is complex due to the incredibly varied properties of different cancers. Therefore, NPs have been developed to target cancers in a variety of ways. First, some NPs have been developed to sensitize the cancerous tissues to currently available drugs. For example, in ovarian cancer, the functionalization of nanoscale gold particles with thio-glucose-targeting ligands has been shown to facilitate the delivery of chemotherapeutic agents into ovarian cancer cells. In addition, NPs also exhibited radio-sensitizing effects upon a human ovarian cancer cell line (SK-OV-3), believed to result from the increased production of ROS.¹³⁷

Enhancing drug delivery can also be facilitated by NPs. This is of particular interest as cancer drugs are often very cytotoxic to other noncancerous tissues. Choriocarcinoma is a malignant, trophoblastic cancer of placental origin, which is typically located in the uterus but may also occur in extrauterine sites such as ovaries. EnGeneIC delivery vehicles (EDVs) have shown potential for use in the targeted NP delivery of doxorubicin into placental tissues with greater antitumor activity in mouse models of choriocarcinoma relative to the free drug. Therefore, these high-capacity nanospheres, which may be targeted to EGRF to reduce non-trophoblastic drug delivery, may prove to be a promising drug delivery system for the treatment of choriocarcinoma.¹³⁸ A phase 1 clinical trial (ACTRN12609000672257) in nonpregnant human subjects with advanced epithelial cancer has shown that EDVs are safe in patients with advanced solid tumors and display modest clinical efficacy.¹³⁹ Neoadjuvant NP-albumin-bound paclitaxel (nab-PTX) is a treatment currently used for certain cancers due to the associated albumin receptor and SPARC affinities to albumin. This has also been suggested as a feasible therapeutic option for recurrent cervical cancer, being tolerable and potentially effective even after patients fail to respond to platinum-taxane or topotecan chemotherapy.¹⁴⁰ A meta-analysis investigated nab-PTX compared with PTX for breast cancer treatment and concluded that in randomized trials, there was a significantly greater chance of achieving a pathological complete response, an indication of better long-term outcome. This review also found that nab-PTX reduced the number of hypersensitivity reactions, one cause of these being the solvents used to make PTX into a soluble form, which is not necessary with nab-PTX. This provides solid evidence to support the use of nab-PTX.¹⁴¹ Ovarian cancer-targeted PTX NPs, which had been modified with FSH beta 81-95 peptide, were shown to successfully deliver chemotherapeutic compounds into ovarian cancer cells.¹⁴² Similarly, folate (FOL)-mediated PLGA-PEG NPs containing PTX, a drug that interferes with normal microtubule function,

were delivered to endometrial carcinoma HEC-1A cells. Results highlighted an enhanced level of tumor targeting and efficiency, which was significantly better than with the free drug alone.¹⁴³

Combination drug therapies have also been manipulated by NPs. Transactivation of transcription-targeted solid lipid NPs are a promising drug delivery system. This may enable the co-delivery of PTX and tocopheryl succinate-cisplatin as a combination therapy, which shows effective and synergistic antitumor activity against cervical cancer.¹⁴⁴ In breast cancer, neuropeptide Y Y1 receptors are overexpressed in comparison with normal breast cells which only express neuropeptide Y Y2. Capitalizing on these properties, one research group developed a conjugate molecule of doxorubicin and PNBL-NPY, the Y1 receptor ligand. This was internalized by the MCF-7 breast cancer cells which caused significant inhibition of cell growth, due to the drug, but also due to the synergistic interactions at the neuropeptide receptor.¹⁴⁵

Cancer cells can develop acquired drug resistance, and in general, drug-resistant cells prevent intracellular drug accumulation. Therefore, NPs are being modified to bypass these cellular defence systems.¹⁴⁶ Several types of NPs have been developed to target cervical cancer. NP delivery of siRNA against TWIST (a transcription factor reactivated in cancer) was used to reduce cisplatin resistance and resulted in reduced tumor burden in mice treated with cisplatin plus MSN-siTWIST, compared with mice treated with cisplatin alone. This was due to the reduction of disseminated tumors.¹⁴⁷ Another method to bypass cisplatin resistance is F3-targeted cisplatin-hydrogel NPs. This has been shown to be an effective therapeutic which can overcome the resistance of human ovarian tumor endothelial vessels to chemotherapy in vivo.¹⁴⁸ PTX can also be loaded into cationic nanostructured lipid NPs and has the potential to overcome PTX resistance and display therapeutic efficacy both in vitro and in vivo.¹⁴⁹

Another mechanism for cancer treatment is the enhancement of apoptosis in cancer tissues by stimulating specific mechanisms and causing a reduction in tumor mass. This has been well studied in cervical cancer. For example, folate receptor α (FR α)-targeted nanoliposomes inhibit proliferation and induce apoptosis of cervical tumor cells in vivo, while exhibiting no significant toxicity, suggesting that this may represent a novel modality for gene therapy in the treatment of cervical cancer.¹⁵⁰ Nanoquinacrine has also been shown to induce apoptosis in cancers through the inhibition of HH-Gli cascade by Gli1-inducing apoptosis of cervical cancer stem cells.¹⁵¹ Also, nanorealgar can inhibit the proliferation of different cervical carcinoma cell lines and

induce apoptosis in cervical carcinoma cells.¹⁵² In ovarian cancer, the combination of salinomycin and silver NPs has been shown to increase the therapeutic potential of the chemotherapy agent by enhancing apoptosis and autophagy in human ovarian cancer cells.¹⁵³ Furthermore, the induction of apoptosis and inhibition of angiogenesis by PEGylated liposomal quercetin showed significant suppression of tumor growth, compared with free quercetin, in in vitro and in vivo models of cisplatin-resistant ovarian cancers.¹⁵⁴ In SKBR-3 (HER2 positive cells) breast cancer cells, the induction of cell death was stimulated by the delivery of YopJ, an effector from the bacteria *Yersinia pestis*, fusing with glutathione S-transferase to form self-assembled protein NPs. This was found to downregulate MAPK and NFκB pathways, induce cell death, and inhibit the MEK1 pathway, and thus has the potential for reversing some drug resistance.¹⁵⁵

Gene therapy is a pioneering area of cancer medicine. The ability to transfer a gene with the intent to cause a change in cellular mechanisms is highly promising. Encapsulating molecules such as siRNA can protect such material from RNase degradation in circulation. For example, T7-LPC/siRNA NPs were shown to deliver EGFR siRNA into breast cancer cells through receptor-mediated endocytosis and then induce the downregulation of EGFR. This inhibited the growth of tumour.¹⁵⁶ Another example is that chitosan/HPV16 E7 siRNA complexes in cervical cancer cells were shown to target two oncoproteins and induce apoptosis, thus suggesting these might represent a useful NP system for the treatment of cervical cancer.¹⁵⁷ In addition, TNF-related apoptosis-inducing ligand/endostatin-loaded NPs have also been suggested as cervical cancer gene therapy modalities, on account of their enhanced cytotoxicity.¹⁵⁸ In ovarian cancer, antitumor effects were observed in studies where PLGA NPs encapsulating the proapoptotic human PNAS-4 (*hPNAS-4*) gene, along with cisplatin, were delivered into mouse ovarian carcinoma cells.¹⁵⁹ Degradable NPs have been used to deliver the proapoptotic survivin *T34A* gene and were shown to inhibit tumor growth in a mouse xenograft model of SKOV3 human ovarian cancer.¹⁶⁰ In addition, it has been found that Fe₃O₄-dextran-anti-βHCG carrying Hpa-antisense oligodeoxynucleotide has the potential to be an effective gene therapy for choriocarcinoma with significant inhibitory effects displayed on transplanted choriocarcinoma tumors in vivo. In this way, NPs can function as a harmless and effective gene vector.^{161,162}

Thus far, the most significant medical research and clinical translation in the field of nanomedicine has been related to the subject of oncology. Specific visualization and quantification of pathological processes, combined with

the delivery of multiple simultaneous targeted payloads of chemotherapeutics, NP-delivered gene therapy, and reduced incidence of drug resistance all offer significant hope of improving the prognosis of women receiving treatment for their respective cancer(s).

Menopause-related health care

Menopause occurs when the ovaries cease to make estrogen. Menopause is marked by the ending of a woman's menstrual cycles and may be initiated by the surgical removal of the ovaries. Menopausal symptoms are typically experienced, and the long-term reduced levels of estrogen can result in health problems, such as osteoporosis and cardiovascular disease.

Hormone therapy is the best available treatment for the vasomotor symptoms of menopause¹⁶³ and has the additional benefit of promoting an increase in bone density, thereby reducing the risk of fracture among postmenopausal women.¹⁶⁴ However, clinical trial results^{165,166} revealed that both estrogen alone and estrogen with progestin significantly increased the risk of stroke. Estrogen and a progestin were also associated with a significantly increased risk of breast cancer, coronary events, and pulmonary embolism. Consequently, the use of hormone therapy has declined.¹⁶⁷ However, micellar NP estradiol emulsions offer hope for enhanced transdermal hormone replacement therapy, which retains the advantages of transdermal administration while reducing adverse local side effects. Potential advantages of this technique include a lower incidence of venous thromboembolism and stroke and avoidance of first-pass metabolism when compared to oral administration.^{168,169} This represents the first product of its kind with the capacity to deliver consistent, therapeutic levels of estradiol systemically and to reduce the vasomotor symptoms observed in postmenopausal women.¹⁷⁰ Additional benefits include improved safety and greater patient compliance than other transdermal delivery systems.¹⁷¹ The findings of a Phase II clinical trial showed that treatment with nanoparticulate transdermal hormone therapy (nanoparticulate estradiol and nanoparticulate progesterone) for 12 weeks had beneficial, or neutral, effects on anthropometric markers of inflammation and hormonal variables in postmenopausal women, with no clinical evidence of cardiovascular disease. Of particular interest was the observed reduction in C-reactive protein and fasting insulin levels; known markers for chronic inflammation and cardiovascular risk, respectively.^{172,173}

