Sodium deoxycholate-decorated zein nanoparticles for a stable colloidal drug delivery system

Introduction

Both natural and synthetic polymers have been used for medical and pharmaceutical applications, and several are recognized as materials suitable for developing innovative formulations. Recently, proteins derived from plants have been receiving a certain degree of interest for potential application in the field of controlled drug delivery, thanks to their features of ample availability, great bio- and cyto-compatibility, poor immunogenicity in comparison with synthetic or semisynthetic polymers, and the possibility of modulating the physicochemical parameters of nanosystems. Considering the numerous advantages resulting from the use of plant proteins, various approaches were investigated in order to develop hydrogels, films, fibers, and nano- and microparticles for food-, biomedical, and drug delivery applications.

In this investigation, we used zein, a natural hydrophobic protein belonging to alcohol-soluble prolamine-rich compounds abundantly contained in corn, for the preparation of polymer-based nanoparticles to be proposed as colloidal drug delivery devices.

Background: The use of biopolymers is increasing in drug delivery, thanks to the peculiar properties of these compounds such as their biodegradability, availability, and the possibility of modulating their physico-chemical characteristics. In particular, protein-based systems such as albumin are able to interact with many active compounds, modulating their biopharmaceutical properties. Zein is a protein of 20–40 kDa made up of many hydrophobic amino acids, generally regarded as safe (GRAS) and used as a coating material.

Methods: In this investigation, zein was combined with various surfactants in order to obtain stable nanosystems by means of the nanoprecipitation technique. Specific parameters, eg, temperature, pH value, Turbiscan Stability Index, serum stability, in vitro cytotoxicity and entrapment efficiency of various model compounds were investigated, in order to identify the nanoformulation most useful for a systemic drug delivery application.

Results: The use of non-ionic and ionic surfactants such as Tween 80, poloxamer 188, and sodium deoxycholate allowed us to obtain nanoparticles characterized by a mean diameter of 100–200 nm when a protein concentration of 2 mg/mL was used. The surface charge was modulated by means of the protein concentration and the nature of the stabilizer. The most suitable nanoparticle formulation to be proposed as a colloidal drug delivery system was obtained using sodium deoxycholate (1.25% w/v) because it was characterized by a narrow size distribution, a good storage stability after freeze-drying and significant feature of retaining lipophilic and hydrophilic compounds.

Conclusion: The sodium deoxycholate-coated zein nanoparticles are stable biocompatible colloidal carriers to be used as useful drug delivery systems.

Keywords: nanoparticles, sodium deoxycholate, stabilizers, zein

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In 1985, zein received “GRAS” (generally regarded as safe) status by the US Food and Drug Administration (FDA) as a suitable material to be used for the film coating of oral pharmaceuticals. Based on solubility and sequence homology, zein has four classifications: α-zein (characterized by a mean molecular weight of between 19 and 22 kDa), β-zein (14 kDa), γ-zein (between 16 and 27 kDa), and δ-zein (10 kDa). Over 50% of the amino acid residues of zein are non-polar, eg, leucine, proline, alanine, and phenylalanine, and this feature makes it one of the few natural proteins that can be solubilized in aqueous/ethanol solutions. Zein is also characterized by a high glutamine content which confers a certain polarity to the structure. Due to this amphiphilic character, the hydrophobic regions of zein can aggregate into colloidal particles which are able to retain lipophilic drugs, while the polar regions can interact with water-soluble compounds. This is why zein has been used to entrap drugs and nutraceuticals, eg, curcumin, 5-fluorouracil, α-tocopherol, lutein, glibenclamide, and essential oils. However, due to their low net charge close to the isoelectric point (pI ≈ 6.2), the poor physical stability and dispersibility of freeze-dried zein nanoparticles at a neutral pH are detrimental to an efficacious application of this material in the alimentary and pharmaceutical fields. In this attempt, sodium caseinate, lecithin, Phoronic F68, and Tween 20 were used as stabilizers to prevent the colloidal aggregation of zein-based nanosystems by decreasing their hydrophobic attraction and increasing steric repulsion.

The aim of this investigation was to evaluate the influence of several factors on the preparation of stable zein nanoparticles made up of yellow derivative, in order to develop a colloidal formulation useful for drug delivery. In particular, experimentation was focused on the physicochemical characterization of zein nanoparticles prepared in the presence of various surfactants, their stability in serum as a function of temperature and different pH values, as well as freeze-drying experiments using various cryoprotectants. The toxicity of the zein-based colloidal formulations was also investigated on the different cell lines used. Moreover, the entrapment efficiency (EE%) of various hydrophobic and hydrophilic drugs was evaluated.

