Hip muscle and hand-grip strength to differentiate between older fallers and non-fallers: a cross-sectional validity study

Simone C Gafner,1,2 Caroline H Bastiaenen,2,3 Serge Ferrari,4 Gabriel Gold,5 Philippe Terrier,6,7 Roger Hilfiker,8 Lara Allet1,9

1Department of Physiotherapy, HES-SO University of Applied Sciences and Arts of Western Switzerland, Geneva, Switzerland; 2Department of Epidemiology, Research Program Functioning and Rehabilitation, CAPHRI, Maastricht University, Maastricht, the Netherlands; 3Department of Health, School of Health Professions, Zurich University of Applied Sciences, Winterthur; 4Department of Internal Medicine Specialties; 5Department of Internal Medicine, Rehabilitation and Geriatrics, University Hospitals and University of Geneva, Geneva, 6Department of Research, Clinique romande de réadaptation SUVACare, 7Department of Research, Institute for Research in Rehabilitation, Sion, 8Department of Physiotherapy, School of Health Sciences, HES-SO Valais-Wallis, University of Applied Sciences and Arts of Western Switzerland, Valais, 9Department of Community Medicine, University Hospitals and University of Geneva, Geneva, Switzerland

Background: Hip muscle weakness in older people seems to be an influencing factor of falls. Currently, it is unclear which muscles out of the hip muscle group play an important role in older people. A validating process in the measurement regarding muscle strength related to falls is necessary before answering that question.

Objective: Firstly, we aimed to investigate which hip muscle group strength shows an acceptable level of distinction between older adult fallers and non-fallers compared to a predefined external criterion regarding falling. Secondly, we aimed to compare the same outcomes and questions for hand-grip strength in relation to the same external criterion.

Design: This study was a cross-sectional validity study.

Methods: The maximum voluntary isometric strength (MVIS) and the rate of force generation of hip abductors (ABD), adductors, internal and external rotators, extensors, and flexors were measured with a dynamometer fixed to a custom-made frame as well as hand-grip strength with a Martin Vigorimeter in 60 older people aged over 65 years (38 females and 22 males).

Results: The area under the curve (AUC) and the results of the mean decrease in Gini index assessed by random forest approach show that of all the assessed parameters, hip ABD MVIS showed the highest discriminative value regarding the chosen external criterion in older people (AUC ABD MVIS 0.825, 95% confidence interval: 0.712–0.938).

Conclusion: Results indicate that ABD MVIS is a useful measure to distinguish between older adult fallers and non-fallers regarding the chosen external criterion.

Keywords: hip muscle strength, accidental falls, older adults, hand-grip strength, measurement study

Introduction

High fall prevalence, especially multiple falls, increases the risk of independency loss,1 admission to nursing homes,2 reduction in quality of life,3 and mortality4 in older people. The World Health Organization (WHO) reports a worldwide fall rate of ~28%–35% for people aged over 65 years. They also report a yearly fall rate of ~30%–50% for people living in long-term care institutions, whereas 40% of these people show recurrent falls.5 The Federal Statistical Office (FSO), Switzerland, reports similar yearly fall rates of 25% for people over 65 years living at home6 and 39% for people in long-term care institutions.7

Lower limb weakness in older people is assumed to be an important influencing factor of falls8 and its preservation potentially contributes to the maintenance of independency.9
There are several reasons for the increasing interest in the relationship between hip muscle strength and fall risk of older people. Approximately 7% of older people suffer from peripheral neuropathy, which is a predominantly distal dysfunction linked to an increased fall risk. Preservation of proximal lower limb strength might enable older people to compensate for distal nerve function losses. Next, older people tend to show a more accentuated hip strategy, whereas younger counterparts use rather, an ankle strategy to keep their balance. Finally, older people, in particular fallers, have a reduced mediolateral stability while standing and increased mediolateral body motion during dynamic balance recovery in forward stepping tasks. This mediolateral control is mainly assured through proximal (hip) frontal plane muscle strength. Therefore, hip muscle strength might be an important parameter to include in fall-risk assessment and can have a role in the prevention and rehabilitation in an older population at risk of falls. Hip muscle strength is an easily assessable parameter, and most importantly, easy to target in physical therapy. To contribute to treatment goal setting, insight into the diagnostic accuracy of hip muscle strength measurement to apply in an older population at risk of falling seems to be important.