Osteoporosis is a major health concern which arises due to long-term estrogen reduction at menopause. However, the application of nanomedicine offers the hope of improved

diagnostics and therapeutics, bone tissue engineering, nanostructure implantable materials, and surface modifications and coatings, which may provide a means of managing postmenopausal osteoporosis. Nanostructured ceramics, polymers, metals, and composites, which enhance osteoblast function and which have greater surface area and roughness to promote osteointegration, are of significant interest. The use of antimicrobial and drug-eluting coatings may help to improve the safety of surgical interventions by preventing infection.¹⁷⁴ The possibility of rebalancing bone turnover, using nanomedicine as a means of stabilizing osteoporosis, is of great interest. For example, calcium phosphate (including hydroxyapatite and β -tricalcium phosphate) NPs exhibit excellent biocompatibility, biodegradability, and biological activity, and therefore seem to be suitable vehicles for bone-specific drug delivery.¹⁷⁵ Furthermore, risedronate/zinc-hydroxyapatite NPs have been shown to represent a positive countermeasure to treat rat-modeled postmenopausal osteoporosis by means of rebalancing bone turnover in favor of bone formation.¹⁷⁶ Another study proposed the use of bisphosphonate (Bis)-conjugated iron (II, III) oxide (Fe_3O_4) NPs as a novel treatment for osteoporosis. These authors used a water-dispersible magnetic NP, which had radiofrequency-induced thermogenic properties to reduce the activity of osteoclasts through thermolysis.¹⁷⁷ Alternatively, the orally available enteric-microencapsulated parathyroid hormone (1-34)-deoxycholic acid nanocomplex may have the potential to effectively treat osteoporosis based on observations showing improvements in osteogenesis and trabecular connectivity in the ovariectomized rat model.¹⁷⁸ These studies reveal that there may be significant improvements to be made in reducing the development of postmenopausal osteoporosis through the administration of targeted nanotherapeutics.

Experimental evidence suggests that NPs may have the capacity to enhance the diagnostic imaging and treatment of postmenopausal cardiovascular disease.¹⁷⁹ Suppression of in-stent neointimal growth was observed in rabbits treated with liposomes carrying prednisolone phosphate¹⁸⁰ while liposomes carrying dexamethasone resulted in anti-inflammatory effects in atherogenic mice.¹⁸¹ Furthermore, anionic micelles and NP-apoB100 antibody conjugates have successfully reduced low-density lipoprotein levels in vivo.¹⁸² Another study showed that fullerenes carrying vimentin displayed antioxidant and anti-inflammatory effects within cells in an adipose tissue model.¹⁸³ Experimentally, perfluorocarbon NPs carrying fumagillin and theranostic NPs carrying 5-(4-carboxyphenyl)-10,15,20-triphenyl-2,3-dihydroxychlorin have been successfully applied to MRI

imaging, targeting $[\alpha]v[\beta]3$ integrin and macrophages respectively.^{184,185}

Menopause can result in the development of significant and potentially life-threatening sequelae such as osteoporosis and cardiovascular disease. Women are almost inevitably subject to the effects of menopause, which makes it an important area for the advancement of health care provision. Nanomedicine may reveal sophisticated approaches to improve the management of menopausal symptoms and the imaging, diagnosis, and treatment of sequelae.

Early-onset dementia health care

Data published by Alzheimer's Research UK suggests that dementia is the leading cause of death among women in the UK. It is estimated that women constitute 61% of people living with dementia, while 39% are men. This proportional difference is likely to result from the fact that age is the largest risk factor for this condition, and women typically live longer than men.¹⁸⁶ However, other factors should be considered. It is necessary to identify gender-specific risk factors in order to substantiate the hypothesis that women are more likely than men to develop dementia at any given age. Currently, there is a lack of firm evidence to support this view, but evaluation of the relative ratio of early onset dementia diagnoses in men and women may help to test this hypothesis.

Although Alzheimer's disease (AD) and other forms of dementia are primarily considered to be degenerative diseases of old age, ~4% of people with AD are under the age of 65 years.¹⁸⁷ This section of the review presents a synopsis of the applications of nanomedicine in the diagnosis and treatment of AD, which in rare circumstances can affect cisgender women between puberty and menopause.

Studies investigating the applications of nanotechnologies in the diagnosis of AD have yielded promising results, suggesting that improvements in both the early imaging of AD-affected brains and the detection of AD biomarkers may be possible.¹⁸⁸ The detection and identification of amyloid plaques by MRI, using NPs doped with contrast agents or tagged with fluorescent probes, is of particular interest. IO and gold NPs, thioflavin T, and QDs have all been explored in this context.

The successful detection of amyloid in transgenic mice using monocrystalline IONPs, covalently tethered to the N terminus of amyloid beta ($A\beta$) peptide for MRI, has already been reported.¹⁸⁹ Furthermore, the synthesis of fluorescent-maghemite NPs has created a method to use multimodal imaging agents to detect and remove amyloid fibrils by

manipulation with an external magnetic field.¹⁹⁰ In addition, the synthesis of superparamagnetic IONPs, coated with a 1,1-dicyano-2-[6-(dimethylamino)naphthalene-2-yl]propene carboxyl derivative, has been investigated *in vitro* for MRI studies of AD. Fluorophotometry results showed that the combination contrast agent resulted in the enhancement of fluorescence.¹⁹¹ The potential of metal NPs is further evident with the example of gold NPs. Noninvasive, label-free nanoplasmonic optical imaging for the real-time monitoring of amyloid fibrogenesis *in vitro* has been developed, observing the random movements of gold NPs in A β solution, and quantifying the kinetics of the fibrogenesis. It is hoped that this technology may eventually enable long-term monitoring of neuronal cells to aid in the identification of the mechanism of amyloid growth.¹⁹² Furthermore, heterodimeric NPs, consisting of a cobalt (II) magnetic core and a platinum shell fused to gold NPs and stabilized by a lipoic acid-PEG coating, have been used successfully in conjunction with MRI to image A β protofibrils in the early reversible stages of A β self-assembly.¹⁹³

Further innovative imaging methods are under development. One study showed that thioflavins, released from NPs administered via intracerebral injection, have the potential to target fibrillar amyloid *in vitro* and *in vivo* in the hippocampus of transgenic mice.¹⁹⁴ Therefore, thioflavin-loaded NPs represent another possible methodology in need of translational experimentation. In addition, novel QD nanoprobe have also been shown to be effective in the real-time imaging and quantification of A β peptide aggregates *in vivo*.¹⁹⁵ Moreover, a QD probe, conjugated with A β antibody for the molecular imaging of AD in a mouse model, confirmed the possibility of tracking the state of A β *in vivo* accumulation in mice, indicating a potential use in the molecular diagnostic imaging of AD in humans.¹⁹⁶

In addition to imaging, detection of biomarkers for AD (A β peptide and tau) is a key area of investigation in nanomedicine. The development of biosensors has been significantly aided by the advent of nanomedicine, with several developments having the potential to improve the diagnosis of AD. Indeed, the development of NP-based bio-barcode, involving oligonucleotide-modified gold NPs and magnetic microparticles, has permitted the detection of soluble pathogenic biomarkers for AD in cerebral spinal fluid.¹⁹⁷ Furthermore, the electrochemical detection of A β by saccharide-immobilized gold NPs on a carbon electrode demonstrated low detection thresholds, making this a promising methodology that requires further investigation.¹⁹⁸ In addition, scanning tunneling microscopy has been applied

to the electrical detection of AD biomarkers with the production of a similarly ultrasensitive immunosensor for A β , capable of detecting concentrations exceeding 10 fg/mL.¹⁹⁹ The development of gold NP-based immuno-polymerase chain reaction (nano-iPCR) further enabled the detection and quantification of tau protein in cerebrospinal fluid. Data indicated that Nano-iPCR is superior than ELISA in terms of sensitivity and detection range for tau protein detection, revealing the possibility of substantial improvements in the detection of biomarkers for AD.²⁰⁰ An alternative exploitation of the properties of gold NPs saw the development of an ultrasensitive and highly selective method of detection suitable for AD biomarker tau protein. Utilizing the two-photon Rayleigh scattering properties of gold NPs, anti-tau antibody-coated gold NPs proved to be highly sensitive to tau protein and suitable for further translational investigation.²⁰¹

Research has already begun into the potential use of nanotechnology applications of nanoscale inhibitors of A β plaque formation, nanoscale antioxidants, and NP-delivered cholinesterase inhibitors to treat AD.²⁰² It could be argued that, to date, the most successful method of minimizing cognitive defects through the nanoscale inhibition of A β plaque formation has been the implementation of hydrophobic chelating agents. The hydrophobicity of these agents aids their passage across the blood-brain barrier, while their ability to sequester metal ions, which can accelerate the formation of A β plaques, reduces plaque development. Such agents have progressed to pilot Phase II clinical trials with metal-protein attenuation demonstrated by iodochlorhydroxyquin showing modest efficacy in AD patients.²⁰³ In addition, NPs carrying novel D-penicillamine have also been proposed for metal chelation therapy in AD as a result of their observed ability to dissolve pre-existing A β aggregates *in vitro*.²⁰⁴ Although most investigation into the use of nanoscale inhibitors of A β plaque formation remains at the preclinical stage of development, there are several promising lines of investigation. For example, resveratrol has been shown to reduce the accumulation and deposition of A β *in vivo* by controlling AMPK signaling. In this way, the neuroprotective action of the kinase against A β plaque accumulation and deposition may suggest appropriate lines of investigation for the development of novel treatments for AD.²⁰⁵ In addition, PEGylated phospholipid nanomicelles have been shown to interact with A β *in vitro*, thus mitigating A β plaque formation, aggregation, and neurotoxicity in the SHSY-5Y human neuroblastoma cell line.²⁰⁶ KLVFF beta sheet blocker peptide-loaded liposomes have also been said to represent a

potential treatment to prevent amyloid aggregation in AD, because of their good colloidal stability and surface tension-lowering abilities.²⁰⁷ An alternative means of diminishing the aggregation and neurotoxicity of amyloid is by using pullulan-modified cholesteryl nanogels which bind to A β oligomers, thus acting as chaperones for misfolded proteins in primary cortical neuron cultures *in vitro*.²⁰⁸