Materials and methods

Materials

Yellow zein, sodium deoxycholate monohydrate (SD), all-trans-retinoic acid (ATRA), red oil, rhodamine B, 3-[4,5-dimethylthiazol-2-yl]-3,5-diphenyltetrazolium bromide salt (used for MTT-tests), phosphate buffered saline (PBS) tablets, dimethyl sulfoxide, and amphotericin B solution (250 μg/mL), were purchased from Sigma-Aldrich Co. (St Louis, MO, USA). Tween 80 (T80) was provided by Acef S.p.a. (Piacenza, Italy). Poloxamer 188 (PLX188) was purchased from BASF (Ludwigshafen, Germany). Ethanol was obtained from Carlo Erba SpA (Rodano [MI], Italy), while cellulose membrane Spectra/Per MWCO 50 kDa was obtained from Spectrum Laboratories Inc. (Eindhoven, the Netherlands).

For the in vitro studies, Dulbecco’s Modified Eagle’s Medium (DMEM) and Roswell Park Memorial Institute 1640 enriched with Glutamax I, tripisin/EDTA, penicillin/streptomycin solution and fetal bovine serum (FBS) were obtained from Gibco (Thermo Fisher Scientific, Waltham, MA, USA). A549 and K562 cells were purchased from the IRCCS Azienda Ospedaliera Universitaria San Martino – IST Istituto Nazionale per la Ricerca sul Cancro.

Preparation of zein nanoparticles

Zein nanoparticles were obtained using the nanoprecipitation method of the preformed polymer in an aqueous solution. Briefly, various amounts of zein were dissolved in 3 mL of an ethanol/water solution (2:1 v/v) at room temperature and added to 5 mL of aqueous phase made up of MilliQ water containing different amounts of surfactants (Table 1), homogenized using an Ultraturrax® (model T25; IKA® Werke GmbH and Co, Staufen, Germany) at 24,000 rpm for 1 min and then mechanically stirred at 600 rpm for 12 h on a magnetic plate to favor the evaporation of the organic solvent. The nanoparticles were suitably purified by means of a dialysis technique (cut-off 50 kDa), which removed the unreacted compounds.

Physicochemical and stability evaluation

Mean size, size distribution, and the Z-potential of the nanoparticles were evaluated with a Zetasizer Nano ZS (a dynamic light scattering spectrophotometer made by Malvern Instruments Ltd., Malvern, UK), using the third-order cumulant fitting as the correlation function. The results were expressed as the mean of three different experiments ± standard deviation. Transmission electron microscopy (TEM) was performed according to a procedure described elsewhere.

The nanoparticle formulations were also submitted to Turbiscan Lab® Expert (Formulaction, Toulouse, France) analysis in order to evaluate their stability profiles as a function of temperature and storage time. The instrument was equipped with a Turby Soft 2.0 for data processing, and the results were reported as kinetic stability profile vs time.

The influence of the pH on the modulation of the physicochemical properties of the various zein-based formulations was investigated by dispersing the samples in deionized water at different pH values (4.0, 6.0, 8.0, 10.0), using 1 mol/L NaOH or HCl.
Table 1 Composition and physico-chemical properties of zein nanoformulations

