Extraglottic airway devices: technology update

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Abstract: Extraglottic airway devices (EADs) have revolutionized the field of airway management. The invention of the laryngeal mask airway was a game changer, and since then, there have been several innovations to improve the EADs in design, functionality, safety and construction material. These have ranged from changes in the shape of the mask, number of cuffs and material used, like rubber, polyvinylchloride and latex. Phthalates, which were added to the construction material in order to increase device flexibility, were later omitted when this chemical was found to have serious adverse reproductive outcomes. The various designs brought out by numerous companies manufacturing EADs resulted in the addition of several devices to the airway market. These airway devices were put to use, many of them with inadequate or no evidence base regarding their efficacy and safety. To reduce the possibility of compromising the safety of the patient, the Difficult Airway Society (DAS) formed the Airway Device Evaluation Project Team (ADEPT) to strengthen the evidence base for airway equipment and vet the new extraglottic devices. A preuse careful analysis of the design and structure may help in better understanding of the functionality of a particular device. In the meantime, the search for the ideal EAD continues.

Keywords: extraglottic airway devices, laryngeal mask airway, other extraglottic airway devices, safety, technology update

Introduction

Extraglottic airway devices (EADs) have revolutionized the field of airway management. These devices also known as supraglottic airway devices or supralaryngeal airways are orally inserted with their distal ends lying in the hypopharynx or esophagus. The American Standards for Testing Materials (ASTM) Committee F29 on Anesthetic and Respiratory Equipment has defined supraglottic airway devices as “Airways that are intended to open, secure, and seal the supraglottic area to provide an unobstructed airway in spontaneously breathing or ventilated patients, typically during anesthetic procedures.”1 The devices produced according to the ASTM facilitate unobstructed access of respiratory gases to glottic inlet by displacing tissue, do not require an (external) facial seal to maintain airway patency, terminate in a 15/22-mm connector to facilitate positive pressure ventilation via an anesthetic breathing system, are capable of maintaining airway patency when the (15/22-mm) airway connector is open to ambient atmosphere and minimize escape of airway gases to the ambient. They are used for primary airway management and rescue ventilation when face mask ventilation is difficult, and as a conduit for endotracheal intubation. There has been a plethora of airway devices and equipment in the market (Figure 1). New EADs have
been described at a rate of one per year for the last 25 years, increasing to two per year since the turn of the century.\(^2\) Unfortunately, not all the devices have been tested with apropos evidence pertaining to their clinical performance or safety. This concern prompted the Difficult Airway Society (DAS) to form the Airway Device Evaluation Project Team (ADEPT), which was tasked with formulating a method to formally evaluate equipment associated with airway management regarding safety issues and clinical performance based on solid evidence.\(^3\)

Technology has tremendous significance in today’s complex professional environment with special emphasis on patient safety. Up-to-date solutions can make for more efficient, cost-effective performance, conserving time and resources. With any new scientific advancement or technology, there is a learning curve followed by clinical studies which evaluate the newly acquired technology for its benefits, limitations and side effects. This review covers the technology aspects of these EADs.

**Objective**
This review was performed to assess and evaluate the update on technology aspects and design specifications of various extraglottic devices in current use.

**Design**
This is a narrative systematic review of the randomized controlled trials (RCTs) and the other available literature on extraglottic devices in contemporary use.

**Methods**
The first two authors independently searched PubMed and Cochrane Database of Systematic Reviews (1935–2017). Data were also obtained from textbooks. The keywords used for PubMed and Cochrane Database of Systematic Reviews were extraglottic airway devices, laryngeal mask airway, other extraglottic airway devices, safety and technology update. A total of 86 articles were selected. Among these, there were 14 review articles including three meta-analyses, 16 comparative studies and two articles from books (Table 1).

**Table 1** Data source

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<td>Supraglottic airway devices and technology update</td>
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Elimination criteria
The articles related to EADs not inserted orally (tracheostomy) and those not so popular and in current use (eg, the Elisha device) were not included. The articles which did not provide information on construction material, functional evolution, safety issues and technology updates were also excluded.

Classification of devices
Classification of the EADs parallels their design and functional evolution. There are several criteria for classifying the EADs based on variations ranging from cuffed versus noncuffed, the number of cuffs, location of the distal end in relation to glottis, sealing mechanism, perilaryngeal versus base of tongue, reusable versus disposable, protection against aspiration and chronological order (though objections were raised regarding this, further complicating the classification) to increasingly complex variations of the original designs.

Cuffed versus noncuffed
Devices such as classic laryngeal mask airway (cLMA) and ProSeal™ laryngeal mask airway (PLMA) are cuffed, while i-gel and Baska mask are examples of noncuffed devices, the latter having the advantages of avoiding the problems associated with cuff-related morbidity. The flip side is that they may be accompanied with increased risks of leaks and associated problems. The cuffless devices could offer the advantage of being magnetic resonance (MR) compatible by obviating the ferromagnetic material in the pilot balloon of the cuff inflation assembly.

Location of the distal end in relation to glottis
Supraglottic devices seal around the glottis inlet and remain superior to the larynx (eg, cLMA, PLMA and Ambu masks). Retroglottic devices are laryngeal tubes that terminate in the upper esophagus, remaining posterior to the glottis (eg, Laryngeal Tube [LT] and Laryngeal Tube Suction II [LTS-II]).

