Effect of rhythmic auditory cueing on gait in cerebral palsy: a systematic review and meta-analysis

This article was published in the following Dove Press journal: Neuropsychiatric Disease and Treatment

Shashank Ghai1
Ishan Ghai2
Alfred O. Effenberg1

1Institute for Sports Science, Leibniz University Hannover, Hannover, Germany; 2School of Life Sciences, Jacobs University, Bremen, Germany

Abstract: Auditory entrainment can influence gait performance in movement disorders. The entrainment can incite neurophysiological and musculoskeletal changes to enhance motor execution. However, a consensus as to its effects based on gait in people with cerebral palsy is still warranted. A systematic review and meta-analysis were carried out to analyze the effects of rhythmic auditory cueing on spatiotemporal and kinematic parameters of gait in people with cerebral palsy. Systematic identification of published literature was performed adhering to Preferred Reporting Items for Systematic Reviews and Meta-Analyses and American Academy for Cerebral Palsy and Developmental Medicine guidelines, from inception until July 2017, on online databases: Web of Science, PEDro, EBSCO, Medline, Cochrane, Embase and ProQuest. Kinematic and spatiotemporal gait parameters were evaluated in a meta-analysis across studies. Of 547 records, nine studies involving 227 participants (108 children/119 adults) met our inclusion criteria. The qualitative review suggested beneficial effects of rhythmic auditory cueing on gait performance among all included studies. The meta-analysis revealed beneficial effects of rhythmic auditory cueing on gait dynamic index (Hedge’s g=0.9), gait velocity (1.1), cadence (0.3), and stride length (0.5). This review for the first time suggests a converging evidence toward application of rhythmic auditory cueing to enhance gait performance and stability in people with cerebral palsy. This article details underlying neurophysiological mechanisms and use of cueing as an efficient home-based intervention. It bridges gaps in the literature, and suggests translational approaches on how rhythmic auditory cueing can be incorporated in rehabilitation approaches to enhance gait performance in people with cerebral palsy.

Keywords: entrainment, spastic diplegia, hemiplegia, ataxia, rehabilitation, balance

Introduction

Cerebral palsy is a common developmental disorder.1,2 The global prevalence of cerebral palsy is approximately 1.5–3.5/1,000 children,3,4 and is supposedly growing in developing countries.5 Cerebral palsy is primarily characterized by pre/postnatal damage to the brain,6 often predisposing to grave neuromuscular and psychological disorders.3,6 The treatment of cerebral palsy inclicts substantial costs7 and adversely impacts quality of life.8,9 Typically, motor dysfunction in cerebral palsy is characterized by spastic or extrapyramidal deficits.10 These neuromuscular dysfunctions might cause dyskinesia, dystonia, ataxia, or hypotonia.11,12 Further, these might lead to increased fatigue, reduced dexterity/coordination, postural instability, muscle contracture, and joint subluxation. Also, these neuromuscular disorders progress with aging.13 For instance, lack of mobility and hypertonia often lead to development of muscle and joint contractures and secondary bone deformities. These neuromuscular deficits among both children and older adults with cerebral palsy considerably impair kinetic and kinematic changes, impair locomotion, and predispose to falls. For instance,
exaggerated anterior stooping posture associated with increased anterior tilt in the pelvis, hip flexion, adduction, and internal rotation\textsuperscript{13–15} adversely impact efficiency in energy expenditure\textsuperscript{16} and spatiotemporal gait parameters.\textsuperscript{17} Bourgeois et al\textsuperscript{18} reported reduction in spatiotemporal gait parameters, such as cadence, stride length, and gait velocity associated with considerable enhancement in gait variability, which might predispose severely toward falls.\textsuperscript{19}

In addition to these musculoskeletal changes, Rosenbaum et al\textsuperscript{2} suggested considerable discrepancies in sensory perceptions, cognition, and behavior. Neuroimaging studies report deficits in the dorsolateral prefrontal cortex, dorsal anterior cingulate gyrus,\textsuperscript{20} somatosensory cortex,\textsuperscript{21} and cerebellum\textsuperscript{22} which might considerably impair intellectual and cognitive performance.\textsuperscript{22–24} Likewise, deficits in corticospinal, thalamocortical, superior occipitofrontal and superior longitudinal pathways have also been reported.\textsuperscript{12,20,25} Together, these psychological constraints might also impair motor performance, such as in a dual-task scenario. For instance, Hung et al\textsuperscript{26} reported drops in gait-performance measures in unilateral cerebral palsy patients while performing a dual task. Studies have suggested that this modification in gait patterns might happen due to an alleviation in “internal” conscious attention toward autonomic control that adversely impacts proprioception and autonomic functioning, possibly because of movement-specific reinvestment.\textsuperscript{27–29} The theory suggests that directing attention internally to control autonomic movements, such as gait, can have an adverse impact on performance,\textsuperscript{29} especially in high-stress situations.\textsuperscript{30} Common treatment strategies to curb motor dysfunctions in cerebral palsy include training with virtual reality,\textsuperscript{31} biocueing,\textsuperscript{32} physical/occupational therapy,\textsuperscript{33} physical exercise,\textsuperscript{34} treadmill,\textsuperscript{35} and orthosis.\textsuperscript{36,37}