<table>
<thead>
<tr>
<th>Sample</th>
<th>Zein (mg)</th>
<th>T80 (% w/v)</th>
<th>PLX188 (% w/v)</th>
<th>SD (% w/v)</th>
<th>Mean sizes (nm)</th>
<th>Polydispersity index</th>
<th>Zeta potential (mV)</th>
</tr>
</thead>
<tbody>
<tr>
<td>A</td>
<td>1</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>40±16</td>
<td>0.28±0.14</td>
<td>−14±1.2</td>
</tr>
<tr>
<td>B</td>
<td>2</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>312±9</td>
<td>0.25±0.01</td>
<td>−2.8±0.5</td>
</tr>
<tr>
<td>C</td>
<td>3</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>140±1</td>
<td>0.23±0.01</td>
<td>5.8±1.4</td>
</tr>
<tr>
<td>D</td>
<td>4</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>131±1</td>
<td>0.21±0.01</td>
<td>7.0±0.6</td>
</tr>
<tr>
<td>E</td>
<td>5</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>120±1</td>
<td>0.22±0.01</td>
<td>12.1±3</td>
</tr>
<tr>
<td>F</td>
<td>10</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>106±1</td>
<td>0.20±0.01</td>
<td>20±0.2</td>
</tr>
<tr>
<td>G</td>
<td>12</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>115±1</td>
<td>0.42±0.01</td>
<td>30±0.6</td>
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<tr>
<td>H</td>
<td>15</td>
<td>1.25</td>
<td>–</td>
<td>–</td>
<td>141±3</td>
<td>0.53±0.02</td>
<td>30±1.3</td>
</tr>
<tr>
<td>I</td>
<td>10</td>
<td>2.5</td>
<td>–</td>
<td>–</td>
<td>274±19</td>
<td>0.51±0.09</td>
<td>9.3±0.6</td>
</tr>
<tr>
<td>J</td>
<td>10</td>
<td>5</td>
<td>–</td>
<td>–</td>
<td>127±1</td>
<td>0.17±0.01</td>
<td>12±0.6</td>
</tr>
<tr>
<td>K</td>
<td>10</td>
<td>1.25</td>
<td>–</td>
<td>–</td>
<td>137±1</td>
<td>0.23±0.01</td>
<td>10±1.6</td>
</tr>
<tr>
<td>L</td>
<td>10</td>
<td>2.5</td>
<td>–</td>
<td>–</td>
<td>106±1</td>
<td>0.21±0.03</td>
<td>20±0.6</td>
</tr>
<tr>
<td>M</td>
<td>10</td>
<td>5</td>
<td>–</td>
<td>–</td>
<td>103±1</td>
<td>0.18±0.01</td>
<td>33±4.8</td>
</tr>
<tr>
<td>N</td>
<td>10</td>
<td>1.25</td>
<td>–</td>
<td>–</td>
<td>93.57±1</td>
<td>0.12±0.01</td>
<td>21±2.4</td>
</tr>
<tr>
<td>O</td>
<td>10</td>
<td>2.5</td>
<td>–</td>
<td>–</td>
<td>110±1</td>
<td>0.11±0.01</td>
<td>−34±2.9</td>
</tr>
<tr>
<td>P</td>
<td>10</td>
<td>–</td>
<td>1.25</td>
<td>2.5</td>
<td>306±153</td>
<td>0.45±0.06</td>
<td>−42±1.1</td>
</tr>
<tr>
<td>Q</td>
<td>10</td>
<td>–</td>
<td>–</td>
<td>5</td>
<td>&gt;1,000</td>
<td>0.72±0.15</td>
<td>−37±4.7</td>
</tr>
<tr>
<td>R</td>
<td>10</td>
<td>–</td>
<td>–</td>
<td>5</td>
<td>&gt;1,000</td>
<td>0.72±0.15</td>
<td>−37±4.7</td>
</tr>
<tr>
<td>S</td>
<td>10</td>
<td>–</td>
<td>–</td>
<td>–</td>
<td>&gt;1,000</td>
<td>0.72±0.15</td>
<td>−37±4.7</td>
</tr>
</tbody>
</table>

Note: Data are presented as mean ± standard deviation.

Abbreviations: T80, Tween 80®; PLX188, Poloxamer 188®; SD, sodium deoxycholate monohydrate.

Nanoparticle stability in serum
The influence of serum protein on the stability of the various zein nanoparticle formulations was investigated following their incubation in 70% FBS. Briefly, the various nanoparticle suspensions (200 μL) were added to 1 mL of FBS solution and incubated at 37°C for 48 h, stirring at 600 rpm. The samples were analyzed at different incubation times, and their average size was measured as reported above.

Freeze drying of nanoparticles
The zein nanoparticles were lyophilized using a freeze-drying system (VirTis SP scientific senter 2.0; SP Industries, Warminster, PA, USA) equipped with a vacuum pump (B14 model; Carpanelli S.p.a., Bologna, Italy). Various samples (0.5 mL) were enriched with different cryoprotectants (glucose, trehalose, sucrose, mannose, mannitol) at various concentrations (5 and 10% w/v), transferred into pyrex glass vials, and frozen in liquid nitrogen for 2 min. The samples were then placed in the freeze-drying chamber and subjected to cryo-drying for 24 h. The resulting powder was stored at room temperature for 1 week, and then it was rehydrated with the same volume of sublimated water by manual shaking and then submitted to physicochemical analysis (size and surface charge evaluation).

