Nanotechnology-based drug delivery systems for control of microbial biofilms: a review

Matheus Aparecido Dos Santos Ramos1
Patrícia Bento Da Silva2
Larissa Spósito1
Luciani Gaspar De Toledo1
Bruna Vidal Bonifácio1
Camila Fernanda Rodero3
Karen Cristina Dos Santos2
Marlus Chorilli2
Taís Maria Bauab1

1 São Paulo State University (UNESP), School of Pharmaceutical Sciences, Campus Araraquara, Department of Biological Sciences, Araraquara, SP, Brazil; 2 São Paulo State University (UNESP), School of Pharmaceutical Sciences, Campus Araraquara, Department of Drugs and Medicines, Araraquara, SP, Brazil

Correspondence: Taís Maria Bauab
São Paulo State University (UNESP), School of Pharmaceutical Sciences, Campus Araraquara, Department of Biological Sciences, Rodovia Araraquara Jau, Km 01 - s/n Campos Ville, Araraquara, SP, Brazil
Tel +55 16 3301 6955
Fax +55 16 3322 0073
Email bauabtm@fcfar.unesp.br

Abstract: Since the dawn of civilization, it has been understood that pathogenic microorganisms cause infectious conditions in humans, which at times, may prove fatal. Among the different virulent properties of microorganisms is their ability to form biofilms, which has been directly related to the development of chronic infections with increased disease severity. A problem in the elimination of such complex structures (biofilms) is resistance to the drugs that are currently used in clinical practice, and therefore, it becomes imperative to search for new compounds that have anti-biofilm activity. In this context, nanotechnology provides secure platforms for targeted delivery of drugs to treat numerous microbial infections that are caused by biofilms. Among the many applications of such nanotechnology-based drug delivery systems is their ability to enhance the bioactive potential of therapeutic agents. The present study reports the use of important nanoparticles, such as liposomes, microemulsions, cyclodextrins, solid lipid nanoparticles, polymeric nanoparticles, and metallic nanoparticles, in controlling microbial biofilms by targeted drug delivery. Such utilization of these nanosystems has led to a better understanding of their applications and their role in combating biofilms.

Keywords: nanotechnology systems, microbial biofilms, anti-biofilm activity

Introduction

The incidence of infectious diseases continues to grow at an exponential rate each year and has a direct association with high rates of morbidity and mortality.1 The complex dynamics of infectious diseases has caught the attention of several scientists to investigate the possible causes that lead to the persistence and spread of acute and chronic infections.2 Acute infections are triggered by microbial cells that are in their planktonic forms; however, over time such microbes develop strategies to ensure their survival and adaptation to the stressful environments. This leads to the formation of a cohesive and strong community of cells that possess intercellular communication, known as biofilm.3,4

Microbial biofilms may be defined as heterogeneous communities (representing species diversity, for instance, a symbiotic association of bacteria and fungi) of aggregated, organized, and functional microbial cells, that remain embedded into the matrix of extracellular polymeric substances (EPS), which allows their irreversible adhesion to biotic or abiotic surfaces.5,6

The EPS matrix is primarily produced by the biofilm constituting microorganisms themselves; the former is especially composed of nucleic acids, extracellular proteins, phospholipids, teichoic acid, and exopolysaccharides. Mineral crystals, silt, milk residues, and blood components or dirt may also be present in EPS matrix, depending upon the conditions and locations in which biofilms are formed.7 Molecular interactions...
between EPS matrix and its various components and the constituents’ contribution toward the integrity of the matrix are not clearly understood yet. However, several EPS functions have been determined that have proved advantageous for biofilms.\(^8\)

The formation of biofilms, usually with the thickness of milli- or even micrometer order, naturally occurs around solid surfaces that are in contact with water, such as living tissues, medical devices, and water bodies/systems.\(^9\) In the environment and even on the abiotic surfaces, it is very common to find microbial biofilms with other commensal species, which are, therefore, called biofilm multispecies.\(^10\) Bacteria and fungi are both capable of forming biofilms on surfaces, but certain factors involved during the course of their formation differ from each other.

Studies conducted by Almeida and França\(^11,12\) and Percival et al\(^13\) demonstrated that biofilms are heterogeneous structures, and these consist of discontinuous phases on the support surface; that is, there may be an area with high density of cells along with areas where there may be no colonization. Furthermore, a great diversity in the morphology of these cells has been recorded; microbes may possess different shapes, such as filamentous, spiral, or rod, or they may exist as cocci or bacilli.\(^11,12\)

At present, the major concern of the medical research scientists working in this field is the adhesion and proliferation of the biofilm-forming microorganisms, inhibition of which may be a successful strategy to combat biofilm formation. Therefore, it is recommended to use stainless steel for manufacturing surgical devices, as this material is resistant to corrosion and fracture. All these measures are imperative owing to the capacity of biofilms to proliferate and get fixed on porous and rough surfaces.\(^13\)

In general, the development of a biofilm over a biotic or abiotic surface is a dynamic process that involves various steps, viz., adhesion, growth, and production of EPS matrix.\(^4\) A cycle indicating the five sequential stages involved in the formation of biofilm is depicted in Figure 1.

The five sequential stages are described below:

Stage 1: In this step, the deposition of free planktonic cells occurs by the arrival of microbes to the adhesion site. The presence of macromolecules, which form the constraint film as a substrate for the microbial cells, initiates biofilm formation.\(^14\)

Stage 2: This stage, known as the reversible adhesion phase, marks the beginning of adhesion of microbial cells and the communication process among them that is responsible for the subsequent steps. Although in small quantities, the EPS matrix can be observed in this stage.\(^15\)

Stage 3: Post initial adhesion to the surface, the cells that still have weak bonds with the surface consolidate the adhesion process by high EPS production that leads to an increase in their reproduction rate. The matrix also acts as a recycling center, as it is known to keep all the available lysed cell components including the DNA; thus, it may be considered as a genetic material reservoir to enable horizontal gene transfer and a source of nutrients, and provides protection against adverse conditions, such as drying, oxidation, exposure to biocides, antibiotics, certain metallic cations, and ultraviolet radiations, and immune responses. The production of the matrix represents the successful formation of biofilm communities, and propagation and survival of the cells in their local environment.\(^16,17\)

Stage 4: The maturation step or biofilm maintenance represents the dynamics between the microbial cells and the biofilm architecture. In this step, replication of the microorganisms occurs resulting in the generation of intense communication via signaling molecules (quorum sensing, QS). Such a mechanism enables individual cells to communicate and coordinate their actions by the production and detection of extracellular signaling molecules that are called the auto-inducers, which are responsible for the uptake of the substrate into the biofilm. Further, in this step, other microorganisms may also get adhered to form a multispecies biofilm.\(^18\)
Stage 5: In this stage, the detachment of the inside of the biofilm cells occurs. The high population density causes the release of the packed cells in an array to the external environment. Planktonic cells are released back into the surroundings, and these cells will start the cycle again.\(^\text{17}\)

The actual mechanism behind the biofilm formation is still unknown and will remain a hot topic of scientific research for many years. Nevertheless, it is known that the biofilm composition and the mechanisms involved are related to the resistance and virulence of the microbes.

According to the complexity of diseases associated with microbial biofilms, in this work we propose a structured review about the impact of microbial biofilms in the infectious diseases and present the main drug delivery systems based on nanotechnology as a strategy for the control and treatment of biofilms focusing in a treatment prospection.

**Bacterial biofilms: general aspects**

In the last 20 years, bacterial infections have posed a considerable threat to human health. The infections may appear as an isolated disease or systemic and primarily occur in hospital environments.\(^\text{19}\)

Among all the microorganisms, the bacterial species are the major biofilm producers, provided that the conditions are favorable, although some may have a greater ability than others. Most of the species demonstrate elevated growth rate, great adaptability, and competence for the production of substances and extracellular structures that protect the microbes in their habitat, and as per the characteristics, make these capable of perfectly colonizing any type of surface, even in adverse conditions.\(^\text{20}\)

Bacteria show two survival states, namely the planktonic form (individual/free cells) and the population aggregates (biofilms). The bacterial development in the planktonic form is an important phenomenon for the propagation of biofilms. Nevertheless, the survival of a biofilm as a defense mechanism is related to its sustenance, which is dependent upon its continued life cycle, if the biofilm offers safety against adverse environmental extrinsic factors.\(^\text{21,22}\)

There are certain advantages of bacterial biofilms, for example, the ecological participation in symbiotic relationships. The examples of this phenomenon are abundant in nature, and those exhibiting such relationships include diazotrophic prokaryotic bacteria that colonize vegetable roots and several other bacteria found in the digestive tract of the ruminants, where they promote the degradation and recycling of insoluble materials.\(^\text{21}\)

During the entire process of bacterial biofilm formation, there are complex factors involved, which have been poorly understood and have inspired the scientific community to analyze the whole dynamics of the complex microbial architecture. The contact of bacteria with biotic and abiotic surfaces is the first stage of biofilm formation, which is considered an important and complex process.\(^\text{23}\)

Considering only the abiotic surfaces, the initial attraction of planktonic bacterial cells to the surface seems to occur randomly by Brownian movement and gravitational force or in a guided way via chemotaxis and motility.\(^\text{24}\)

Motility is one of the extremely important characteristics since studies have shown that flagellated bacteria or the bacteria that have greater locomotion capacity form more complex and structured biofilms. Besides, the facility to migrate to other places gets increased.\(^\text{25}\)

Bacteria promote a variety of adhesion strategies to remain in contact with the fixation surface; after that, the microbes promote the release of EPS mixture, which increases their affinity for different types of surfaces, for example, porous, rough, and chemically heterogeneous surfaces.\(^\text{8}\)

The reversible adhesion occurs by nonspecific physicochemical interactions between the bacteria and the material, including the hydrodynamic forces, electrostatic interactions, van der Waals forces, and hydrophobic interactions.\(^\text{21,26}\)

In addition, the bacteria make use of some of their proteinaceous structures, for example, pili and fimbriae, in order to enhance the adhesion on surfaces. Besides, bacteria also have mechanisms to overcome the repulsive forces between the cell membrane and abiotic surfaces, especially in the presence of a conditioning film, which can easily be found in biomedical devices.\(^\text{8,27,28}\)

The composition of a conditioning film or an organic film is variable and depends upon the site of biofilm formation. Nevertheless, its basic constitution includes proteins, such as albumin, immunoglobulin, fibrinogen, and fibronectin.\(^\text{29}\)

Therefore, the film acts as a substrate for initial establishment of the biofilm. When adequate proximity and other predisposing factors are reached for appropriate elongation of biofilm formation, the bacterial cells promote enhanced production, release, and detection of self-inducing signaling molecules that regulate the biofilm formation.\(^\text{30,31}\)

As the adhesion process progresses, the accumulation of such signaling molecules results in the induction and transcription of specific genes, which regulate various bacterial functions, such as motility, virulence, and production of the matrix containing EPS, and consequently, exacerbate the development of biofilm (formation of stronger structures...
with dynamic complexity). The generation of EPS matrix facilitates colonization by other species as well. It is presumed that within a multispecies biofilm, the EPS increase the stability of the other species by mediating interactions between the polymers of different species.32

After the completion of reversible adhesion step, the irreversible adhesion phase occurs, which is due to the bacteria that still have weak interactions with the surface but manage to stick to the substratum due to the high production of EPS and cell signaling-based communication.33

The cell-to-cell communication process, referred to as QS, is found in several pathogenic bacteria which offers benefits such as the ability of sporulation, expression of virulence genes, DNA transfer, biofilm formation, and even antibiotic production. The molecular events in bacteria are partially controlled by QS via chemical signals, and such a mechanism of intracellular communication is dependent upon the population density within a biofilm.34

In bacterial biofilms, QS is a common phenomenon that favors the access to nutrients or more favorable environmental sites, thus allowing bacteria to induce defense responses against eukaryotic hosts while optimizing their ability to differentiate into most appropriate forms for their sustenance and survival in harsh environments.

The chronic bacterial infections are mainly related to the total biofilm formation cycle. Some of the major bacterial species, which are capable of triggering an infection in internal human organs, are _Pseudomonas aeruginosa_, the main causal agent of pneumonia and cystic fibrosis (CF),35 _Escherichia coli_, the causative microbe of the urinary tract infections (UTIs),36 and _Mycobacterium tuberculosis_, which causes human tuberculosis.37

In dental infections caused by _Streptococcus mutans_ (dental caries), the bacteria overcome the mechanical cleaning and antimicrobial treatments38 by forming biofilms. Since the amount of colonized bacteria in the oral cavity is high and the renewal of biofilm mass is easily achieved, _S. mutans_, very peacefully, acquires resistance against the drugs.

The implantation of medical devices, such as intravenous catheters, prosthetic heart valves, joint prosthetics, peritoneal dialysis catheters, heart pacemakers, and endotracheal tubes, is a viable alternative that ensures the maintenance of a patient’s life. However, the presence of bacterial biofilms on such medical devices has been identified as the foremost cause of clinical infections. The reason is the ease of formation of biofilms due to the inflammatory responses generated by the host, which further allow bacteria to adhere to the surfaces of the devices.23,39 The Gram-positive species, such as _Staphylococcus epidermidis_ and _Staphylococcus aureus_, colonize and form biofilms on medical devices, followed by Gram-negative species, like _P. aeruginosa_.40

The presence of biofilms on the cardiovascular electronic devices (CEDs) is very commonly witnessed in medical routine, which poses considerable risk to host’s health leading to a compromised immune system.41 The main bacterial species found in biofilms that are adhered to the CED surface belong to the genus _Staphylococcus_, for example, _S. epidermidis_ and _S. aureus_, and these correspond to about 70% of the total infections.41

Although _S. aureus_ is the major Gram-positive bacteria that forms biofilms on CED,42 the other species with same characteristics may also be related to the infections. A study by Madhavan et al43 evaluated the presence of Gram-positive cocci with a coagulase-negative profile in the blood samples of 74 patients, who were having CED implants and sequentially developed bacteremia. The results demonstrated a high prevalence of Gram-positive cocci, _S. aureus_, among the infectious cases.