Recently, several studies have tried to address the sensorimotor deficits in people with cerebral palsy by applying rhythmic auditory entrainment.\textsuperscript{38–41} Cueing aims to counteract sensory deficits, and has been shown to modulate neuro-magnetic β-oscillations,\textsuperscript{42} cortical reorganization, enhance biological motion perception,\textsuperscript{43,44} motor imagery,\textsuperscript{45,46} neural plasticity,\textsuperscript{47} reduce shape variability in musculoskeletal-activation patterns,\textsuperscript{48} and movement-specific reinvestment.\textsuperscript{49} Moreover, as a cheap\textsuperscript{50} and viable\textsuperscript{51} treatment strategy, this approach can provide substantial benefits in developing countries, where prevalence of cerebral palsy due to socioeconomic factors is more prominent.\textsuperscript{52,53} We identified high-quality systematic reviews analyzing the effects of external auditory cueing on gait performance among healthy,\textsuperscript{121} Parkinsonism\textsuperscript{54–56,122} and stroke participants.\textsuperscript{57–59} However, to the best of our knowledge, no systematic or narrative analysis has been carried out to analyze the effects of auditory entrainment on gait in people with cerebral palsy. Therefore, we attempted to develop a state of knowledge for the use of cerebral palsy patients and medical practitioners, where both qualitative and quantitative data from high-quality studies can be interpreted.

Materials and methods
This review was conducted according to the guidelines outlined in the PRISMA (Preferred Reporting Items for Systematic Reviews and Meta-Analyses) statement\textsuperscript{50} and American Academy for Cerebral Palsy and Developmental Medicine (AACPDM) methodology for systematic reviews.\textsuperscript{61}

Data sources and search strategy
The academic databases Web of Science, PEDro, EBSCO, Medline, Cochrane Central Register of Controlled Trials, Embase and ProQuest were searched from inception until July 2017. A sample-search strategy is provided in Table 1.

Data extraction
Upon selection for review, data extracted from each article were study aim, selection criteria, sample size, sample description (sex, age, health status), intervention, characteristics of auditory cueing, dual tasks, outcome measures, results, and conclusions. The data were then summarized and tabulated (Table 2). The inclusion criteria for the studies were: randomized controlled trials, cluster-randomized controlled trials, or controlled clinical trials; reporting reliable and valid spatiotemporal gait and kinematic parameters; including dynamic aspects of gait stability; use of PEDro methodological quality scale (score ≥4); conducted on human participants; published in a peer-reviewed academic journal; and published in English, German, or Korean.

Quality and risk-of-bias assessment
The quality of the studies was assessed using the PEDro methodological quality scale.\textsuperscript{62} The scale consists of eleven items addressing external validity, internal validity, and interpretability, and can detect potential bias with high reliability,\textsuperscript{63} and validity.\textsuperscript{62} A blinded rating of the methodological quality of the studies was carried out by the first (SG), second (IG) and third (AOE) reviewers. Ambiguous issues were discussed between reviewers and consensus was reached. Included studies were rated and interpreted according to scoring of 9–10, 6–8, and 4–5 for “excellent”, “good”, and “fair” quality,\textsuperscript{64} respectively. Inadequate randomization,
nonblinding of assessors, no intention-to-treat analysis, and no measurement of compliance were considered as major threats for biasing.65

Data analysis
This systematic review also included a meta-analysis approach to develop a better understanding of the incorporated interventions.66 Presence and lack of heterogeneity drove the use of either random- or fixed-effect meta-analysis.67 A narrative synthesis of the findings structured according to intervention, population characteristics, methodological quality, and type of outcome is provided (Table 2). A meta-analysis was conducted between pooled studies using Comprehensive Meta-Analysis software (version 2.0; Biostat, Englewood, NJ, USA). Heterogeneity among the studies was assessed using I² statistics. The data in this review were systematically distributed, and for each available variable pooled, dichotomous data were analyzed and forest plots with 95% CIs reported. Effect sizes were adjusted and reported as Hedge’s g.68 Thresholds for interpretation of effect sizes were as follows: standard mean effect of 0 meant no change, negative effect meant a negative change, and a positive effect meant a positive change.

