Comparison of cellular effects of starch-coated SPIONs and poly(lactic-co-glycolic acid) matrix nanoparticles on human monocytes

Dominik Gonnissen¹
Ying Qu¹,²
Klaus Langer³
Cengiz Öztürk⁴
Yuliang Zhao²
Chunying Chen²
Guiscard Seebohm⁵
Martina Düfer⁶
Harald Fuchs¹
Hans-Joachim Galla⁷
Kristina Riehemann¹

¹Center for Nanotechnology, Institute of Physics, University of Münster, Münster, Germany; ²National Center for Nanoscience and Technology, Chinese Academy of Sciences, Beijing, People’s Republic of China; ³Institute of Pharmaceutical Technology and Biopharmacy, University of Münster, Münster, Germany; ⁴chemicell GmbH, Berlin; ⁵Department of Cardiovascular Medicine, Institute for Genetics of Heart Diseases, University Hospital Münster; ⁶Department of Pharmacology, Institute of Pharmaceutical and Medicinal Chemistry; ⁷Department of Cell Biology/Biophysics, Institute of Biochemistry, University of Münster, Münster, Germany

Abstract: Within the last years, progress has been made in the knowledge of the properties of medically used nanoparticles and their toxic effects, but still, little is known about their influence on cellular processes of immune cells. The aim of our comparative study was to present the influence of two different nanoparticle types on subcellular processes of primary monocytes and the leukemic monocyte cell line MM6. We used core-shell starch-coated superparamagnetic iron oxide nanoparticles (SPIONs) and matrix poly(lactic-co-glycolic acid) (PLGA) nanoparticles for our experiments. In addition to typical biocompatibility testing like the detection of necrosis or secretion of interleukins (ILs), we investigated the impact of these nanoparticles on the actin cytoskeleton and the two voltage-gated potassium channels Kv1.3 and Kv7.1. Induction of necrosis was not seen for PLGA nanoparticles and SPIONs in primary monocytes and MM6 cells. Likewise, no alteration in secretion of IL-1β and IL-10 was detected under the same experimental conditions. In contrast, IL-6 secretion was exclusively downregulated in primary monocytes after contact with both nanoparticles. Two-electrode voltage clamp experiments revealed that both nanoparticles reduce currents of the aforementioned potassium channels. The two nanoparticles differed significantly in their impact on the actin cytoskeleton, demonstrated via atomic force microscopy elasticity measurement and phalloidin staining. While SPIONs led to the disruption of the respective cytoskeleton, PLGA did not show any influence in both experimental setups. The difference in the effects on ion channels and the actin cytoskeleton suggests that nanoparticles affect these subcellular components via different pathways. Our data indicate that the alteration of the cytoskeleton and the effect on ion channels are new parameters that describe the influence of nanoparticles on cells. The results are highly relevant for medical application and further evaluation of nanomaterial biosafety.

Keywords: actin cytoskeleton, cell elasticity, AFM, ion channels, patch clamp, TEVC

Introduction

Nanoparticles are low-sized materials established in the medical field. Due to their high surface/volume ratio which is related to the small size, and the variety of surface modifications, nanoparticles are suitable for applications like medical imaging or drug delivery.¹,² With regard to material and architecture, there are different species of nanoparticles described. Two general classes of nanoparticles are the core–shell¹ and the matrix⁷ nanoparticles. Core–shell nanoparticles, which in our case are based on a magnetite core and a starch shell, are built up by two main components: the central part which is usually the active agent in the medical field and an encasing, for example, targeting or to improve bioavailability. The matrix nanoparticles on the other hand consist of a component where the active agent is entrapped.³ In our work, we used...
poly(lactic-co-glycolic acid) (PLGA) as a carrier material. These two systems were chosen because of their comparable hydrodynamic diameters, zeta potentials, and densities. Both types of nanoparticles are intensely used in diagnostics and therapy and have been reported to be highly biocompatible and nontoxic as well.\(^6\) Thus, they act as well-defined model systems for our studies on the influence of nanomaterials on cellular reactions.