Infectious endocarditis (IE) is classified as a major disease that originates from the incidence of biofilms, primarily formed by _S. aureus_ and _P. aeruginosa_. The establishment of such infection is directly related to the ability of the microorganisms to colonize in normal or abnormal valves or altered endothelial surfaces in the heart due to contamination of bloodstream of the host.44

As per the published reports, the episodes of IE caused due to the contamination by _P. aeruginosa_ are rare in comparison to those caused by _Staphylococcus_ spp., although to a lesser extent. However, the IE caused by the former tends to be more aggressive and is associated with a higher mortality rate than the latter.45 In contrast, the presence of biofilms formed by _P. aeruginosa_ is widely observed in cases of CF.46

Even though lifelong drug therapy is continued for patients, a high proportion of CF cases shows respiratory failure due to the chronic bacterial infection caused by the biofilm-induced inflammation of lungs.40,47

Chronic wounds (CWs) that behave as biofilm reservoirs are of major concern due to the risk of development of systemic infections. A CW is often colonized by a wide range of bacterial species that includes _S. aureus_, _P. aeruginosa_, _Enterococcus faecalis_, coagulase-negative _Staphylococci_, _Proteus_ spp., and anaerobic bacteria.46 _S. aureus_ has been considered to be the main agent of biofilm formation in CWs; however, there are reports that define the role of other bacteria, such as _P. aeruginosa_, as well in CW. The infection
caused by the latter reportedly reaches even the deeper layers of cells, thus aggravating the infection.49

The bacterial infections of female reproductive systems, such as bacterial vaginosis, are characterized by the disturbance of the vaginal microbiota. Lactobacilli that are normally commensal inhabitants of vagina are replaced due to significant increase in the concentration of a diverse set of bacteria, like Gardnerella vaginalis, Chlamydia trachomatis, and the bacterial species belonging to the genus Mobilancus,50 which are capable of developing biofilms in the female genital tract, thereby triggering chronic infections for which effective therapies are not available.51

Biofilms have also been reported in the auditory tracts causing infections, such as otitis media, which is characterized as a middle-ear infection and occurs especially in children. However, in certain cases of biofilms, particularly those formed by S. aureus, the infection may persist or reemerge frequently, and so such infections have been characterized as chronic otitis media (COM). Furthermore, in otolaryngology, the presence of biofilms in the ear canal has been associated with chronic sinusitis and COM with effusion.52

Gastric infections are still of great concern in gastroenterology, and particularly, oncology, owing to the association of Gram-negative bacteria Helicobacter pylori. This bacterium forms biofilm in order to ensure its integrity and survival53 and is frequently involved in chronic gastritis, functional dyspepsia, peptic or duodenal ulcer, and gastric cancer or lymphomas. Further, H. pylori also displays a survival profile in acidic environments; it remains intact in the stomach environment and promotes the destruction of the gastric mucosa making the organ sensitive and vulnerable to ulcerative lesions. In addition, it also blocks the sterilization process of food, thus interfering in the digestion process.54 The currently available therapy to eradicate this bacterium is complex and costly and presents severe side effects for the patients.55

Bacterial prostatitis is a UTI that affects males of all ages. A wide spectrum of bacterial species is involved in this disease; the acute phase exhibits the presence of E. coli (67%), P. aeruginosa (13%), Klebsiella spp. (6%), Gram-positive species (5%), and others (9%).56 In the chronic phase, the major aggravating factor is the presence of biofilms mainly of Gram-negative species, such as E. coli,57 which is responsible for most cases of chronic UTIs (E. coli uropathogenic), thus causing about 40% of the total hospital infections. Moreover, E. coli has been directly related to biofilm formation in urinary catheters, since direct contact of the bacterial cells with the urine can carry infection to internal organs which, in turn, may trigger local and even systemic infections.58

Thus, to devise novel therapeutic strategies, the scientific community has shifted focus to nanotechnology59–61 for the effective prevention of biofilm formation.62 In view of this, the present review draws the attention of the readers to the factors involved in adhesion of bacterial cells leading up to the establishment of biofilms.18,63

Fungal biofilms: general aspects

Fungal infections are a major issue for clinicians because of their high rate of incidence, especially in the immunocompromised patients. The risk factors that determine acquisition and high prevalence of fungal infections are host immunity, prolonged use of broad-spectrum antibiotics, long-term use of intravascular and urethral catheters, hemodialysis, treatment with corticosteroids, parenteral nutrition, the use of immunosuppressive anticancer drugs, and transplants among others.54,65

Fungi can dwell as biofilms in different body niches and subsequently induce infections. The site of infection depends on several factors, such as the amount and type of the available nutrients, host immune response, flow conditions and pH at the infection site, and substrate for cell adhesion and growth of the biofilm.66

The substrate for adhesion may be considered as a major factor for the formation of fungal biofilms. The materials that prevent adhesion of microorganisms with satisfactory in vitro results are used to manufacture medical devices. However, in the case of in vivo application of such models, several precautions, for example, a sepsis, need to be taken by the medical team, as contact of the device with the host body fluids, such as urine, saliva, and blood nutrients, provides favorable conditions for the formation of biofilms.57,68

The flow conditions may also play an important role in the development of fungal biofilms; for instance, the majority of the Candida spp. form biofilms at different flow rates of body fluids, which can be low (salivary flow: prosthetic stomatitis, intermittent (urinary catheters and vascular circulation), and rapid (bloodstream: fungal endocarditis).69,70 Furthermore, the flow is directly related to the transport of oxygen and nutrients that are essential for the development of biofilms.

The nutritional composition of different body niches varies; thus, some species develop better at some places compared to others; for example, blood is rich in nutrients, sugars, and proteins, so the biofilm development is high, which is further facilitated by high vascularization.66

The yeast species Candida albicans is known to frequently form biofilms and has been extensively studied by medical researchers, as it is the third most common cause
of intravascular infections (catheters) among the other types. However, in recent years, several other biofilm-forming species of the genus Candida, Candida tropicalis, Candida krusei, Candida glabrata, and Candida parapsilosis, that affect human body have been identified. Further, some other types of fungi, such as Malassezia spp., Pneumocystis spp., Histoplasma capsulatum, Cryptococcus neoformans, and Cryptococcus gatti, may also be associated with the infections in humans.

Yeasts and the cells of filamentous fungi may naturally occur as two different phenotypes, that is, the planktonic form (free cells) or the sessile form (biofilms). According to Ramage et al., the sessile phenotype involves the development of a group of strains on a polymeric matrix that is rich in water and allows passage of nutrients and oxygen. In addition, the polymeric matrix confers protection against the host immune response and prevents diffusion of antimicrobial drugs. Moreover, since fungi are eukaryotes and more complex than bacteria, the infections caused due to fungal biofilms remain difficult to diagnose and treat. The detailed analysis of such fungal biofilms has been done during the last years.

Since long, the sequences of fungal biofilm formation were thought to be same as in the case of bacteria. However, some studies conducted on the dynamics of genetics and the interactions of fungi, host, and environment have changed this scenario. Even though the overall process is the same, that is, primary adhesion, irreversible adhesion, maturation, and dispersion, depending on the characteristics of fungi, the dynamics involved is different.

The genus Candida has hyphae or pseudohyphae that are associated with the proliferation and development of the biofilms. The hyphal formation is critical for tissue invasion, as it is more resistant to phagocytosis in comparison to yeast. The virulence of C. albicans has been closely linked to the hyphae-forming ability. The hyphae of C. tropicalis are similar in morphology to C. albicans and are related to the invasion of oral epithelium. However, the ability of C. parapsilosis to invade oral epithelium is not related to the production of pseudohyphae. The hyphae promote the ability of the fungus to evade the host defense responses and thus serve as an essential factor for pathogenicity to form biofilms.

The models for the formation of fungal biofilms have been described by Douglas and Harding et al. that can be studied to understand the characteristics of fungal biofilms as well. The authors, in both the studies, used C. albicans as the model organism and reported that although the biofilm formed by the fungal species has several similarities with the bacterial biofilm, the presence of hyphae and pseudohyphae is the primary difference between the two. The proposed model includes five steps: (i) adsorption of yeast cells on a surface (biotic or abiotic), (ii) adhesion to the surface, (iii) formation of microcolonies (this step occurs after the initial growth and development of hyphae followed by the formation of microcolonies in the upper layer that predominantly comprises hyphae and production of EPS matrix), (iv) maturation of biofilm, and (v) dispersion of the mature biofilm cells and restart of the cycle.

A preliminary model for the sequential development of filamentous fungi has been proposed and consists of six steps: (i) adsorption of fungal propagules, such as spores, conidia, or hyphae, on solid surfaces (the authors compare this step with reversible adhesion stage of the bacterial biofilms); (ii) promotion of adherence and attachment by release of adhesive substances by germinating spores; (iii) stage 1 of formation of microcolonies (involves apical elongation and branching of hyphae during early growth and colonization of the surface with concomitantly increased production of EPS, which enables colony growth and adhesion to the substrate); (iv) stage 2 of formation of microcolonies or beginning of maturation, which involves the formation of compact hyphal network or mycelia and the formation of water channels that enable the passage of nutrients; (v) maturation phase, which is characterized by high production of fruiting bodies, spores, and other survival structures (this is an extremely important stage since aerial growth is a predisposing factor that allows the dispersion of yeast for new colonization); and (vi) dispersion or planktonic phase, which is similar to the dispersion step in the case of bacterial biofilms, the only difference being the release of spores and fungal filaments that act as propagules to initiate the next cycle.

During the formation of fungal biofilms, QS plays a significant role in the communication between the fungal cells. QS allows the development of the cooperative relationship between the cells that leads to the coordination of different cell behaviors and secretion of signaling molecules. However, there are certain signaling molecules involved in QS of fungal biofilms that need a special reference. A pioneering study by Hornby et al. demonstrated farnesol as the QS molecule that is responsible for inhibition of hyphae formation of C. albicans in the stationary phase. The study was important to understand the dynamics of C. albicans biofilms and inspired other researchers for further analysis.
Chen et al\textsuperscript{93} identified tyrosol to be a molecule that is involved in QS of \textit{C. albicans}; thus, these two molecules (farnesol and tyrosol) became well-known regulators of QS in the fungal species.\textsuperscript{98}

The control of fungal biofilms has been studied in the context of various fields, such as biotechnology, mycology, and medical research. The infection is complex and results in a poor response to a therapy. The knowledge of the mechanisms that are related to the dynamics involved in the architecture of biofilms is still insufficient.

Routinely, in hospitals, it is common to observe the development of fungal biofilms on the surfaces of medical devices, such as artificial valves, pacemakers, defibrillators, endotracheal tubes, dialysis devices, prosthetic joints, catheters, urinary/intrauterine devices, and contact lenses, which is classified as extreme risk to the patient’s health.\textsuperscript{94}

Since long, \textit{C. albicans} and \textit{Aspergillus fumigatus} have been considered as prevalent fungi in infectious cases. However, in recent years, other fungal species have also been observed to cause infection in clinical practice.\textsuperscript{94} \textit{Candida} spp. are often found in normal human biota which facilitates their interaction with the implanted biomaterials and surfaces of the host. The treatment of infections that are caused by the fungal biofilms can be inefficient, as the infection often recurs when the therapy ends, and thus, to overcome it, the removal of the device becomes necessary.\textsuperscript{95}

Invasive candidiasis (IC), especially candidemias (blood infection caused by \textit{Candida} spp.), is directly related to the presence of biofilms in body niches and abiotic surfaces of medical devices.\textsuperscript{96} Nowadays, candidemias have been reported as the fourth most common blood infections affecting more than 0.25 million people each year and are responsible for about 50,000 deaths. According to population-based studies, candidemias occupy the seventh position in the ranking of ten most prevalent infections of the human blood that may be fatal.\textsuperscript{97}

The prevalence of IC in hospitals is still a major concern, and the presence of biofilms makes this infection yet more complicated. A recent observational survey conducted over 16 years by Caggiano et al\textsuperscript{19} demonstrated that the infection by \textit{Candida} spp. was responsible for triggering heart failure in the patients of different age groups, who visited the Southern Hospital in Italy. The authors concluded that \textit{C. albicans} infection was the most prevalent among all the hospital departments. Moreover, the researchers identified that the incidence of IC caused by \textit{C. albicans} has exponentially elevated over the years and the non-\textit{albicans} cases have increased by 75%.

Although \textit{C. albicans} is the prevalent species among the cases of candidemias, the presence of other species has been observed in clinical settings causing concern, as certain species, such as \textit{C. krusei}, show high levels of resistance, which poses difficulty in the effectiveness of treatment.\textsuperscript{83} Candidemias are very common in neonates. Recently, Rongpharpi et al\textsuperscript{90} reported seven episodes of IC that were caused by \textit{C. krusei} in neonates, and extreme measures were taken to prevent the subsequent nosocomial infections.

In a recent case, D’Acuto et al\textsuperscript{91} identified \textit{C. parapsilosis} to be responsible for generalized IC in two neonates. The authors reported the use of drugs, fluconazole and amphotericin B, for control of the infection, but with no success. Therefore, voriconazole was used to treat the patients. However, voriconazole is classified as a drug of choice in the cases of systemic fungal infections that are caused by the species of the genus \textit{Aspergillus}.\textsuperscript{101} Furthermore, the drug exhibits several side effects, such as fever, gastrointestinal symptoms, reversible visual disorders, hepatitis, jaundice, and skin reactions.

The ability of \textit{Candida} spp. to develop and consequently form biofilms on mucous membranes of the human body is associated with various types of diseases, for example, vulvovaginal candidiasis (VVC). This disease is the most common cause of yeast infection in women with 80% of the cases caused by \textit{C. albicans}.\textsuperscript{102} However, in 20% of the cases, other non-\textit{albicans} species may be involved in the infectious processes.\textsuperscript{83} Moreover, the episodes of recurrent VVC are the most common cause of morbidity in women and predispose the development of cervical cancer.\textsuperscript{102,103} A major problem with fungal dissemination through VVC is the use of intrauterine contraceptive devices as the yeast can adhere to their abiotic surface by increasing the density of biofilms.\textsuperscript{104}

The respiratory tract is a perfect habitat for the formation of fungal biofilms. Respiratory fungal infections are chiefly caused by filamentous fungi. Invasive pulmonary aspergillosis (IPA) caused by airborne opportunistic fungi belonging to the \textit{Aspergillus} spp. (especially \textit{A. fumigatus}) is one example. IPA is characterized as severe pneumonia leading to the life-threatening invasion of the lung parenchyma and involving erosion in the vasculature leading to necrosis.\textsuperscript{105}

Intensive care unit (ICU) patients, especially those with chronic obstructive pulmonary disease, are at a risk of developing nosocomial IPA. Other species of \textit{Aspergillus}, viz., \textit{Aspergillus flavus}, \textit{Aspergillus niger}, \textit{Aspergillus terreus}, and \textit{Aspergillus nidulans}, are also known to trigger respiratory tract diseases in humans.\textsuperscript{106} \textit{A. fumigatus} may also be
associated with the cases of CF, although at a less frequency as compared to P. aeruginosa cases.\textsuperscript{107}

Another fungal respiratory disease, which is acquired by inhalation and has a high level of morbidity, is the histoplasmosis. It is one such respiratory fungal infection that accounts for about half a million cases per year only in the US.\textsuperscript{108} The ability of H. capsulatum to form biofilms remained unknown for a long time until identified by Suárez-Alvarez et al.\textsuperscript{109} The researchers showed that H. capsulatum yeasts could adhere to the cryosections of different organs and further provided evidence for an important mechanism of colonization and spread of the yeasts, which involves adhesion of the microorganisms to the host tissues, including the cell surface and extracellular components. Two years later, Pitangui et al\textsuperscript{110} demonstrated the in vitro ability of H. capsulatum to form biofilms and evaluated its invasion potential in cell lines.

The species of the genus Pneumocystis have been known as the major cause of infections in immunocompromised individuals, especially those who have HIV infection, as it is the major cause of lethal pneumonia in such cases.\textsuperscript{111} The main species associated with the development of pneumonia in humans are Pneumocystis jirovecii and Pneumocystis carinii,\textsuperscript{112,113} and the diseases caused by these generally involve the formation of biofilms in host’s lungs as the latter are suitable for reproduction provided the immunodeficient state of the patient.

Cryptococcosis is an opportunistic fungal disease that affects individuals from different age groups and is induced by Cryptococcus, especially C. neoformans and C. gatti.\textsuperscript{113} Both the species are responsible for triggering infectious processes, such as pneumonia, meningitis, and meningoencephalitis, which often cause the death of the affected patients, especially the transplant recipients and the immunocompromised ones.\textsuperscript{114} The progress of infection by these species involves the formation of biofilms in organs, such as the lungs and brain, that further complicates the therapy. The fungus possesses a polysaccharide capsule that completely surrounds it for the protection against phagocytosis by the cells of the immune system and has a direct relationship with the formation of biofilms.\textsuperscript{77} Fungal infections that are caused by Trichosporon spp. are also considered as a serious threat to humans as their diagnosis and therapy are also complex.\textsuperscript{115} Since long, the species of this genus have been detected in the cases of skin surface mycoses, such as “piedra”, which is white, and hypersensitivity pneumonitis. However, in recent decades, the medical field has associated the presence of Trichosporon spp. with the cases of systemic infections, especially in immunocompromised patients, such as those who are neutropenic and those who use central venous catheters.\textsuperscript{116}

The potential of certain uncommon Trichosporon spp. to form biofilms, mainly on intravenous catheters, is an issue that needs to be addressed soon. A study performed by de Pavia Fagundes Júnior et al\textsuperscript{117} demonstrated emerging cases of systemic infections that were triggered by Trichosporon asahii in ICU patients with heart failure. The species belonging to Trichosporon genus have a significant adaptation as recently reported by Mattede et al\textsuperscript{118} who confirmed the presence of these species in urinary catheters causing UTIs in ICU patients.