As outlined earlier, nanomedical innovation is promoting the investigation of curcumin as an alternative therapeutic across a wide range of medical applications. Indeed, curcumin-associated nanoliposomes are known to inhibit the aggregation of Alzheimer's A β peptide *in vitro*.²⁰⁹ Similarly, nanoliposomes carrying a curcumin-lipid derivative, and decorated with an anti-transferrin monoclonal antibody conferring brain targeting functionality, have proven to be successful in delaying A β peptide aggregation, thus indicating a potential role in the treatment of AD.²¹⁰

C60 fullerene is a well-characterized free-radical scavenger and in its hydrated form has demonstrated the ability to inhibit fibrillization of A β peptide. In addition, the intraventricular administration of hydrated C60 has been shown to reduce A β -induced cognitive impairments in rats. C60 fullerenes therefore exhibit multiple synergistic mechanisms which could potentially be exploited in the treatment of AD, warranting further translational investigation of fullerenes as neuroprotectants.²¹¹

Increasing cholinergic activity, through the delivery of cholinesterase inhibitors using nanoscale drug delivery systems, is another therapeutic route being explored. Rivastigmine, a hydrophilic cholinesterase inhibitor, delivered in liposomes, offered a profound therapeutic effect that was greater than when delivered as a solution in an aluminum chloride (AlCl₃)-induced Alzheimer's rat model. The liposomes offered greater improvement than the solution in terms of spatial memory; histopathological examination of rat brains also showed substantially reduced amyloid plaque formation.²¹² Furthermore, nanodelivery systems may also enable the therapeutic use of acetylcholine. For example, the administration of acetylcholine alone in a kainic-acid-induced mouse model of AD did not bring about any significant effect, probably due to its poor ability to cross the blood-brain barrier and its short half-life.²¹³ However, single-walled nanotubes loaded with acetylcholine restored cognitive function to pre-AD levels. If administered within a lysosome-specific, cytotoxicity-free dose range, it is possible that translational research may enable the implementation of therapeutic acetylcholine alongside cholinesterase inhibitors to increase cholinergic activity.

The development of effective treatments for AD has been hindered by the uncertain mechanisms underlying progression of the disease and limited investigational capacity in humans, on account of the complexity and relative isolation of the brain, which frequently demands invasive procedures. The existence of just two main biomarkers for AD makes diagnosis of the disease challenging. Such challenges may potentially interfere with the results of clinical trials, and incorrectly diagnosed patients could even be recruited by such trials. Although the health care and clinical outcomes of AD patients currently lag behind that of many other diseases such as cancer, nanomedicine has the potential to support developments in this field. These developments might include improved imaging, which could enable research to offer a better understanding of the disease processes, more sensitive diagnostic tools to improve the early and accurate diagnoses of the disease or provide more effective treatments by exploiting the properties of nanomedicine to enhance the efficacy of the existing and novel therapies. Nanomedicine can thus assist in bringing about landmark developments necessary to improve the well-being of AD patients. That being said, much investigative work is still to be done to devise methodologies appropriate for translation into humans.

Conclusion

The clear advancements being made in the field of NPs can, in part, be attributed to their highly favorable characteristics. A vital property of NPs is their ability to target a specific ligand/receptor of a cell (Figure 4). This adaptable feature of NPs allows researchers to manipulate the natural biology of diseased cells, creating NPs containing pharmaceuticals which can then target the specific diseased cells. Coupled with the enhanced surface area of NPs, this also leads to a greater ability to detect small numbers of cells, with specific target ligands/receptors in samples, and thus provides an excellent way of detecting disease. Furthermore, loading NPs with pharmaceuticals has been shown to improve the bioavailability of drugs, for example, by protecting the drugs from the internal environment, and therefore improving pharmacological performance. Loading can also lead to the sustained release of pharmaceuticals, as NPs can act as local deposits for drugs. This could thereby reduce noncompliance problems associated with drug efficacy.

Although significant progress is being made, there are still many potential pitfalls in the translation of nanomedicine into clinical practice. One of the most important issues is the potential toxicity of the particles themselves. These foreign, and synthetic, molecules are known to exhibit a

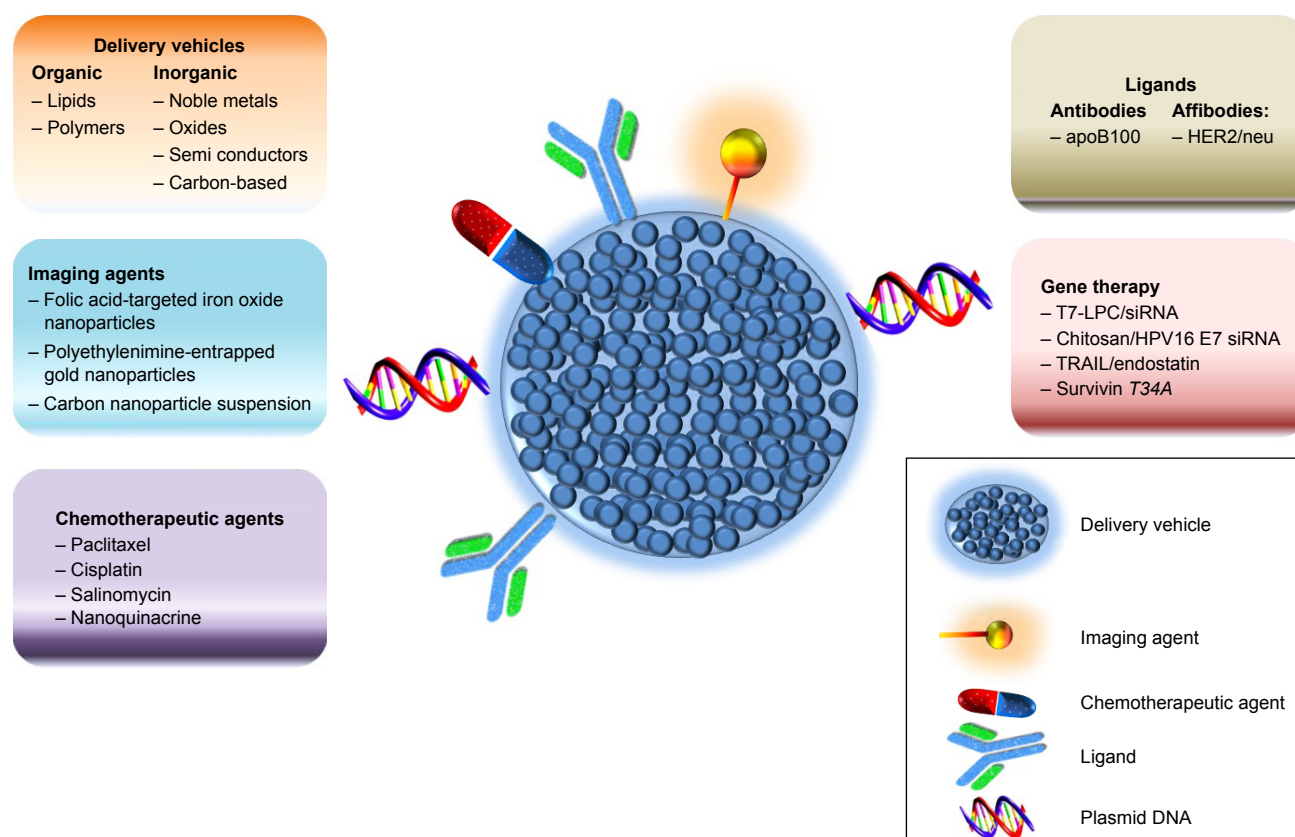


Figure 4 Clinical applications of nanoparticle-based delivery system in women's health. Nanoparticles have been used in drug delivery, imaging, and gene therapy. **Abbreviations:** TRAIL, TNF-related apoptosis-inducing ligand; TNF, tumor necrosis factor.

variable degree of cytotoxic effects upon human cells. Further research must now concentrate on this potential barrier, focusing particularly on the composition of the NPs and the ligands present on their exterior, together with the metabolic fate of such particles. Particular emphasis should be directed toward finding techniques to form NPs at a low cost with as little specialist equipment as necessary. This would make such treatment more accessible in the future.

The life course of a woman presents a unique set of medical challenges that are yet to be adequately addressed by the medical field. It is hoped that nanomedicine can provide promising and novel therapeutic applications, to allow physicians and patients to address these challenges more effectively. This review was intended to present a synopsis of the contribution nanomedicine could offer to the treatment of women's health and to encourage researchers to assist in the translation of this exciting technology to the clinic. Ample justification for such future effort is clearly evident in the primary literature, which already shows an abundance of primary research papers offering exciting and efficacious applications for nanomedicine in the treatment of women's health.

Disclosure

EA is funded by the "National Teaching Assistant Program" of United Arab Emirates University. The other authors report no conflicts of interest in this work.

References

- Koopmans RJ, Aggeli A. Nanobiotechnology – quo vadis? *Curr Opin Microbiol.* 2010;13(3):327–334.
- Emerich DF. Nanomedicine – prospective therapeutic and diagnostic applications. *Expert Opin Biol Ther.* 2005;5(1):1–5.
- Albanese A, Tang PS, Chan WCW. The effect of nanoparticle size, shape, and surface chemistry on biological systems. In: Yarmush ML, editor. *Palo Alto, CA: Annual Review of Biomedical Engineering.* Vol 14. 2012:1–16.
- High Quality Women's Health Care: a proposal for change [webpage on the Internet]. London: Royal College of Obstetrics and Gynaecologists; 2011. Available from: <http://www.rcog.org.uk/high-quality-womens-health-care>. Accessed February 20, 2017.
- Tomorrow's Specialist RCOG [webpage on the Internet]. London: Royal College of Obstetrics and Gynaecologists; 2011. Available from: <https://www.rcog.org.uk/en/guidelines-research-services/guidelines/tomorrows-specialist>. Accessed February 20, 2017.
- Bitzer J, Horne AW. A new age has come: the redefinition of women's health care. *J Fam Plan Reprod H.* 2012;38(2):68–69.
- Stephenson JA. Life-course approach to women's health: implications for health care and implementation in the United Kingdom (UK) [webpage on the Internet]. London: WHO/Europe; 2015. Available from: http://www.euro.who.int/__data/assets/pdf_file/0016/292201/Life-Course-Approach-Womens-Health-UK.pdf?ua=1. Accessed February 21, 2017.