Sealing mechanism: perilaryngeal versus base of tongue
Base-of-tongue sealers such as LT, LTS-II, Streamlined Liner of the Pharynx Airway (SLIPA) and Cobra Perilaryngeal Airway (Cobra PLA™) are also known as pharyngeal sealers. The laryngeal mask airways (LMAs) and laryngeal masks (LMs) seal the perilaryngeal area and are known as perilaryngeal sealers. The cLMA, invented by Dr Archie II Brain, was the first perilaryngeal sealer.

Reusable versus disposable
Original EADs (cLMA, LTS) were manufactured as reusable equipment; however, disposable devices (eg, i-gel, Ambu AuraGain) now available are cheaper and easier to maintain than the reusable devices and preclude concerns about prion disease. Disposable devices are of special importance in the following situations: 1) resuscitation and field situations and 2) prevention of disease transmission.

Protection against aspiration
The addition of a gastric tube such as PLMA, i-gel and devices with reservoir (eg, SLIPA) provides some protection against aspiration. Higher oropharyngeal seal pressure (OSP), the first seal and the hypopharyngeal seal, the second seal, are important safety factors for protection against aspiration (eg, PLMA). The SLIPA has a different mechanism separating respiratory and gastrointestinal tracts and allowing storage of gastric fluid, being a hollow liner of the pharynx under pressure, thus providing a liquid trap within the device.

Device generation
The idea of classifying the EADs as first or second generation was introduced by Cook and Howes. The first-generation EADs fit the description “simple airway devices”. These airway devices have a single airway tube. They are devoid of any specific design characteristics aimed at reducing the risk of pulmonary aspiration of gastric contents. The classic examples of first-generation devices are LMA and Combitube, both of which became available during the second half of the 1980s. On the other hand, the second-generation EADs (PLMA, i-gel) incorporate specific design features to improve positive pressure ventilation and reduce the risk of aspiration.

A controversial new term, third-generation EADs, has been introduced in anesthesia literature. Initially, the term was used to indicate facilitated intubation through EADs. However now, the term is used to denote the presence of a self-energizing sealing cuff (Baska). No consensus has been reached regarding the classification of these devices; therefore, a proper scientific classification of extraglottic airways is still awaited.

Design evolution
The first device which can be described as extraglottic was introduced by Dr Francis Shipway in 1935, a pharyngeal airway comprising an inflatable rubber balloon added to the shaft of the Guedel airway to prevent aspiration of blood during nasal procedures. Two years later, a Canadian doctor Beverley Charles Leech invented a “pharyngeal bulb gasway”...
which would fit more closely to the larynx. It consisted of an anatomically shaped, hollow rubber bulb which would be stuck in the pharynx. However, neither device became popular.

It took almost 50 years for another supraglottic airway (LMA) to be designed in 1983. The LMA consists of an airway tube connected to an inflatable mask. The invention of the LMA was a game changer in airway management, and it came about when Brain came across two difficult airway scenarios in his practice. An inspiring lecture about airway management needing a new direction by Dr Lucien Morris, an American anesthesiologist, led to Brain renewing his work on an alternate airway device which would be somewhere between a face mask and an endotracheal tube, and he came up with the LMA. Of course, the final product was created after much experimentation, making plaster casts of cadaver larynxes, using a combination of the Goldman nasal mask (used for dental anesthesia) and a diagonally slit red rubber endotracheal tube. The obstacles on the way to making a device that was capable of changing the management of the difficult airway were many: discovering the appropriate material for the cuff, safety design issues (how to keep the epiglottis from obstructing the airway), misinterpretation of experimental LMs as being of sexual nature and even after the LMA was commercially manufactured being chastised by a religious society for producing such “evil things”; acceptance of the device by a skeptical anesthesia community, and the last but not the least, finding someone to finance the manufacturing of the LMA.

Specific EADs
A brief review of EADs in common use is given below.

LMA family
The LMA standard, now known as cLMA, was the first airway device to directly encircle the laryngeal structures with the end of its bowl located very close to the vocal cords. The development of LMA continued, with several additions to its family (Figure 2): the LMA Unique, a disposable device ready to use especially in field scenarios and to avoid cross contamination and prevention of certain diseases; the LMA Flexible designed for intraoral procedures and the Intubating LMA (Fastrach) which allowed blind intubation through the device in difficult airway scenarios. The addition of integrated fiber optics with a monitor resulted in the LMA CTtrach which visualized the dynamics of tracheal intubation. The ProSeal and LMA Supreme have a gastric or drain tube in addition to the airway tube separating the respiratory and the gastrointestinal tracts.

cLMA
It consists of a mask with an inflatable cuff and an airway tube connecting the mask to the anesthesia circuit or a self-inflating bag. It can easily be placed by paramedics. However,
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the device provides low OSP (10–20 cm H₂O), may produce gastric insufflation and offers no protection against pulmonary aspiration (Figure 3).²¹

**ProSeal LMA**

It is a reusable device with dorsal and ventral cuffs allowing for a higher OSP and a drain tube to access to the gastrointestinal tract. The airway and the drain tubes are joined together to form the rigid bite block which prevents obstruction in case the patient bites it (Figure 4).¹⁹