To the best of our knowledge, no study exists that simultaneously assessed and compared all six hip muscle groups to investigate diagnostic values to discriminate between older adults with and without fall history (as an assumed external criterion). Fall history is known as a risk factor for future falls. However, its assessment does not give us a directly targetable parameter for physical therapy treatment.

In addition, a separate comparison between hip muscle strength and hand-grip strength with the same external criterion has not yet been investigated. At the moment, hand-grip strength is assumed to be a parameter related to whole body strength and fall risk.

To validate the new measurement tool, the first step is to compare the currently used assessments with the new, to-be-developed fall-risk assessment tool to get an idea about its discriminating ability between older adult fallers and non-fallers. Future studies will have to prospectively assess the strength of hip muscle groups with the highest diagnostic accuracy.

Our aims were as follows:
1) To identify the distinction level of the different hip muscle strength groups, evaluated by the area under the curve (AUC) >0.7, compared to a predefined external criterion regarding falling by measuring maximal voluntary isometric strength (MVIS) and rate of force generation (RFG).
2) To compare the outcomes of hip muscle strength with hand-grip strength compared to the same external criterion.

We hypothesized that, 1) within the group of hip muscles, the hip frontal plane muscle groups, essentially hip abductor (ABD) strengths, show the highest level of AUC >0.7, and 2) that the outcomes of frontal plane hip muscle strength expressed in AUC have higher values than hand-grip strength compared to the same external criterion.

**Methods**

We examined the concurrent validity of the strength of different hip muscle strength groups as well as hand-grip strength compared to older participants’ history of falling as external criterion. The data collection was performed cross-sectionally. The study was designed according to the guidelines of the COSMIN taxonomy regarding criterion validity.

**Participants**

In a limited period of time, from March to October 2015, sixty participants were simultaneously recruited from the Geriatric Department of the University Hospital of Geneva as well as from an ambulatory setting. The two different settings guaranteed the heterogeneous sample needed for a validity study. Participants admitted to physical therapy for musculoskeletal or vascular disorders were consecutively checked for the inclusion and exclusion criteria (see the following section), and thereafter asked if they agreed to participate in this study (Figure 1). The protocol was approved by the ethics committee of Geneva (Commission cantonale d’éthique de la recherche [CCER] 14-235). All participants received written and verbal information relating to the study and signed written informed consent was received from 67 participants.

Participants >65 years old, with a body mass index (BMI) between 17 and 35, and who were able to walk household distances were included in the study. They were excluded in the case of a positive history or evidence of any significant central nervous system dysfunction, neuromuscular disorders except a distal symmetric peripheral neuropathy, evidence of vestibular dysfunction, moderate or severe dementia (Mini Mental State Examination [MMSE] <18), a fracture of the lower limb and/or joint replacement within the previous year, and any lower limb or back pain that would adversely affect the strength tests.

**Measures**

**External criterion**

The external criterion was defined as a positive fall history within the previous 12 months. Participants reporting one or
more falls in the past year were classified as fallers. An event that did not fall were classified as non-fallers. An event that results in a person coming to rest inadvertently on the ground or floor or other lower level was defined as a fall. The fall history was chosen as external criterion in this study because of the ultimate importance of this discriminating factor within our theoretical construct of contributing factors regarding fall risk in older people. Identifying a suitable criterion that is considered to represent the true state of the construct of interest is a challenge. As the construct of interest is discriminating older people in groups based on a directly targetable parameter related to a high risk of falling or not having a high risk of falling, fall history is a suitable external criterion.

**Index measures**

Hip strength was measured in Newton (N) using an analog dynamometer (SENSIX®; Sensix, Poitiers, France) with a measuring range from 0 to 667 N and a precision of 0.002 N. The DELSYS System (Trigno Sensor; Delsys, Inc, Boston, MA, USA) coupled with the calibrated dynamometer digitalized the output (3.3 V) with a sampling rate of 1,926 Hz and a resolution of 16 bit. To avoid bias induced by the testing people, the dynamometer was fixed to a frame for all strength tests. Hip MVIS (N/kg) and RFG (N/s/kg) were assessed in all anatomic planes. Subjects pushed as fast and as hard as possible against the dynamometer, held the pressure for three seconds, and then relaxed. Participants repeated all tests three times per leg with a break of 1 minute between each trial. The mean of the six trials was retained for further analyses. The starting position for each test was supported by the examiner in 1 cm distance of the dynamometer. The tester counted loudly from one to three to give the starting signal. Strong verbal encouragement was given during all measurements. The testing positions for the hip strength tests as well as the hand-grip strength are described in Table 1.