Cell cultures and in vitro cytotoxicity
A549 (human lung cancer cells) and K562 (human chronic myelogenous leukemia cells) were incubated in plastic culture dishes (100×20 mm) in a Water-Jacketed CO2 incubator at 37°C (5% CO2) using a DMEM with glutamine and Roswell Park Memorial Institute 1640, respectively, supplemented with penicillin (100 UI/mL), streptomycin (100 μg/mL), amphotericin B (250 μg/mL), and FBS (10%, v/v), as previously described. To investigate the cytotoxicity of zein nanoparticles with and without surfactants, MTT-testing was carried out. Briefly, cells were plated in 96-well culture dishes (5×104 cells/0.2 mL for A549 cells and 10×104 cells/0.2 mL for K562) and treated with different amounts of nanoparticles (1, 10, 50, and 100 μg/mL of protein) at various incubation times (24, 48, and 72 h). Untreated cells were used as control. After each incubation period, 20 μL of tetrazolium salt solubilized in PBS (5 mg/mL) was added to each well, and the plates were incubated again for 3 h. The plates containing the K562 cells were centrifuged at 1,500 rpm for 5 min (ALC PK130 Centrifuge; Thermo Fisher Scientific), in order to obtain the deposition of salts on the bottom of the wells.

Successively, the medium was removed, and the formazan salts precipitated on the well bottoms were dissolved with 200 μL of a mixture of dimethyl sulfoxide/ethanol (1:1 v/v) by shaking the plates for 20 min at 230 rpm (IKA® KS 130 Control, IKA®; Werke GmbH and Co.). The solubilized formazan was analyzed with a microplate spectrophotometer (xMARK™; Bio-Rad Laboratories Inc., Hercules, CA, USA) at a wavelength of 540 nm, with reference at 690 nm. Cell viability, expressed as a percentage, was reported as the mean.
of five different experiments ± standard deviation, and was obtained through the following equation, in which Abs_{T} is the absorbance of treated cells and Abs_{C} is the absorbance of control (untreated) cells:

\[
\text{Cell viability (\%)} = \frac{\text{Abs}_{T}}{\text{Abs}_{C}} \times 100
\]  

EE% of model drugs

The EE% of hydrophilic (Rhodamine B) and hydrophobic compounds (Red Oil and ATRA) in zein nanoparticles was evaluated by means of suitable spectrophotometric analyses.

The colloidal formulations prepared with various amounts of drugs (20–200 μg/mL) were centrifuged at 90 k rpm for 1 h using a Beckman Optima™ Ultracentrifuge (Fullerton, Canada). The pellets were disaggregated by a sonicator (UW70; Bandelin Electronic GmbH & Co. KG, Berlin, Germany) and incubated in water or ethanol as a function of the entrapped compound. The amount of drug(s) contained in the solutions was spectrophotometrically determined (Lambda 35; Perkin Elmer, Waltham, MA, USA) at \( \lambda_{\text{max}} \) 553 nm, 544 nm, and 350 nm for Red Oil, Rhodamine B, and ATRA, respectively. No interference deriving from the empty zein formulations was observed. The amount of drug entrapped in the nanoparticles was determined as the difference between the amount added during the nanoparticle preparation and the unentrapped amount. The EE% was expressed as the percentage of the total amount of drug that became entrapped, according to the following equation:

\[
\text{EE}\% = \frac{\text{De}}{\text{Da}} \times 100
\]

where De is the amount of entrapped drug and Da is the drug amount added during preparation of the nanoparticles.

Statistical analysis

Statistical analysis of the various experiments was performed by ANOVA, and the results were confirmed by a Bonferroni \( t \)-test, with a \( P \)-value of <0.05 considered statistically significant.

Results and discussion

Physico-chemical characterization

Various amounts of zein were nanoprecipitated in order to evaluate the average size, polydispersity index, and surface charges of nanoparticles (Table 1); these parameters are of great importance for a carrier to be proposed for systemic administration. In fact, the possibility of modifying these parameters is fundamental to achieve smart nanodevices, the physicochemical features of which have to be modulated as a function of therapeutic requirements.

As reported in Table 1, the samples showed a mean diameter of ~100–150 nm and a smooth morphology when the amount of zein was ≥3 mg, thus evidencing a correlation between the protein concentration and the formation of well-defined colloidal structures (Figure S1). On the other hand, aggregates were obtained when more than 10 mg of zein (2 mg/mL) were initially used, as demonstrated by the high values resulting on the polydispersity index (Table 1), which is in agreement with data previously reported.

Interestingly, the surface charges were negative when 1 or 2 mg of zein were used, while the zeta-potential shifted towards positive values when the polymer concentration was increased (Table 1). A possible explanation of this finding could be due to the modulation of the protein conformation, or to non-covalent binding between the various molecules of the compound.

The nanoparticles obtained using 10 mg of zein (2 mg/mL, sample F) were chosen for further investigation, because no aggregates were observed during their preparation, and they were able to retain a suitable amount of drug(s).