**LMA Supreme**

The LMA Supreme is a disposable version of PLMA with a reinforced cuff preventing folding of the mask with an oval airway cross section for more stability to the device. It has a built-in bite block and fixation tab to secure the airway. Its

**Figure 3** Classic LMA.
Abbreviation: LMA, laryngeal mask airway.

**Figure 4** (A) ProSeal™ LMA. (B) LMA Supreme™.
Abbreviation: LMA, laryngeal mask airway.
performance is comparable to the PLMA and superior to the cLMA (Figure 4).20

LMs and others
Encouraged by the success of this device, many other EADs have subsequently been invented since 1990s. Devices with a similar design to the LMA family are known as LMs and were introduced in the following years (eg, AuraOnce, SoftSeal® or Solus LMs).7,22 The designs of other EADs differed from that of the LMA family devices such as the SLIPA, Elisha airway device, i-gel, Cobra PLA or LT, LTS-II, intubating laryngeal airway, intubating Laryngeal Tube Suction Disposable (iLTS-D), Baska mask and Totaltrack VLM (Figure 5).9,23–32

LT and LTS-II
The LT and LTS-II comprise a simple airway tube with oropharyngeal and esophageal cuffs with an opening between the two cuffs for the passage of gas into the larynx. The LTS-II has an additional lumen opening into the esophagus beyond the distal cuff. Similar to the Combitube, its use is recommended only for emergencies or failure to intubate and ventilate.33,34 The LTS-II has a high oropharyngeal seal, and insertion of the device is considered easy. Postinsertion ventilation is less reliable than that with the PLMA, and the device is associated with a relatively high rate of airway obstruction and occasional glottic placement has been reported. The device is not suitable as a tracheal tube conduit due to its small airway orifice.

Cobra PLA
Its tip is shaped like the head of a Cobra and has a grating allowing for ventilation while avoiding obstruction. Just proximal to the tip of the device is a low-pressure and large-volume pharyngeal cuff. It was found to be similar to the cLMA in terms of ease of insertion but achieved higher sealing pressures and can be used for airway rescue (Figure 5).27,35

Streamlined Liner of the Pharynx Airway
This is a cuffless device, pre-shaped to sit in the pharynx, with a heel and a hump to fit the soft palate and the base of the tongue, respectively. It has a hollow chamber that can store up to 50 mL of drained gastric fluid. It was designed for short general anesthetic procedures. A study in children comparing SLIPA and LMA Unique reported that SLIPA provided a better airway seal and stability.36 Another study reported that the SLIPA offers

Figure 5 Laryngeal mask and others: (A) Totaltrack VLM, (B) Ambu mask, (C) Baska mask, (D) Laryngeal Tube, (E) Laryngeal Tube Suction, (F) Cobra PLA™, (G) LMA-Protector™, (H) Ambu AuraGain and (I) i-gel.
Abbreviations: PLA, Perilaryngeal Airway; LMA, laryngeal mask airway.
the advantage of less perilaryngeal gas leakage than the PLMA with change in head position and during insufflation of the peritoneal cavity.\textsuperscript{37} SLIPA can be used as a useful alternative to PLMA in patients undergoing lower abdominal laparoscopic surgery with muscle relaxant and controlled ventilation.

Epiglottic downfolding was reported to be significantly lower with the SLIPA as compared to the PLMA in patients undergoing lower abdominal laparoscopic surgery (Figure 6).\textsuperscript{38}

\textbf{i-gel}

It is a single-use preshaped cuffless device, made of a gel-like material. The shape, softness and contours accurately mirror the perilaryngeal anatomy. There is also a narrow drain tube for insertion of a gastric tube. It is easy to insert, MR safe and allows a standard high-diameter tracheal tube to negotiate through the airway tube. The OSP and the gastric insertion rates are comparable with PLMA, but the insertion time is shorter and the incidence of sore throat is lower (Figure 5).\textsuperscript{39}

\textbf{Ambu AuraGain}

It is an anatomically curved single-use device and can be easily inserted. It integrates gastric access and intubation capability. It is made up of phthalate-free material and is MR safe. Similar to PLMA, it has an integrated bite block which prevents airway occlusion. Pilot balloon identifies mask size and provides tactile indication of degree of inflation. There are navigation marks for guiding flexible scope. The pilot balloon identifies mask size. A study comparing it with LMA Supreme reported that both devices had similar OSPs but the AuraGain resulted in less postoperative sore throat despite being harder and taking longer to insert (Figure 5).\textsuperscript{40}

\textbf{Baska mask}

The Baska mask is a new noncuffed EAD which provides a superior seal as compared to the cLMA. It also has additional safety features: 1) a large sump cavity with two aspiratable gastric drain tubes; 2) a tab for manually curving the mask to ease insertion; and 3) a suction elbow integral to one port with a second port acting as a free air flow access. The drain tubes can also work as ventilatory tubes in case the ventilatory tube gets obstructed. These features may reduce the risk of pulmonary aspiration of secretions or gastric contents that accumulate in the supraglottic area (Figure 5).\textsuperscript{31}

The details of a few specific EADs are given in Table 2, and the salient features of some EADs are discussed as follows.