**Characteristics of the population**

The collected variables were age, gender, weight, BMI, the highest educational level achieved, reported dominant hand, the level of concern about falling assessed with the Falls Efficacy Scale International (FES-I) and cognitive impairments with the MMSE.
Table 1 Hip strength test position, dynamometer placement, and hand-grip strength measurement position with Martin Vigorimeter

<table>
<thead>
<tr>
<th>Strength tests</th>
<th>Test position</th>
<th>References for test positions</th>
<th>Dynamometer position</th>
<th>Special aspects to consider</th>
</tr>
</thead>
<tbody>
<tr>
<td>Hip flexors</td>
<td>Supine with knee and hip in 90° flexion Neutral position according to rotations</td>
<td>Mendis et al&lt;sup&gt;22&lt;/sup&gt;</td>
<td>5 cm cranial to the knee cap</td>
<td>No special aspects to consider for this testing position</td>
</tr>
<tr>
<td>Hip extensors (EXT)</td>
<td>Standing with the hip in neutral position according to rotations</td>
<td>Kollock et al&lt;sup&gt;23&lt;/sup&gt;</td>
<td>In the middle of the line between the os calcaneum and the knee joint gap on the posterior side of the calf</td>
<td>The knee had to stay extended and the trunk in a neutral, upright position. If participants could not perform the test in the correct position, EXT was reported as missing value</td>
</tr>
<tr>
<td>Hip internal rotators</td>
<td>Sitting position with the knee and hip flexed at 90°</td>
<td>Thorborg et al&lt;sup&gt;24&lt;/sup&gt;</td>
<td>5 cm cranial to the external malleolus</td>
<td>Special attention was paid so that participants did not execute an abduction movement of the hip</td>
</tr>
<tr>
<td>Hip external rotators</td>
<td>Sitting position with the knee and hip flexed at 90°</td>
<td>Thorborg et al&lt;sup&gt;24&lt;/sup&gt;</td>
<td>5 cm cranial to the internal malleolus</td>
<td>Special attention was paid so that participants did not execute an adduction movement of the hip</td>
</tr>
<tr>
<td>Hip abductors</td>
<td>Side-lying position with the upper leg at 10° abducted position. The lower leg was in 45° of knee and hip flexion for stabilization</td>
<td>Krause et al&lt;sup&gt;25&lt;/sup&gt;</td>
<td>5 cm cranial to the external malleolus</td>
<td>The tested leg was extended, with the hip in a neutral or slightly extended position</td>
</tr>
<tr>
<td>Hip adductors</td>
<td>Side-lying position with the tested lower leg in a neutral position. The participant’s upper leg was placed on a pillow at 90° hip and knee flexion</td>
<td>Thorborg et al&lt;sup&gt;24&lt;/sup&gt;</td>
<td>5 cm cranial to the medial malleolus</td>
<td>The tested leg was extended, with the hip in a neutral or slightly extended position</td>
</tr>
<tr>
<td>Hand-grip strength</td>
<td>Sitting on a chair with the elbow at 90° flexion position. The forearm was in a neutral position and the wrist at 0°–30° extension</td>
<td>Desrosiers et al&lt;sup&gt;26&lt;/sup&gt;</td>
<td>Participants were asked to squeeze the rubber bulb of the Martin Vigorimeter as hard as possible and to relax after three seconds</td>
<td>No special aspects to consider for this testing position</td>
</tr>
</tbody>
</table>

FES-I
Fear of falling is known to be an influencing factor of falls.<sup>28</sup> FES-I is a validated questionnaire including 16 questions assessing the level of concern about falling of older people.<sup>29</sup>

MMSE
Cognitive impairment influences the fall risk in older adults.<sup>30</sup> The MMSE is a widely used<sup>30</sup> and validated assessment tool for cognitive impairments in older people consisting of 11 questions.<sup>31</sup>

Data collection
After obtaining informed consent, we collected participants’ sociodemographic data: age, gender, weight, and BMI – extracted from the clinical database – and the highest educational level achieved, dominant hand, and external criterion fall history via an interview. To further investigate the characteristics of our study population, a trained physical therapist assessed the MMSE and the FES-I. Then the subjects’ hip strength and hand-grip strength were tested in the same way.