**Major factors leading to the development of antimicrobial resistance to biofilms**

Due to the genetic and structural dynamics of microbial biofilms, the treatment and eradication of the same seem to be complex. Certain resistance mechanisms that have been attributed to the sessile cells provide favorable conditions for survival and reproduction of microbes, making them less susceptible to elimination in contrast to the planktonic forms of the same microorganisms.\textsuperscript{79} The incidence of infections caused by microbial biofilms is a problem for the entire health care system and our society. Thus, efforts need to be continued in the pharmaceutical industry to develop novel products for the treatment of drug-resistant infections as there are only limited number of agents that are effective against biofilms.\textsuperscript{119}

Besides, the planktonic-form microbes employ mechanisms of resistance, such as the transfer of resistance genes by QS processes, the production of specific enzymes, and the evolution of natural mutations, and certain other processes explain the increased resistance by biofilms against the antimicrobial agents presently used in clinical practice.\textsuperscript{120}

The sessile state of microorganisms is crucial for the formation of biofilms. The success of an antibiotic treatment against an infection depends on the drug concentration at the site of infection which must be high enough to inhibit the proliferation of pathogenic microorganisms. Thus, the antibiotics must reach their target sites, in their active forms, in order to promote efficient binding to the target and finally interfere with the target function. In bacterial biofilms, the bacteria involved in the biofilm have high resistance to the antimicrobial agents that are effective against cells of the same species in planktonic form. The minimum inhibitory concentration (MIC) for the bacteria that are in biofilms may be 10–1,000 times greater than that for their planktonic form.\textsuperscript{121}
The main and most studied component of biofilms is the EPS, which has been classified as a physical and chemical barrier for the prevention of the action of antibiotics and protection against attack from the host immune response. In addition, EPS matrix provides resistance to thermal stress and mechanical strength, and limits the spread of sanitizers. The EPS matrix can react with sanitizers and promote inactivation as it is already known that certain chemical sanitizers (sodium hypochlorite) may have their action reduced or even eliminated in the presence of organic compounds, such as proteins, polysaccharides, and lipids. The microorganisms that exist as biofilms, particularly those dwelling in the inner layers, have low rates of metabolism and growth, and the EPS matrix acts as an adsorber that reduces the amount of drug available for the interaction with the biofilm microbes. In other words, the EPS matrix is capable of reducing the physical penetration of the antimicrobial agents. It can be understood in this way that the EPS matrix has pores that are very small and do not allow the larger drug molecules to pass through. Moreover, antibiotics may be adsorbed on the matrix itself owing to its hydrophilic and anionic nature, and an adequate amount of the antimicrobial drug does not reach the host tissues, which renders the therapy ineffective. Another aspect to consider is that the cells in the inner part of a biofilm often lack oxygen and nutrients, which forces the microbes to enter the stationary (or dormant) phase of growth. Thus, the microorganisms in the inner layers of biofilms become less susceptible to the action of chemotherapeutic agents since these agents require active growth of microbes. In this regard, it has been noted that within a biofilm, there are two microbial subpopulations with different phenotypes, one being active and the other inactive, metabolically. The former is on the surface and in contact with the external environment, and thus susceptible to antibiotics, while the latter is submerged in the EPS matrix within the biofilm with a slow rate of cell division, and thus remains resistant to the drugs.

According to Mah, a biofilm can acquire antibiotic resistance by natural mutation or acquisition of resistance genes (for conjugation, transformation, or transduction) as well. These genes may alter the expression of antibiotic-modifying enzymes leading to the production of modified proteins that may be the targets of antibiotics. Another phenomenon that may lead to the development of resistance to antibiotics and allow sustenance of cells even during the exposure to chemotherapeutic agents is the induction of reversible phenotypic state, primarily, due to the action of the efflux pumps. The expression of efflux pumps is mainly based on the expulsion of antimicrobial agents from the cells, which has been associated with increased resistance by microbial cells in biofilms, especially the Gram-negative bacteria. The system AcrAB-TolC, belonging to the family RND, is well characterized in E. coli and confers resistance to antibiotics, such as chloramphenicol, tetracyclines, and quinolones. However, these positively regulated genes are observed in the biofilm-forming cells; additionally, this mechanism may also be found in the strains of Salmonella typhimurium. In P. aeruginosa, the pumps, MexAB-OprM and MexCD-OprJ, appear to be involved in the resistance to macrolides and are directly related to the formation of biofilms.

The efflux pump mechanism is also observed in yeasts, such as C. albicans. The species has two types of efflux pumps: the first one is known as the ATP-binding cassette and the second type is the multidrug resistant (MDR). The genes that encode the pumps are upregulated during the formation and maturation of biofilms. Thus, it has been recorded that during the development of biofilms, the tolerance to fluconazole is quickly acquired and is mainly attributed to the expression of genes CDR1, CDR2, and MDR1.

Since biofilms represent the mixture of different types of microorganisms living as one community, it is likely that the resistance to multiple drugs may also occur. Not only the planktonic cells but the sessile microbes in biofilms also display specific resistance to antimicrobial agents. However, it is speculated that the classical individual mechanisms provide additional resistance to plaques, thus contributing to the overall resistance.

The currently available drugs have limitations, such as the inability to reach the biofilm microbes and even inefficiency in the cases of strains with a resistance profile. Novel alternatives have been applied for the control and eradication of biofilms. Thus, the present article intends to highlight the use of nanotechnology in drug delivery systems, which aims to enhance the pharmacological action of the bioactive compounds.

**Nanotechnology**

The term nanotechnology is related to the development and use of the systems and materials at the nanoscale size (1–1,000 nm) and the application of the concepts of manipulating materials at atomic, molecular, and macromolecular levels. The advantages of nanotechnology are mainly due to the unique characteristics of the materials at the nanoscale, which usually differ from the macrolevel characteristics of...
the materials. The change in the properties of materials is primarily due to the high surface area-to-volume ratio causing them to be highly reactive, affecting their mechanical and electrical properties. Thus, at the nanoscale, quantum effects dominate the behavior of the materials leading to interesting changes in their electromagnetic and optical properties.136

Nanotechnology has played important roles in various fields of science and contributed to the progress in physics, chemistry, engineering, medicine, and pharmaceutical industries. Owing to the ability to control mechanical, magnetic, optical, and catalytic properties of materials, nanotechnology has provided numerous benefits to all areas of science. Nanotechnology has substantially contributed to various fields, such as chemical synthesis, energy supply, food production, data storage, and biotechnology, to name a few. In medicine, nanotechnology gained importance due to its applications in the prevention, diagnostics, and treatment of various diseases.137

If one thinks of the disadvantages, the problem that is mostly encountered in the area of nanotechnology is the limited size of these materials, as these can penetrate any living system. Besides, enough investigations have not yet been conducted to allow commenting on the duration for which these materials may remain in the environment or the long-term consequences, which may entail accumulation of such materials in the ecological and living systems. Therefore, short-, medium-, and long-term effects of these nanomaterials are yet to be understood completely.138

Ranging from the combination of materials or devices with drugs and biomolecules, adding benefits like slow and controlled drug release, promoting greater efficiency of tissue penetration to greater protection against drug degradation, nanotechnology can be used to prevent, monitor, control, and cure diseases in several ways.137 At present, the main types of nanosystems used for the delivery of bioactive substances are liposomes (LIPs), microemulsions (MEs), nanoemulsions, cyclodextrins (CDs), solid lipid nanoparticles (SLNs), polymeric nanoparticles (PNs), and metallic nanoparticles (MNPs). The nanostructured systems have become promising tools for the treatment of infectious diseases, which are resistant to conventional treatments or persistent, improving the quality and expectancy of life of patients who suffer from such diseases.139

Due to the resistance mechanisms and biofilm formation, which these microorganisms eventually develop, the effectiveness of conventional antimicrobial agents is gradually declining. A promising strategy to overcome bacterial resistance is nanotechnology, which makes use of nanocarriers for delivery of drugs and biomolecules for the prevention and treatment of bacterial biofilms.140

The applicability of these systems in the treatment of biofilms is variable; however, nanotechnology-based drug delivery systems can facilitate drugs to directly interact with the complex structure of biofilms and exert action during the different stages of the biofilm formation.

Among the main abilities of these systems, two are predominantly studied by researchers, the direct interaction with planktonic cells (single cells) and the interaction with or denaturation of the EPS matrix. Figure 2 schematizes the interaction of a drug delivery system containing nanoparticles for drug release and their interaction in the biofilm formation stages.141

The direct interaction of nanoparticles with individual cells (Figure 2B) that are involved in the initial event of the process of biofilm formation (primary adhesion) may prevent the continuous process of formation, since the direct interaction between the nanoparticles and membranes of the microorganisms (eg, lipid nanoparticles, LIPs, and others) facilitates entry of the drug into the intracellular medium. This type of interaction can also be attributed during the final event (dispersion), where individual cells are detached from the polymer matrix making them able to restart the formation cycle.

The interaction of nanostructured systems such as nanomulsions LIPs, SLNs, lipoproteins and micelles, and others can also exert direct action on the biofilm polymer matrix (Figure 2C), promoting the fusion of the nanoparticles and

Figure 2 Interactions of nanoparticles based in drug delivery system on biofilm formation process.

Notes: Interaction of nanoparticles based in drug delivery systems in different stages of biofilm formation (A): adherence of microbial cells (1), reversible adhesion (2), irreversible adhesion (3), maturation (4), and detachment of cells (5). Nanoparticles interaction with single cells (B) and EPS matrix (C).

Abbreviation: EPS, extracellular polymeric substances.
provoking the denaturation of the proteins and the fusion of the lipid bilayers, facilitating the entry of the nanoparticles inside the biofilm to promote contact with the microbial cells.\textsuperscript{142,143}

**Liposomes**

Since the delivery of aqueous drugs through biological membranes is considered a challenge, it was devised to develop a system of similar nature to deliver such drugs. Some delivery systems, such as LIPs, were analyzed first to solve this problem.\textsuperscript{144} LIPs may be described as small spherical vesicles composed of a phospholipid bilayer or sphingolipids in the membrane that are used to deliver desired drugs at the target sites in the body. Figure 3 presents the structure of LIPs and the difference in comparison with a micelle.

These bilayer molecules can be made from cholesterol (CHOL) or other nontoxic phospholipids, and depending upon their composition, the properties, such as rigidity or fluidity and the charge of the bilayer, can be regulated.\textsuperscript{145}

According to Al-Jamal et al,\textsuperscript{144} LIPs are established nanometric systems that can be used to deliver antifungals, cytotoxic drugs, vaccines, and imaging agents. In addition, LIPs offer other advantages, such as biodegradability and biocompatibility, lower toxicity and doses, and the capacity of loading lipophilic and hydrophilic drugs, all of which make them more efficient than the other nanosystems. On the contrary, LIPs also exhibit certain limitations such as poor solubility, short half-life, and the possibility of oxidation and hydrolysis of phospholipids, besides their high costs.\textsuperscript{145}

Ahmed et al\textsuperscript{146} investigated the use of PEGylated LIPs to improve the interaction of drug with the bacterial biofilms. The authors prepared LIPs that comprised lipid mixtures by vesicle extrusion method and evaluated if their adsorption to the biofilms of *S. aureus* would improve after changing the concentrations of lipid and phospholipid-grafted poly(ethylene)glycol (PEG). The results demonstrated the “stealth” property of PEGylated LIPs that also applies to bacterial biofilms, which showed a considerable reduction.

Robinson et al\textsuperscript{147} investigated the difference between cationic and anionic LIPs, which were developed by the extrusion method, in order to deliver hydrophobic bactericide triclosan (TCS) to bacterial biofilms. Cationic LIPs with varying concentrations of dimyristoylphosphatidylcholine (DMPC), CHOL, and dimethyldioctadecylammonium bromide (DDAB) were tested against various bacteria, viz., *Streptococcus oralis*, *Streptococcus sanguis* C104, *Streptococcus gordonii*, *Streptococcus salivarius* DBD, and *S. salivarius* 8618. Among all, the best cationic LIP absorption was displayed by *S. salivarius* DBD, and the least absorption was displayed by *S. sanguis* C104. For the anionic LIPs, which were composed of DMPC and phosphatidylinositol (PI), the best results were observed against *S. sanguis* C104, while the strategy did not work against *S. salivarius* biofilm. The findings demonstrated the significance of electrostatic interactions for delivery of TCS, as the use of LIP formulations had a substantial effect on the mixed species of the biofilms.

Catuogno and Jones\textsuperscript{148} studied the antibacterial property of the solid-supported LIPs that were produced by zinc citrate particles against the biofilms formed by the most common oral bacterium, *S. oralis*. The authors tested the capacity of anionic (PI and 1,2-dipalmitoyl-sn-glycero-3-phosphocholine [DPPC], 4–19 mol\% PI) and cationic (DDAB, DPPC, and CHOL, 4–19 mol\% DDAB) LIPs that would be able to work as carriers for drugs, such as TCS, a lipid-soluble agent, and the aqueous-soluble penicillin-G. The results showed that the adsorption of LIPs to the bacterial biofilms was dependent on the concentrations of PI and DDAB used; however, an improvement in the antimicrobial efficacy was observed, as demonstrated by the better stability of the drug-loaded LIPs. The balance between attractive hydroxyl interactions and repulsive electrostatic forces that are associated with hydrogen bonding could explain the anionic LIP–biofilm interactions, while the cationic ones may be attributed to the electrostatic forces of attraction, and hence the content of positively charged phospholipids.

Drulis-Kawa et al\textsuperscript{149} developed anionic and cationic LIPs that encapsulated meropenem (MER) and compared the differences of interaction to *P. aeruginosa* biofilms. The authors revealed that the cationic LIPs, especially the ones that were composed of phosphatidylcholine (PC), 1,2-dioleoyloxy-3-trimethylammonium-propane (DOTAP),
and CHOL (at 5:2:3 mol/mol/mol ratio) or PC, 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine (DOPE), and stearylamine (SA) (at 4:4:2 mol/mol/mol ratio), had higher efficacy than the anionic ones, which may probably be explained by their ionic interactions with the bacterial cell envelope. It is also important, here, to highlight that these formulations showed MIC values that were less than the usual ones, besides demonstrating improved stability and diminished drug leakage. In order to investigate more deeply the reason why cationic LIPs presented a better interaction, further studies were conducted using 23 ATCC and clinical strains of *P. aeruginosa* that displayed varying susceptibility to certain antibiotics. The results demonstrated a high interaction of nanoparticles with the bacterial cells, specifically of the cationic LIPs that can be explained by the negatively charged external membrane of the microbes with the positively charged LIPs. In addition, some hydrophobic areas in the membrane may also contribute toward the enhanced interaction of the LIPs with the bacterial cell membranes.

Gubernator et al.\(^{150}\) studied in vitro antimicrobial activity of cationic LIPs (the compositions studied were PC/CHOL/DOTAP 3:4:3 and PC/DOPE/DOTAP 3:4:3) that harbored ciprofloxacin (cipro), MER, or gentamicin (GEN) against the Gram-negative clinical bacterial strains of *K. pneumoniae* and clinical strains of *E. coli*. The results confirmed that the MIC of the liposomal formulations was less than that of the free drug. The formulations presented the same or reduced MIC values in comparison to the free drugs. However, the liposomal GEN showed higher MIC values than the free drug against all the microorganisms, especially *P. aeruginosa*. The authors concluded that these differences could be due to the characteristics of the different drugs used, highlighting that the success of an antimicrobial treatment depends upon the complete formulation and not just on the delivery system employed for a drug.

Omri et al.\(^{151}\) investigated the effect of free and LIP-encapsulated polymyxin B (POLY B) against the ability of *P. aeruginosa* to produce pulmonary biofilms. LIPs were composed of DPPC and CHOL (2:1), and *P. aeruginosa* samples were obtained from the sputum of patients with CF. In general, the LIP formulations of the drug showed improved antibacterial activity, presenting reduced MIC values than the ones recorded for the free drug.\(^{152-154}\)

Alhajlan et al.\(^{155}\) performed an in vivo experiment on rats that had lung infections of *P. aeruginosa*. The study was conducted in four treatment groups, and all administrations were done via pulmonary route: (i) group 1, treated with saline; (ii) group 2, treated with free POLY B; (iii) group 3, treated with empty LIPs; and (iv) group 4, treated with POLY B loaded into the LIP composed of DPPC:CHOL in 2:1 molar ratio. The results showed that the animals that were treated with liposomal POLY B presented significantly reduced bacterial count in the lung tissues (3.7±0.4 log10 colony-forming unit [CFU]/pair of lungs), while the animals that received POLY B alone presented 5.1±0.2 log10 CFU/pair of lungs. In addition, the group 4 rats showed better accumulation of the drug in their lungs, around five times higher than the group 2.

Alipour et al.\(^{156}\) studied the effect of liposomal POLY B against *P. aeruginosa* and also against several other Gram-negative bacteria, such as *Bordetella bronchiseptica*, *E. coli*, *K. pneumoniae*, *Acinetobacter lwoffii*, and *Acinetobacter baumannii*. The findings by the research group highlighted that all the microorganisms showed a higher sensitivity profile when the drug was used in combination with LIPs in comparison to the free drug, especially the resistant strain, *P. aeruginosa* (PAM13641-1).