\textbf{Mask, cuff and bowl}

EADs have masks with or without inflatable cuffs. The cuff could be part of the LMAs, the LMs or the pharyngeal sealers. The i-gel has a mask with a non-inflatable gel-filled cuff. A larger cuff as seen in the PLMA with its posterior component improves the oropharyngeal seal without increasing the cuff pressure.\textsuperscript{41} Both the LMA Supreme and LMA-Protector\textsuperscript{TM} have reinforced tips to prevent posterior folding of the mask. The cuff of Ambu mask is tapered at the tube. The Baska mask and the recently introduced LMA-Protector have self-energizing cuffs.\textsuperscript{31,42}

The earlier introduced pharyngeal sealers had single cuffs. However, the present pharyngeal sealers have two cuffs: the smaller hypopharyngeal and the bigger pharyngeal which forms a seal with the respiratory tract (eg, LT, LTS-II and iLTS-D). The iLTS-D, a modified LT, allows intubation similar to an intubating LM.

A deeper bowl of the mask is superior to a shallow bowl as it improves the oropharyngeal seal. The PLMA has a larger and deeper mask bowl which lacks the semirigid shell of the cLMA. A correctly placed PLMA provides higher OSP (10 cm H\textsubscript{2}O or more) than the cLMA. The storage capacity of the cLMA is only 4 mL in comparison to 50 mL of that of SLIPA device, and therefore, the risks of aspiration with regurgitation are theoretically higher (Figure 7).\textsuperscript{9}

\textbf{Mask aperture bars (MABs), epiglottis-elevating bar, Cobra head, fins and epiglottic rest}

The original cLMA was developed with two MABs to prevent the epiglottis from obstructing the airway; nevertheless, its function has been questioned as the presence of MABs may interfere with endotracheal intubation if it is necessary to pass a tube through the EAD.\textsuperscript{43–46} Several of the newer EADs (Baska and LMA-Protector) have no MABs, while others contain a varying number of epiglottic bars or show

\begin{figure}[h]
\centering
\includegraphics[width=0.5\textwidth]{streamlined_liner_of_the_pharynx_airway.png}
\caption{Streamlined Liner of the Pharynx Airway.}
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<tr>
<th>Extraglottic airway device, year of manufacture, construction material</th>
<th>Sealing site</th>
<th>Strengths</th>
<th>Weaknesses</th>
<th>Effectiveness</th>
<th>Safety of the device</th>
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<td>No integrated bite block</td>
<td>Difficult and failed intubation</td>
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<td>No malposition diagnosis</td>
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<td>Reinforced, long, narrow, airway tube</td>
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<td>Easy to use</td>
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<td>Failure rates are higher for blind intubation versus lightwand- or fiber optic-guided intubation</td>
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<td>Short wide rigid tube to accommodate ETT integrated bite block</td>
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<td>Pediatric sizes not available</td>
<td>High success rate</td>
<td>No aspiration protection</td>
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<td>PLMA, 2000, silicone*</td>
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<td>First time success rate and insertion time longer than cLMA, bulky cuff</td>
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<td>Allows ventilation at higher airway pressures</td>
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<td>OSP may be less than PLMA</td>
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<td>Some aspiration protection</td>
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<td>Difficult and failed intubation</td>
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<td>Perilaryngeal</td>
<td>Multipurpose dynamic curve</td>
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<td>Similar to PLMA though no clinical data available</td>
<td>Phthalate-free dual gastric ports</td>
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<td>MR safe, cuff pilot technology</td>
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<td>Dual gastric channel and suction port</td>
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<td>Should perform better than PLMA but no clinical data available</td>
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<td>Base of tongue</td>
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<td></td>
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<td>Easy insertion</td>
<td></td>
<td>Difficult and failed intubation</td>
<td>Easy atraumatic aspiration</td>
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<td>Drain tube present</td>
<td>Out-of-hospital use</td>
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<td>King LTS-II, 2004, silicone* and PVC</td>
<td>Base of tongue</td>
<td>High OSP</td>
<td>Airway obstruction more common</td>
<td>Recommended for emergencies or failed intubation and ventilation</td>
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<td>Drain tube present</td>
<td>Insertion success rate lower</td>
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<td>Better ventilation, less gastric insufflation as compared to LT</td>
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### Table 2 (Continued)