The addition of various surfactants during the preparation of the zein nanoparticles allowed the formation of stable complexes by reducing the hydrophobic attraction of the lipophilic residues and increasing colloidal repulsion; in particular, the influence of these surfactants (T80, PLX188, and SD) on the physicochemical characteristics of the zein nanoparticles was evaluated (Table 1). Namely, the addition of non-ionic surfactants to the water phase produced homogeneous, monodispersed zein nanoparticles. The amounts of 2.5% and 5% w/v of T80 and PLX188, respectively, produced nanoparticles with a mean size of ~100 nm and a narrow size distribution (Table 1). No significant influence on the surface charges of the zein nanoparticles was elicited by PLX188, while the addition of T80 elicited a significant decrease in this parameter. In fact, the ~20 mV zeta-potential of surfactant-free zein nanoparticles decreased to ~10 mV when T80 was used (Table 1). This finding may be due to the adsorption of the surfactant onto the particle surface, leading to a modulation of the shearing plane as a consequence of the interaction between the polysorbate-residues and the protein.

The addition of moderate amounts of SD (1.25% w/v), an anionic surfactant, did not influence the mean nanoparticle size, but greater concentrations of surfactant induced a significant increase in the particle size, as well as the formation
of macroaggregates (Table 1). The addition of SD also influenced the surface charge of the nanoparticles, shifting the zeta-potential from positive to negative values. This is probably a result of the binding between the negatively-charged headgroups of SD with the positively charged amino acid moieties of zein, which would lead to significant exposure of the negatively-charged residues.31

The morphological analysis carried out by TEM evidenced a spherical shape of the various zein nanoformulations, and confirmed the data obtained by dynamic light scattering (DLS) (Figure 1).

Turbiscan Lab analyses were carried out to evaluate the stability profile of the various nanoparticle formulations as a function of incubation time and temperature, and the obtained data were expressed as Turbiscan Stability Index (TSI).32 As shown in Figure 1, the TSI results for the various surfactant-free zein nanoparticles at 20°C are very similar, thus evidencing the absence of destabilizing phenomena, eg, sedimentation, migration, and/or flocculation.27 When the temperature was increased to 37°C, a significant variation in the TSI showed on the sample prepared with 5 mg of zein, probably as a consequence of the specific rearrangement of the protein; on the contrary, the formulation prepared with 10 mg of protein showed suitable stability. The TSI profiles of the samples prepared with 12 and 15 mg of zein confirmed the DLS data by evidencing the sedimentation of the macroaggregates (data not shown).

The TSI profiles of the zein nanoparticles prepared with surfactants further confirmed the stabilizing effect of the surfactant on the colloidal structure (Figure 2). In fact, the TSI profiles of the nanoparticles containing 2 mg/mL of protein (Sample F) and prepared with the surfactants PLX188 5%, T80 2.5% w/v, and SD 1.25% showed no significant modification either at 20°C or 37°C (Figure 2). Other concentrations of stabilizers provided no improvement in the TSI profiles, confirming the DLS results (Figure S2).

**Effect of pH**

Many pharmaceutical formulations are administered at various pHs as a function of the body compartment to be reached and the pharmacological effect to be exerted by the entrapped compound.31 Therefore, it is important to investigate the
influence of the pH on the physicochemical parameters of zein nanoparticles.

As shown in Figure 3, the sizes of the various nanoparticles were evaluated as a function of different pHs. Surfactant-free zein nanoparticles preserved their mean diameter (<300 nm) only at pH 4.0, while a significant increase (>1,000 nm) was observed at pH values greater than 6.0, probably as a consequence of destabilizing phenomena related to the isoelectric point of protein (pI 6.2). The zeta potential of the zein nanoparticles showed a gradual decrease when the incubation medium moved from acidic to alkaline conditions, probably as a consequence of the modulation of the shearing plane characteristics (Table 2).

The presence of non-ionic surfactants during preparation prevented the formation of zein macroaggregates and, hence, the sedimentation and the surface charges of the nanoparticles showed a zeta potential (±10 mV) close to neutrality (Table 2) only at pHs 4.0 and 8.0. Also in this case, the pH close to the pI of protein caused a lack of stability, thus confirming the previous data.\textsuperscript{15}

The use of SD provided the most suitable results in terms of zein nanoparticle stability by showing no significant variation in the mean size and only a slight decrease in zeta potential at basic pH, further confirming the strong contribution of this surfactant to the colloidal stability of zein nanoparticles (Figure 3 and Table 2). Sodium cholate

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**Figure 2** TSI of surfactant-free zein nanoparticles as a function of zein concentration (A and B). TSI of zein nanoparticles (2 mg/mL of protein) prepared with various surfactants (PLX188 5% w/v, T80 2.5% w/v, and SD 1.25% w/v) (C and D). T =20°C (A and C); T =37°C (B and D).