Alipour et al.\(^{157}\) also performed an in vivo experiment in rats with pulmonary *P. aeruginosa* infection. After the generation of the liposomal bismuth-ethanedithiol-loaded tobramycin, the authors administered it via intratracheal route into the infected rats and compared those rats to the ones which were treated with the free drug. The results indicated lung bacterial counts of 3 and 4.7 log10 CFU/lung in the rats treated with liposomal tobramycin and free tobramycin, respectively. Since the drug did not accumulate in kidneys of the LIP-encapsulated drug recipients, the authors suggested that LIPs ensured targeted delivery of the drug, which was not the case for the administration of the free drug.

Alhajlan et al.\(^{155}\) evaluated the efficacy and safety of liposomal clarithromycin (CAM) and its effect on virulence of *P. aeruginosa*. The LIPs were synthesized by the dehydration–rehydration technique with different compositions: positively charged liposomal formulation was composed of DDAB, DPPC, and CHOL in a ratio of 4:2:1; the negatively charged liposomal formulation was composed of dicetyl phosphate, DPPC, and CHOL in a ratio of 4:2:1; and the uncharged liposomal formulation was composed of DPPC and CHOL in a ratio of 6:1. The strains were obtained from the lungs of patients who suffered from CF. The results revealed that LIP-encapsulated delivery of CAM led to reduced MIC of 8 mg/L in contrast to 256 mg/L MIC in the case of naked drug delivery. Further, the use of LIPs also aided in the inhibition of the bacterial growth (as observed in biofilm assay) and cytotoxicity of A549 cells by 3–4 logs.

Table 1 summarizes the results of several studies related to the application of LIPs most used for control of microbial biofilms.
Table 1 LIPs used for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Applications of nanostructured formulations</th>
<th>Composition (w/w)</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>LIP+</td>
<td>NA</td>
<td>Improve the interaction of drug to the bacterial biofilms</td>
<td>DPPC, DDAB, CHOL, DPPE, and PEG-2000 (83.74:9.8:0–9)</td>
<td>Staphylococcus aureus</td>
<td>146</td>
</tr>
<tr>
<td>LIP+</td>
<td>NA</td>
<td>Improve the interaction of drug to the bacterial biofilms</td>
<td>DPPC, DDAB, CHOL, DPPE, and PEG-2000 (87.5:78.5:4.5:8.0–9)</td>
<td>S. aureus</td>
<td>146</td>
</tr>
<tr>
<td>LIP−</td>
<td>NA</td>
<td>Improve the interaction of drug to the bacterial biofilms</td>
<td>DPPC, PI, DPPE, and PEG-2000 (91:82:9:0–9)</td>
<td>S. aureus</td>
<td>146</td>
</tr>
<tr>
<td>LIP−</td>
<td>NA</td>
<td>Improve the interaction of drug to the bacterial biofilms</td>
<td>DPPC, PI, DPPE, and PEG-2000 (95.5:86.5:4.5:0–9)</td>
<td>S. aureus</td>
<td>146</td>
</tr>
<tr>
<td>TCS-LIP</td>
<td>Triclosan</td>
<td>Inhibition of growth of the mixed biofilms of the oral bacteria</td>
<td>DMPC, CHOL, and DDAB (64:23:13)</td>
<td>Streptococcus oralis, Streptococcus sanguis C104, Streptococcus gordonii, Streptococcus salivarius DBD, and S. salivarius 8618</td>
<td>147</td>
</tr>
<tr>
<td>Zn-TCS-LIP+</td>
<td>Triclosan</td>
<td>Antibacterial effect of LIPs adsorbed on solid particulate zinc citrate</td>
<td>DDAB (4%–19%), DPPC, and CHOL</td>
<td>S. oralis</td>
<td>148</td>
</tr>
<tr>
<td>Zn-TCS-LIP−</td>
<td>Triclosan</td>
<td>Antibacterial effect of LIPs adsorbed on solid particulate zinc citrate</td>
<td>PI (4%–19%) and DPPC</td>
<td>S. oralis</td>
<td>148</td>
</tr>
<tr>
<td>MER-LIP+</td>
<td>Meropenem</td>
<td>Kinds of bacterial structure or envelope properties have a major influence on the fusion process</td>
<td>PC, DOTAP, and CHOL (5:2:3)</td>
<td>Pseudomonas aeruginosa</td>
<td>149</td>
</tr>
<tr>
<td>MER-LIP−</td>
<td>Meropenem</td>
<td>Kinds of bacterial structure or envelope properties have a major influence on the fusion process</td>
<td>PC, DOPE, and SA (4:4:2)</td>
<td>P. aeruginosa</td>
<td>149</td>
</tr>
<tr>
<td>Cipro-LIP</td>
<td>Ciprofloxacin</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, CHOL, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, Klebsiella pneumoniae, and Escherichia coli</td>
<td>150</td>
</tr>
<tr>
<td>MER-LIP</td>
<td>Meropenem</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, CHOL, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, K. pneumoniae, and E. coli</td>
<td>150</td>
</tr>
<tr>
<td>GEN-LIP</td>
<td>Gentamicin</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, CHOL, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, K. pneumoniae, and E. coli</td>
<td>150</td>
</tr>
<tr>
<td>Cipro-LIP(2)</td>
<td>Ciprofloxacin</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, DOPE, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, K. pneumoniae, and E. coli</td>
<td>150</td>
</tr>
<tr>
<td>MER-LIP(2)</td>
<td>Meropenem</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, DOPE, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, K. pneumoniae, and E. coli</td>
<td>150</td>
</tr>
<tr>
<td>GEN-LIP(2)</td>
<td>Gentamicin</td>
<td>Improve in vitro bacterial activity</td>
<td>PC, DOPE, and DOTAP (3:4:3)</td>
<td>P. aeruginosa, K. pneumoniae, and E. coli</td>
<td>150</td>
</tr>
<tr>
<td>POLY B-LIP</td>
<td>Polymyxin B</td>
<td>Therapeutic effectiveness of the liposomal polymyxin B formulation administered intratracheally in a rat model of chronic lung infection</td>
<td>DPPC and CHOL (2:1)</td>
<td>P. aeruginosa</td>
<td>151</td>
</tr>
<tr>
<td>CAM-LIP+</td>
<td>Clarithromycin</td>
<td>Formulations’ ability to prevent biofilm formation, virulence factor production, and motility of clarithromycin-resistant strains of P. aeruginosa</td>
<td>DDAB, DPPC, and CHOL (4:2:1)</td>
<td>P. aeruginosa</td>
<td>155</td>
</tr>
<tr>
<td>CAM-LIP−</td>
<td>Clarithromycin</td>
<td>Formulations’ ability to prevent biofilm formation, virulence factor production, and motility of clarithromycin-resistant strains of P. aeruginosa</td>
<td>DCP, DPPC, and CHOL (4:2:1)</td>
<td>P. aeruginosa</td>
<td>155</td>
</tr>
<tr>
<td>CAM-LIP</td>
<td>Clarithromycin</td>
<td>Formulations’ ability to prevent biofilm formation, virulence factor production, and motility of clarithromycin-resistant strains of P. aeruginosa</td>
<td>DPPC and CHOL (6:1)</td>
<td>P. aeruginosa</td>
<td>155</td>
</tr>
</tbody>
</table>

**Abbreviations:** LIP, liposome; DPPC, 1,2-dipalmitoyl-sn-glycero-3-phosphocholine; DDAB, dimethyldioctadecylammonium bromide; CHOL, cholesterol; DPPE, 1,2-bis(diphenylphosphino)ethane; PEG, poly(ethylene)glycol; PI, phosphatidylinositol; TCS, trisalam; DMPC, dimyristoylphosphatidylcholine; MER, meropenem; PC, phosphatidylincholine; DOTAP, 1,2-dioleoyloxy-3-trimethylammonium-propane; DOPE, 1,2-dioleoyl-sn-glycero-3-phosphoethanolamine; SA, stearylamine; Cipro, ciprofloxacin; GEN, gentamicin; POLY B, polymyxin B; CAM, clarithromycin; DCP, dicetyl phosphate; Ref, reference; NA, not applicable.
MEs and nanoemulsions

MEs, as a drug delivery system, have become a highlight in the pharmaceutical research and industry. This is attributed to their potential to load a wide variety of molecules with different properties and deliver them efficiently to various parts of the body. MEs can be defined as transparent emulsions or phase-transition systems with either oil microdroplets dispersed in water or water microdroplets dispersed in oil. These are surrounded by an amphiphilic compound known as surfactant or amphiphile that is frequently associated with a suitable co-surfactant, thereby producing a thermodynamically stable system consisting of nanometric droplets in an internal phase. MEs are considered as reservoir systems; once the active constituent is isolated from the dissolution medium through a membrane or interface, it must be transposed for release. One of the characteristic features of MEs is their ability to separate from a dimensionally restricted environment and associate with different molecular compounds. Their versatile nature, such as low surface tension, in turn, improves the properties of the associated molecules, for example, solubility, stability, and bioavailability profile, consequently resulting in their increased absorption and permeation. When a surfactant is incapable of achieving nanometric droplets, it becomes indispensable to use a co-surfactant to enhance the surface area of droplets, thereby reducing the size of the particle and providing a better therapeutic effect.

MEs can be spontaneously generated, which makes them more advantageous than other delivery systems. In addition, MEs demonstrate an excellent thermodynamic stability, adequate appearance, and increased capacity to load drugs, which in turn result in their easy penetration through biological membranes, improved bioavailability, and reduced toxicity. Moreover, these systems serve as potent antimicrobial agents due to the inability of microbes to survive in pure fat or oil. In addition, some studies show that the structure of MEs contributes significantly to their antimicrobial activity by especially targeting the bacterial cytoplasmic membrane.

There are many advantages that make MEs to be considered as the first choice of nanotechnology-based systems. First, they can be prepared without any kind of energy once they are considered thermodynamically stable systems that can be spontaneously formed. Also, they are able to load both hydrophilic and lipophilic drugs, improving the efficiency and thus reducing total dose and side effects. Regarding their limitations, MEs are not a good choice when high-melting substances need to be solubilized. In addition, a high amount of surfactant is needed to stabilize droplets formed during the formation, and there are some problems related to their stability, which depends on pH and temperature levels.

Similar to MEs, nanoemulsions can be defined as heterogeneous systems in which one liquid (the inner phase) is dispersed in another (the outer phase) in the form of droplets in the presence of an emulsifying agent. The physicochemical properties of nanoemulsions are influenced by both their qualitative and quantitative compositions, and hence, they should be synthesized under strictly controlled conditions. Certain inconsistencies exist in the literature with respect to the concept of nanoemulsions in relation to MEs. Although both systems have similar structural and visual characteristics, they differ in their thermodynamic stability. Contrary to the nanoemulsions, MEs constitute thermodynamically more stable systems. Further, ironically, the droplet size of MEs is generally smaller than the nanoemulsions (as opposed to the nomenclature). Nevertheless, despite low thermodynamic stability, nanoemulsions are kinetically stable systems and exhibit several potentialities, such as drug delivery systems, especially for hydrophobic molecules with reduced water solubility. Figure 4 schematizes the organization of a micro- and nanoemulsion (oil-in-water and water-in-oil).

Numerous studies have been conducted by various groups on MEs and nanoemulsions. Ramalingam et al performed studies to analyze the efficacy of an oil-in-water nanoemulsion containing cetylpyridinium chloride (CPC) on dental unit waterline biofilms. The nanoemulsion was synthesized using soybean oil (25 vol%), deionized water (65 vol%), Triton X-100 (10 vol%), and CPC (1 wt%). The bacterial count was observed after exposing the formulation for 1, 6, 12, 24, 48, and 72 h to the biofilm formed by microorganisms, including Staphylococcus spp. All experiments resulted in a tremendous reduction in the number of microbial colonies, especially after 12 and 24 h (67 CFU/mL). However, the authors obtained even better results after 48 and 72 h of exposures when no visible colonies could be observed.

Figure 4 Micro- and nanoemulsion structure: oil-in-water and water-in-oil.
In 2011, Ramalingam et al\textsuperscript{169} tested the antimicrobial activity of a nanoeulsion on cariogenic \textit{S. mutans} to control biofilm formation. The results displayed an inhibition of \textit{S. mutans} grown in the concentrations ranging from 1:100 to 1:10,000. In addition, mature biofilms of the microorganism were significantly reduced after the treatment with the formulation.

In 2012, Ramalingam et al\textsuperscript{168} evaluated the activity of CPC loaded onto a nanoeulsion against planktonic \textit{S. mutans}, \textit{Lactobacillus casei}, \textit{Actinomyces viscosus}, \textit{C. albicans}, and a mixed culture using microdilution technique and biofilm assay. The results demonstrated that compared to the components alone, the application of the formulation exhibited a better and enhanced activity against microorganisms, both individually and in mixed culture. Teixeira et al\textsuperscript{170} studied the ability of MEs and nanoemulsions to inhibit the synthesis of biofilms by \textit{S. aureus NCTC 1803}, \textit{S. typhimurium PSB 367}, \textit{Listeria monocytogenes}, \textit{P. aeruginosa}, and \textit{E. coli O157:H7}. Although both systems were capable of removing biofilms of \textit{E. coli}, \textit{S. aureus}, and \textit{S. typhimurium}, ME was also effective against \textit{P. aeruginosa}, a nosocomial agent with very high resistance to antimicrobial agents. However, \textit{L. monocytogenes} was found to be resistant to both the systems.

Liu and Huang\textsuperscript{171} developed curcumin (CUR)-loaded myristic acid-based MEs to study their antibacterial activity against skin infections caused by \textit{S. epidermidis} BCRC-11030 (ATCC 12228). During formulation, myristic acid, a middle-chain fatty acid, was mixed dropwise with isopropanol (1:2) to improve the solubility followed by the preparation of surfactants, namely Tween\textsuperscript{80} and F127. The components were mixed for 10 min leading to the formation of transparent MEs. Myristic acid was chosen as one of the constituents because it demonstrated the best antibacterial activity compared with other fatty acids. Its antibacterial activity was found to be even higher than azelaeic acid, commonly used to treat acne vulgaris. The results showed that before being loaded into the ME, CUR was 12 times less effective against the bacterium, but showed an MIC\textsubscript{50} of 0.86 µg/mL after being loaded into the ME. In addition, when CUR was loaded together with myristic acid into the ME, it produced a synergistic inhibitory effect against \textit{S. epidermidis}, implying that myristic acid may serve as an efficient vehicle for ME to load CUR.

Instead of encapsulating antimicrobial agents into an ME, some studies have demonstrated the use of MEs that are directly composed of components exhibiting antimicrobial properties so as to augment their effectiveness against microbial biofilms. Al-Adham et al\textsuperscript{172} evaluated the effect of MEs as anti-biofilm agents after validating their effects against planktons. They formulated an ME containing 15% Tween 80, 6% pentanol, and 3% ethyl oleate in water and checked its efficiency against established \textit{P. aeruginosa} biofilm. The results exhibited three log-cycle reductions in viabilities when biofilms were treated with an ME as compared to the control treatment that resulted in only one log-cycle reduction.

Table 2 summarizes the results of several studies related to the application of MEs and nanoemulsions most used for control of microbial biofilms.