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<th>Weaknesses</th>
<th>Effectiveness</th>
<th>Safety of the device</th>
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<td>Base of tongue</td>
<td>Higher sealing pressure than cLMA</td>
<td>A rigid head of device and soft pharyngeal cuff</td>
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<td>No aspiration protection</td>
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<td>Aspiration protection similar to PLMA but better than cLMA</td>
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<td>Cuffless</td>
<td>Bloods on device more frequent</td>
<td>No integrated bite block</td>
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<td>SLiPA</td>
<td>Perilaryngeal</td>
<td>Higher insertion success</td>
<td>Narrow drain tube</td>
<td>OSP between cLMA and PLMA</td>
<td>Reliable seal</td>
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<td>i-gel, 2007, SEBS</td>
<td>Perilaryngeal</td>
<td>Cuffless</td>
<td>Sitting over hypopharynx not as good as PLMA</td>
<td>Decrease pharyngolaryngeal morbidity</td>
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<td></td>
<td>Rigid tube working as bite block</td>
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<td></td>
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<tr>
<td>Baska, 2012, silicone*</td>
<td>Perilaryngeal</td>
<td>Anatomic seal</td>
<td>Insertion success rate lower than PLMA</td>
<td>Suitable for spontaneous and controlled ventilation</td>
<td>Should provide better protection against aspiration</td>
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<tr>
<td></td>
<td></td>
<td>Cuff inflation and monitoring not required</td>
<td></td>
<td>Difficult and failed intubation</td>
<td>Insufficient data</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Two gastric drainage ports</td>
<td></td>
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</tr>
<tr>
<td>AuraOnce, 2007, PVC</td>
<td>Perilaryngeal</td>
<td>Preformed curve (70°) with convenient depth marks</td>
<td>Low OSP</td>
<td>Suitable for spontaneous short elective procedures</td>
<td>No aspiration protection</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Reinforced mask tip</td>
<td>No integrated bite block</td>
<td>Difficult and failed intubation</td>
<td>Softer, more flexible cuff than LMA</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Higher insertion success rate</td>
<td></td>
<td></td>
<td>MR-safe new versions phthalate free</td>
</tr>
<tr>
<td>Ambu AuraGain, 2014, PVC (phthalates free)</td>
<td>Perilaryngeal</td>
<td>Higher insertion success rate</td>
<td>Narrow drain tube</td>
<td>High OSP</td>
<td>Should provide better protection against aspiration, not much literature available</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Short wide preformed airway tube</td>
<td></td>
<td>Suitable for spontaneous and controlled ventilation</td>
<td>MR safe, phthalate free</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Drain tube</td>
<td></td>
<td>Difficult and failed intubation</td>
<td></td>
</tr>
<tr>
<td>Totaltrack VLM, 2013, PVC and silicone*</td>
<td>Perilaryngeal</td>
<td>Allows simultaneous ventilation and intubation with continuous visualization</td>
<td>Insufficient clinical data</td>
<td>Suitable for spontaneous and controlled ventilation</td>
<td>Difficult and failed intubation</td>
</tr>
<tr>
<td></td>
<td></td>
<td>Dedicated aspiration system of internal mask secretions</td>
<td></td>
<td></td>
<td>Allows positive pressure oxygenation in the ventilation, intubation and extubation mode with continuous visualization</td>
</tr>
</tbody>
</table>

**Note:** *Medical-grade silicone.

**Abbreviations:** cLMA, classic LMA; OSP, oropharyngeal seal pressure; LMA, laryngeal mask airway; PVC, polyvinylchloride; ETT, endotracheal tube; IPPV, intermittent positive pressure ventilation; PLMA, ProSeal™ LMA; MR, magnetic resonance; LT, Laryngeal Tube; LTS-II, Laryngeal Tube Suction II; PLA, PeriLaryngeal Airway; SLiPA, Streamlined Liner of the Pharynx Airway; SEBS, styrene ethylene butadiene styrene.
modified versions such as epiglottic-elevating bar, Cobra head, epiglottic rest or fins.

Van Zundert et al in a prospective, randomized, crossover comparison of three EADs studied whether EADs with or without MABs result in similar anatomical positions in patients undergoing surgery. The endoscopic evaluation did not demonstrate any difference between the EADs with or without MABs. The morphometric studies of the adult human epiglottis have reported the width of the epiglottis as ±27 mm for males and ±21 mm for females which is in contrast to the width of the aperture of EADs (±15 mm) and therefore questions the need for the MABs.

The epiglottis-elevating bar is present in the Intubating LMA to lift the epiglottis during intubation. In LMA Supreme, the MABs have been modified into two “fins” to prevent epiglottic downfolding. The Cobra head of the Cobra PLA, in addition to providing stability, levers the epiglottis away from the airway tube. In i-gel, an artificial epiglottis and a protective ridge prevent the downfolding or obstruction of the distal opening of the airway (Figure 7).

Airway tube

The cLMA has a single airway tube with radius of curvature greater than the natural curvature in the mouth as opposed to the LMA Fastrach, LMA Supreme and Ambu Aura LM devices which have anatomical preformed curves. A short wide tube facilitates tracheal intubation and decreases airway resistance, as seen in the Cobra PLA. Preforming the airway tube makes for easy insertion and avoids finger insertion while using the Fastrach or Ambu LMAs. It has been reported that an oval airway cross section of the tube as seen in the LMA Supreme improved stability of the airway, in comparison to PLMA which had a circular cross section.

Wire reinforcing of the airway tube makes it nonkinkable and flexible as seen in LMA Flexible and PLMA. This also makes convenient the use of airway tube in nonsupine positions including prone position. The LMA Supreme has two lateral ventilation paths divided by the drain tube (Figure 8).

Drain or gastric tube

The addition of a second or drain tube, positioned laterally (PLMA, i-gel) or posteriorly (LMA Supreme) to the airway tube, separates the alimentary and respiratory tracts. It allows escape of fluids from the stomach and reduces the risk of gastric insufflation and pulmonary aspiration, helps in optimal placement of the device, determines its correct position and permits monitoring (temperature and cardiac output). Other advantages include opportunity to pass a gastric tube. The distal drain tubes of LMA Supreme and LMA-Protector have a slant of 10° thereby allowing the cuff to follow the contours of upper esophageal sphincter which may improve the placement of the device and the hypopharyngeal seal. However, in the latest modification of LMA Supreme, this slant has been removed. The Baska mask and LMA-Protector have two drain tubes which emerge proximally as separate ports.