8. Jain RK, Stylianopoulos T. Delivering nanomedicine to solid tumors. *Nat Rev Clin Oncol*. 2010;7(11):653–664.
9. Sargent J. Cardiovascular disease: new nanomedicines for treating atherosclerotic plaques. *Nat Rev Endocrinol*. 2015;11(5):256.
10. Lamprecht A. Nanomedicines in gastroenterology and hepatology. *Nat Rev Gastroenterol Hepatol*. 2015;12(4):195–204.
11. Barranco C. Autoimmunity: nanomedicine, meet autoimmune disease. *Nat Rev Rheumatol*. 2016;12(4):193.
12. Bell IR, Schwartz GE, Boyer NN, Koithan M, Brooks AJ. Advances in integrative nanomedicine for improving infectious disease treatment in public health. *Eur J Integr Med*. 2013;5(2):126–140.
13. Srikanth M, Kessler JA. Nanotechnology-novel therapeutics for CNS disorders. *Nat Rev Neurol*. 2012;8(6):307–318.
14. Denning TJ, Rao S, Thomas N, Prestidge CA. Oral nanomedicine approaches for the treatment of psychiatric illnesses. *J Control Release*. 2016;223:137–156.
15. Mazaheri M, Eslahi N, Ordikhani F, Tamjid E, Simchi A. Nanomedicine applications in orthopedic medicine: state of the art. *Int J Nanomedicine*. 2015;10:6039–6053.
16. Barkalina N, Charalambous C, Jones C, Coward K. Nanotechnology in reproductive medicine: emerging applications of nanomaterials. *Nanomedicine*. 2014;10(5):921–938.
17. Uskokovic V. Entering the era of nanoscience: time to be so small. *J Biomed Nanotechnol*. 2013;9(9):1441–1470.
18. Mahajan SD, Aalinkkel R, Law WC, et al. Anti-HIV-1 nanotherapeutics: promises and challenges for the future. *Int J Nanomedicine*. 2012;7:5301–5314.
19. McManus SBP, Jenkins R, Brugha T. Mental health and wellbeing in England: Adult Psychiatric Morbidity Survey 2014: Leeds [web-page on the Internet]. Available from: <http://content.digital.nhs.uk/catalogue/PUB21748/apms-2014-full-rpt.pdf>. Accessed February 21, 2017.
20. Vermeiden M, van den Broek WW, Mulder PGH, Birkenhager TK. Influence of gender and menopausal status on antidepressant treatment response in depressed inpatients. *J Psychopharmacol*. 2010;24(4):497–502.
21. Goel N, Plyler KS, Daniels D, Bale TL. Androgenic influence on serotonergic activation of the HPA stress axis. *Endocrinology*. 2011;152(5):2001–2010.
22. El-Hage W, Leman S, Camus V, Belzung C. Mechanisms of antidepressant resistance. *Front Pharmacol*. 2013;4:146.
23. Alyautdin R, Khalin I, Nafeeza MI, Haron MH, Kuznetsov D. Nanoscale drug delivery systems and the blood–brain barrier. *Int J Nanomedicine*. 2014;9:795–811.
24. Löscher W, Potschka H. Blood-brain barrier active efflux transporters: ATP-binding cassette gene family. *NeuroRx*. 2005;2(1):86–98.
25. Uhr M, Steckler T, Yassouridis A, Holsboer F. Penetration of amitriptyline, but not of fluoxetine, into brain is enhanced in mice with blood-brain barrier deficiency due to mdr1a P-glycoprotein gene disruption. *Neuropsychopharmacol*. 2000;22(4):380–387.
26. Uhr M, Grauer MT, Holsboer F. Differential enhancement of antidepressant penetration into the brain in mice with abcb1ab (mdr1ab) P-glycoprotein gene disruption. *Biol Psychiatry*. 2003;54(8):840–846.
27. Uhr M, Grauer MT. abcb1ab P-glycoprotein is involved in the uptake of citalopram and trimipramine into the brain of mice. *J Psychiatr Res*. 2003;37(3):179–185.
28. Karlsson L, Carlsson B, Hiemke C, et al. Altered brain concentrations of citalopram and escitalopram in P-glycoprotein deficient mice after acute and chronic treatment. *Eur Neuropsychopharmacol*. 2013;23(11):1636–1644.
29. Kato M, Fukuda T, Serretti A, et al. ABCB1 (MDR1) gene polymorphisms are associated with the clinical response to paroxetine in patients with major depressive disorder. *Prog Neuropsychopharmacol Biol Psychiatry*. 2008;32(2):398–404.
30. Uhr M, Tontsch A, Namendorf C, et al. Polymorphisms in the drug transporter gene ABCB1 predict antidepressant treatment response in depression. *Neuron*. 2008;57(2):203–209.
31. Sarginson JE, Lazzeroni LC, Ryan HS, Ershoff BD, Schatzberg AF, Murphy GM. ABCB1 (MDR1) polymorphisms and antidepressant response in geriatric depression. *Pharmacogenet Genomics*. 2010;20(8):467–475.
32. Lin KM, Chiu YF, Tsai IJ, et al. ABCB1 gene polymorphisms are associated with the severity of major depressive disorder and its response to escitalopram treatment. *Pharmacogenet Genomics*. 2011;21(4):163–170.
33. Singh AB, Bousman CA, Ng CH, Byron K, Berk M. ABCB1 polymorphism predicts escitalopram dose needed for remission in major depression. *Transl Psychiatry*. 2012;2:e198.
34. Roberts RL, Joyce PR, Mulder RT, Begg EJ, Kennedy MA. A common P-glycoprotein polymorphism is associated with nortriptyline-induced postural hypotension in patients treated for major depression. *Pharmacogenomics J*. 2002;2(3):191–196.
35. Jensen BP, Roberts RL, Vyas R, Bonke G, Jardine DL, Begg EJ. Influence of ABCB1 (P-glycoprotein) haplotypes on nortriptyline pharmacokinetics and nortriptyline-induced postural hypotension in healthy volunteers. *Br J Clin Pharmacol*. 2012;73(4):619–628.
36. de Klerk OL, Nolte IM, Bet PM, et al. ABCB1 gene variants influence tolerance to selective serotonin reuptake inhibitors in a large sample of Dutch cases with major depressive disorder. *Pharmacogenomics J*. 2013;13(4):349–353.
37. Laika B, Leucht S, Steimer W. ABCB1 (P-glycoprotein/MDR1) gene G2677T/a sequence variation (polymorphism): lack of association with side effects and therapeutic response in depressed inpatients treated with amitriptyline. *Clin Chem*. 2006;52(5):893–895.
38. Mihaljevic Peles A, Bozina N, Sagud M, Rojnic Kuzman M, Lovric M. MDR1 gene polymorphism: therapeutic response to paroxetine among patients with major depression. *Prog Neuropsychopharmacol Biol Psychiatry*. 2008;32(6):1439–1444.
39. Menu P, Gressier F, Verstuyft C, Hardy P, Becquemont L, Corruble E. Antidepressants and ABCB1 gene C3435T functional polymorphism: a naturalistic study. *Neuropsychobiology*. 2010;62(3):193–197.
40. Ashok B, Arleth L, Hjelm RP, Rubinstein I, Onyukel H. In vitro characterization of PEGylated phospholipid micelles for improved drug solubilization: effects of PEG chain length and PC incorporation. *J Pharm Sci*. 2004;93(10):2476–2487.
41. Leyva-Gómez G, González-Trujano ME, López-Ruiz E, et al. Nanoparticle formulation improves the anticonvulsant effect of clonazepam on the pentylenetetrazole-induced seizures: behavior and electroencephalogram. *J Pharm Sci*. 2014;103(8):2509–2519.
42. Kim IS, Jeong YI, Kim SH. Self-assembled hydrogel nanoparticles composed of dextran and poly(ethylene glycol) macromer. *Int J Pharmacol*. 2000;205:109–116.
43. Jana S, Maji N, Nayak AK, Sen KK, Basu SK. Development of chitosan-based nanoparticles through inter-polymeric complexation for oral drug delivery. *Carbohydr Polym*. 2013;98(1):870–876.
44. Tomoyasu Y, Yasuda T, Maeda S, Higuchi H, Miyawaki T. Liposome-encapsulated midazolam for oral administration. *J Liposome Res*. 2011;21(2):166–172.
45. Patel K, Padhye S, Nagarsenker M. Duloxetine HCl lipid nanoparticles: preparation, characterization, and dosage form design. *AAPS PharmSciTech*. 2012;13(1):125–133.
46. Ganesh M, Hemalatha P, Mei PM, Rajasekar K, Jang HT. A new fluoride mediated synthesis of mesoporous silica and their usefulness in controlled delivery of duloxetine hydrochloride a serotonin re-uptake inhibitor. *J Ind Eng Chem*. 2012;18(2):684–689.
47. Zhou Y, Zhang G, Rao Z, et al. Increased brain uptake of venlafaxine loaded solid lipid nanoparticles by overcoming the efflux function and expression of P-gp. *Arch Pharm Res*. 2015;38(7):1325–1335.
48. Shah S, Pal A, Kaushik VK, Devi S. Preparation and characterization of venlafaxine hydrochloride-loaded chitosan nanoparticles and in vitro release of drug. *J Appl Polym Sci*. 2009;112(5):2876–2887.
49. Yang H, Lopina ST. Extended release of a novel antidepressant, venlafaxine, based on anionic polyamidoamine dendrimers and poly(ethylene glycol)-containing semi-interpenetrating networks. *J Biomed Mater Res A*. 2005;72(1):107–114.