### Table 2 MEs and nanoemulsions used for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Applications of nanostructured formulations</th>
<th>Composition</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>CPC-Na</td>
<td>Cetylpyridinium chloride</td>
<td>Improved efficacy against microorganisms involved in the caries process in excess of the efficacy of the unemulsified components</td>
<td>Soybean oil (25 vol%), deionized water (65 vol%), Triton X-100 (10 vol%), and CPC (1 wt%)</td>
<td>Streptococcus mutans, Lactobacillus casei, Actinomyces viscosus, and Candida albicans</td>
<td>168, 169</td>
</tr>
<tr>
<td>Nano</td>
<td>NA</td>
<td>Capacity to destroy biofilms formed by different pathogens</td>
<td>Soybean oil (16%), tri-n-butyl phosphate (2%), Triton X-100 (2%), and water</td>
<td>Staphylococcus aureus NCTC 1803, Salmonella typhimurium PSB 367, Listeria monocytogenes, Pseudomonas aeruginosa, and Escherichia coli O157:H7</td>
<td>170</td>
</tr>
<tr>
<td>Micro</td>
<td>NA</td>
<td>Capacity to destroy biofilms formed by different pathogens</td>
<td>Ethyl oleate (3%), n-pentanol (6%), Tween\textsuperscript{80} (15%), and water</td>
<td>\textit{S. aureus NCTC 1803}, \textit{S. typhimurium PSB 367}, \textit{L. monocytogenes}, \textit{P. aeruginosa}, and \textit{E. coli O157:H7}</td>
<td>170</td>
</tr>
<tr>
<td>CUR-ME</td>
<td>Curcumin</td>
<td>Inhibit the pathogen Staphylococcus epidermidis on the skin</td>
<td>Myristic acid and isopropanol (1:2), surfactants (Tween\textsuperscript{80} and F127), and water</td>
<td>\textit{S. epidermidis}</td>
<td>171</td>
</tr>
<tr>
<td>ME</td>
<td>NA</td>
<td>Anti-biofilm effects of pharmaceutical microemulsions</td>
<td>15% Tween\textsuperscript{80} (15%), pentanol (6%), and ethyl oleate (3%) in water</td>
<td>\textit{P. aeruginosa PA01}</td>
<td>172</td>
</tr>
</tbody>
</table>

**Abbreviations:** ME, microemulsion; CPC, cetylpyridinium chloride; CUR, curcumin; Ref, reference; NA, not applicable.
**Cyclodextrins**

Cyclodextrins (CDs) are a family of cyclic oligosaccharides that are obtained from starch-containing materials by enzymatic means. CDs were discovered in 1891 by the French researcher, Villiers, who noticed the ability of these molecules to form crystals. Natural CDs are formed by the treatment of starch with amylase from *Bacillus macerans*, producing at least six glucose units. Among them, α-cyclodextrin (α-CD, six units), β-cyclodextrin (β-CD, seven units), and γ-cyclodextrin (γ-CD, eight units) are the most common members (Figure 5).

The external surface of the CD that offers protons (H1, H2, H4, H6) provides it a hydrophilic nature, whereas its cavity displays hydrophobic characteristics due to the presence of rings of C–H groups (H3 and H5) together with a ring of oxygen atoms forming glycosidic linkages. Therefore, CDs are truncated cone-shaped molecules with a relatively hydrophobic cavity and an external hydrophilic surface that can form supramolecular structures (inclusion complexes, ICs) with various molecules, mainly small molecules. The interactions, such as van der Waals, hydrophobic, and hydrogen bonding, contribute to the driving forces of IC formation, which can modify the biological, physical, and chemical properties of guest molecules.

Due to their ability to form ICs, CDs are considered as efficient drug-carrying and drug-delivering systems. Besides, CDs are excellent solubilizers and physical and chemical stabilizers, and provide protection to the guest molecules from degradation in the gastrointestinal tract, thereby enhancing drug bioavailability. CDs have been used as a pharmaceutical excipient, mainly to solubilize drugs with poor solubility in an aqueous environment through the synthesis of drug–CD complexes. The naturally occurring CDs have been used at a large scale in the evaluation and development of pharmaceutical formulations. However, their applications suffer from certain limitations; for example, β-CD exhibits a restricted solubility in water. Thus, new approaches to improve the action of CDs as drug carriers, such as the use of several chemically modified CDs, are required. CD derivatives are classified into three groups: hydrophilic, hydrophobic, and ionizable derivatives. Each group performs a specific action. For example, in the hydrophilic group, 2,6-dimethyl-β-CD, 2,3,6-trimethyl-β-CD, 2-hydroxypropyl-β-CD (HP-β-CD), and maltosyl-β-CD can enhance the water solubility of poorly water-soluble substances. Similarly, molecules within the hydrophobic group, such as 2,6-diethyl-β-CD, are capable of delaying the dissolution rate of poorly water-soluble drugs. Besides, the ionizable derivatives, such as O-carboxymethyl-β-CD (CM-β-CD), O-carboxymethyl-O-ethyl-β-CD, β-CD sulfate, and sulfobutyl ether β-CD, can improve the inclusion ability and decrease the localized irritation caused by drugs.

The properties exhibited by CDs are relevant for pharmaceutical area given the fact that they can improve the

![Figure 5: Structure and properties of α-, β-, and γ-cyclodextrin.](https://www.dovepress.com/.../176-178)
solubility of water-soluble drugs, augment the chemical and physical stability, and provide protection to the guest molecules from the action of molecules and enzymes present in the gastrointestinal tract.\textsuperscript{186,187} However, there are limitations for parenteral formulation with CD, based on the type of CD used. For example, only $\alpha$-CD can be used in parenteral formulation; $\beta$-CD affects the urinary volume and kidney and liver enzymes\textsuperscript{188} and $\gamma$-CD exhibits nephrotoxicity, and hence, both these CDs are unsuitable for parenteral use.\textsuperscript{189} Besides, the type and concentration of CD–drug complex also affect the encapsulation efficiency\textsuperscript{190} and the bioavailability of the drugs.\textsuperscript{191} The other limitation with the native CD is the difficulty in the incorporation of large and hydrophilic substances. Thus, many chemical modifications have been performed to solve this disadvantage.\textsuperscript{192}

In the past years, several alternatives have been implemented and utilized to control and treat various microbial biofilms.\textsuperscript{187,189–195} The characteristics exhibited by CDs, including lower toxicity, increased solubility of drugs, and an ability to act as stabilizers, make them eligible agents as drug carriers. These above-mentioned properties have attracted interest in the utilization of CDs to boost the action of drugs against bacterial and fungal biofilms.\textsuperscript{196–198}

Brackman et al\textsuperscript{190} developed gauzes functionalized with HP-$\beta$-CD to load vancomycin (VAN), hamamelitannin (HAM) (a natural product isolated from \textit{Hamamelis virginiana}), and a quorum sensing inhibitor (QSI) of \textit{S. aureus}. The authors evaluated the anti-biofilm activity of HP-$\beta$-CD complex against \textit{S. aureus} and \textit{P. aeruginosa} in vitro in a CW model. The functionalized HP-$\beta$-CD gauzes inhibited QS and the formation of biofilms when compared with nonfunctionalized gauzes. The results demonstrated the utilization of HP-$\beta$-CD-functionalized gauzes containing a combination of VAN and HAM to be a promising approach against both single-species and mixed-species biofilms. Hence, HP-$\beta$-CD-functionalized gauzes may serve as an alternative to the treatment and prevention of wound infections caused by bacteria.

In a study performed by Garcia-Fernandez et al,\textsuperscript{197} HP-$\beta$-CD was utilized for the loading and release of benzalkonium chloride (BzCl), for inhibiting \textit{S. aureus} biofilm. The authors assessed the utilization of CDs to endow hydrogels and gauzes to increase and maintain the antimicrobial and delivery capacity for several hours. In this study, the CDs displayed an efficient delivery of BzCl, which in turn could successfully inhibit biofilm formation in the initial stage. They also decreased the number of living microbial cells in preformed biofilms in an in vitro CW biofilm model. Based on the results, the researchers concluded that BzCl-loaded functionalized HP-$\beta$-CD gauzes may be employed for the prevention and treatment of infectious wounds, although in vivo assays are necessary to confirm the findings.

Fidaleo et al\textsuperscript{190} evaluated the anti-biofilm activity of TCS complexed with HP-$\beta$-CD and CM-$\beta$-CD. The two complexes (TCS–CD) were observed to exhibit anti-QS activity by interfering with cell-to-cell communication mechanisms in \textit{Chromobacterium violaceum} model system. Thus, the authors suggested the use of TCS–CD complexes for producing antimicrobial hydrogels or hydrophilic coatings for medical devices to inhibit biofilm formation on the devices and promote the release of antimicrobial agents.

A recent study demonstrated the potential of HP-$\beta$-CD to clean reverse osmosis membranes contaminated and fouled by \textit{P. aeruginosa}. The CD, HP-$\beta$-CD, removed the biofilm forming complex with the EPS of bacteria. Although the mechanism of removal of the biofilm by HP-$\beta$-CD was unknown, the authors attributed it to the structural distribution of HP-$\beta$-CD on the surface of the biofilm. In addition, the authors believed that there could be a destabilization of the biofilm due to the generation of free energy, making the detachment an energetically propitious process.\textsuperscript{191}

Iordache et al\textsuperscript{198} developed a thin film consisting of $\beta$-CD complexed with usnic acid, a dibenzofuran with pharmacological properties, to improve the release of a drug into the bacterial cells. The thin film was observed to be successful in preventing the adhesion of cells and development of \textit{S. aureus} biofilm at all stages. Besides, the film demonstrated good biocompatibility, an attribute that may lead it to serve as an alternative for promoting medical surfaces capable of preventing microbial colonization.

Shanmuga Priya et al\textsuperscript{200} formulated a solid complex with $\beta$-CD and drug rifabutin (RFB) to increase the solubility and antimicrobial activity of the drug. The conjugation to the solid complex enhanced the effectiveness of the drug in reducing the biofilm formation by \textit{E. faecalis}, \textit{S. aureus}, \textit{Proteus vulgaris}, and \textit{P. aeruginosa}, when compared to the control. The study related the in vitro anti-biofilm action of pure RFB and its $\beta$-CD complex against both Gram-positive and Gram-negative microorganisms.

$\beta$-CDs have been used for the stable delivery of silver nanoparticles (AgNPs) due to their physicochemical properties, such as hydrophilicity, high molecular weight, the presence of a large number of hydrogen donors and acceptors, and inclusion capacities.\textsuperscript{203,204} A recent study involving AgNPs–$\beta$-CD complex demonstrated an excellent antibacterial activity of the complex, which inhibited the formation of
biofilm by *S. epidermidis*, the common bacteria isolated from medical devices, such as catheters, prosthetic implants, and intrauterine devices. In addition, the AgNPs–β-CD complex was more effective than AgNPs. The authors used different concentrations of silver (Ag, 8 and 16 ppm) on biofilm of *S. epidermidis*; the AgNPs–β-CD complex inhibited biofilm formation to more than 90%, whereas AgNPs could inhibit only 10%–15%.204

In a recent work performed by Oprea et al.,205 the anti-biofilm activity of zinc oxide-β-CD-cefepime (ZnO-CD-Cfp) complex against *E. coli* was assessed. The complex was selected and evaluated owing to its enzymatic resistance to β-lactam antibiotics. ZnO nanoparticles are used as antibacterial agents; however, the primary problem with them is their poor solubility in water. Thus, the use of CDs can enhance the solubility and bioavailability of these nanoparticles. Besides, the authors demonstrated that ZnO/CD complex displays an efficient release of Cfp, consequently leading to an improvement in the anti-biofilm activity. The results also demonstrated that the obtained coatings can prevent the biofilm formation and adhesion after 24–48 h, and the complex also demonstrated inhibitory effect against mature biofilm on the coated surfaces.

The last few years have witnessed studies involving CDs to improve the delivery of drugs to control fungal biofilms. Nava-Ortiz et al.206 used medical devices designed from polyethylene and polypropylene functionalized with HP-β-CD and β-CD to incorporate miconazole (MICO). Since the drug MICO is insoluble in water, CDs serve as an efficient option to assist the solubilization, thereby providing adequate bioavailability. Besides, the surface functionalization involved the grafting of glycidyl methacrylate after pre-irradiation with oxidative γ-rays. These complexes demonstrated positives results, including a reduction in microbial adhesion and prevention of the development of *Candida* biofilm.

In another work, a topical formulation of amphotericin B (AmB) solubilized in γ-CD (AmB–CD complex) inhibited the biofilm formation by *Candida* spp., *C. albicans*, *Candida dubliniensis*, *C. glabrata*, *Candida guilliermondii*, and *C. parapsilosis*, except for *C. krusei*, which was resistant to AmB–CD. The other yeasts, such as *Saccharomyces* and *Trichosporon*, were found to be sensitive to the complex. The AmB–CD, compared to AmB dissolved in dimethylsulfoxide, exhibited a high penetration through these biofilms. Despite the suggestion by the authors that the AmB–CD could be employed in catheters and prostheses to prevent fungal infections of bloodstream, a requirement for further toxicological and clinical studies is warranted before its use in humans.207

In another study, the authors elaborated gold surfaces functionalized to anidulafungin (ANF) or thymol (THY) with HP-β-CD and randomly methylated β-CD (RAMEB) complexes. Both antifungal complexes displayed similar anti-biofilm action. The results indicated that CDs improved the solubility of ANF, and together, the complexes inhibited the adherence of *C. albicans* biofilm. In addition, THY–CD complex could potentially eliminate the biofilm synthesized by *C. albicans*. However, a considerable difference exists between THY and ANF molecules; ANF is more than seven times larger than THY and cannot be completely incorporated into the cavity of CD, while THY is a small molecule. Thus, the THY molecule loaded into RAMEB could interact efficiently with the cells and prevent the growth of *C. albicans*.177

Table 3 summarizes the results of several studies related to the application of CDs most used for control of microbial biofilms.

### Solid lipid nanoparticles

SLNs are colloidal drug delivery systems in which the matrix is formed by solid lipids and usually consists of physiologically well-tolerated substances; thus, the system offers low cytotoxicity. The structure of SLNs is very similar to nanoemulsions, but their core is formed by lipids that are solid at room temperature. This structural rigidity provides less mobility to the incorporated drug, which is manifested in terms of a better control during the release of drugs. The production of SLNs can be easily scaled to the level of pharmaceutical industry.140 SLNs comprise one or more solid lipids, and their structure is stabilized by the presence of surfactants.

SLNs show the properties of different colloidal carriers. For instance, these are physiologically acceptable compounds like emulsions and LIPs and capable of yielding a controlled release of drugs from lipid matrices such as PNs. The mentioned advantages include the incorporation of lipophilic and hydrophilic drugs, physical stability, controlled drug release, biocompatibility, potential for site-specific drug delivery, improved drug stability, better formulation stability, ability to freeze-dry and reconstitute, high drug payload, controllable particle size, avoidance of carrier toxicity, low production cost, and easy scale-up and manufacturing.208 Figure 6 schematizes the SLNs structure for drug delivery.