Maximal diameters of orogastric tubes that can be inserted through the gastric channels of the size 3, 4 and 5 of the LMA Supreme are 14, 16 and 16 Fr, respectively, compared with 16, 16 and 18 Fr for the LMA-Protector and the PLMA.
Extraglottic airway devices

Figure 8 shows the gel displacement test for diagnosing correct placement of PLMA.

**Integral bite block/buccal cavity stabilizer**

The length of the integral bite block may vary depending on the size of the device. It helps in preventing the patient biting and obstructing the airway tube, diagnosing device malposition and thus improving patient safety (PLMA, i-gel). The buccal cavity stabilizer in i-gel provides vertical strength to aid insertion. It is wide and concave with a built-in natural curvature and an inherent propensity to adapt its shape to the oropharyngeal curvature of the patient. It eliminates the potential for rotation and also reduces the risk of malposition.

**Tab**

The Baska mask tab can improve the insertion success rate by increasing the angulation for easy negotiation of the oropharyngeal curve (Figure 9).

**Fixation tab**

It aids in securing the device with adhesive tape and may also help in choosing the proper size of the device (eg, LMA-Protector and LMA Supreme). The tab should sit between 0.5 and 2.0 cm from the upper lip; otherwise, a different size should be chosen (Figure 9).

**Tracheal conduit/integrated fiber optics**

The Fastrach was primarily designed for tracheal intubation through the mask. It is not easy to perform endotracheal intubation through PLMA and LMA Supreme as they have narrow airway tubes in comparison to Ambu airway mask, i-gel, Baska mask and LMA-Protector. Therefore, they need extra adjuncts, such as a bronchoscopic/Aintree Intubation Catheter-guided technique, to place an adequate size tube through them. The airway lumen of the LMA-Protector (maximal internal diameter 13 mm) is wide enough to pass an adequately sized adult tracheal tube directly, without the use of an intermediate exchange catheter (ie, a maximal size tracheal tube of 6.5, 7.5 and 7.5 mm for the device sizes 3, 4 and 5 respectively). As such, use of the LMA-Protector as a conduit for fiber optic-assisted rescue intubation should be easier to accomplish than using an LMA Supreme or PLMA. However, these hypotheses require investigation as no clinical evidence is available.

The LMA CTrach and the Totaltrack VLM allow simultaneous ventilation and intubation with continuous visualization of the laryngeal structures and the dynamics of tracheal intubations due to integrated fibreoptics. The Totaltrack VLM has a dedicated gastric aspiration tube and laryngeal tube for aspiration of internal mask secretions (Figure 10).
Red Plug/Integrated Cuff Pilot™

Red Plug or the manual vent is a modification of the PLMA and is incorporated into the pilot balloon. It should be kept open during autoclaving to prevent damage such as herniation of the cuff from resultant built-up of undue pressures due to residual fluid or air.53 Integrated Cuff Pilot has an integrated cuff pressure indicator for single-use airway management devices (LMA-Protector) that allows continuous cuff pressure monitoring and is another improvement of the pilot balloon (Figure 10).42

Construction material issues

Several materials have been tried for the construction of the different components of the EADs varying from latex and silicone to polyvinylchloride (PVC). Vulcanized rubber is natural rubber with additives such as sulfur and other curatives. Vulcanization makes rubber much stronger and more flexible and increases resistance to heat and other environmental conditions. Vulcanized rubber cuffs obtained from the Goldman nasal mask were used for the first prototypes of LMA in 1981.14 Later on, they were replaced by materials such as latex and medical-grade silicone.

Latex is a mixture of organic compounds produced by some plants in special cells called caticifers. There is a high incidence of allergy reported with the use of latex-based devices: 1–2% in normal population and rising up to 10% among the health care professionals.54 Medical-grade silicone is a near-ideal construction material with an indefinite shelf life.53 Silicone rubber is an elastomer (rubber-like material) composed of silicone, a polymer containing silicon along with carbon, hydrogen and oxygen. Silicone rubber offers good resistance to extreme temperatures, being able to operate normally from −100 to 300°C (−148 to 572°F).55 Silicone offers the advantages of making the device reusable as it allows mechanical cleaning and sterilization. The cuffs of the reusable LMAs and the Baska mask are manufactured from a silicone. The distal tip of the laryngeal blade of the Totaltrack VLM is protected by a patented silicone sleeve, decreasing the possibility of tip breakage and tissue injury.32

Medical-grade PVC was used to construct disposable devices to accommodate concerns about disease transmission and the costs of cleaning and sterilization of reusable EADs. The first disposable EAD was the LMA Unique, made of PVC.56 Most available disposable LMs on the market, such as the LMA Supreme, AuraOnce or Solus LM, are made of PVC. The Cobra PLA and Cobra PLUS contain PVC with different softness. The head of the Cobra PLUS device is rigid, while the pharyngeal cuff is soft.27