50. Childs SL, Chyall LJ, Dunlap JT, Smolenskaya VN, Stahly BC, Stahly GP. Crystal engineering approach to forming cocrystals of amine hydrochlorides with organic acids. Molecular complexes of fluoxetine hydrochloride with benzoic, succinic, and fumaric acids. *J Am Chem Soc.* 2004;126(41):13335–13342.
51. Varshosaz J, Tabbakhian M, Mohammadi MY. Formulation and optimization of solid lipid nanoparticles of buspirone HCl for enhancement of its oral bioavailability. *J Liposome Res.* 2010;20(4):286–296.
52. Gao B, Wang J, Wang D, et al. A novel preparation method for drug nanocrystals and characterization by ultrasonic spray-assisted electrostatic adsorption. *Int J Nanomedicine.* 2013;8:3927–3936.
53. Yan Y, Chen JM, Geng N, Lu TB. Improving the solubility of agomelatine via cocrystals. *Cryst Growth Des.* 2012;12(5):2226–2233.
54. He XL, Zhu YJ, Wang M, Jing GX, Zhu RR, Wang SL. Antidepressant effects of curcumin and HU-211 coencapsulated solid lipid nanoparticles against corticosterone-induced cellular and animal models of major depression. *Int J Nanomedicine.* 2016;11:4975–4990.
55. Qin J, Yang X, Mi J, et al. Enhanced antidepressant-like effects of the macromolecule trefol factor 3 by loading into negatively charged liposomes. *Int J Nanomedicine.* 2014;9:5247–5257.
56. Qin J, Yang X, Zhang RX, et al. Monocyte mediated brain targeting delivery of macromolecular drug for the therapy of depression. *Nanomedicine.* 2015;11(2):391–400.
57. Huang CT, Tsai MJ, Lin YH, et al. Effect of microemulsions on transdermal delivery of citalopram: optimization studies using mixture design and response surface methodology. *Int J Nanomedicine.* 2013;8:2295–2304.
58. Wei XL, Han YR, Quan LH, Liu CY, Liao YH. Oily nanosuspension for long-acting intramuscular delivery of curcumin didecanoate prodrug: preparation, characterization and in vivo evaluation. *Eur J Pharm Sci.* 2013;49(2):286–293.
59. Grabrucker AM, Garner CC, Boeckers TM, et al. Development of novel Zn²⁺ loaded nanoparticles designed for cell-type targeted drug release in CNS neurons: in vitro evidences. *PLoS One.* 2011;6(3):e17851.
60. Lifesyles Team. Statistics on Sexual and Reproductive Health Services England 2015/16 [webpage on the Internet]. Available from: <http://www.content.digital.nhs.uk/catalogue/PUB21969/srh-serv-eng-15-16-rep.pdf>. Accessed February 21, 2017.
61. Gaurav C, Goutam R, Rohan KN, Sweta KT, Abhay CS, Amit GK. (Copper-curcumin) beta-cyclodextrin vaginal gel: Delivering a novel metal-herbal approach for the development of topical contraception prophylaxis. *Eur J Pharm Sci.* 2014;65:183–191.
62. Liu HF, Liu ZL, Xie CS, Yu J, Zhu CH. The antifertility effectiveness of copper/low-density polyethylene nanocomposite and its influence on the endometrial environment in rats. *Contraception.* 2007;75(2):157–161.
63. Yu J, Li J, Li HG, Li JX, Xie CS, Zhu CH. Comparative study on contraceptive efficacy and clinical performance of the copper/low-density polyethylene nanocomposite IUD and the copper T220C IUD. *Contraception.* 2008;78(4):319–323.
64. Nandedkar TD, Sagvekar P, Thakur B, et al. Polymeric nanoparticle formulation of octapeptide (NP-OP): in vitro release and in vivo effect in common marmosets, *Callithrix jacchus* Linn. *Indian J Exp Biol.* 2013;51(12):1055–1062.
65. Boonthum C, Namdee K, Boonrunsiman S, et al. Chitosan-based DNA delivery vector targeted to gonadotropin-releasing hormone (GnRH) receptor. *Carbohydr Polym.* 2017;157:311–320.
66. Jha RK, Jha PK, Guha SK. Smart RISUG: a potential new contraceptive and its magnetic field-mediated sperm interaction. *Int J Nanomedicine.* 2009;4(1):55–64.
67. Guha SK, Singh G, Anand S, Ansari S, Kumar S, Koul V. Phase-I clinical-trial of an injectable contraceptive for the male. *Contraception.* 1993;48(4):367–375.
68. Guha SK, Singh G, Ansari S, et al. Phase II clinical trial of a vas deferens injectable contraceptive for the male. *Contraception.* 1997;56(4):245–250.
69. Chaki SP, Das HC, Misro MM. A short-term evaluation of semen and accessory sex gland function in phase III trial subjects receiving intravaginal contraceptive RISUG. *Contraception.* 2003;67(1):73–78.
70. Marfatia YS, Pandya I, Mehta K. Condoms: past, present, and future. *Indian J Sexual Transm Dis.* 2015;36(2):133–139.
71. Fayaz AM, Ao ZJ, Girilal M, et al. Inactivation of microbial infectiousness by silver nanoparticles-coated condom: a new approach to inhibit HIV- and HSV-transmitted infection. *Int J Nanomedicine.* 2012;7:5007–5018.
72. Banerjee S, Guha SK. RISUG (R): a potential candidate for the entry inhibitor group of antiretroviral drugs. *Med Hypotheses.* 2009;73(2):150–152.
73. Kirwan PD, Chau C, Brown AE, Gill ON, Delpech VC and contributors. HIV in the UK – 2016 report [webpage on the Internet]. Public Health England, London; December 2016. Available from: http://judahtrust.org/HIV_in_the_UK_2016.pdf. Accessed February 23, 2017.
74. Mamo T, Moseman EA, Kolishetti N, et al. Emerging nanotechnology approaches for HIV/AIDS treatment and prevention. *Nanomedicine.* 2010;5(2):269–285.
75. Roy U, Rodriguez J, Barber P, das Neves J, Sarmento B, Nair M. The potential of HIV-1 nanotherapeutics: from in vitro studies to clinical trials. *Nanomedicine.* 2015;10(24):3597–3609.
76. Bioavailability of MK-1439 Experimental Nano Formulations in Healthy Adults (MK-1439-046) [webpage on the Internet]. Bethesda, MD: National Library of Medicine (US). Identifier NCT02549040; September 11, 2015 [cited February 4, 2016]. Available from: <https://clinicaltrials.gov/ct2/show/NCT02549040?term=nano&draw=1&rank=27>. Accessed August 1, 2017.
77. PK of Efavirenz & Lopinavir Nano-formulations in Healthy Volunteers [webpage on the Internet]. Bethesda (MD): National Library of Medicine (US). Identifier NCT02631473; December 6, 2016. Available from: <https://clinicaltrials.gov/ct2/show/NCT02631473?term=NCT02631473&rank=1>. Accessed August 1, 2017.
78. Phase II safety and acceptability of an investigational injectable product, TMC278LA, for pre-exposure prophylaxis (TMC278LA) [webpage on the Internet]; Bethesda (MD): National Library of Medicine (US). Identifier NCT02165202; May 21, 2014 [cited March 31, 2017]. Available from: <https://clinicaltrials.gov/ct2/show/NCT02165202>. Accessed April 3, 2017.
79. Study to evaluate the safety tolerability and acceptability of long acting injections of the human immunodeficiency virus (HIV) integrase inhibitor, GSK1265744, in HIV Uninfected Men (ECLAIR) [webpage on the Internet]. Bethesda (MD): National Library of Medicine (US). Identifier NCT02076178; February 27, 2014 [cited November 23, 2016]. Available from: <https://clinicaltrials.gov/ct2/show/NCT02076178>. Accessed February 21, 2017.
80. Rodriguez B, Asmuth DM, Matining RM, et al. Safety, tolerability, and immunogenicity of repeated doses of DermaVir, a candidate therapeutic HIV vaccine, in HIV-Infected patients receiving combination antiretroviral therapy: results of the ACTG 5176 trial. *J Acquir Immune Defic Syndr.* 2013;64(4):351–359.
81. Caron M, Besson G, Etenna SLD, et al. Protective properties of non-nucleoside reverse transcriptase inhibitor (MC1220) incorporated into liposome against intravaginal challenge of Rhesus Macaques with RT-SHIV. *Virology.* 2010;405(1):225–233.
82. Kovarova M, Council OD, Date AA, et al. Nanoformulations of rilpivirine for topical pericoital and systemic coitus-independent administration efficiently prevent HIV transmission. *PLoS Pathog.* 2015;11(8):e1005075.
83. Lee JH, Oh BK, Choi JW. Development of a HIV-1 virus detection system based on nanotechnology. *Sensors.* 2015;15(5):9915–9927.
84. Smith JS, Lindsay L, Hoots B, et al. Human papillomavirus type distribution in invasive cervical cancer and high-grade cervical lesions: a meta-analysis update. *Int J Cancer.* 2007;121(3):621–632.
85. Howell-Jones R, Bailey A, Beddows S, et al. Multi-site study of HPV type-specific prevalence in women with cervical cancer, intraepithelial neoplasia and normal cytology, in England. *Br J Cancer.* 2010;103(2):209–216.