However, certain limitations are also associated with the SLN system. These include limitation of drug load due to the solubility of the drug in the solid lipid, drug expulsion phenomenon when lipid crystallizes to the stable β-form,
Table 3 CDs for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Applications of nanostructured formulations</th>
<th>Composition</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>BzCl-HP-β-CD</td>
<td>Benzalkonium chloride</td>
<td>The ability to take up antiseptics and sustain their delivery for several hours</td>
<td>HP-β-CD</td>
<td>Staphylococcus epidermidis and Escherichia coli</td>
<td>197</td>
</tr>
<tr>
<td>UA-CD</td>
<td>Usnic acid</td>
<td>Improve the release of a drug into the bacterial cells</td>
<td>γ-cyclodextrin</td>
<td>Staphylococcus aureus</td>
<td>198</td>
</tr>
<tr>
<td>VAN-HP-β-CD</td>
<td>Vancomycin</td>
<td>Anti-biofilm activity of HP-β-CD complex</td>
<td>HP-β-CD</td>
<td>Pseudomonas aeruginosa and S. aureus</td>
<td>199</td>
</tr>
<tr>
<td>HAM-HP-β-CD</td>
<td>Hamamelitannin</td>
<td>Anti-biofilm activity of HP-β-CD complex</td>
<td>HP-β-CD</td>
<td>P. aeruginosa and S. aureus</td>
<td>199</td>
</tr>
<tr>
<td>TCS-HP-β-CD</td>
<td>Triclosan</td>
<td>Influence on its antibacterial and anti-QS activity</td>
<td>HP-β-CD</td>
<td>E. coli and S. aureus</td>
<td>200</td>
</tr>
<tr>
<td>TCS-CM-β-CD</td>
<td>Triclosan</td>
<td>Influence on its antibacterial and anti-QS activity</td>
<td>CM-β-CD</td>
<td>E. coli and S. aureus</td>
<td>200</td>
</tr>
<tr>
<td>HP-β-CD</td>
<td>NA</td>
<td>Removed the biofilm-forming complex with the extracellular polymeric substances</td>
<td>HP-β-CD</td>
<td>P. aeruginosa</td>
<td>201</td>
</tr>
<tr>
<td>RFB-β-CD</td>
<td>Rifabutin</td>
<td>Improvement of solubility and antimicrobial activity of rifabutin</td>
<td>β-CD</td>
<td>Enterococcus faecalis, S. aureus, Proteus vulgaris, and P. aeruginosa</td>
<td>202</td>
</tr>
<tr>
<td>AgNPs-β-CD</td>
<td>AgNPs</td>
<td>Inhibit the formation of biofilm</td>
<td>β-CD</td>
<td>S. epidermidis</td>
<td>204</td>
</tr>
<tr>
<td>ZnO-Cfep</td>
<td>ZnO-NPs and cefepime</td>
<td>Lead to an improvement in the anti-biofilm activity</td>
<td>β-CD</td>
<td>E. coli</td>
<td>205</td>
</tr>
<tr>
<td>MICO-HP-β-CD</td>
<td>Miconazole</td>
<td>Improve water solubility</td>
<td>HP-β-CD</td>
<td>Candida albicans</td>
<td>206</td>
</tr>
<tr>
<td>MICO-β-CD</td>
<td>Miconazole</td>
<td>Improve water solubility</td>
<td>β-CD</td>
<td>C. albicans</td>
<td>206</td>
</tr>
<tr>
<td>AmB-γ-CD</td>
<td>Amphotericin</td>
<td>Formulate a topical amphotericin preparation</td>
<td>γ-CD</td>
<td>C. albicans, Candida dubliniensis, Candida glabrata, Candida guilliermondii, Candida parapsilosis, and Candida krusei</td>
<td>207</td>
</tr>
<tr>
<td>ANF-HP-β-CD</td>
<td>Anidulafungin</td>
<td>Improve the solubility of ANF</td>
<td>HP-β-CD</td>
<td>C. albicans</td>
<td>177</td>
</tr>
<tr>
<td>THY-HP-β-CD</td>
<td>Thymol</td>
<td>Improve the solubility of THY</td>
<td>HP-β-CD</td>
<td>C. albicans</td>
<td>177</td>
</tr>
<tr>
<td>ANF-β-CD</td>
<td>Anidulafungin</td>
<td>Improve the solubility of ANF</td>
<td>β-CD</td>
<td>C. albicans</td>
<td>177</td>
</tr>
<tr>
<td>THY-β-CD</td>
<td>Thymol</td>
<td>Improve the solubility of THY</td>
<td>β-CD</td>
<td>C. albicans</td>
<td>177</td>
</tr>
</tbody>
</table>

Abbreviations: CDs, cyclodextrins; BzCl, benzalkonium chloride; HP-β-CD, 2-hydroxypropyl-β-CD; UA, usnic acid; VAN, vancomycin; HAM, hamamelitannin; TCS, triclosan; QS, quorum sensing; CM-β-CD, O-carboxymethyl-β-CD; RFB, rifabutin; AgNPs, silver nanoparticles; Cfep, cefepime; ZnO-NPs, zinc oxide nanoparticles; MICO, miconazole; AmB, amphotericin B; ANF, anidulafungin; THY, thymol; Ref, reference; NA, not applicable.

and particle concentration in the aqueous dispersions ranging from about 1% to a maximum of only 30%.209

Singh et al,210 with an aim to increase antimicrobial activity against S. aureus biofilms, developed SLNs containing cefuroxime axetil (CA). The authors used stearic acid (SA) as a single lipid and SA and tristearin (TRI) as a binary lipid; the emulsification–evaporation method was used for the formation of SLNs. The nanosystem displayed a low efficiency of encapsulation. To improve this parameter, an SLN formulation (CA-SLN) was developed using binary lipid that exhibited an encapsulation efficiency of 70.62%±0.82%. The high efficiency of SLNs consisting of binary lipids was attributed to the large deformation of the crystal structure of SA in the presence of TRI, leading to the formation of cavities in its structure and efficient accommodation of drug molecules. The size of the formed nanoparticles was in the range of 279.2±28.5 nm, and the zeta potential (ZP) was −23.58 to −25.95 mV. The in vitro analysis of the release of free CA displayed a 99.68% release in just 2 h, whereas CA-SLN exhibited a 53.68% release in 2 h and 95.58% within 12 h, indicating that nanoparticles provide an additional feature of prolonged drug release owing to the diffusion of the drug through the lipid matrix of the nanoparticles. The in vitro anti-biofilm studies exhibited an inhibition zone of 9 mm for the free drug, whereas the treatment with CA-SLN created an inhibition zone of 13 mm. According to the
authors, the above-mentioned observation was attributed to the enhanced diffusion and accumulation of CA-SLN in the polysaccharide matrix of the biofilm/microbial cells. The CA-SLN exhibited an MIC of 4 μg/mL, whereas free drug solution displayed an MIC of 10 mg/mL. Therefore, the authors believe that the bilipid SLNs consisting of SA and TRI meet the requirements for use as carriers of cefuroxime to inhibit S. aureus biofilm.

Nafee et al211 developed SLNs with an aim to optimize the delivery of QSIs in lung tissue of patients with CF. SLNs were synthesized by hot-melt homogenization with glyceryl palmi-
tostearate, glyceryl behenate, and TRI. The lipophilic nature of QSI facilitated its incorporation into SLNs demonstrating an encapsulation efficiency of 68%–95%. The release of QSI from different SLNs was studied in phosphate-buffered saline (PBS) buffer and simulated lung fluid (SLF). A controlled release of QSI in PBS buffer was observed with 60%–95% of drug release over 8 h. Therefore, SLF was considered to be a more relevant and a better medium for in vivo conditions; the release of QSI was prolonged in SLF showing greater than 20% burst in all SLNs. Mucus interaction assay demonstrated that the SLN could not alter physicochemical characteristics even when in contact with the highly characteristic thick mucus in patients with CF. Further, no significant aggregation was observed in maintaining its potential for carrying QSIs. The cytotoxic property of plain and loaded SLNs was checked on Calu-3 cells (human airway cell line) representing the bronchial area. The experiment demonstrated 80%–100% of cells to be viable after incubation with SLNs. Pyocyanin, the virulence factor, produced by P. aeruginosa is required for complete virulence in animal models. It promotes virulence by interfering with numerous cellular processes involved in the inhibition of pyocyanin. The inhibition of pyocyanin demonstrated that the formulation not only maintained the activity of the free QSI but was superior at all the tested concentrations. The QSI-loaded SLNs were superior to the free QSI in inhibiting pyocyanin. The authors reported an inhibition of the growth of P. aeruginosa upon treatment with SLN. According to the authors, SLNs, efficiently loaded with the novel QSIs, could be formulated with a release of the payload over more than 8 h. The hydrophilic surface of SLNs allowed the QSIs to efficiently penetrate the mucus, thereby acting as an efficient drug carrier for an effective therapy for CF. Thus, the use of SLNs reflects a new perspective in the nano-based delivery of novel anti-infectives.

Taylor et al,212 with the aim of preventing and treating nosocomial infections in surgical implants, synthesized SLNs composed of SA, lauric acid (LA), and oleic acid (OA). The strategy was based on the use of SLNs to destabilize bacterial adhesion in tissues and surfaces, thus preventing the formation of biofilms. Furthermore, the antibacterial action of LA and OA stimulated the disruption of bacterial cell membrane. All SLN formulations depicted a hydrodynamic radius below 200 nm and a negative surface charge; the SLN solutions were coated with silicone polyvinyl chloride (PVC) to produce coatings with antimicrobial potential. Confocal microscopy was used to analyze the bacterial adhesion that revealed the ability of bacteria to adhere to the coating surfaces in the absence of SLN; however, after coating the surface, no bacteria could adhere to the endotracheal tube surface coated with SLN. The observation was reflected in the adhesion rate, which was 96.93% lower than in the uncoated surfaces. In the case of uncoated surfaces, the presence of bacteria and integral membrane morphologies was observed, whereas amorphous fragments and free bacterial DNA were observed on the coated surfaces, indicating a disruption of the cell wall and bacterial killing. According to the authors, potential adhesion was drastically reduced due to the presence of roughness on the surface, a decrease in the contact area, and weakening of the bacterial adhesion mechanism. Moreover, the small percentage of bacteria that achieved adhesion displayed destabilized walls due to the presence of fatty acids in the SLN with bactericidal effect. The authors postulated that it is essential to search for new alternatives, such as SLNs, which are not dependent on the antimicrobial drug action due to the multidrug resistance of microbes to antibiotics. Such SLNs may be applied as coatings of surgical implants to exert an anti-biofilm activity.

Table 4 summarizes the results of several studies related to the application of SLNs most used for control of microbial biofilms.

### Polymeric nanoparticles

PNs may be defined as solid colloidal particles with a size less than 1 μm and carrying bioactive molecules or substances. These can be synthesized using different methods with a feature size of 100–500 nm.213

The early 1970s witnessed the introduction of methods for the preparation of nanoparticles. According to their composition and structural organization, nanoparticles can be classified as nanospheres and nanocapsules. The nanospheres do not contain oil in their composition and comprise a polymeric matrix with the active substance retained or adsorbed in the matrix. Nanocapsules consist of a polymeric shell disposed around an oily core, where the active substance can be dissolved in the core and/or adsorbed onto the polymer wall.214
PNs have some advantages over other nanoparticulate systems. These include high stability in the body, long storage stability, and increased biocompatibility and biodegradability. These features allow the development of nanosystems with different degradation times and controlled drug release. The main polymers include polycaprolactone, poly lactic-co-glycolic acid (PLGA), poly lactic acid, and chitosan (CS), a polysaccharide of natural origin that has been widely used due to its biodegradability and mucoadhesive capacity. The disadvantages of nanoparticles in relation to PNs could be attributed to the possible toxicity of the biodegradation products and a higher cost compared to other nanostructured systems, depending on the material and process used for the development of the nanosystem. The main polymers include polycaprolactone, poly lactic-co-glycolic acid (PLGA), poly lactic acid, and chitosan (CS), a polysaccharide of natural origin that has been widely used due to its biodegradability and mucoadhesive capacity. The disadvantages of nanoparticles in relation to PNs could be attributed to the possible toxicity of the biodegradation products and a higher cost compared to other nanostructured systems, depending on the material and process used for the development of the nanosystem. The main polymers include polycaprolactone, poly lactic-co-glycolic acid (PLGA), poly lactic acid, and chitosan (CS), a polysaccharide of natural origin that has been widely used due to its biodegradability and mucoadhesive capacity. The disadvantages of nanoparticles in relation to PNs could be attributed to the possible toxicity of the biodegradation products and a higher cost compared to other nanostructured systems, depending on the material and process used for the development of the nanosystem.

Numerous reports in the literature cite the utilization of PNs for controlled drug release and as a vector for a wide range of diseases; however, with the advent of bacterial resistance to antibiotics and the recent reports on the biofilm production, the data involving the use of PNs against biofilms are still scarce.

Da Silva et al evaluated the biofilm formation in the sealant–dentin interface when treated with phosphorylated chitosan (PHCS) and chitosan connected to Rose Bengal (CSRB), which is a photo sensitizer. A combination of PHCS and CSRB (RBPH), and CS nanoparticles was incorporated into the sealant (zinc oxide–eugenol) used to explore the benefits of applying CS in endodontics. The roots of bovine teeth were used because they are physiologically and histologically very similar to human teeth and facilitate the application of the treatments due to their size. Biofilm formation was induced by applying E. faecalis and subsequent subjection to PHCS, CSRB, RBPH, and CS nanoparticles embedded in the sealant. The group submitted to CS nanoparticles incorporated into the sealant displayed a lower tendency of biofilm formation, demonstrating antimicrobial action; this action was probably due to the electrostatic interaction between the bacterial components and CS that resulted in the destabilization of the bacterial wall. However, CS nanoparticles have a positive surface charge that influences their interaction with the negatively charged dentin; this interaction hinders the adhesion of bacteria onto the tooth tissue, thereby preventing biofilm formation. Biofilm growth was also inhibited within the sealant–dentin interface when treated with PHCS, but there was a moderate inhibition when treated with CSBH followed by photodynamic therapy.

Abdelghany et al developed a strategy to increase GEN retention in PLGA nanoparticles to verify the effectiveness of these nanoparticles in controlled drug release in vitro and in vivo against infection by P. aeruginosa. Two methodologies were employed to obtain the PNs: water-in-oil-in-water method (w/o/w) and solid-in-oil-in-water method (s/o/w). Nanoparticles generated by the w/o/w method had a size up to 251 nm, encapsulating 6.4 µg of GEN per milligram of PLGA. The authors reported that an alteration of the pH of the aqueous phase from 5.0 to 7.4 resulted in an increase of about three times in the drug-entrapping rate of PLGA nanoparticles, without significantly changing the

---

**Table 4 SLNs for control of microbial biofilms**

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Applications of nanostructured formulations</th>
<th>Composition</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>CA-SLN</td>
<td>Cefuroxime axetil</td>
<td>Improve inhibitory activity against S. aureus biofilm</td>
<td>Stearic acid and tristearin</td>
<td>S. aureus</td>
<td>210</td>
</tr>
<tr>
<td>QSI-SLN</td>
<td>Quorum sensing inhibitor</td>
<td>Improve the pulmonary delivery of novel quorum sensing inhibitors</td>
<td>Glyceryl palmitostearate, glyceryl behenate, and tristearin</td>
<td>Pseudomonas aeruginosa</td>
<td>211</td>
</tr>
<tr>
<td>FA-SLN</td>
<td>Fatty acids</td>
<td>Coatings with nontoxic chemistries that act against bacteria by multiple mechanisms at the nanoscale</td>
<td>Stearic acid, lauric acid, and oleic acid</td>
<td>P. aeruginosa</td>
<td>212</td>
</tr>
</tbody>
</table>

**Abbreviations:** SLN, solid lipid nanoparticle; CA, cefuroxime axetil; QSI, quorum sensing inhibitor; FA, fatty acid; Ref, reference.
particles diameter. An increased entrapment rate was also observed for the particles generated by s/o/w method when changing the aqueous phase pH from 5.0 to 7.4, yielding particles of 359 nm size. The release profile was similar for nanoparticles obtained by both methodologies at pH 7.4 with a 50% release in 24 h and a slower and continuous release for 16 days. For the nanoparticles obtained at pH 5.0, an initial release of only 25% was observed after 24 h; however, after 7 days of release, the released drug concentration was similar to the nanoparticles prepared at pH 7.4. These differences in the release profiles resulted from the differences in the drug distribution in the polymeric network and core of the nanoparticles. With respect to bacterial growth in planktonic form, an MIC of 1.5 and 3.0 mg/mL for free and nanocoated GEN was observed, respectively, although free GEN in the planktonic form led to a more efficient inhibition of bacterial growth as compared to the nanocoated drug (on observing the GEN activity on preformed biofilm of P. aeruginosa). This offered an improved, efficient, and greater inhibition compared to the free drug, probably due to the slow and controlled release. In the in vivo studies, 96 h after the infection, the animals treated with nanoparticles exhibited a significant reduction in bacterial CFU compared to the untreated controls. Further, a significant decrease was also observed in interleukin-6 (an inflammatory mediator), indicating the severity of the injury in animals treated with polymeric PLGA nanoparticles. According to the authors, nanoparticles and microparticles harbor the potential to be utilized in aerosol delivery and may increase the therapeutic efficacy of GEN and other aminoglycosides for the treatment of lung infections.

Cai et al. developed lipid polymer nanoparticles (LPNs) in order to carry amoxicillin (AMOXIL) to enhance antimicrobial efficacy against planktonic and biofilm forms of H. pylori. According to the authors, the outer lipid bilayer of the PNs can merge easily into the polysaccharide matrix (main component of the biofilm) and then destroy this protective layer of bacterial microenvironment, leading AMOXIL directly through the free bacterial cells. The core of the PNs consists of pectin sulfate (PEC) and mixed lipids including rhamnolipids and phospholipids. The PEC inhibited H. pylori by competing with target cells, and the presence of rhamnolipids and phospholipids contributed to a second antibacterial activity due to their anti-adhesive properties, making the biofilm formation difficult. All LPNs displayed a size range from 147 to 243 nm, and AMOXIL encapsulation efficiency rate was 93.6%–96.7%. In the antibacterial activity tests, approximately 53% of live bacteria were observed in planktonic form, with no significant difference between the two treatments; however, in the assays involving biofilm, 90.2% of live bacteria were observed when treated with free AMOXIL, and when treated with LPNs, the bacterial viability dropped to a range of 18.6%–32.6%, indicating that the LPNs have a superior effect to the conventional antibiotic treatment. Fluorescence tests indicated that bacteria treated with LPNs were not able to invade AGS cells, whereas approximately 100% of AGS cells were invaded and lysed in the presence of free AMOXIL, showing that LPNs may be a promising strategy for tissue protection against H. pylori and a tool against the formation of bacterial biofilms.