Mean effect of 0.2 was interpreted as a small effect, 0.5 a medium effect, and 0.8 a large effect.69 Interpretation of heterogeneity via I² statistics was 25%, 50%, 75% as negligible, moderate and substantial heterogeneity, respectively. 75% as negligible, moderate, and substantial heterogeneity, respectively. Meta-analysis reports, including heterogeneity among studies, were evaluated to determine the reason for heterogeneity, and studies included were then pooled separately and analyzed again in a sub-group analysis. The α-level was set at 95%.

Table 1 Sample search strategy – Embase

<table>
<thead>
<tr>
<th>Date</th>
<th>July 10, 2017</th>
</tr>
</thead>
<tbody>
<tr>
<td>Strategy</td>
<td>#1 AND #2 AND #3 AND #4 AND #5 AND #6 AND #7</td>
</tr>
<tr>
<td>#1</td>
<td>(“rhythmic auditory cueing” OR “rhythmic acoustic cueing” OR “rhythmic auditory entrainment” OR “metronome cueing” OR “metronome” OR “rhythmic metronome cueing” OR “acoustic stimulus” OR “acoustic cueing” OR “acoustic cueing” OR “external stimuli” OR “external cueing” OR “external cueing” OR “music therapy” OR “Neurological music therapy” OR “tempo” OR “beat” OR “rhythm” OR “RAC” OR “NMT”)/de OR (rhythmic auditory cueing OR rhythmic auditory cueing OR rhythmic acoustic cueing OR rhythmic auditory entrainment OR metronome cueing OR metronome OR rhythmic metronome cueing OR acoustical cueing OR external stimuli OR external cueing OR music therapy OR Neurological music therapy OR tempo OR beat OR rhythm OR RAC OR NMT)/ti,ab</td>
</tr>
<tr>
<td>#2</td>
<td>(“CP” OR “Cerebral Palsy” OR “Cerebral Palsy athetoid” OR “Cerebral Palsy congenital” OR “Cerebral Palsy Diplegic infantile” OR “Cerebral Palsy dystonic-rigid” OR “Cerebral Palsy hypotonic” OR “Cerebral Palsy mixed” OR “Cerebral Palsy monophasic, infantile” OR “Cerebral Palsy quadriplegic infantile” OR “Cerebral Palsy Rolandic type” OR “Cerebral Palsy Spastic” OR “Congenital Cerebral Palsy” OR “diplegia-spastic” OR “Diplegic infantile cerebral palsy” OR “infantile cerebral palsy-diplegic” OR “infantile cerebral palsy-monophasic” OR “infantile cerebral palsy-quadriplegic” OR “little’s disease” OR “little’s disease” OR “Monophasic cerebral palsy” OR “Monophasic infantile cerebral palsy” OR “Quadriparesis infantile cerebral palsy” OR “Spastic diplegia”)/de OR (CP OR Cerebral Palsy OR Cerebral Palsy athetoid OR Cerebral Palsy congenital OR Cerebral Palsy Diplegic infantile OR Cerebral Palsy dystonic OR Cerebral Palsy dystonic-rigid OR Cerebral Palsy hypotonic OR Cerebral Palsy mixed OR Cerebral Palsy monophasic infantile OR Cerebral Palsy quadriplegic infantile OR Cerebral Palsy Rolando OR Cerebral Palsy Spastic OR Congenital Cerebral Palsy OR diplegia-spastic OR Diplegic infantile cerebral palsy OR infantile cerebral palsy-diplegic OR infantile cerebral palsy-monophasic OR infantile cerebral palsy-quadriplegic OR little’s disease OR little’s disease OR Monophasic cerebral palsy OR Monophasic infantile cerebral palsy OR Quadriplegic cerebral palsy OR Spastic diplegia)/ti,ab</td>
</tr>
<tr>
<td>#3</td>
<td>(“cognitive task” OR “concurrent task” OR “dual task” OR “dual task paradigm” OR “dual task paradigm” OR “cognitive task training” OR “dual task training” OR “dual task training”)/de OR (cognitive task OR concurrent task OR dual task OR dual task OR dual task paradigm OR dual task paradigm OR cognitive task training OR dual task training OR dual task training)/ti,ab</td>
</tr>
<tr>
<td>#4</td>
<td>(“walking” OR “gait” OR “locomotion” OR “range of motion” OR “ROM” OR “ambulation” OR “mobility” OR “treadmill gait” OR “balance” OR “stability” OR “stride” OR “gait training” OR “gait rehabilitation”)/de OR (walking OR gait OR locomotion OR range of motion OR ROM OR ambulation OR mobility OR treadmill gait OR balance OR stability OR stride OR gait training OR gait rehabilitation)/ti,ab</td>
</tr>
<tr>
<td>#5</td>
<td>(“rehabilitation” OR “treatment” OR “rehab” OR “management” OR “therapy” OR “physiotherapy” OR “physical therapy” OR “prevention” OR “risk prevention”)/de OR (rehabilitation OR treatment OR rehab OR management OR therapy OR physiotherapy OR physical therapy OR prevention OR risk prevention)/ti,ab</td>
</tr>
<tr>
<td>#6</td>
<td>(“age groups” OR “adolescent” OR “young” OR “elderly” OR “old” AND (“gender” OR “male” OR “female”))/de OR (age groups OR adolescent OR young OR elderly OR old AND (gender OR male OR female))/ti,ab</td>
</tr>
<tr>
<td>#7</td>
<td>(“intervention study” OR “cohort analysis” OR “longitudinal study” OR “cluster analysis” OR “crossover trial” OR “cluster analysis” OR “randomized trial” OR “major clinical study”)/de OR (longitudinal OR cohort OR crossover trial OR cluster analysis OR randomized trial OR clinical trial OR controlled trial)/ti,ab</td>
</tr>
<tr>
<td>Study</td>
<td>Research aim</td>
</tr>
<tr>
<td>------------------</td>
<td>------------------------------------------------------------------------------</td>
</tr>
<tr>
<td>Efraimidou et al</td>
<td>Effects of RAC on gait in people with CP</td>
</tr>
<tr>
<td>Shin et al</td>
<td>Effects of RAC on gait in people with hemiplegia (stroke/CP)</td>
</tr>
<tr>
<td>Wang et al</td>
<td>Effect of auditory feedback on motor capacity, strength, mobility, and gait in people with CP (spastic diplegia)</td>
</tr>
<tr>
<td>Author(s)</td>
<td>Effect of RAC on gait performance in people with CP</td>
</tr>
<tr>
<td>----------</td>
<td>-----------------------------------------------</td>
</tr>
<tr>
<td>Jiang</td>
<td>Effect of RAC on gait performance in people with CP</td>
</tr>
<tr>
<td>Varsamis et al.</td>
<td>Effect of RAC on gait performance in people with CP</td>
</tr>
<tr>
<td>Baram and Lenger</td>
<td>Effect of real-time auditory feedback on gait performance in people with CP</td>
</tr>
<tr>
<td>Kim et al.</td>
<td>Effect of RAC on gait for people with CP</td>
</tr>
</tbody>
</table>