86. Garland SM, Hernandez-Avila M, Wheeler CM, et al. Quadrivalent vaccine against human papillomavirus to prevent anogenital diseases. *N Engl J Med*. 2007;356(19):1928–1943.
87. Villa LL, Perez G, Kjaer SK, et al. Quadrivalent vaccine against human papillomavirus to prevent high-grade cervical lesions. *N Engl J Med*. 2007;356(19):1915–1927.
88. Paavonen J, Jenkins D, Bosch FX, et al. Efficacy of a prophylactic adjuvanted bivalent L1 virus-like-particle vaccine against infection with human papillomavirus types 16 and 18 in young women: an interim analysis of a phase III double-blind, randomised controlled trial. *Lancet*. 2007;369(9580):2161–2170.
89. Herrero R, Hildesheim A, Rodriguez AC, et al. Rationale and design of a community-based double-blind randomized clinical trial of an HPV 16 and 18 vaccine in Guanacaste, Costa Rica. *Vaccine*. 2008;26(37):4795–4808.
90. Foldvari M. HPV infections: can they be eradicated using nanotechnology? *Nanomedicine*. 2012;8:131–135.
91. Foldvari M, Badea I, Kumar P, et al. Biphasic vesicles for topical delivery of interferon alpha in human volunteers and treatment of patients with human papillomavirus infections. *Curr Drug Deliv*. 2011;8(3):307–319.
92. Frias IAM, Avelino K, Silva RR, Andrade CAS, Oliveira MDL. Trends in biosensors for HPV: identification and diagnosis. *J Sensors*. 2015;2015:913640.
93. Public Health England. Sexually transmitted infections and chlamydia screening in England [webpage on the Internet]; 2015. Available from: https://www.gov.uk/government/uploads/system/uploads/attachment_data/file/617025/Health_Protection_Report_STIs_NCSP_2017.pdf. Accessed March 3, 2017.
94. Liu YR, Egilmez NK, Russell MW. Enhancement of adaptive immunity to *Neisseria gonorrhoeae* by local intravaginal administration of microencapsulated interleukin 12. *J Infect Dis*. 2013;208(11):1821–1829.
95. Singh R, Verma R, Sumana G, et al. Nanobiocomposite platform based on polyaniline-iron oxide-carbon nanotubes for bacterial detection. *Bioelectrochemistry*. 2012;86:30–37.
96. Singh R, Verma R, Kaushik A, et al. Chitosan-iron oxide nanocomposite platform for mismatch-discriminating DNA hybridization for *Neisseria gonorrhoeae* detection causing sexually transmitted disease. *Biosens Bioelectron*. 2011;26(6):2967–2974.
97. Rauta PR, Das NM, Nayak D, Ashe S, Nayak B. Enhanced efficacy of clindamycin hydrochloride encapsulated in PLA/PLGA based nanoparticle system for oral delivery. *IET Nanobiotechnol*. 2016;10(4):254–261.
98. Fairley SJ, Singh SR, Yilma AN, et al. Chlamydia trachomatis recombinant MOMP encapsulated in PLGA nanoparticles triggers primarily T helper 1 cellular and antibody immune responses in mice: a desirable candidate nanovaccine. *Int J Nanomedicine*. 2013;8:2085–2099.
99. Dixit S, Singh SR, Yilma AN, Agee RD, Taha M, Dennis VA. Poly(lactic acid)-poly(ethylene glycol) nanoparticles provide sustained delivery of a Chlamydia trachomatis recombinant MOMP peptide and potentiate systemic adaptive immune responses in mice. *Nanomedicine*. 2014;10(6):1311–1321.
100. Cambridge CD, Singh SR, Waffo AB, Fairley SJ, Dennis VA. Formulation, characterization, and expression of a recombinant MOMP Chlamydia trachomatis DNA vaccine encapsulated in chitosan nanoparticles. *Int J Nanomedicine*. 2013;8:1759–1771.
101. Mishra MK, Kotta K, Hali M, et al. PAMAM dendrimer-azithromycin conjugate nanodevices for the treatment of Chlamydia trachomatis infections. *Nanomedicine*. 2011;7(6):935–944.
102. Yilma AN, Singh SR, Dixit S, Dennis VA. Anti-inflammatory effects of silver-polyvinyl pyrrolidone (Ag-PVP) nanoparticles in mouse macrophages infected with live Chlamydia trachomatis. *Int J Nanomedicine*. 2013;8:2421–2432.
103. Stary G, Olive A, Radovic-Moreno AF, et al. A mucosal vaccine against Chlamydia trachomatis generates two waves of protective memory T cells. *Science*. 2015;348(6241):aaa8205.
104. Tang JF, Xu ZH, Zhou L, Qin H, Wang YF, Wang HH. Rapid and simultaneous detection of *Ureaplasma parvum* and *Chlamydia trachomatis* antibodies based on visual protein microarray using gold nanoparticles and silver enhancement. *Diagn Microbiol Infect Dis*. 2010;67(2):122–128.
105. Yang H, Li D, He R, et al. A novel quantum dots-based point of care test for syphilis. *Nanoscale Res Lett*. 2010;5(5):875–881.
106. Tang Z, Liang ZS, Nong Y, Wu XC, Luo H, Gao K. Application of Goldmag immune probe in timely detection of syphilis based on GIS platform. *Artif Cell Nanomed Biotechnol*. 2017;45(3):460–466.
107. Yang D, Ma J, Zhang Q, et al. Polyelectrolyte-coated gold magnetic nanoparticles for immunoassay development: toward point of care diagnostics for syphilis screening. *Anal Chem*. 2013;85(14):6688–6695.
108. Dunselman GAJ, Vermeulen N, Becker C, et al. ESHRE guideline: management of women with endometriosis. *Hum Reprod*. 2014;29(3):400–412.
109. Polat MYI, Boynukalin K, Yarai H. In vitro fertilization for endometriosis-associated infertility. *Womens Health (Lond)*. 2015;11(5):633–641.
110. Hue JJ, Lee HJ, Jon S, et al. Distribution and accumulation of Cy5.5-labeled thermally cross-linked superparamagnetic iron oxide nanoparticles in the tissues of ICR mice. *J Vet Sci*. 2013;14(4):473–479.
111. Zhang H, Li JC, Sun WJ, et al. Hyaluronic acid-modified magnetic iron oxide nanoparticles for MR imaging of surgically induced endometriosis model in rats. *PLoS One*. 2014;9(4):e94718.
112. Zhao MD, Sun YM, Fu GF, et al. Gene therapy of endometriosis introduced by polymeric micelles with glycolipid-like structure. *Biomaterials*. 2012;33(2):634–643.
113. Chaudhury K, Babu KN, Singh AK, Das S, Kumar A, Seal S. Mitigation of endometriosis using regenerative cerium oxide nanoparticles. *Nanomedicine*. 2013;9(3):439–448.
114. Jiang J, Bischof J. Effect of timing, dose and interstitial versus nanoparticle delivery of tumor necrosis factor alpha in combinatorial adjuvant cryosurgery treatment of ELT-3 uterine fibroid tumor. *Cryoletters*. 2010;31(1):50–62.
115. Ali HKG, Vincent K, Motamedi M, Rytting E. Nanomedicine for uterine leiomyoma therapy. *Ther Deliv*. 2013;4(2):161–175.
116. Shalaby SM, Khater MK, Perucho AM, et al. Magnetic nanoparticles as a new approach to improve the efficacy of gene therapy against differentiated human uterine fibroid cells and tumor-initiating stem cells. *Fertil Steril*. 2016;105(6):1638.
117. Office for National Statistics. Statistical Bulletin: Cancer Registration Statistics [webpage on the Internet]. England: First Release; 2015. Available from: <https://www.ons.gov.uk/peoplepopulationandcommunity/healthandsocialcare/conditionsanddiseases/bulletins/cancerregistrationstatisticsengland/firstrelease2015>. Accessed February 21, 2017.
118. Wang X, Yang LL, Chen Z, Shin DM. Application of nanotechnology in cancer therapy and imaging. *CA Cancer J Clin*. 2008;58(2):97–110.
119. Beeghly-Fadel A, Kataoka N, Shu XO, et al. Her-2/neu amplification and breast cancer survival: results from the Shanghai breast cancer study. *Oncol Rep*. 2008;19(5):1347–1354.
120. Artemov D, Mori N, Okolie B, Bhujwala ZM. MR molecular imaging of the Her-2/neu receptor in breast cancer cells using targeted iron oxide nanoparticles. *Magnet Res Med*. 2003;49(3):403–408.
121. Yang HM, Park CW, Woo MA, et al. HER2/neu antibody conjugated poly(amino acid)-coated iron oxide nanoparticles for breast cancer MR imaging. *Biomacromolecules*. 2010;11(11):2866–2872.
122. Chen H, Wang L, Yu Q, et al. Anti-HER2 antibody and ScFvEGFR-conjugated antifouling magnetic iron oxide nanoparticles for targeting and magnetic resonance imaging of breast cancer. *Int J Nanomedicine*. 2013;8:3781–3794.
123. Popovtzer R, Agarwal A, Kotov NA, et al. Targeted gold nanoparticles enable molecular CT imaging of cancer. *Nano Lett*. 2008;8(12):4593.
124. Low PS, Kularatne SA. Folate-targeted therapeutic and imaging agents for cancer. *Curr Opin Chem Biol*. 2009;13(3):256–262.