Takahashi et al developed and evaluated the antimicrobial potential of PLGA-PNs and chitosan-associated PLGA (CS-PLGA)-PNs carrying CAM in biofilms of S. epidermidis using the field emission-scanning electron microscopy (FE-SEM) technique. The PNs were prepared by emulsification–solvent diffusion method with a diameter of 252–416.5 nm and a ZP between −15.2±0.6 and 19.9±1.7 mV. The ZP of PLGA-PNs remained negative due to dissociation of the carboxyl group of PLGA in water, whereas the ZP of CS-PLGA-PNs remained positive due to the protonation of the amino group of CS. In trials conducted to evaluate the antimicrobial potential of nanoparticles on biofilms, the highest antimicrobial potential was exhibited by the PLGA-PNs carrying CAM with 62% of dead bacteria. Confocal laser scanning microscopy (CLSM) demonstrated that biofilms treated with PLGA-PNs carrying CAM displayed pores, showing an antimicrobial activity on their polysaccharide matrix. The images obtained by FE-SEM depicted that biofilms treated with CS-PLGA-PNs consisted of small pores in the polysaccharide matrix with no bacterial killing. However, the images of biofilms treated with PLGA-PNs carrying CAM exhibited a highly eroded and disturbed matrix with large pores. In addition, a decrease in the thickness of the biofilms was observed, indicating the bacterial death. The authors concluded that PNs made of PLGA may serve as effective carriers of CAM in anti-biofilm treatment. They suggested that FE-SEM could be a useful technique to obtain important information, thereby allowing the development and improvement of strategies in the medical area.

Table 5 summarizes the results of several studies related to the application of PNs most used for control of microbial biofilms.

**Metallic nanoparticles**

MNPs are metallic particles with one or more dimensions (length, width, and thickness) in the range of 1–100 nm. Faraday recognized for the first time the presence of MNPs in solution, and Gustav Mie in 1908 gave a quantitative
The major bottleneck during experimental synthesis of MNPs is obtaining stable colloidal suspensions, as MNPs have a high surface energy, favoring thermodynamically the aggregation of those ready to form metal–metal bonds. In order to prevent the aggregation of nanoparticles, the preparation of colloidal systems is generally performed in the presence of agents known as stabilizers that are adsorbed onto the surfaces of the nanoparticles, forming a self-assembled layer, which prevents coalescence. Some of the most effective stabilizers are polymeric, for example, polyvinylpyrrolidone, polyvinyl alcohol, and polyacrylic acid, which possess basic sites of Lewis with high affinity for nanoparticles, and sufficiently long organic chains that create a steric hindrance to prevent interactions among them.

The MNPs have immense potential for several technological applications and are being tremendously investigated for their antimicrobial and antifungal perspective. Zinc, titanium, silver, and gold are some of the most widely studied nanoparticles among several others.

### Zinc

Khan et al\(^2\) studied the effect of zinc oxide nanoparticles (ZnO-NPs) on oral cavity bacteria (*S. oralis* ATCC 35037). ZnO-NPs were prepared by sol–gel method and were characterized by X-ray diffraction (XRD) and transmission electron microscopy (TEM) that confirmed a polycrystalline wurtzite structure and crystalline polygonal shape, respectively. The particle showed a size distribution of 491 nm and a ZP of 16.4 mV, as determined by dynamic light scattering (DLS). The oral bacterial population was treated with ZnO-NPs, and a reduction in total bacterial counts was observed. The authors applied a concentration of 10 mg/mL of ZnO-NPs, and the CFU was reduced to be 66% and 59% on NA and MRS agar plates, respectively. At 50 mg/mL concentration, up to 92% reduction in the bacterial survival was recorded as compared to the untreated controls. However, at 100 mg/mL level, the ZnO-NPs inhibited the biofilm formation on polystyrene and glass surfaces and acrylic denture.

In another study, Khan et al\(^2\) also studied the antimicrobial and anti-biofilm potential of ZnO-NPs against the oral bacterial isolates of *Rothia dentocariosa* (Ora-7) and *Rothia mucilaginosa* (Ora-16). They used the sol–gel method for obtaining the ZnO-NPs and characterized them by TEM and XRD. The ZnO-NPs showed a smooth-surface polygonal shape with an average size of 35.23 nm. The growth inhibition activity of ZnO-NPs against *R. dentocariosa* and *R. mucilaginosa* was determined by *IC*\(_{50}\) to be 53 and 76 µg/mL, respectively. The authors coated the artificial teeth and dental prostheses with *R. dentocariosa* and *R. mucilaginosa* and conducted a study on the effect of nanoparticles on biofilm formation, and the results showed that ZnO-NPs inhibited the bacterial biofilm formation on the surfaces; the NPs were more effective against Ora-7 at all concentrations tested, while the clove oil was active at a concentration of 10 mg/mL.

### Table 5 PNs for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Applications of nanostructured formulations</th>
<th>Composition</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>CS-PNs</td>
<td>Zinc oxide–eugenol</td>
<td>Explore the benefits of applying chitosan in endodontics</td>
<td>Chitosan</td>
<td><em>Enterococcus faecalis</em></td>
<td>218</td>
</tr>
<tr>
<td>PLGA-PNs</td>
<td>Gentamicin</td>
<td>Increase the half-life of the drug</td>
<td>Poly lactic-co-glycolic acid</td>
<td><em>Pseudomonas aeruginosa</em></td>
<td>219</td>
</tr>
<tr>
<td>PEC-LPNs</td>
<td>Amoxicillin</td>
<td>Enhance the antimicrobial efficacy against planktonic and biofilm forms</td>
<td>Pectin sulfate and mixed lipids containing rhamnolipids and phospholipids</td>
<td><em>Helicobacter pylori</em></td>
<td>220</td>
</tr>
<tr>
<td>PLGA-PNs</td>
<td>NA</td>
<td>Determine the antibacterial activity of NPs on the biofilm</td>
<td>Poly(DL-lactide-co-glycolide)</td>
<td><em>Staphylococcus epidermidis</em></td>
<td>221</td>
</tr>
<tr>
<td>CS-PLGA-PNs</td>
<td>NA</td>
<td>Determine the antibacterial activity of NPs on the biofilm</td>
<td>Poly(DL-lactide-co-glycolide) and chitosan</td>
<td><em>S. epidermidis</em></td>
<td>221</td>
</tr>
<tr>
<td>CAM-PLGA-PNs</td>
<td>Clarithromycin</td>
<td>Determine the antibacterial activity of NPs on the biofilm</td>
<td>Poly(DL-lactide-co-glycolide)</td>
<td><em>S. epidermidis</em></td>
<td>221</td>
</tr>
</tbody>
</table>

**Abbreviations:** PN, polymeric nanoparticle; CS, chitosan; PLGA, poly lactic-co-glycolic acid; PEC, pectin sulfate; LPN, lipid polymer nanoparticle; NP, nanoparticle; CAM, clarithromycin; Ref, reference; NA, not applicable.

---

Sangani et al \(^{230}\) synthesized ZnO-NPs by a sol–gel procedure and characterized them by TEM. This method yielded particles with an average size of 20 nm. The study aimed to assess the biofilm formation by 15 clinical isolates and one reference (ATCC 9027) strain of \(P.\ aeruginosa\) and the antibacterial activity of ZnO-NPs. The ZnO-NPs were tested at different concentrations in the range of 0–400 \(\mu\)g/mL, MIC was determined by broth dilution method, and minimum bactericidal concentration (MBC) was also determined. The average MIC and MBC of ZnO-NPs for the 15 isolates were 158 and 325 \(\mu\)g/mL, respectively, while those for the reference strain were 150 and 325 \(\mu\)g/mL, respectively. The MIC \(_{50}\) and MIC \(_{90}\) of the ZnO-NPs were 150 and 175 \(\mu\)g/mL, respectively. The biofilms were formed in 96-well flat-bottom tissue culture plates (TCPs), and the ZnO-NPs levels were tested in the range of 50–350 \(\mu\)g/mL. The results showed about 75% and 94% reduction in the optical densities (ODs) at 250 and 350 \(\mu\)g/mL level, respectively, and the ZnO-NPs were able to eliminate preformed biofilm.

Dwivedi et al \(^{231}\) employed a soft chemical/solution process to obtain ZnO-NPs and characterized them by TEM, atomic force microscopy, and XRD. The ZnO-NPs showed a smooth surface, spherical shape, and wurtzite phase, and the size was in the range of 10–15 nm. The disk diffusion assay was chosen to evaluate the antibacterial activity against \(P.\ aeruginosa\) which showed the best zone inhibition of 16 mm at 100 mg/mL of ZnO-NPs. The inhibition of the biofilm formation was also evaluated in this study, and the ZnO-NPs were able to inhibit biofilm formation at the concentrations of 50 and 100 \(\mu\)g/mL. The interaction of ZnO-NPs with bacterial solution produces reactive oxygen species (ROS) that is an important factor in the inhibition of biofilm. An increased production of ROS was directly proportional to the increase in antibacterial activity of ZnO-NPs; therefore, it can be presumed that the mechanism of action is related to the higher production of ROS. This study advocates the potential of ZnO-NPs usage as future nano-antibiotics.

Bacteria can stay in biomaterials such as polymers and consequently form antibiotic-resistant bacterial biofilms. Seil and Webster \(^{232}\) studied the effect of incorporation of ZnO nanoparticles into PVC. The ZnO-NPs of about 60 nm diameters were procured from Nanophase Technologies and were incorporated into PVC by sonication to facilitate the homogenization. The presence of ZnO-NPs on the PVC surface was confirmed via SEM. In order to evaluate the antimicrobial activity of ZnO-NPs against biofilms of \(S.\ aureus\) (ATCC 25923), they treated a PVC membrane with different concentrations of ZnO-NPs (0%, 2%, 10%, 25%, and 50%, w/v) to superimpose coverslips and inoculated 3×10^6 CFU on each coverslip. The ODs were recorded after 24 and 72 h of the inoculation and analyzed by crystal violet staining. The polymer composites containing ZnO-NPs clearly showed a reduction in the number of total bacterial count as compared to those without ZnO-NPs (control).

A reduction of 24% and 28% in the biofilm formation by the composite containing ZnO-NPs at 25% and 50% (w/v) concentration was observed, respectively, over the control. The crystal violet staining analysis showed about 55% reduction in the biofilm formation on the surface of the composites containing different concentrations of ZnO-NPs against the control. The difference in the reduction in biofilm formation at the different concentrations of ZnO-NPs composites was not significant (\(P<0.05\)).

Lee et al \(^{233}\) studied the anti-biofilm activity of Zn\(^+\) and/or ZnO-NPs against \(P.\ aeruginosa\) PAO1, \(E.\ coli\) O157:H7 (ATCC 43895), and a methicillin-sensitive \(S.\ aureus\) (MSSA; ATCC 6538) and a methicillin-resistant \(S.\ aureus\) (MRSA; ATCC BA-1707) strain. The test biofilm was formed on polystyrene plates in accordance with Pratt and Kolter.\(^{234}\) The formation of \(P.\ aeruginosa\) biofilm on polystyrene surfaces was inhibited by ZnCl\(_2\) and Zn(NO\(_3\))\(_2\) in a dose-dependent manner, while ZnO (1 mM; average diameter 50 nm) reduced biofilm formation by 95%. ZnCl\(_2\) and ZnO also actively inhibited the biofilm formation on a glass surface. ZnO at 5 mM level was able to inhibit the biofilm formation of \(E.\ coli\) O157:H7, MSSA (ATCC 6538), and MRSA (ATCC BA-1707).

Table 6 summarizes the results of several studies related to the application of ZnO-NPs most used for control of microbial biofilms.

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Method of preparation</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>ZnO-NPs-So</td>
<td>Zinc oxide</td>
<td>Sol–gel</td>
<td>Streptococcus oralis</td>
<td>228</td>
</tr>
<tr>
<td></td>
<td></td>
<td></td>
<td>Rothia dentocariosa and</td>
<td></td>
</tr>
<tr>
<td></td>
<td></td>
<td></td>
<td>Rothia mucilaginosa</td>
<td>229</td>
</tr>
<tr>
<td>ZnO-NPs-Rd</td>
<td>Zinc oxide</td>
<td>Sol–gel</td>
<td>Pseudomonas aeruginosa</td>
<td>230</td>
</tr>
<tr>
<td>ZnO-NPs-Pa</td>
<td>Zinc oxide</td>
<td>Sol–gel</td>
<td>P. aeruginosa</td>
<td></td>
</tr>
<tr>
<td>ZnO-NPs-Pasc</td>
<td>Zinc oxide</td>
<td>Soft chemical/solution process</td>
<td>Staphylococcus aureus</td>
<td>231</td>
</tr>
<tr>
<td>ZnO-PVC-NPs</td>
<td>Zinc oxide</td>
<td>Nanophage</td>
<td>P. aeruginosa, Escherichia coli, and S. aureus</td>
<td>232</td>
</tr>
<tr>
<td>ZnO-NPs-Ec</td>
<td>Zinc oxide</td>
<td>NM</td>
<td></td>
<td>233</td>
</tr>
</tbody>
</table>

Abbreviations: ZnO, zinc oxide; NPs, nanoparticles; PVC, polyvinyl chloride; NM, not mentioned; Ref, reference; Sol–gel, chemical process used for the synthesis of a colloidal suspension; So, Streptococcus oralis; Rd, Rothia dentocariosa; Pa, Pseudomonas aeruginosa; Pasc, Pseudomonas aeruginosa-soft chemical; Ec, Escherichia coli.
Titanium

Haghighi et al\(^{232}\) evaluated the application of titanium dioxide nanoparticles (TiO\(_2\)-NPs) and ethylene diamine tetra acetic acid (EDTA) as an antifungal agent against \(C.\) albicans biofilms. Titanium tetrachloride (TiCl\(_4\)) was used as a precursor in TiO\(_2\)-NPs synthesis. The TiO\(_2\)-NPs were further characterized for their shape and size using SEM and the type of crystalline structure using XRD. Fluconazole-sensitive (ATCC 10231) and fluconazole-resistant (ATCC 76615) reference strains of \(C.\) albicans were used to form biofilms. TiO\(_2\)-NPs and EDTA were tested in the range of 4–8 and 6.5–15 \(\mu\)g/mL, respectively, and fluconazole was used as a control. The antifungal activity of the samples was estimated via XTT reduction and ATP bioluminescence assays. The results obtained from both the methods showed that the biofilms of a fluconazole-sensitive strain of \(C.\) albicans were inhibited by TiO\(_2\)-NPs (5.14 \(\mu\)g/mL), EDTA (8.09 \(\mu\)g/mL), and fluconazole (4 \(\mu\)g/mL). The fluconazole-resistant strain required relatively higher concentrations of these agents, that is, 5.35, 11.33, and 8 \(\mu\)g/mL, respectively (\(P<0.05\)). The authors proposed that the antifungal activity of TiO\(_2\)-NPs is probably associated with the intracellular ROS produced by them leading to cell death by altering normal respiratory activity. In order to explain the antifungal activity of EDTA, different theories such as the inhibition of filamentation process or chelation of some constituents essential to biofilm matrix have been proposed. These findings were further verified by both XTT and ATPase assays which showed the same outcomes, and these can also be a good choice to evaluate the anti-biofilm activity of TiO\(_2\)-NPs.

Ibrahim et al\(^{236}\) carried out the biosynthesis of titanium nanoparticles (TiNPs) using vaginal \textit{Lactobacillus crispatus} isolated from healthy Iraqi women. The nanoparticles were evaluated for their antibacterial and anti-adhesive properties against \textit{E. coli}, \textit{K. pneumoniae}, \textit{Morganella morganii}, \textit{A. baumannii}, and \textit{S. aureus} isolated from urine samples of the Iraqi women exposed to recurrent urinary infection. The antibacterial activity was evaluated using microdilution method, and the sample concentration ranged from 4 to 128 \(\mu\)g/mL. The effect of these nanoparticles on bacterial biofilm was tested using Congo Red agar and tube method, and the anti-adhesive property was tested by TCP method. The TiNPs exhibited anti-adhesive activity against all clinical isolates (except for \textit{E. coli}), and the highest and lowest efficiency were recorded against \textit{M. morganii} (48\%) and \textit{A. baumannii} (6\%), respectively. Tube test method also showed similar results related to the inhibitory effect on biofilm formation, as TiNPs were effective against all strains except \textit{E. coli}. The Congo Red agar method showed the presence of pink or pale gray colonies of \textit{K. pneumoniae}, \textit{M. morganii}, and \textit{S. aureus} representing a reduced slime production by these strains; however, they typically formed black colonies in this specific medium. The black colonies formed by other strains indicated that the TiNP treatment did not alter the slime-producing property. The authors concluded that TiNPs can be considered as a promising antibacterial agent in the treatment of UTIs as they are cost effective, nontoxic, and ecofriendly.