**Abbreviations:** TSI, Turbiscan Stability Index; T80, Tween 80\textsuperscript{®}; PLX188, Poloxamer 188\textsuperscript{®}; SD, sodium deoxycholate monohydrate; T, temperature.
derivatives merely demonstrated their ability to stabilize various colloidal polymeric structures, as was true in the case of polyesters with respect to other surfactants such as PVA and polysorbates.\(^{34}\)

**Effect of heating**

Heating is an important parameter to be investigated in order to establish the thermal stability of a colloidal system, which is evaluated during the preformulation phases of a pharmaceutical.\(^{35}\) For this reason, the influence of the temperature on the various zein nanoparticles was investigated. The surfactant-free formulation showed a considerable increase of size and polydispersity index when it was heated, while the zeta potential analysis provided negative values (Table 3). This finding suggested that the temperature increase probably caused a rearrangement of the protein and the collapse of the colloidal structure.\(^{14}\) The addition of ionic and non-ionic surfactants during preparation of the nanoparticles significantly improved the colloidal stability of the nanoparticles against the destabilizing phenomena promoted by the heating process; this trend further confirms their fundamental role in developing a suitable formulation for efficient drug delivery.

**Serum stability**

The behavior of zein nanoparticles in medium containing serum is another essential issue to be investigated before using these colloids in vitro and in vivo experiments. In fact, serum proteins may interact with nanosystems inducing the formation of a corona, which is able to promote the binding of biomolecules to the surfaces of the nanoparticles as well as increase their hydrodynamic ray.\(^{26,36}\)

Zein nanoparticles were incubated in 70% FBS at 37°C, and their size was monitored up to 48 h. The surfactant-free nanoparticles showed an increase of the mean size in the first few hours and then remained unmodified up to 48 h (Figure 4). Interestingly, the use of T80 elicited an increase of the mean size of the nanoparticles similar to that observed for surfactant-free nanoparticles, even though this trend was emphasized as a function of the incubation times, ie, the longer the incubation the greater the size increase. The obtained
results confirm the ability of polysorbate derivatives to adsorb protein onto the surface of various colloids.17

Conversely, the zein nanoparticles prepared in the presence of PLX188- and SD-provided suitable serum stability by showing an average size <200 nm for up to 24 h. This feature is appealing for possible in vivo administration of zein nanoparticles, because the change in the physicochemical properties of the colloidal systems, caused by the adsorption of the serum protein, still remains an open issue to be investigated.

Freeze-drying of zein nanoparticles

The evaluation of the physicochemical features of a colloidal system following a freeze-drying process is required in order to forecast its long-term storage stability, so that a nanoparticle formulation with a long shelf-life can be designed, thus increasing the potentiality of its marketability. For this reason, lyophilization studies were carried out on the various zein nanoparticles as a function of different cryoprotectant agents.

As shown in Table 4, the formulation prepared with SD provided the best results in terms of ability to be resuspended after the freeze-drying procedure, except for mannose 10% and glucose 10%, both of which evidenced a significant increase in the particle size and polydispersity. Moreover, the anionic surfactant-coated nanoparticles were characterized by a negative surface charge (—30 mV), while the other nanoparticles and cryoprotectants showed a zeta potential close to neutrality (Table 4). This feature could explain the complexity of obtaining stable freeze-dried

Table 4 Physico-chemical properties of zein nanoparticles prepared using a protein concentration of 2 mg/mL after the freeze-drying process as a function of surfactant and cryoprotectant used

<table>
<thead>
<tr>
<th>Sample</th>
<th>Cryoprotectant (% w/v)</th>
<th>Mean size (nm)</th>
<th>Polydispersity index</th>
<th>Zeta potential (mV)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Surfactant free</td>
<td>Glucose 5%</td>
<td>836±41</td>
<td>0.71±0.03</td>
<td>—4±0.1</td>
</tr>
<tr>
<td></td>
<td>Glucose 10%</td>
<td>435±20</td>
<td>0.62±0.04</td>
<td>—3.5±0.1</td>
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<tr>
<td></td>
<td>Trehalose 5%</td>
<td>691±34</td>
<td>0.63±0.03</td>
<td>—5.4±0.1</td>
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<td>Trehalose 10%</td>
<td>695±34</td>
<td>0.59±0.02</td>
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<td>Mannose 5%</td>
<td>&gt;1,000</td>
<td>0.89±0.04</td>
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<td>Mannose 10%</td>
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<td>Sucrose 5%</td>
<td>&gt;1,000</td>
<td>0.59±0.27</td>
<td>—2.3±0.1</td>
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<tr>
<td>Sucrose 10%</td>
<td>&gt;1,000</td>
<td>0.84±0.21</td>
<td>—1.5±0.1</td>
<td></td>
</tr>
<tr>
<td>Mannitol 5%</td>
<td>&gt;1,000</td>
<td>0.99±0.05</td>
<td>—2.6±0.1</td>
<td></td>
</tr>
<tr>
<td>Mannitol 10%</td>
<td>&gt;1,000</td>
<td>0.80±0.04</td>
<td>—1.1±0.1</td>
<td></td>
</tr>
</tbody>
</table>