125. Zhang H, Li JC, Hu Y, Shen MW, Shi XY, Zhang GF. Folic acid-targeted iron oxide nanoparticles as contrast agents for magnetic resonance imaging of human ovarian cancer. *J Ovarian Res.* 2016;9:19.
126. Zhou BQ, Yang J, Peng C, et al. PEGylated polyethylenimine-entrapped gold nanoparticles modified with folic acid for targeted tumor CT imaging. *Col Surf B.* 2016;140:489–496.
127. Xi L, Satpathy M, Zhao Q, Qian W, Yang L, Jiang H. HER-2/neu targeted delivery of a nanoprobe enables dual photoacoustic and fluorescence tomography of ovarian cancer. *Nanomedicine.* 2014;10(3):669–677.
128. Nida DL, Rahman MS, Carlson KD, Richards-Kortum R, Follen M. Fluorescent nanocrystals for use in early cervical cancer detection. *Gynecol Oncol.* 2005;99(3 Suppl 1):S89–S94.
129. Palantavida S, Guz NV, Woodworth CD, Sokolov I. Ultrabright fluorescent mesoporous silica nanoparticles for prescreening of cervical cancer. *Nanomedicine.* 2013;9(8):1255–1262.
130. Liu W, Nie L, Li F, et al. Folic acid conjugated magnetic iron oxide nanoparticles for nondestructive separation and detection of ovarian cancer cells from whole blood. *Biomater Sci.* 2016;4(1):159–166.
131. Kim DJ, Choi MK, Jeong JT, et al. Enhancement of capture sensitivity for circulating tumor cells in a breast cancer patient's blood by silicon nanowire platform. *J Biomed Nanotechnol.* 2016;12(4):645–655.
132. Jo H, Her J, Ban C. Dual aptamer-functionalized silica nanoparticles for the highly sensitive detection of breast cancer. *Biosens Bioelectron.* 2015;71:129–136.
133. Niebling MG, Pleijhuis RG, Bastiaannet E, Brouwers AH, van Dam GM, Hoekstra HJ. A systematic review and meta-analyses of sentinel lymph node identification in breast cancer and melanoma, a plea for tracer mapping. *Eur J Surg Oncol.* 2016;42(4):466–473.
134. Albo D, Wayne JD, Hunt KK, et al. Anaphylactic reactions to isosulfan blue dye during sentinel lymph node biopsy for breast cancer. *Am J Surg.* 2001;182(4):393–398.
135. Wu X, Lin Q, Chen G, et al. Sentinel lymph node detection using carbon nanoparticles in patients with early breast cancer. *PLoS One.* 2015;10(8):e0135714.
136. Kim SJ, Bae PK, Chung BH. Self-assembled levan nanoparticles for targeted breast cancer imaging. *Chem Commun (Camb).* 2015;51(1):107–110.
137. Geng F, Song K, Xing JZ, et al. Thio-glucose bound gold nanoparticles enhance radio-cytotoxic targeting of ovarian cancer. *Nanotechnology.* 2011;22:285101.
138. Kaitu'u-Lino TJ, Pattison S, Ye L, et al. Targeted nanoparticle delivery of doxorubicin into placental tissues to treat ectopic pregnancies. *Endocrinology.* 2013;154:911–919.
139. Solomon BJ, Desai J, Rosenthal M, et al. A first-time-in-human phase I clinical trial of bispecific antibody-targeted, paclitaxel-packaged bacterial minicells. *PLoS One.* 2015;10(12):e0144559.
140. Minion LE, Chase DM, Farley JH, Willmott LJ, Monk BJ. Safety and efficacy of salvage nano-particle albumin bound paclitaxel in recurrent cervical cancer: a feasibility study. *Gynecol Oncol Res Pract.* 2016;3:4.
141. Zong Y, Wu J, Shen K. Nanoparticle albumin-bound paclitaxel as neoadjuvant chemotherapy of breast cancer: a systematic review and meta-analysis. *Oncotarget.* 2017;8(10):17360–17372.
142. Zhang X, Chen J, Kang Y, et al. Targeted paclitaxel nanoparticles modified with follicle-stimulating hormone beta 81-95 peptide show effective antitumor activity against ovarian carcinoma. *Int J Pharm.* 2013;453:498–505.
143. Liang C, Yang Y, Ling Y, Huang Y, Li T, Li X. Improved therapeutic effect of folate-decorated PLGA-PEG nanoparticles for endometrial carcinoma. *Bioorg Med Chem.* 2011;19:4057–4066.
144. Liu B, Han L, Liu J, Han S, Chen Z, Jiang L. Co-delivery of paclitaxel and TOS-cisplatin via TAT-targeted solid lipid nanoparticles with synergistic antitumor activity against cervical cancer. *Int J Nanomedicine.* 2017;12:955–968.
145. Li J, Shen Z, Ma X, et al. Neuropeptide Y Y1 receptors mediate targeted delivery of anticancer drug with encapsulated nanoparticles to breast cancer cells with high selectivity and its potential for breast cancer therapy. *ACS Appl Mater Interfaces.* 2015;7(9):5574–5582.
146. Peetla C, Vijayaraghavalu S, Labhasetwar V. Biophysics of cell membrane lipids in cancer drug resistance: implications for drug transport and drug delivery with nanoparticles. *Adv Drug Deliv Rev.* 2013;65(13–14):1686–1698.
147. Roberts CM, Shahin SA, Wen W, et al. Nanoparticle delivery of siRNA against TWIST to reduce drug resistance and tumor growth in ovarian cancer models. *Nanomedicine.* 2017;13(3):965–976.
148. Winer I, Wang S, Lee YE, et al. F3-targeted cisplatin-hydrogel nanoparticles as an effective therapeutic that targets both murine and human ovarian tumor endothelial cells in vivo. *Cancer Res.* 2010;70(21):8674–8683.
149. Wang L, Jia E. Ovarian cancer targeted hyaluronic acid-based nanoparticle system for paclitaxel delivery to overcome drug resistance. *Drug Deliv.* 2016;23(5):1810–1817.
150. Yang Y, He L, Liu Y, et al. Promising nanocarriers for PEDF gene targeting delivery to cervical cancer cells mediated by the over-expressing FR α . *Sci Rep.* 2016;6:32427.
151. Nayak A, Satapathy SR, Das D, et al. Nanoquinacrine induced apoptosis in cervical cancer stem cells through the inhibition of hedgehog-Gli1 cascade: Role of Gli-1. *Sci Rep.* 2016;6:20600.
152. Li L, Wang L, Xiao S, Li Y, Cheng C, Xue M. [Effect of nano-realgar on proliferation and apoptosis of human cervical carcinoma cells]. *Zhong Nan Da Xue Xue Bao Yi Xue Ban.* 2015;40(10):1068–1075. Chinese.
153. Zhang XF, Gurunathan S. Combination of salinomycin and silver nanoparticles enhances apoptosis and autophagy in human ovarian cancer cells: an effective anticancer therapy. *Int J Nanomedicine.* 2016;11:3655–3675.
154. Long QD, Xie Y, Huang YQ, et al. Induction of apoptosis and inhibition of angiogenesis by PEGylated liposomal quercetin in both cisplatin-sensitive and cisplatin-resistant ovarian cancers. *J Biomed Nanotechnol.* 2013;9:965–975.
155. Herrera Estrada L, Padmore TJ, Champion JA. Bacterial effector nanoparticles as breast cancer therapeutics. *Mol Pharm.* 2016;13(3):710–719.
156. Yu MZ, Pang WH, Yang T, et al. Systemic delivery of siRNA by T7 peptide modified core-shell nanoparticles for targeted therapy of breast cancer. *Eur J Pharm Sci.* 2016;92:39–48.
157. Yang J, Li S, Guo F, Zhang W, Wang Y, Pan Y. Induction of apoptosis by chitosan/HPV16 E7 siRNA complexes in cervical cancer cells. *Mol Med Rep.* 2013;7:998–1002.
158. Zheng Y, Chen H, Zeng X, et al. Surface modification of TPGS-b-(PCL-ran-PGA) nanoparticles with polyethyleneimine as a co-delivery system of TRAIL and endostatin for cervical cancer gene therapy. *Nanoscale Res Lett.* 2013;8(1):161.
159. Qi X, Song X, Liu P, et al. Antitumor effects of PLGA nanoparticles encapsulating the human PNAS-4 gene combined with cisplatin in ovarian cancer. *Oncol Rep.* 2011;26:703–710.
160. Luo L, Du T, Zhang J, et al. Efficient inhibition of ovarian cancer by degradable nanoparticle-delivered survivin T34A gene. *Int J Nanomedicine.* 2016;11:501–512.
161. Jingting C, Huining L, Yi Z. Preparation and characterization of magnetic nanoparticles containing Fe(3)O(4)-dextran-anti- β -human chorionic gonadotropin, a new generation choriocarcinoma-specific gene vector. *Int J Nanomedicine.* 2011;6:285–294.
162. Huining L, Yi Z, Dihong T, et al. Inhibition of choriocarcinoma by Fe3O4-dextran-anti- β -human chorionic gonadotropin nanoparticles containing antisense oligodeoxynucleotide of heparanase. *Int J Nanomedicine.* 2013;8:4371–4378.
163. Grady D. Management of menopausal symptoms. *N Engl J Med.* 2006;355(22):2338–2347.
164. Cauley JA, Robbins J, Chen Z, et al. Effects of estrogen plus progestin on risk of fracture and bone mineral density – the Women's Health Initiative randomized trial. *J Am Med Assoc.* 2003;290(13):1729–1738.