Sample size
We expected to find AUC values between good (0.8) and excellent (0.9).<sup>32</sup> To test the null hypothesis \( H_0: \text{AUC} = 0.7 \) (\( H_1: \text{AUC} \neq 0.7 \)) with an expected AUC of 0.85, a sample of \( n = 48 \) is appropriate to achieve a significance level of 5% and a power of 80%.<sup>33</sup> In order to compensate for an expected drop-out rate of 20%, we aimed to include a total of 60 participants.

Statistical analyses
Statistics were performed with Stata version 14.1 (Stata Corporation, College Station, TX, USA) and the statistical environment R.<sup>34</sup> Descriptive data (gender, age, weight, BMI, MMSE, FES-I) and the outcome data for strength are described in Tables 2 and 3. Missing data were not imputed in our statistics.

Data processing
The raw force signals were exported to Matlab (Mathworks, Natick, MA, USA; version 8.3.0.532). A low-pass filter (75 ms moving average) was applied to attenuate high-frequency noise. MVIS was defined as the peak value reached
Results
Sixty participants with a mean age of 82.0 years and a standard deviation (SD) of 6.61 were finally included in this study (Figure 1). Due to missing data (extensors: n = 3; internal rotator: n = 2; external rotator: n = 2) of a total of four participants, the analyses of the AUC and DGI were performed including 56 participants. Most of our participants were right handed (n = 53) and had a medium educational level (terminated apprenticeship) (n = 34). Twenty participants had a low- (mandatory school) and six a high-educational level (university degree). Thirty-two participants reported one or more falls within the past 12 months (12 participants fell once, seven had two falls, 13 fell three times and more in the previous year). Twenty-eight participants did not fall in the past year (Table 2). The mean and SD of hip strength and hand-grip strengths are presented in Table 2.

The only hip muscle strength test with an AUC > 0.7 based on the external criterion was the ABD MVIS (0.825, 95% confidence interval [95% CI]: 0.721–0.938) (Table 4). The importance of the variables of the strength was investigated by random forest method with a consensus prediction of individual recursive partitioning tree models. A training set was drawn from the original data using bootstrap with replacement, and a classification tree was built. This was repeated 50,000 times and the final classification is the one that appears the most. The mean decrease in Gini index (DGI), which indicates the quality of a split for every variable by means of the Gini index, was calculated with the package randomForest within the statistical environment R.

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Table 2 Characteristics of our study participants

<table>
<thead>
<tr>
<th>Variables</th>
<th>All group; mean (SD)</th>
<th>Fallers; mean (SD)</th>
<th>Non-fallers; mean (SD)</th>
</tr>
</thead>
<tbody>
<tr>
<td>Sex (F/M)</td>
<td>38/22</td>
<td>21/11</td>
<td>17/11</td>
</tr>
<tr>
<td>Age (years)</td>
<td>82.0 (6.6)</td>
<td>83.3 (6.2)</td>
<td>80.4 (6.8)</td>
</tr>
<tr>
<td>Weight (kg)</td>
<td>65.9 (12.1)</td>
<td>63.8 (12.7)</td>
<td>68.3 (11.2)</td>
</tr>
<tr>
<td>BMI</td>
<td>24.3 (3.4)</td>
<td>24.3 (3.9)</td>
<td>24.3 (2.9)</td>
</tr>
<tr>
<td>MMSE</td>
<td>26.0 (3.5)</td>
<td>24.3 (3.6)</td>
<td>27.8 (2.1)</td>
</tr>
<tr>
<td>FES-I</td>
<td>24.5 (7.1)</td>
<td>26.5 (7.0)</td>
<td>22.2 (6.5)</td>
</tr>
</tbody>
</table>

Abbreviations: BMI, body mass index; MMSE, Mini Mental State Examination; FES-I, Falls Efficacy Scale International; F, female; M, male.

Table 3 Mean and standard deviation (SD) for hip muscle strength groups and hand-grip strength presented for all group, fallers, and non-fallers separately