(Continued)
<table>
<thead>
<tr>
<th>Study</th>
<th>Research aim</th>
<th>Sample description, age (years), mean ± SD/range</th>
<th>PEDro score</th>
<th>Assessment tools</th>
<th>Research design</th>
<th>Auditory cueing</th>
<th>Conclusion</th>
</tr>
</thead>
<tbody>
<tr>
<td>Kwak</td>
<td>Effect of RAC on gait performance in people with CP</td>
<td>Exp I: 10 patients (30, 6–20)</td>
<td>4</td>
<td>Cadence, stride length, gait velocity, gait cycle, gait symmetry, and foot-contact pattern</td>
<td>Pretest, (Exp I and II) gait training at +5%, +10%, and +15% of preferred cadence in first, second, and third weeks, respectively, training for RAC at +5%, +10%, and +15% of preferred cadence by music, steady-beat pattern with 4/4 meter, ie, 80-120 bpm</td>
<td>Significant enhancement in stride length, gait velocity, and gait symmetry for Exp I in preferred cadence by music, steady-beat pattern with 4/4 meter, ie, 80-120 bpm compared to Ct</td>
<td></td>
</tr>
<tr>
<td>Kim et al</td>
<td>Effect of RAC on gait in children with CP</td>
<td>Exp I (community ambulators): 3F, 5M (25.1 ± 8.1) Exp II (household ambulators): 2F, 4M (26.3 ± 6.6) Ct: 15F, 15M (21.5 ± 1.7)</td>
<td>4</td>
<td>Cadence, gait velocity, stride length, step length, step time, stance phase, swing phase, gait-deviation index, kinematic data for pelvis, hip sagittal plane (anterior tilt/flexion at initial contact, maximal–minimal angle of anterior tilt/flexion), coronal plane (abduction–adduction at initial contact, maximal adduction–abduction angle), transverse plane (internal–external rotation at initial contact, maximal–minimal internal–external rotation), knee sagittal plane (flexion at initial contact, maximal flexion at swing, minimal flexion at stance), ankle sagittal plane (flexion at initial contact, maximal dorsi/plan flexion at stance, minimal plantar flexion at preswing), foot transverse plane (internal–external rotation at initial contact, maximal–minimal internal–external rotation)</td>
<td>Gait performance with/without rhythmic metronome cueing at preferred cadence</td>
<td>Rhythmic metronome cueing at preferred cadence</td>
<td>Significant reduction in pelvis: sagittal plane (anterior tilt initial contact, maximal, minimal angle of anterior tilt) and hip: sagittal plane (maximal, minimal flexion angle) and transverse plane (maximal internal–external rotation) in Exp after training with RAC (Exp I &gt; Exp II) Significant enhancement in gait-deviation index with RAC in Exp (Exp I &gt; Exp II) Significant reduction in step length for household-ambulator group with RAC</td>
</tr>
</tbody>
</table>

Table 2 (Continued)
Results

Characteristics of studies included

Our initial search across academic databases yielded a total of 387 studies; 175 studies were included from a personal library. After implementing our inclusion/exclusion criteria, nine studies were left (Figure 1). Data from the studies included have been summarized in Table 2. Of the nine studies included, all were controlled clinical trials.