165. Rossouw JE, Anderson GL, Prentice RL, et al. Risks and benefits of estrogen plus progestin in healthy postmenopausal women – principal results from the Women’s Health Initiative randomized controlled trial. *J Am Med Assoc*. 2002;288(3):321–333.
166. Anderson GL, Limacher M, Assaf AR, et al. Effects of conjugated, equine estrogen in postmenopausal women with hysterectomy – the Women’s Health Initiative randomized controlled trial. *J Am Med Assoc*. 2004;291(14):1701–1712.
167. Haas JS, Kaplan CP, Gerstenberger EP, Kerlikowske K. Changes in the use of postmenopausal hormone therapy after the publication of clinical trial results. *Ann Intern Med*. 2004;140(3):184–188.
168. Canonico M, Oger E, Plu-Bureau G, et al. Hormone therapy and venous thromboembolism among postmenopausal women – impact of the route of estrogen administration and progestogens: the ESTHER study. *Circulation*. 2007;115(7):840–845.
169. Renoux C, Dell’Aniello S, Garbe E, Suissa S. Transdermal and oral hormone replacement therapy and the risk of stroke: a nested case-control study. *BMJ*. 2010;340:c2519.
170. Simon JA; ESTRASORB Study Group. Estradiol in micellar nanoparticles: the efficacy and safety of a novel transdermal drug-delivery technology in the management of moderate to severe vasomotor symptoms. *Menopause*. 2006;13(2):222–231.
171. Valenzuela P, Simon JA. Nanoparticle delivery for transdermal HRT. *Maturitas*. 2012;73(1):74–80.
172. Nanoparticulate Versus Micronized Steroids Delivery for Transdermal Hormone Replacement Therapy (Nanoparticle) [webpage on the Internet]. Bethesda (MD): National Library of Medicine (US). Identifier NCT02467673, June 7, 2015 [cited May 21, 2016]. Available from: <https://clinicaltrials.gov/ct2/show/NCT02467673?term=nano&draw=1&rank=59>. Accessed August 1, 2017.
173. Botelho MA, Queiroz DB, Silva I. Micronized versus nanoparticles in transdermal hormone replacement therapy: effects on blood pressure and inflammatory parameters in Brazilian postmenopausal women. MedCrave Group LLC. June 13, 2017. Available from: http://medcraveonline.com/ebooks/Micronized_Versus_Nanoparticles_in_Transdermal_Hormone_Replacement_Therapy_Effects_on_Blood_Pressure_and_Inflammatory_Parameters_in_Brazilian_Postmenopausal_Women.pdf. Accessed August 1, 2017.
174. Mazaheri M, Eslahi N, Ordikhani F, Tamjid E, Simchi A. Nanomedicine applications in orthopedic medicine: state of the art. *Int J Nanomedicine*. 2015;10:6039–6053.
175. Roohani-Esfahani SI, Zreiqat H. Nanoparticles: a promising new therapeutic platform for bone regeneration? *Nanomedicine (Lond)*. 2017;12:419–422.
176. Khajuria DK, Disha C, Vasireddi R, Razdan R, Mahapatra DR. Risedronate/zinc-hydroxyapatite based nanomedicine for osteoporosis. *Mater Sci Eng C Mater Biol Appl*. 2016;63:78–87.
177. Lee MS, Su CM, Yeh JC, Wu PR, Tsai TY, Lou SL. Synthesis of composite magnetic nanoparticles Fe₃O₄ with alendronate for osteoporosis treatment. *Int J Nanomedicine*. 2016;11:4583–4594.
178. Hwang SR, Seo DH, Byun Y, Park JW. Preparation and in vivo evaluation of an orally available enteric-microencapsulated parathyroid hormone (1–34)-deoxycholic acid nanocomplex. *Int J Nanomedicine*. 2016;11:4231–4246.
179. Psarros C, Lee R, Margaritis M, Antoniadis C. Nanomedicine for the prevention, treatment and imaging of atherosclerosis. *Maturitas*. 2012;73(1):52–60.
180. Joner M, Morimoto K, Kasukawa H, et al. Site-specific targeting of nanoparticle Prednisolone reduces in-stent restenosis in a rabbit model of established atheroma. *Arterioscler Thromb Vasc Biol*. 2008;28(11):1960–1966.
181. Chono S, Tauchi Y, Deguchi Y, Morimoto K. Efficient drug delivery to atherosclerotic lesions and the antiatherosclerotic effect by dexamethasone incorporated into liposomes in atherogenic mice. *J Drug Target*. 2005;13(4):267–276.
182. Chnari E, Lari HB, Tian L, Uhrich KE, Moghe PV. Nanoscale anionic macromolecules for selective retention of low-density lipoproteins. *Biomaterials*. 2005;26(17):3749–3758.
183. Xiao L, Aoshima H, Saitoh Y, Miwa N. Highly hydroxylated fullerene localizes at the cytoskeleton and inhibits oxidative stress in adipocytes and a subcutaneous adipose-tissue equivalent. *Free Radic Biol Med*. 2011;51(7):1376–1389.
184. Winter PM, Neubauer AM, Caruthers SD, et al. Endothelial alpha(v) beta(3) integrin-targeted fumagillin nanoparticles inhibit angiogenesis in atherosclerosis. *Arterioscler Thromb Vasc Biol*. 2006;26(9):2103–2109.
185. McCarthy JR, Jaffer FA, Weissleder R. A macrophage-targeted theranostic nanoparticle for biomedical applications. *Small*. 2006;2(8–9):983–987.
186. Alzheimer’s Research UK. Women and dementia: a marginalised majority. March 2015. Available from: <http://www.alzheimersresearchuk.org/wp-content/uploads/2015/03/Women-and-Dementia-A-Marginalised-Majority1.pdf>. Accessed June 8, 2017.
187. Alzheimer’s Association. Alzheimer’s Disease Facts and Figures, Alzheimer’s & Dementia, Volume 9, Issue 2; 2013. Available from: http://www.alz.org/downloads/facts_figures_2013.pdf. Accessed September 8, 2017.
188. Brambilla D, Le Droumaguet B, Nicolas J, et al. Nanotechnologies for Alzheimer’s disease: diagnosis, therapy, and safety issues. *Nanomedicine*. 2011;7(5):521–540.
189. Wadghiri YZ, Sigurdsson EM, Sadowski M, et al. Detection of Alzheimer’s amyloid in transgenic mice using magnetic resonance microimaging. *Magn Reson Med*. 2003;50(2):293–302.
190. Skaat H, Margel S. Synthesis of fluorescent-maghemite nanoparticles as multimodal imaging agents for amyloid-beta fibrils detection and removal by a magnetic field. *Biochem Biophys Res Commun*. 2009;386(4):645–649.
191. Zhou JT, Fa HB, Yin W, et al. Synthesis of superparamagnetic iron oxide nanoparticles coated with a DDNP-carboxyl derivative for in vitro magnetic resonance imaging of Alzheimer’s disease. *Mater Sci Eng C Mater Biol Appl*. 2014;37:348–355.
192. Lee SS, Lee LP. Noninvasive label-free nanoplasmonic optical imaging for real-time monitoring of in vitro amyloid fibrogenesis. *Nanoscale*. 2014;6(7):3561–3565.
193. Choi JS, Choi HJ, Jung DC, Lee JH, Cheon J. Nanoparticle assisted magnetic resonance imaging of the early reversible stages of amyloid beta self-assembly. *Chem Commun (Camb)*. 2008;19:2197–2199.
194. Siegmund T, Paulke BR, Schmiedel H, et al. Thioflavins released from nanoparticles target fibrillar amyloid beta in the hippocampus of APP/PS1 transgenic mice. *Int J Dev Neurosci*. 2006;24(2–3):195–201.
195. Tokuraku K, Marquardt M, Ikezu T. Real-time imaging and quantification of amyloid-beta peptide aggregates by novel quantum-dot nanoprobe. *PLoS One*. 2009;4(12):e8492.
196. Feng L, Long HY, Liu RK, et al. A quantum dot probe conjugated with a beta antibody for molecular imaging of Alzheimer’s disease in a mouse model. *Cell Mol Neurobiol*. 2013;33(6):759–765.
197. Georganopoulou DG, Chang L, Nam JM, et al. Nanoparticle-based detection in cerebral spinal fluid of a soluble pathogenic biomarker for Alzheimer’s disease. *Proc Natl Acad Sci U S A*. 2005;102(7):2273–2276.
198. Chikae M, Fukuda T, Kerman K, Idegami K, Miura Y, Tamiya E. Amyloid-beta detection with saccharide immobilized gold nanoparticle on carbon electrode. *Bioelectrochemistry*. 2008;74(1):118–123.
199. Kang DY, Lee JH, Oh BK, Choi JW. Ultra-sensitive immunosensor for beta-amyloid (1–42) using scanning tunneling microscopy-based electrical detection. *Biosens Bioelectron*. 2009;24(5):1431–1436.
200. Stegurova L, Draberova E, Bartos A, Draber P, Ripova D, Draber P. Gold nanoparticle-based immuno-PCR for detection of tau protein in cerebrospinal fluid. *J Immunol Methods*. 2014;406:137–142.
201. Neely A, Perry C, Varisli B, et al. Ultrasensitive and highly selective detection of Alzheimer’s disease biomarker using two-photon Rayleigh scattering properties of gold nanoparticle. *ACS Nano*. 2009;3(9):2834–2840.
202. Srikanth M, Kessler JA. Nanotechnology – novel therapeutics for CNS disorders. *Nat Rev Neurol*. 2012;8(6):307–318.

203. Ritchie CW, Bush AI, Mackinnon A, et al. Metal-protein attenuation with iodochlorhydroxyquin (clioquinol) targeting A beta amyloid deposition and toxicity in Alzheimer disease – a pilot phase 2 clinical trial. *Arch Neurol*. 2003;60(12):1685–1691.
204. Cui Z, Lockman PR, Atwood CS, et al. Novel D-penicillamine carrying nanoparticles for metal chelation therapy in Alzheimer's and other CNS diseases. *Eur J Pharm Biopharm*. 2005;59(2):263–272.
205. Marambaud P, Vingtdeux V, Giliberto L, Davies P. Resveratrol lowers beta-amyloid accumulation and deposition in vivo by controlling AMPK signaling. *Alzheimers Dement*. 2010;6(4):S406.
206. Pai AS, Rubinstein I, Onyuksel H. PEGylated phospholipid nanomicelles interact with beta-amyloid((1-42)) and mitigate its beta-sheet formation, aggregation and neurotoxicity in vitro. *Peptides*. 2006; 27(11):2858–2866.
207. Kumaraswamy P, Sethuraman S, Krishnan UM. Liposomal delivery of a beta sheet blocker peptide for the treatment of Alzheimer's disease. *Alzheimers Dement*. 2012;8(4 Suppl):P705.
208. Ikeda K, Okada T, Sawada S, Akiyoshi K, Matsuzaki K. Inhibition of the formation of amyloid beta-protein fibrils using biocompatible nanogels as artificial chaperones. *FEBS Lett*. 2006;580(28–29):6587–6595.
209. Taylor M, Moore S, Mourtas S, et al. Effect of curcumin-associated and lipid ligand-functionalized nanoliposomes on aggregation of the Alzheimer's A beta peptide. *Nanomedicine*. 2011;7(5):541–550.
210. Mourtas S, Lazar AN, Markoutsas E, Duyckaerts C, Antimisiaris SG. Multifunctional nanoliposomes with curcumin-lipid derivative and brain targeting functionality with potential applications for Alzheimer disease. *Eur J Med Chem*. 2014;80:175–183.
211. Podolski IY, Podlubnaya ZA, Kosenko EA, et al. Effects of hydrated forms of C-60 fullerene on amyloid beta-peptide fibrillization in vitro and performance of the cognitive task. *J Nanosci Nanotechnol*. 2007; 7(4–5):1479–1485.
212. Ismail MF, ElMeshad AN, Salem NAH. Potential therapeutic effect of nanobased formulation of rivastigmine on rat model of Alzheimer's disease. *Int J Nanomedicine*. 2013;8:393–406.
213. Yang Z, Zhang YG, Yang YLA, et al. Pharmacological and toxicological target organelles and safe use of single-walled carbon nanotubes as drug carriers in treating Alzheimer disease. *Nanomedicine*. 2010;6(3):427–441.

International Journal of Nanomedicine

Publish your work in this journal

The International Journal of Nanomedicine is an international, peer-reviewed journal focusing on the application of nanotechnology in diagnostics, therapeutics, and drug delivery systems throughout the biomedical field. This journal is indexed on PubMed Central, MedLine, CAS, SciSearch®, Current Contents®/Clinical Medicine,

Submit your manuscript here: <http://www.dovepress.com/international-journal-of-nanomedicine-journal>

Dovepress

Journal Citation Reports/Science Edition, EMBase, Scopus and the Elsevier Bibliographic databases. The manuscript management system is completely online and includes a very quick and fair peer-review system, which is all easy to use. Visit <http://www.dovepress.com/testimonials.php> to read real quotes from published authors.