<table>
<thead>
<tr>
<th>Variables</th>
<th>All group; mean (SD)</th>
<th>Fallers; mean (SD)</th>
<th>Non-fallers; mean (SD)</th>
</tr>
</thead>
<tbody>
<tr>
<td>ABD MVIS (N/kg)</td>
<td>1.0 (0.5)</td>
<td>0.7 (0.3)</td>
<td>1.2 (0.5)</td>
</tr>
<tr>
<td>ABD RFG (N/kg/s)</td>
<td>6.3 (4.5)</td>
<td>4.2 (2.7)</td>
<td>8.8 (5.0)</td>
</tr>
<tr>
<td>ADD MVIS (N/kg)</td>
<td>1.1 (0.5)</td>
<td>0.9 (0.4)</td>
<td>1.3 (0.4)</td>
</tr>
<tr>
<td>ADD RFG (N/kg/s)</td>
<td>4.4 (3.1)</td>
<td>3.3 (2.3)</td>
<td>5.7 (3.4)</td>
</tr>
<tr>
<td>ER MVIS (N/kg)</td>
<td>0.8 (0.3*)</td>
<td>0.7 (0.2**)</td>
<td>0.9 (0.3)</td>
</tr>
<tr>
<td>ER RFG (N/kg/s)</td>
<td>3.7 (2.1* )</td>
<td>3.2 (1.9**)</td>
<td>4.3 (2.1)</td>
</tr>
<tr>
<td>IR MVIS (N/kg)</td>
<td>1.2 (0.3*)</td>
<td>1.1 (0.3**)</td>
<td>1.2 (0.4)</td>
</tr>
<tr>
<td>IR RFG (N/kg/s)</td>
<td>4.2 (2.1*)</td>
<td>3.8 (1.8**)</td>
<td>4.7 (2.4)</td>
</tr>
<tr>
<td>EKT MVIS (N/kg)</td>
<td>1.3 (0.5***)</td>
<td>1.2 (0.4***)</td>
<td>1.4 (0.6***)</td>
</tr>
<tr>
<td>EKT RFG (N/kg/s)</td>
<td>5.9 (3.5***)</td>
<td>5.2 (3.7***)</td>
<td>6.7 (3.1***)</td>
</tr>
<tr>
<td>FLEX MVIS (N/kg)</td>
<td>1.7 (0.6)</td>
<td>1.4 (0.4)</td>
<td>2.0 (0.6)</td>
</tr>
<tr>
<td>FLEX RFG (N/kg/s)</td>
<td>9.9 (5.4)</td>
<td>8.2 (4.9)</td>
<td>11.9 (5.5)</td>
</tr>
<tr>
<td>Hand-grip strength (kPa)</td>
<td>52.8 (24.8)</td>
<td>47.1 (21.0)</td>
<td>59.4 (27.4)</td>
</tr>
</tbody>
</table>

Table 4 Area under the curve (AUC) for the hip muscle strength groups and hand-grip strength (n = 56)

<table>
<thead>
<tr>
<th>Hip muscle group</th>
<th>AUC</th>
<th>95% CI</th>
</tr>
</thead>
<tbody>
<tr>
<td>ABD MVIS</td>
<td>0.825</td>
<td>0.712–0.938</td>
</tr>
<tr>
<td>ABD RFG</td>
<td>0.787</td>
<td>0.667–0.906</td>
</tr>
<tr>
<td>ADD MVIS</td>
<td>0.773</td>
<td>0.648–0.897</td>
</tr>
<tr>
<td>FLEX MVIS</td>
<td>0.755</td>
<td>0.628–0.882</td>
</tr>
<tr>
<td>ER MVIS</td>
<td>0.741</td>
<td>0.610–0.871</td>
</tr>
<tr>
<td>ADD RFG</td>
<td>0.706</td>
<td>0.568–0.844</td>
</tr>
<tr>
<td>FLEX RFG</td>
<td>0.678</td>
<td>0.536–0.820</td>
</tr>
<tr>
<td>ER RFG</td>
<td>0.651</td>
<td>0.506–0.797</td>
</tr>
<tr>
<td>Hand-grip strength</td>
<td>0.649</td>
<td>0.497–0.802</td>
</tr>
<tr>
<td>IR RFG</td>
<td>0.617</td>
<td>0.467–0.766</td>
</tr>
<tr>
<td>EXT RFG</td>
<td>0.610</td>
<td>0.460–0.761</td>
</tr>
<tr>
<td>IR MVIS</td>
<td>0.576</td>
<td>0.422–0.730</td>
</tr>
<tr>
<td>EXT MVIS</td>
<td>0.558</td>
<td>0.404–0.712</td>
</tr>
</tbody>
</table>