Phthalate-free PVC has been employed for manufacturing Ambu AuraGain and the recently introduced LMA-Protec-
tor.42,57 Phthalates are used primarily as plasticizers in flexible PVC products to impart flexibility to plastics. Their use is approved in several medical devices.58,59 Components used in plastics, such as bisphenol A, polybrominated diphenyl ethers, tetrabromobisphenol A and phthalates, are released from plastic products and are also known as endocrine-disrupting compounds owing to their ability to modulate the endocrine system.60

The immature male reproductive tract is the most sensitive to phthalates, with exposure resulting in increased incidence of undescended testes, decreased testicular weight, decreased anogenital distance and other effects.61 Human studies increasingly report associations of phthalates with various adverse reproductive effects on steroid genesis and luteal function.62 Ethylene–vinyl acetate copolymer, a plastic material with limited flexibility, has been used for manufacturing the SLIP A. This material is hard, and there were reports of more frequent traces of blood on the device.63

A very soft gel-like transparent thermoplastic elastomer called styrene ethylene butadiene styrene (SEBS) has been used to construct the bowl of the i-gel airway which is a cuffless device.64 Initially, it was expected that this material may warm up to body temperature and change its properties with subsequent improvement in perilaryngeal seal. This specula-
tion has not been confirmed in clinical practice.\(^{65}\) SEBS is also very stable in high altitude and hyperbaric conditions which might create potential for its use during helicopter transfers and in diving medicine.\(^{26}\)

The inflation valve of the PLMA is similar to that of the cLMA and Intubating LMA. It has a white polypropylene core and a stainless steel spring.\(^{27}\) The MR-compatible EADs such as MR-safe LMA, Solus LMA and Ambu disposable LMA have nonferromagnetic material in the valve assembly. i-gel and Ambu AuraGain are also MR compatible. The PLMA contains metal wires which makes it MR incompatible.

**Available sizes**

Earlier, only the adult sizes of EADs were available. Presently, both adult and pediatric sizes are available for most of the devices. However, pediatric sizes are not available for Intubating LMA. All sizes are available for Cobra PLA including a pediatric 0.5 size. There is no standardization of the sizes. Manufacturers have their own sizes of the devices. The appropriate size for any patient is device specific mostly on weight basis; however, it may also be based on gender.

**Functional evolution**

The LMA fills the gap between a face mask and a tracheal tube. The entry of the LMA in the anesthesiologists armamentarium changed the way anesthesiologists approached the management of the airway inexorably changing daily practice and algorithms. The LMA allowed the anesthesiologists to be hands free and also broadened the scope of EADs. This popularity stems directly from their ease of use, simplicity of training, predictability and speed of insertion. These devices have several advantages over the endotracheal tube like increased speed and ease of placement, improved hemodynamic stability at induction and during emergence of anesthesia, reduced anesthetic requirements, lower frequency of coughing during emergence and lower incidence of sore throat.\(^{21}\)

The last 30 years of clinical anesthesia practice have witnessed several modifications with increasing use of these devices and a widening scope of the EADs right from conduits for tracheal intubation in difficult airway scenarios or as airway adjuncts in resuscitation, cardiac arrest or in prehospital medicine in pediatric and adult population leading to several important improvements in the design and functional evolution of the device.\(^{66,67}\) LMA has been used for delivery of surfactant in preterm babies.\(^{68}\)

EADs are not suitable alternatives for prolonged ventilation in the ICU, and intensivists without anesthesia background are not familiar with these devices. However, the devices have been used in ICU setting for failed and difficult intubation, postoperative ventilation and for their role in percutaneous dilatational tracheostomy and postoperative care.\(^{69,70}\)

This enthusiastic acceptance has triggered the search for new designs and use in previously contraindicated locations, patients and surgery, thus spreading the reach of the airway safety net the EADs impart. Since these new devices provide alternate ways to secure the airway, they can help avert the disastrous consequences of failed face mask ventilation or intubation and as such have now been accepted by the anesthesia community.

This functional evolution would of course have been impossible without appropriate patient selection, device size, knowledge and experience of optimum and atraumatic device placement and maintenance of adequate OSP.

The Vortex approach is a new thought process based on the principle that there are three “nonsurgical” techniques to establish a patent airway: use of a face mask, a supraglottic airway or an endotracheal tube.\(^{71}\)

**Complications and safety issues**

The correct use of EADs is seldom associated with serious complications as the majority of them are minor in nature and are often associated with a divergence from the manufacturers’ advice on usage of these devices. Postoperative sore throat, dysphagia, pain on swallowing or hoarseness and nerve injuries may result from excessive unmonitored cuff volume and pressure of the devices on cervical vasculature and microcirculation of the pharyngeal mucosa. Paying attention to the recommended cuff pressures may decrease the incidence of these complications.\(^{72}\)

Tracheal intubation is accompanied by increased airway resistance resulting from turbulent flow due to a tube within a tube (tracheal tube within the trachea), and this fact inspired Brain to invent the LMA. There is recorded actual and potential damage associated with the use of tracheal tube during routine anesthesia, and this remains a driving force for the development of future EADs. A meta-analysis involving 29 randomized prospective controlled trials in adults compared LMAs versus tracheal tube for airway maintenance in patients under general anesthesia and found that LMAs have a lower incidence of postoperative sore throat, hoarseness, coughing and laryngospasm during recovery from anesthesia.\(^{73}\) Similar results along with decreased incidence of vomiting were confirmed in pediatric population by another RCT.\(^{74}\)
A disadvantage of the LMAs was the increased probability of failure to insert the device on the first attempt. There is a 5–10% failure rate of insertion of these devices on the first attempt due to anatomical differences in the perilyngeal area, and it may be advisable that the operator should keep the sealing sites of these devices in mind. If insertion fails with one device, then the alternate chosen EAD should have a different sealing site to ensure successful placement (failure rate less than 1%).