**Abbreviations:** T80, Tween 80; PLX188, Poloxamer 188; SD, sodium deoxycholate monohydrate.
nanoparticles. The use of 5% mannitol showed an acceptable increase of the mean size of T80-zein nanoparticles, while all the other formulations were characterized by aggregates and unstable structures upon rehydration. These results demonstrated the possibility of dehydrating SD-enriched zein nanoparticles by freeze-drying, providing access to a functional powdered formulation to be used in pharmaceutically.

**Evaluation of cytotoxicity**

The safety evaluation of a new formulation is another fundamental issue to be addressed. Although zein has already been approved by the FDA,44 different amounts of polymeric nanoparticles were tested as a function of both polymer concentration and incubation time. K562 cells were used as a model of a non-adhesive cell line, while the A549 cells were investigated as models of a solid tumor.

The idea was to investigate the influence of surfactants on the cell viability as a function of the modulation of the interfacial tension existing between cell and plate, or as a function of their action on the cell membrane. A549 cells were used because it was demonstrated that a positive charge of a colloidal system could favor its uptake into lung cancer tissue.28 As shown in Figure 5, the surfactant-free zein nanoparticles exerted a certain cytotoxicity only after 24 h incubation at the greatest protein concentration tested; namely, 100 μg/mL of zein nanoparticles induced a decrease in cell viability of 25%–30% on both the cell lines, thus confirming the potentially safe use of this biomaterial (Figure 5).

Surfactant-coated zein nanosystems showed significant toxicity at a polymer concentration of 50 μg/mL after only 24 h incubation (Figure 5). Although the nanoparticles had been previously purified, the augmented toxicity, found in the formulations containing surfactant, contrarily to those composed exclusively of protein, could be due to the quantity of surfactant that remains in the colloidal structure, which reduces the surface tension between the culture plate and the cells (inducing their detachment), and also destabilizes the bilayer structure.38 This result demonstrated the maximum concentration of stabilizing surfactant in zein nanoparticles that can be used in in vitro experiments.

**Drug entrapment efficiency**

Taking into consideration the physicochemical features of zein nanoparticles as a function of the various environmental conditions, the 1.25% SD-coated zein nanoparticles were chosen as suitable drug carriers, and the EE% of various molecules was investigated. Namely, rhodamine B was used as a model of a hydrophilic drug, while ATRA and Red Oil were chosen as lipophilic compounds. As reported in Table 5, 100 μg/mL of hydrophobic compound was the maximum concentration supported by the colloidal system because macroaggregates formed at greater concentrations. In particular, EE values of ~14 and ~28% were obtained for ATRA and Red Oil, respectively, when an initial concentration of 500 μg was used (Table 5). The low degree of encapsulation that resulted for lipophilic drugs disagrees with other scientific investigations, even though zein does contain many hydrophobic moieties.39 This finding could be explained by the presence of high levels of xanthophylls strongly bound to yellow zein, thus inducing low EE values of lipophilic drugs with respect to decolorized zein.11 Conversely, the zein nanoparticles were able to retain a significant amount of the hydrophilic compound, thus evidencing their potential application as a useful carrier for water-soluble drugs (Table 5).

**Conclusion**

Zein is a very attractive polymer, which has been widely explored for novel applications in the fields of food science, pharmaceutics, and biomedicine.40 We investigated yellow zein as a biocompatible material for developing innovative nanoparticles. The physicochemical characteristics of zein nanoparticles were influenced by the addition of various surfactants. The most suitable nanoparticle formulation to be proposed as a colloidal drug delivery system was obtained using SD (1.25% w/v), which allowed the formation of stable zein nanoparticles with a mean size of ~100 nm, a low polidispersity index, and a negative surface charge (~30 mV). The SD-coated zein nanoparticles also showed high storage stability, and were not destabilized by heat treatments up to 50°C, pH alterations, and the freeze-drying process, thus evidencing a great degree of maneuverability. Its incubation with 70% FBS also confirmed the excellent stability and compatibility of this nanoparticle formulation in biological fluids, and its incubation with various cell lines revealed suitable safety up to 50 μg/mL of protein. The zein nanoparticles were able to retain different amounts of hydrophilic and lipophilic drugs, so ulterior investigations on the release rate of entrapped compounds as a function of the modulation of various parameters are in due course. Additional in vivo experiments on murine models are needed to evaluate the pharmacokinetic and biodistribution profiles of zein nanoparticles in order to appreciate the potential.
applications of this nanoformulation as a drug delivery system. The peculiar properties of zein nanoparticles could be useful for their application in various scenarios (drug delivery, contrast agents for neuroimaging, optimization of radiotracers for nuclear medicine, radiosensitizers), as has been possible with other biopolymers.\textsuperscript{41,42}