Abbreviations: MVIS, maximum voluntary isometric strength; RFG, rate of force generation; CI, confidence interval; ABD, hip abductors; ADD, hip adductors; FLEX, hip flexors; EXT, hip extensors; ER, hip external rotators; IR, hip internal rotators; SD, standard deviation.
The increasing interest in hip muscle strength as a possible contributing factor to the fall risk of older people led to some studies in this field.9,21,39 However, none of them have given an indication on the muscle strength variable that influences the outcome parameter, falls, the most. The importance of the leading ABD variables as analyzed by DGI is followed by ADD MVIS, but the AUC, as well as ABD RFG, of this variable remains below 0.7. This particularly supports our hypothesis of the importance of not only the ABD but also the whole frontal plane muscle strengths. The ADD RFG was ranked clearly lower in the DGI than ADD MVIS. The findings regarding the ABD RFG and ADD RFG seem surprising as a fast recovery step is necessary to regain balance after tripping.40 Therefore, one could assume that the RFG is more important to prevent a fall than the MVIS. The literature shows controversial findings regarding the importance of RFG10,40 and MVIS21 for the fall risk of older people. However, a recent article of Morcelli et al21 supports our findings, although they did not use the same strategy to analyze the data. Morcelli et al21 assessed hip ABD and ADD MVIS and RFG of older women classified as fallers and non-fallers according to their fall history of the previous 12 months. They identified significant differences between fallers and non-fallers regarding the late values of RFG of the ABD. Late values of RFG (≥90 ms after onset of contraction) are more related to MVIS than to the rate of force development.41

Our second hypothesis regarding diagnostic accuracy, comparison between the hip muscle strength and hand-grip strength with the same external criterion, was confirmed for ABD and ADD. Hand-grip strength is assumed to be less accurate for fall-risk assessment than lower limb strength as it is, for example, not directly linked to balance recovery.17 Our findings are supported by this study.

This project was the first to investigate the strength of all hip muscle groups in a population of older age to identify hip muscle groups above a predefined level of diagnostic accuracy for fall history, and consequently their clinical use. The reduction observed in the total test battery to only one parameter (hip ABD strength), measurable in a short time frame, is very important for this age group.

Therefore, this outcome is a perfect starting point. Future research should investigate the value of hip ABD strength for the assessment of the fall risk in older people. If hip ABD strength shows a clear association with falls, then a proper evaluation of hip strength deficits besides the assessment of other risk factors should be integrated in the commonly used assessments in order to enable clinicians to design better-tailored treatment programs.
The method of measuring hip ABD, by a dynamometer fixed to a custom-made frame attached to a regular physical therapy treatment table, we chose in this study is practicable and feasible with older adults in everyday clinics. The time to install and measure participants’ hip ABD is 10.58±1.56 minutes. Further, our measurement method was proven in our earlier article to have a good reliability.

Our investigation on the strength of hip muscle groups in hospitalized and outpatient settings allowed us to get detailed information on the full range of applicability of this new measurement tool. The reduced test battery, an easily practicable measurement method in daily clinics, and wide applicability range further facilitate the investigation and implementation of this easily targetable fall-risk parameter.

A point to consider in future investigations of ABD MVIS as a fall-risk assessment tool is the fall prevalence of the sample under study. Some of our participants were recruited in a geriatric hospital known for its fall-risk prevention interventions. This led to our higher fall prevalence (53%); the worldwide fall rate of older people as reported by WHO is 28%–35%. This higher prevalence only slightly influences the results of the AUC and DGI but can possibly lead to a small overestimation of the diagnostic accuracy of a measurement instrument.

Our sample size was calculated prospectively to achieve a power of 80%; nonetheless, sixty participants is a rather small sample size for this heterogeneous population. Therefore, to allow a wide clinical use, hip ABD MVIS should be further investigated in a broader setting of older people to gather insight into its diagnostic accuracy for daily clinical use as a fall-risk assessment tool. Lastly, we assessed our participants MVIS and RFG in the same trial and found only a slightly weaker ability to distinguish between fallers and non-fallers based on ABD RFG compared to the ABD MVIS. Due to the complexity of this task for older people, this combined measurement of MVIS and RFG could have influenced the study results and should be investigated in two different trials to allow a stricter differentiation of the results for MVIS and RFG.

Conclusion
Hip ABD seemed to be an important hip muscle group to distinguish between older adult fallers and non-fallers compared with the chosen external criterion, history of falling. In our population, hand-grip strength has a lower ability to distinguish between the two groups than ABD and ADD. Future studies should focus on the diagnostic accuracy of ABD MVIS and a specific hip ABD muscle training to decrease fall risk.

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Disclosure
The authors report no conflicts of interest in this work.

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