Participants

A total of 227 participants were analyzed in the incorporated studies. In the studies included, eight studies incorporated mixed-sex patients. Only one study included male participants.70 The studies provided data on 227 participants (n=119 females/108 males). Moreover, in 108 children, the sex distribution was 57 females to 51 males, and for adults 62 females to 57 males. Descriptive statistics relating to the age (means ± SD) of the participants were tabulated across the studies (Table 2).

Risk of bias

To reduce the risks of bias, studies scoring ≥4 on PEDro were included in the review. Moreover, research protocols to be included in the review were limited to gold-standard randomized controlled trials, cluster-randomized controlled trials, and controlled clinical trials. The individual scores attained by studies using the PEDro scale are reported in Table 2, and Table S1. The average PEDro score for the nine studies was 5 of 10, indicating fair quality for studies overall. Three studies scored 7, and six studies scored 4. Risk of bias across the studies is shown in Figure 2.

Outcomes

The results provided evidence for a positive impact of rhythmic auditory cueing on spatiotemporal and kinematic gait parameters among adults and children with cerebral palsy. In all studies, significant enhancement in primary spatiotemporal and kinematic gait parameters were reported.

Meta-analyses

The evaluation of research studies via meta-analysis requires strict inclusion criteria to limit heterogeneity efficiently.71 However, among the pooled group of studies after strict inclusion criteria, some unexplained heterogeneity was still observed. Subgroup analyses were then performed for identical studies to evaluate the cause of the heterogeneity. The parameters evaluated were spatiotemporal gait parameters, such as cadence, stride length, gait velocity, and kinematic
parameters. Further analyses were conducted to evaluate the effects of rhythmic auditory cueing at preferred cadence on gait velocity in both adults and children separately. We included a generalized group analysis by first combining all the pooled studies. The studies excluded differed considerably in assessment methods or if descriptive statistics were not mentioned in the manuscript. However, attempts were made to contact the coauthors for the data.
Gait velocity

Gait velocity was analyzed in six studies. Here, two studies evaluated the effects of rhythmic auditory cueing on gait velocity in adults \(^{38,72}\) and four in children \(^{41,73–75}\) with cerebral palsy. One study included assessment of gait velocity while using patterned sensory enhancement \(^{73}\) as the mode of auditory feedback. Analysis of studies revealed (Figure 3) a large positive effect \((g=1.13, 95\% \text{ CI } 0.33–1.94)\). Substantial heterogeneity was observed between studies \((I^2=81\%; P<0.01)\). Subgroup analyses were conducted to explore heterogeneity.

An analysis for effects of rhythmic auditory cueing on gait velocity in children revealed (Figure S1), large positive effect with substantial heterogeneity \((g=1.24, 95\% \text{ CI } 0.31–2.17, I^2=82\%; P<0.01)\). Here, the heterogeneity could possibly be attributed to different training regimes in the studies, ie, no training was included by one, \(^{41}\) while others \(^{73–75}\) had training regimes for \(\geq 3\) weeks. Subgroup analysis revealed (Figure S2) a large positive effect with substantial heterogeneity \((g=1.53, 95\% \text{ CI } 1.07–1.98, I^2=82\%; P<0.01)\). Moreover, Jiang \(^{75}\) included only one training session per week. Whereas, others performed training for three (Wang et al. \(^{73}\)) and five times (Kwak \(^{74}\)), per week. Subgroup analysis revealed a large positive effect with negligible heterogeneity \((g=2.05, 95\% \text{ CI } 1.5–2.6, I^2=0; P>0.05)\). Finally, subgroup analysis evaluating the effects of rhythmic auditory cueing on gait velocity in adults revealed a large positive effect with negligible heterogeneity \((g=0.95, 95\% \text{ CI } -0.95 \text{ to } 2.85, I^2=0; P>0.05)\).

<table>
<thead>
<tr>
<th>Study name</th>
<th>Hedges’s g and 95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td>Shin et al (^{38}) A</td>
<td></td>
</tr>
<tr>
<td>Jiang (^{75}) C</td>
<td></td>
</tr>
<tr>
<td>Wang et al (^{73}) C</td>
<td></td>
</tr>
<tr>
<td>Kim et al (^{39}) A</td>
<td></td>
</tr>
<tr>
<td>Baram and Lenger (^{11}) C</td>
<td></td>
</tr>
<tr>
<td>Kwak (^{74}) C</td>
<td></td>
</tr>
</tbody>
</table>

Figure 3 Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on gait velocity in people with cerebral palsy.