Maurer-Jones et al\(^{237}\) evaluated several types of TiO\(_2\)-NPs including acid-catalyzed TiO\(_2\)-NPs synthesized in house, and Evonik Aeroxide Degussa P25 and Eusolex T-Eco (both commercially available) for their competence to inhibit \textit{Shewanella oneidensis} biofilm using quartz crystal microbalance and riboflavin secretion by high-performance liquid chromatography. When compared to the controls, no differences were observed in the strain viability after an exposure to various concentrations of the three types of TiO\(_2\), but when exposed to all samples of TiO\(_2\) some sort of dose-dependent decline in the growth of strain could be observed. The changes were observed in the mass added to the crystal in order to form biofilm and viscoelastic properties irrespective of TiO\(_2\)-NP exposure to the strains, although this alteration did not confer any resistance property. When the strain was exposed to high concentrations of TiO\(_2\) (all samples), an unexpected increase in riboflavin secretion was recorded. Riboflavin is a direct way to measure the bacterial growth, as it results from the molecule flavin mononucleotide, normally secreted by \textit{S. oneidensis}. The authors suggested that these changes could not be considered a consequence of oxidative stress, but the altered gene expression in the bacteria due to TiO\(_2\)-NPs exposure may lead to subtle changes in the bacterial function.

Table 7 summarizes the results of several studies related to the application of TiNPs and TiO\(_2\)-NPs most used for control of microbial biofilms.

Silver

Namasivayam et al\(^{238}\) analyzed the anti-biofilm property of catheters coated with AgNPs against clinical isolates of \textit{S. aureus}. AgNPs synthesized by \textit{Azadirachta indica} leaf extract were applied to a catheter and were characterized by SEM, which showed the complete dispersion of the uniform spherical nanoparticles of 50–60 nm size on the surface of the catheter fiber. A differential effect on biofilm inhibition was observed in the catheter coated with nanoparticles, and the highest inhibition was observed after 72 h of incubation.
In the biochemical composition, the total number of carbohydrates and the biofilm matrix proteins were greatly reduced. This study could be insightful toward the development of medical devices coated with antimicrobials against pathogenic microorganisms.

Park et al analyzed the antimicrobial activity of AgNPs against PA01 planktonic bacteria and biofilm of P. aeruginosa, and the activity was compared with that of silver ions. The inactivation of biofilms by AgNPs was very sensitive to stirring, which caused a high AgNP bio-absorption. Although AgNPs activity against planktonic cells was approximately 10% of the activity of the silver ions, their activity against biofilm cells was comparable to that of the silver ions at the same concentration, after 90 min of agitation (about 3.5 log inactivation of biofilm cells). This study pointed out that AgNPs inactivate biofilms by bio-absorption; however, the same did not occur with the ionic silver as such.

Martinez-Gutierrez et al explained how biofilms protect pathogenic organisms from adverse environmental conditions and can be reservoirs and sources of disease outbreaks, especially in medical equipment. The major objective of their study was to evaluate the anti-biofilm activity of AgNPs against various microorganisms of clinical interest. The antimicrobial activity of AgNPs was tested in biofilms obtained under static conditions and high fluid shear conditions in a bioreactor. After exposure to 100 mg/mL AgNPs, a 4 log reduction was recorded in the CFU of P. aeruginosa under turbulent fluid conditions in a biofilm reactor. The antibacterial activity of AgNPs against various microbial strains grown in polycarbonate membranes was well documented. It was concluded that AgNPs effectively prevent the formation of biofilms and also kill the bacteria in established biofilms, suggesting the potential role of AgNPs in the prevention and treatment of biofilm-related infections. The AgNPs at 250 mg/mL or a higher concentration were able to inhibit bacterial growth without using any antibiotics; this indicates the behavior of AgNPs as an antimicrobial agent and as a potential modifier of the bacterial cell wall. However, further research is still required to utilize AgNPs for preventive and therapeutic strategies.

The work of Gurunathan et al focused on the application of AgNPs as antibacterial, antifungal, antiviral, anti-inflammatory, and anti-angiogenic agents due to their unique biological, physical, and chemical properties. The study aimed to investigate the antibacterial and anti-biofilm activity of isolated AgNPs alone or in combination with conventional antibiotics against various human pathogenic bacteria. The authors showed a reliable, simple, cost-efficient, and natural synthesis of AgNPs by treating silver ions with Allophylus cobbe leaf extract. The AgNPs synthesis was characterized by UV–Vis absorption spectroscopy, XRD, Fourier transform infrared spectroscopy (FTIR), X-ray photoelectron spectroscopy (XPS), DLS, and TEM. Further, the antibiotic, antibacterial, and anti-biofilm activity of AgNPs or AgNPs combined with an antibiotic was evaluated using a series of tests such as in vitro, disk diffusion, biofilm inhibition, and generation of ROS against P. aeruginosa, Shigella flexneri, S. aureus, and Streptococcus pneumoniae. A significant antimicrobial and anti-biofilm activity was observed with antibiotics in combination, with the lowest dose of AgNPs using the plant extract of A. cobbe, and in other cases sublethal doses of antibiotics. A significant synergistic effect was observed for ampicillin and vancomycin against Gram-negative and Gram-positive bacteria, respectively. The study proposed that the biogenic AgNPs in combination with antibiotics can be used for the treatment of infectious bacterial diseases. This study also showed evidence of antibacterial and anti-biofilm properties of AgNPs facilitated by A. cobbe and their resilience against various human pathogenic bacteria, which advocate the use of AgNPs as coadjuvants for the treatment of infectious diseases.

Kalishwaralal et al proposed that biofilms are formed by the bacteria that attach to the surface and aggregate to form a hydrated polymeric matrix. The formation of these sessile
colonies and their inbuilt resistance to antimicrobial agents are a cause of many important and chronic bacterial infections. Such biofilms play a key role in the development of infectious eye disease in humans such as microbial keratitis. Various approaches have been attempted to avert infections related to biofilms in health institutes. These methods have their own limitations such as chemical barriers, emerging antibiotics-resistant strains, and so on. AgNPs are well known for their antimicrobial activity; therefore, in this study, biologically synthesized AgNPs showed an anti-biofilm activity, which was tested in vitro on biofilms formed by P. aeruginosa and S. epidermidis after 24 h of treatment. The treatment resulted in more than 95% inhibition of biofilm formation, and it was uniform in the test species. This study recommends the future application of AgNPs in the treatment of microbial keratitis owing to their anti-biofilm potential.

Monteiro et al.231 investigated the effect of AgNPs on the susceptibility of biofilm development in C. albicans and C. glabrata during middle and maturation stages. The AgNP suspensions (5 nm) were synthesized by reducing silver nitrate with sodium citrate solution and were used to treat biofilms of Candida developed after 5, 12 (intermediate phase), and 48 h (maturation phase) of growth on acrylic surfaces. Their efficacy was measured by determining total biomass (using crystal violet staining) and the number of CFU. The AgNPs caused a significant decline in the total biomass and the number of CFU of Candida biofilms, ranging from 23% to 51.5% and 0.63 to 1.59 log10 (CFU/cm²), respectively. Thereafter, no significant differences were recorded in the total biomass of biofilm on exposure to AgNPs at different developmental stages (24 or 48 h). However, the number of CFU after 24 and 48 h of exposure of the biofilm to AgNPs was significantly different only in C. albicans strain 324LA/94. Generally, the developmental phases (transitional as well as maturation) do not affect the susceptibility of biofilms of C. albicans and C. glabrata to AgNPs. These findings are fundamental to the adoption of new therapies to prevent denture stomatitis. In the future, these nanoparticles can be incorporated into denture base resins in a safer way or may be used as a dental decontamination solution for the elderly people, especially in developing countries.

Qin et al.234 examined the prevention of periprosthetic infection via biofilm inhibition by AgNPs (20 nm) produced in situ and fixed on a titanium surface by silver plasma immersion ion implantation. The surface was characterized by FE-SEM and XPS. Spherical nanoparticles were homogeneously distributed on the titanium surface, and an increase in the immersion time led to an increase in the average diameter and distribution of the metallic AgNPs. The AgNPs immobilized on the titanium surface did not show any cytotoxicity against MC3T3-E1 cell line. The immobilized metallic silver particles were tested against biofilms of S. epidermidis (ATCC 35984) on the surface and analyzed by crystal violet staining, spread plate method, CLSM, and SEM, and the results showed an in vitro decrease in biofilm formation via inhibition of bacterial adhesion.

Table 8 summarizes the results of several studies related to the application of AgNPs most used for control of microbial biofilms.

### Table 8 AgNPs for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Method of preparation</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>AgNPs</td>
<td>Silver</td>
<td>Synthesized by Azadirachta indica leaf extract</td>
<td>Staphylococcus aureus</td>
<td>238</td>
</tr>
<tr>
<td>AgNPs-PA</td>
<td>Silver</td>
<td>Purchased from ABC Nanotech Co. (STU206011; Daejeon, South Korea)</td>
<td>PA01 planktonic bacteria and Pseudomonas aeruginosa</td>
<td>239</td>
</tr>
<tr>
<td>AgNPs-Ab</td>
<td>Silver</td>
<td>Reduction of silver nitrate</td>
<td>Acinetobacter baumannii, P. aeruginosa, S. aureus, Streptococcus mutans, and Candida albicans</td>
<td>240</td>
</tr>
<tr>
<td>AgNPs-SP</td>
<td>Silver</td>
<td>Bioreduction of silver nitrate with Allophylus cobbe leaves</td>
<td>P. aeruginosa, Shigella flexneri, S. aureus, and Streptococcus pneumoniae</td>
<td>241</td>
</tr>
<tr>
<td>AgNPs-Se</td>
<td>Silver</td>
<td>Reduction of silver nitrate with Bacillus licheniformis biomass</td>
<td>P. aeruginosa and Staphylococcus epidermidis</td>
<td>242</td>
</tr>
<tr>
<td>AgNPs-Ca</td>
<td>Silver</td>
<td>Reduction of silver nitrate with sodium citrate</td>
<td>C. albicans and Candida glabrata</td>
<td>243</td>
</tr>
<tr>
<td>AgNPs-Ti</td>
<td>Silver</td>
<td>NM</td>
<td>S. epidermidis</td>
<td>244</td>
</tr>
</tbody>
</table>

**Abbreviations:** AgNPs, silver nanoparticles; AgNPs-PA, AgNPs to Pseudomonas aeruginosa; AgNPs-Ab, AgNPs to Acinetobacter baumannii; AgNPs-SP, AgNPs to Streptococcus pneumoniae; AgNPs-Se, AgNPs to Staphylococcus epidermidis; AgNPs-Ca, AgNPs to Candida albicans; AgNPs-Ti, AgNPs immobilized on titanium; NM, not mentioned; Ref, reference.

Gold

Khan et al.245 explored gold nanoparticles (AuNPs) to enhance the efficacy of photodynamic therapy by methylene blue against resistant C. albicans and biofilm formation. The AuNPs and AuNP–methylene blue conjugates were characterized by physicochemical methods such as XRD, UV–Vis absorption spectrophotometry, cross-correlation of photons, FTIR, fluorescence spectroscopy, and electron microscopy.
The properties of the conjugates were elucidated by several methods such as anti-biofilm testing, laser scanning, confocal, and electron microscopy. The microscopic analysis showed a significant reduction in biofilm formation as well as the activity of *C. albicans* in the presence of conjugates. Fluoro-spectroscopic analyses confirmed type I phototoxicity against the biofilms. These findings indicate that the conjugated AuNPs generated by photodynamic treatment of methylene blue can be used for the control of acquired nosocomial infection and inhibit the formation of biofilm by *C. albicans*.

AuNPs (10 nm) were prepared to store and release nitric oxide (NO) by the activation of their surfaces with functional polymers modified with NO donor molecules. Initially, the copolymer chains consisting of poly (methyl methacrylate oligo-ethylene glycol ether) and poly (benzyl vinyl chloride) were synthesized via reversible addition fragmentation chain transfer polymerization. The chloride functional groups reacted with cyclohexylamine to introduce secondary amine groups in the copolymer chains. The surface of AuNPs was coated with the copolymers by exploiting the affinity of the terminal group for gold to reach a thickness of 0.6 nm. The secondary amine functional groups were converted to N-diazene diolate, NO donor molecules, at high pressure (5 atm). The AuNPs carrying NO were further characterized by TEM, DLS, thermal gravimetric analysis, and XPS. The nanoparticles showed the slow release of NO in biological media. TEM showed an enhancement in the stability of nanoparticles, while DLS confirmed an improved particle size and hydrodynamics. The results concluded that NO can be released slowly at pH 6.8, which can be explored for various applications such as dispersal of *P. aeruginosa* biofilm and destruction of cancer cells.

Boda et al. explained about the challenges in eliminating the microbial biofilms in implant biomaterials or devices by antibiotics. They observed that exopolymeric substances protect the microorganisms from most of the antibiotics and make the cell immune. The applications of MNP have now been widely considered to control bacterial infections. Gold and iron oxide nanoparticles are extensively used in various medical applications; however, their potential to eradicate biofilms from biomaterial implants is still under investigation. In a recent study, the growth of *S. aureus* and *P. aeruginosa* biofilm was significantly inhibited at higher concentrations of AuNPs and iron oxide compared to the control.

Table 9 summarizes the results of several studies related to the application of AuNPs most used for control of microbial biofilms.

**Table 9** AuNPs for control of microbial biofilms

<table>
<thead>
<tr>
<th>Formulation</th>
<th>Active ingredients</th>
<th>Method of preparation</th>
<th>Pathogen</th>
<th>Ref</th>
</tr>
</thead>
<tbody>
<tr>
<td>AuNP-methylene</td>
<td>Methylene blue</td>
<td>Turkevich–Frens method</td>
<td><em>Candida albicans</em></td>
<td>245</td>
</tr>
<tr>
<td>AuNP-NO</td>
<td>NO</td>
<td>Reduction of HAuCl₄ with trisodium citrate</td>
<td><em>Pseudomonas aeruginosa</em></td>
<td>246</td>
</tr>
<tr>
<td>Ultrasound AuNPs</td>
<td>Gold</td>
<td>NM</td>
<td>Staphylococcus aureus, Staphylococcus epidermidis, Escherichia coli, and <em>P. aeruginosa</em></td>
<td>247</td>
</tr>
<tr>
<td>AuNPs</td>
<td>Gold</td>
<td>Reduction of HAuCl₄ with trisodium citrate</td>
<td><em>S. aureus</em> and <em>P. aeruginosa</em></td>
<td>248</td>
</tr>
</tbody>
</table>

**Abbreviations:** AuNPs, gold nanoparticles; NM, not mentioned; Ref, reference.

**Final considerations**

The exploration of novel approaches toward the improvement of human life is everlasting, and it is evident that the search for alternatives for the treatment and control of microbial biofilms
diseases associated with biofilms is a complex path. According to the scientific reports presented in this review article, it may be concluded that the application of nanotechnology in drug delivery systems has enormous potential and can be considered as an effective alternative for the treatment of microbial biofilms in the near future. The ability of the nanoparticles to synergize the active molecules for the inhibition of biofilms is a promising characteristic as it allows the use of drugs available in clinical practice in a more efficient manner that guarantees overcoming of the constraints related to the bioavailability of the antimicrobials.

Acknowledgments

We thank São Paulo Research Foundation - FAPESP (grant #2014/24626-9 and #2016/08559-5) and the Scientific Support and Development Program of School of Pharmaceutical Sciences (UNESP). We also thank Reinier Bron for their support with the figures.

Disclosure

The authors report no conflicts of interest in this work.

References


219. Schaffazick SR, Guterres SS. Caracterização e estabilidade físico-qua


221. Duong HTT, Adnan NM, Barraud N, et al. Functional gold nano