In fact, one of the most important goals to be reached will be the development of a novel nanomedicine able to increase

\begin{figure}[h]
\centering
\includegraphics[width=\textwidth]{figure5.png}
\caption{Evaluation of in vitro cytotoxicity of zein nanoparticles on A549 (A) and K562 (B) cells as a function of zein concentration and incubation time. Data are the percentages of cellular viability as evaluated by MTT-testing. Results are the mean of four different experiments ± standard deviation. Error bars, if not shown, are within symbols. Statistical analysis by one-way ANOVA and a posteriori Bonferroni $t$-test: *$P<0.05$; **$P<0.001$.}
\end{figure}

\textbf{Abbreviations:} T80, Tween 80\textsuperscript{®}; PLX188, Poloxamer 188\textsuperscript{®}; SD, sodium deoxycholate monohydrate.
Table 5 EE% of various active compounds in zein nanoparticles prepared by a protein concentration of 2 mg/mL and 1.25% w/v of SD as a function of the drug concentration initially used

<table>
<thead>
<tr>
<th>Sample</th>
<th>Amount of drug used (µg/mL)</th>
<th>EE (%)</th>
<th>Drug entrapped (µg)</th>
</tr>
</thead>
<tbody>
<tr>
<td>ATRA</td>
<td>20</td>
<td>3.88±0.14</td>
<td>3.88±0.15</td>
</tr>
<tr>
<td></td>
<td>50</td>
<td>7.3±0.29</td>
<td>18.25±0.74</td>
</tr>
<tr>
<td></td>
<td>100</td>
<td>14.26±0.45</td>
<td>71.3±2.85</td>
</tr>
<tr>
<td></td>
<td>200</td>
<td>-</td>
<td>-</td>
</tr>
<tr>
<td>Red Oil</td>
<td>20</td>
<td>10±0.4</td>
<td>10±0.43</td>
</tr>
<tr>
<td></td>
<td>50</td>
<td>18±0.45</td>
<td>45±1.8</td>
</tr>
<tr>
<td></td>
<td>100</td>
<td>28±0.66</td>
<td>140±5.6</td>
</tr>
<tr>
<td></td>
<td>200</td>
<td>-</td>
<td>-</td>
</tr>
<tr>
<td>Rhodamine B</td>
<td>20</td>
<td>27.26±1.09</td>
<td>27.26±1.09</td>
</tr>
<tr>
<td></td>
<td>50</td>
<td>29.14±1.16</td>
<td>72.85±2.91</td>
</tr>
<tr>
<td></td>
<td>100</td>
<td>34.15±1.36</td>
<td>170.75±6.83</td>
</tr>
<tr>
<td></td>
<td>200</td>
<td>65.4±2.62</td>
<td>654±26.16</td>
</tr>
</tbody>
</table>

Abbreviations: EE%, entrapment efficiency; ATRA, all-trans-retinoic acid; SD, sodium deoxycholate monohydrate.

the pharmacological efficacy of the entrapped drug(s), but also to be used in imaging applications in order to obtain a useful theranostic nanomedicine.\(^{45}\)

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Author contributions
All authors made substantial contributions to conception and design, acquisition of data, or analysis and interpretation of data; took part in drafting the article or revising it critically for important intellectual content; gave final approval of the version to be published; and agree to be accountable for all aspects of the work.

Disclosure
The authors report no conflicts of interest in this work.

References
Supplementary materials

Figure S1 Scanning electron microscope micrograph of zein nanoparticles characterized by a protein concentration of 2 mg/mL. Scale bar = 100 nm.

Figure S2 (Continued)
Figure S2 TSI of zein nanoparticles prepared by using 2 mg/mL of protein as a function of stabilizer concentration and incubation temperature. Abbreviations: TSI, Turbiscan Stability Index; T80, Tween® 80; PlX188, Poloxamer 188®; SD, sodium deoxycholate monohydrate.