Notes: Negative effects indicate reduction in gait velocity, positive effects enhancement in gait velocity. Weighted-effect sizes – Hedges’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

Abbreviations: A, adults; C, children.

Stride length

Stride length was analyzed in five studies. Two and three studies evaluated the effects of rhythmic auditory cueing on stride length in adults \(^{38,72}\) and children \(^{41,73–75}\) respectively. Analysis revealed (Figure 4) a medium positive effect \((g=0.58, 95\% \text{ CI } -0.02 \text{ to } 1.19)\). Moderate heterogeneity was observed between studies \((I^2=65\%; P>0.01)\). Subgroup analyses were conducted to explore the cause of heterogeneity. Analysis for effects of rhythmic auditory cueing on stride length in children revealed (Figure S3) a medium positive effect with negligible heterogeneity \((g=0.75, 95\% \text{ CI } 0.01–1.48, I^2=0; P>0.05)\). Subgroup analysis evaluating the effects of rhythmic auditory cueing on stride length in adults revealed a comparably smaller medium effect with negligible heterogeneity \((g=0.3, 95\% \text{ CI } -1.07 \text{ to } 1.67, I^2=0; P>0.05)\).

<table>
<thead>
<tr>
<th>Study name</th>
<th>Hedges’s g and 95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td>Shin et al (^{38}) A</td>
<td></td>
</tr>
<tr>
<td>Jiang (^{75}) C</td>
<td></td>
</tr>
<tr>
<td>Kim et al (^{39}) A</td>
<td></td>
</tr>
<tr>
<td>Baram and Lenger (^{11}) C</td>
<td></td>
</tr>
<tr>
<td>Kwak (^{74}) C</td>
<td></td>
</tr>
</tbody>
</table>

Figure 4 Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on stride length in people with cerebral palsy.

Notes: Negative effects indicate reduction in stride length, positive effects enhancement in stride length. Weighted-effect sizes – Hedges’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

Abbreviations: A, adults; C, children.
rhythmic auditory cueing on cadence in adults revealed a large positive effect with negligible heterogeneity ($g=1.04, 95\% \text{CI} 0.44–1.64, I^2=0; P>0.05$).

Kinematic parameters

Three studies analyzed the effects of rhythmic auditory cueing on gait-dynamic index (a combined measure of lower-limb kinematic performance). Data for subgroup analysis on the gait-dynamic index concerning community and household dwellers were extracted from two studies. Analysis revealed (Figure 6) a large positive effect ($g=0.92, 95\% \text{CI} 0.07–1.76, I^2=0; P<0.01$) with negligible heterogeneity. Further, an analysis of gait-dynamic index in community dwellers revealed a small positive effect with negligible heterogeneity ($g=0.07, 95\% \text{CI} -0.66 \text{ to } 0.8, I^2=0; P>0.05$). Comparably, analysis of household dwellers revealed a large positive effect with negligible heterogeneity ($g=1.11, 95\% \text{CI} 0.24–1.98, I^2=0; P>0.05$). Subgroup analysis was also conducted on individual kinematic parameters to specify the magnitude of effects of rhythmic auditory cueing on specific joint kinematics.

Subgroup analysis evaluating changes at the pelvis revealed (Figure S4) small negative effects with negligible heterogeneity ($g=-0.23, 95\% \text{CI} -0.68 \text{ to } 0.21, I^2=0; P>0.05$). At the hip joint, medium negative effects with moderate heterogeneity ($g=-0.43, 95\% \text{CI} -0.89 \text{ to } 0.01, I^2=33.5\%; P>0.01$) were observed (Figure S5). At the knee joint, medium positive effects with negligible heterogeneity ($g=0.26, 95\% \text{CI} -0.18 \text{ to } 0.71, I^2=0; P>0.05$) were observed (Figure S6). At the ankle joint, medium positive effects with moderate heterogeneity ($g=0.36, 95\% \text{CI} -0.09 \text{ to } 0.81, I^2=32.7\%; P>0.01$) were observed (Figure S7). Finally, at the foot, small negative effects with moderate heterogeneity ($g=-0.18, 95\% \text{CI} -0.62 \text{ to } 0.26, I^2=0; P>0.05$) were observed (Figure S8).

![Figure 5](image-url) Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on cadence in people with cerebral palsy.

**Notes:** Negative effects indicate reduction in step frequency, positive effects enhancement in step frequency. Weighted-effect sizes – Hedges’ $g$ (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

**Abbreviations:** A, adults; C, children.

![Figure 6](image-url) Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on gait-dynamic index in people with cerebral palsy.