There has been the fear of aspiration associated with EAD use, though the clinical evidence of pulmonary aspiration using the LMA was comparable to anesthesia administered with an endotracheal tube. Evidence-based RCTs are not easy to get since the overall incidence of pulmonary aspiration associated with the use of EADs is low and RCTs would require about a million patients if a significant conclusion (50% decrease in aspiration and a power of 80%) is to be reached.75,76 There has, however, been a large prospective study of 65,712 patients comparing aspiration associated with trachéal intubation versus LMAs. There were seven cases of aspiration with the trachéal tube against three cases where the LMA had been used (cLMA and LMA Unique).77 Sharma et al tested the efficacy and safety of the PLMA as a ventilatory device for a variety of commonly performed elective laparoscopic surgeries in 1,000 patients and concluded that in experienced hands and following a strict protocol of insertion, the PLMA is an efficient and safe tool for airway management. Twenty-five (2.5%) patients showed gastric regurgitation, suctioned through the esophageal channel of the PLMA, but no case of pulmonary aspiration was detected.78

A Cochrane database comparing EADs versus trachéal intubation for airway management during general anesthesia in obese patients (BMI>35 kg/m²) concluded that there is inadequate information to draw conclusion about safety of these devices and commented only on one design of EAD (PLMA) in these patients. During routine and laparoscopic surgery, PLMAs may take a few seconds longer to insert: a failure rate of 3–5% and higher leak fraction. PLMAs provide significant improvement in oxygenation during and after surgery, and reduced postoperative coughing, suggesting better recovery of patients.79

The 4th National Audit Project of the Royal College of Anesthetists and the Difficult Airway Society (NAP4) examined issues related to the EADs and found that the commonest complication associated with anesthesia was airway complication and EADs use-related aspiration was a contributor to this. NPA4 also revealed that 80% of EADs used for airway management in Britain were first-generation devices (eg, cLMA and LMAs). The complications were more in the obese population where a first-generation device had been employed. The report recommended use of the second-generation devices to improve the outcome, since these devices have been shown to be safer than the first-generation devices.80 This safety rests on the understanding by the concerned anesthesiologists of the device design, patient factors as well as the surgical scenario.

Cook and Kelly have devised a safety scoring system to help decide the choice of EAD which suits the needs of a particular patient.76 Greenland and Irwin have elaborated on seven axioms for selecting difficult airway devices.81

Pharyngeal rupture, pneumomediastinum, mediastinitis or arytenoid dislocation and nerve injuries are other very rare but serious complications of EADs.82–84

EADs play a major role in difficult airway scenario and have a place in the latest American Society of Anesthesiologists and Obstetric Anesthetists’ Association and DAS guidelines for difficult airway management.85,86 Knowing the physical characteristics of the airway device helps in generating hypotheses and better understanding of the working of an equipment before using it in clinical practice.51

Limitations of the study
We were unable to get all the relevant data. The maximum number of studies is available for cLMA which is not much in use, and it is recommended that it should be withdrawn as it has served its purpose. The EADs are continuously evolving, and since new devices are introduced each year (about two new EADs every year), there is insufficient literature available for every device, so evidence-based conclusion cannot be drawn from the studies. It is also becoming increasingly difficult to conduct research because of safety concerns. Reporting bias cannot also be ruled out.

Conclusion
The last three decades have witnessed several new airway devices and techniques with radical changes in airway practice and management. The introduction of EADs has resulted in a paradigm shift in airway management from a face mask versus trachéal tube to face mask versus EAD versus trachéal tube model. New EADs such as LMA-Protector, Baska mask and miscellaneous multipurpose device (eg, Totaltrack VLM) have been new additions to the EADs family, but their impact on patient safety and outcome still awaits scientific evaluation. Aspiration remains the single most-dreaded complication of these devices. Pharyngolaryngeal morbidity
and nerve injuries may be avoided to a large extent by paying careful attention to insertion and careful monitoring of the cuff pressure of the EADs. Providing adequate oxygenation and ventilation remains the gold standard of any patient safety goal and airway management technique. The anesthesia community is still waiting for the ideal EAD: simple design, excellent seal, high success rate of insertion on the first attempt even in the hands of novices, reliable drainage mechanism, zero aspiration, use in a full-stomach patient with a difficult airway in the emergent situation, low incidence of postoperative discomfort, affordable, with a low risk–benefit ratio, and in a nutshell with all the desirable features of an endotracheal tube and none of its drawbacks.

**Disclosure**

The authors report no conflicts of interest in this work.

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