**Notes:** Negative effects indicate reduction in gait-dynamic index, positive effects enhancement in gait-dynamic index. Weighted effect sizes – Hedges’ $g$ (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate a favorable outcome for control groups, positive mean differences a favorable outcome for experimental groups.

**Abbreviations:** A, adults; C, children; H, household dwellers.

### Discussion

The primary objective of this systematic review and meta-analysis was to synthesize the current state of knowledge for the effects of rhythmic auditory cueing on gait in people with cerebral palsy. All nine studies reported beneficial effects of rhythmic auditory cueing on gait parameters in children and adults with cerebral palsy. Further, the meta-analysis found significant small–large standardized effects for the benefits of rhythmic auditory cueing on spatiotemporal and kinematic parameters of gait among patients affected with cerebral palsy.

Typically, spatiotemporal parameters of gait may worsen over time in those with cerebral palsy. Deficits in periventricular white matter, gray matter, cerebellum, basal ganglia, and thalamus have been well documented. These neural centers play an integral role in managing stabilization and performance during automated tasks, such as posture and gait. In addition, increasing psychological stress might be exerted on automated control for posture, gait, and cognitive processing by deficits reported in corticospinal, thalamocortical, superior occipitofrontal, and longitudinal pathways possibly also explaining the loss of gait rhythmicity. Likewise, increased energy expenditure associated variability in muscle contraction, and force production...
add to the instability. Rhythmic auditory cueing seems to counter these deficits efficiently. The current meta-analysis reported enhancements in gait velocity (1.24) and stride length (0.75) in children and gait velocity (0.95), stride length (0.3), and cadence (1.04) in adults. Beneficial effects were also observed in gross gait–dynamic index (a combined measure of kinematic variables during gait) for adult patients affected with cerebral palsy (0.92).

Several mechanisms have been suggested for the beneficial effects of rhythmic auditory cueing. For instance, auditory entrainment might aid in reducing errors while executing gait by guiding specific movement patterns. External entrainment might act as guidance for “heel-contact” and “push-off” timing and/or muscle contractions. Likewise, such cross-sensory cueing might also reduce information overload in the native sensory modality by directing task-relevant information toward the underused sensory modality. The application of auditory entrainment is believed to allow enhancement in gait performance by bypassing or facilitating the frontostratial pathway via alternative pathways. Cunningham et al reaffirmed and suggested that rhythmic cueing might directly serve as an input supplementary motor area, thereby reducing the onset of motor deficits and aiding in performance. Moreover, cueing has been shown to allow modulation of neuromagnetic β-oscillations in the auditory cortex, cerebellum, inferior frontal gyrus, somatosensory area, and sensorimotor cortex and reduce hemispheric asymmetry. Also, enhanced activation in inferior colliculi, cerebellum, brain stem, and sensorimotor cortex have been reported. This might also suggest the facilitation of corticocerebellar network reorganization. Finally, entrainment has also been shown to reduce variability in electro- myographic activity and optimize velocity/acceleration profiles of joint motions by scaling movement time, thereby allowing stable pattern generation.

Studies have shown that rhythmic auditory cueing might also be an efficient tool to counteract dual-task-associated information-processing constraints. For instance, Lohnes and Earhart suggested that rhythmic entrainment might allow alleviation in gait performance by possibly freeing up cognitive resources for dual-task execution. Although dual-task performance has been shown to reduce performance in people with cerebral palsy, we did not identify any study analyzing the effects of rhythmic auditory cueing under higher information-processing constraints. We suggest future studies address this substantial gap in the literature. Moreover, recent studies evaluating the effects of rhythmic entrainment have revealed beneficial effects of action-relevant acoustic input on gait performance as compared to normal isosynchronous cueing. Ecologically valid action-related sounds have been suggested to enhance salience of sensory information concerning spatiotemporal information, thereby aiding movement execution. Moreover, recent research has revealed the possibilities of including emotional, motivational, and expressiveness components in auditory entrainment to portray differential effects on gait parameters. Unfortunately, a lack of pertinent literature concerning the specific type of modified auditory cueing in cerebral palsy limits our interpretation of the type of auditory cueing that might be beneficial in rehabilitation. Therefore, we suggest future studies address this gap.

Finally, we believe that auditory entrainment might be efficient because of its economical nature and high viability. The rhythmic entrainment factor could be utilized with music in rehabilitation and day-to-day lives. This could allow benefits in psychophysiological domains. Moreover, it is important to consider that the retention of enhancements in gait parameters relies not only on the training received in the clinic but also largely on how much the patient follows the treatment protocol at home. In the present meta-analyses, enhancements in kinematic gait parameters observed for household ambulators (1.11) were considerably larger compared to community ambulators (0.07). We believe that delivering this type of home-based intervention could be beneficial for people lacking access to medical interventions in developing countries. The growing number of smartphone devices in developing countries can be used as a delivery tool while using a simple metronome app, such as WalkMate or ListenMee, which with proper medical guidance might allow curbing of motor deficits associated with aging. We also suggest the use of rhythmic auditory cueing as an adjunct to other rehabilitation strategies, eg, assistive devices, swimming, or other aquatic exercise regimes as it might enhance stability-associated quality of life and rehabilitation progress by focusing on psychophysiological components.

In conclusion, to the best of our knowledge, this review analyzes for the first time the effects of auditory entrainment on adults and children with cerebral palsy. The present findings are in agreement with systematic reviews and meta-analyses carried out to analyze auditory entrainment effects on healthy, stroke and parkinsonism population groups. This review suggests the incorporation of rhythmic auditory cueing for enhancing gait performance and stability in people with cerebral palsy.

Acknowledgment

Publication of this article was funded by the Open Access Fund of Leibniz Universität, Hannover.
**Author contributions**

SG conceptualized the study, carried out the systematic review and statistical analysis, and wrote the paper. IG and AOE were involved in the systematic review process and reviewed the final manuscript. All authors contributed toward data analysis, drafting and revising the paper and agree to be accountable for all aspects of the work.

**Disclosure**

The authors report no conflicts of interest in this work.

**References**


Supplementary materials

Table S1 Individual PEDro scores

<table>
<thead>
<tr>
<th>Study</th>
<th>PEDro</th>
<th>Point estimates and variability</th>
<th>Between-group comparison</th>
<th>Intention to treat</th>
<th>Adequate follow-up</th>
<th>Random allocation</th>
<th>Blinded assessors</th>
<th>Blinded therapists</th>
<th>Blinded subjects</th>
<th>Baseline comparability</th>
<th>Concealed allocation</th>
<th>Eligibility criteria</th>
<th>Concealed allocation</th>
</tr>
</thead>
<tbody>
<tr>
<td>efraimidou et al</td>
<td>7</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Shin et al</td>
<td>3</td>
<td>4</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Wang et al</td>
<td>7</td>
<td>7</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Baram and Lenger</td>
<td>4</td>
<td>4</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>varsamis et al</td>
<td>7</td>
<td>4</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Kim et al</td>
<td>3</td>
<td>7</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Kim et al</td>
<td>4</td>
<td>4</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
<tr>
<td>Kwak</td>
<td>7</td>
<td>4</td>
<td>1</td>
<td>1</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
<td>0</td>
</tr>
</tbody>
</table>

Figure S1 Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on gait velocity in children with cerebral palsy.

Notes: Negative effects indicate reduction in gait velocity, positive effects enhancement in gait velocity. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

Abbreviation: C, children.

Figure S2 Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on gait velocity in children with cerebral palsy posttraining.

Notes: Negative effects indicate reduction in gait velocity, positive effect sizes enhancement in gait velocity. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

Abbreviation: C, children.

Figure S3 Forest plot illustrating individual studies evaluating the effects of rhythmic auditory cueing on stride length in children with cerebral palsy.

Notes: Negative effects indicate reduction in stride length, positive effects enhancement in stride length. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean difference favorable outcomes for experimental groups.

Abbreviation: C, children.
**Study name**

**Hedges’s g and 95% CI**

Shin et al^{28}

Kim et al^{28}

Kim et al^{28}

**Notes:** Negative effects indicate reduction in ankle kinematics, positive effects enhancement in ankle kinematics. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicates favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

---

**Study name**

**Hedges’s g and 95% CI**

Shin et al^{28}

Kim et al^{28}

Kim et al^{28}

**Notes:** Negative effects indicate reduction in foot kinematics, positive effects enhancement in foot kinematics. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

---

**Study name**

**Hedges’s g and 95% CI**

Shin et al^{28}

Kim et al^{28}

Kim et al^{28}

**Notes:** Negative effects indicate reduction in pelvic kinematics, positive effects enhancement in pelvic kinematics. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

---

**Study name**

**Hedges’s g and 95% CI**

Shin et al^{28}

Kim et al^{28}

Kim et al^{28}

**Notes:** Negative effects indicate reduction in hip kinematics, positive effects enhancement in hip kinematics. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.

---

**Study name**

**Hedges’s g and 95% CI**

Shin et al^{28}

Kim et al^{28}

Kim et al^{28}

**Notes:** Negative effects indicate reduction in knee kinematics, positive effects enhancement in knee kinematics. Weighted-effect sizes – Hedge’s g (boxes) and 95% CI (whiskers) – demonstrate repositioning errors for individual studies. The diamond represents pooled effect sizes and 95% CI. Negative mean differences indicate favorable outcomes for control groups, positive mean differences favorable outcomes for experimental groups.