As soon as nanomaterials come into contact with biological fluids, they are covered with a protein layer,\(^2\) the so-called protein corona, a process which is dependent on nanoparticle characteristics\(^8\)–\(^10\) and serves as a mechanism protecting the body against unwanted side reactions caused by nanoparticles. Nonetheless, nanoparticle–cell interaction may result in different molecular reactions, like change in gene expression and signaling events or alteration of calcium homeostasis,\(^11\) even if the nanoparticles are covered by a protein layer. To prevent unwanted or life-threatening side reactions like allergic shock, it is crucial to know about the effects of nanoparticles on key cells of the immune system. Macrophages and their precursors, the monocytes, play a pivotal role in the identification of foreign materials. As soon as the nanomaterials enter the blood stream, they mediate the following reaction of the immune system by activation of phagocytosis and secretion of chemokines. Accordingly, for the successful medical application of nanoparticles, these cells play a central role. Monocytes of the peripheral blood are in our focus because these primary cells present reactions of healthy cells, while MM6 cells reflect the reactivity related to cancerous conditions. In the case of ion channels, we tested whether the results obtained from transfected oocytes can be transferred to a leukemic cell line, as an overexpression of Kv channels was reported for cancer cells.\(^12\) MM6 cells provided the advantage to study potential effects of nanoparticles on potassium channels, while their phenotype is still closely related to mature monocytes.\(^13\)

During the first contact between cells and nanoparticles, the latter might interfere with ion channels located at the cell surface. Ion channels are pivotal in processes like maintaining osmolarity and membrane potential,\(^14\) shaping action potentials,\(^15\) or regulating other physiological signals.\(^16\) They can also play a relevant part in the development of cancer\(^12\) and are needed for differentiation and activation of cells.\(^17\) For developmental processes in immune cells, especially potassium channels have a significant impact.\(^18\) The connection between ion channels and the cytoskeleton is tight and quite important to keep the ion channels working. With proteins like cortactin, the connections between ion channels and cytoskeleton are established. This is reported to help maintain the function and integrity of the channels.\(^19\) The actin cytoskeleton is also directly and indirectly bound to lipid rafts which are known for the enrichment of Kv channels.\(^20\) A change in cytoskeleton may cause alteration of the ion channels or vice versa. This effect is known especially in highly mobile, secreting cells like macrophages.\(^21\) Alteration of the actin cytoskeleton is also described to be a symptom for cancerous transformation of cells\(^22\) and is related to cell properties like protrusion and adhesion during cellular migration.\(^23\) In general, the cytoskeleton is responsible for the location of proteins embedded within the membrane.\(^24\) The elasticity of cells is a significant marker of the change in the status of the cytoskeleton network.\(^25\)

In this work, we investigated the influence of starch-coated superparamagnetic iron oxide nanoparticles (SPIONs) and PLGA nanoparticles as examples for core–shell and matrix nanoparticles, respectively, on primary monocytes and the leukemic monocyte cell line MM6. In particular, we compared the formation of protein corona, nanoparticle uptake, induction of interleukin (IL) secretion, modulation of cell elasticity, and influence on distribution of the actin cytoskeleton in primary monocytes as well as the MM6 cell line. To investigate cytokine secretion, we analyzed IL-1β as an inflammatory marker,\(^26\) IL-10 as an anti-inflammatory marker,\(^27\) and IL-6 as a marker of cancer and autoimmune diseases.\(^28\)–\(^31\)

Modulation of ion channel activation was studied in a proof-of-concept experiment on two voltage-gated potassium channels in a Xenopus laevis oocyte expression system using the two-electrode voltage clamp (TEVC) setup. The obtained results demonstrate that clinically relevant nanoparticles can modify basic structural assemblies like cytoskeleton proteins and functional properties like ion channel function or IL secretion.

**Materials and methods**

**Nanoparticles**

Commercially available SPIONs (nano-screenMAG/R-D 200 nm), used for magnetic resonance imaging diagnostic procedure and covalent coupling of bioligands, were obtained from chemicell GmbH (Berlin, Germany). SPIONs coated with a red fluorescent (excitation/emission maximum of 578/613 nm) dye and an outer layer of starch with a hydrodynamic diameter of 200 nm were chosen for experiments.

The PLGA nanoparticles were prepared according to the method described by Grünebaum et al.\(^32\) PLGA nanoparticles with 5,10,15,20-Tetrakis-(3-hydroxyphenyl)-porphyrin
Iron(II, III)oxide – PLGA – starch – carboxyl groups – Negative ~200

Plga hydroxyl groups 240 – ~

Red fluorescent dye mTHPP – β

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(mTHPP) as entrapped active agent and a hydrodynamic diameter of 240 nm were used for this work. The active agent mTHPP has an excitation/emission maximum of 420/650 nm. The properties of the nanoparticles are summarized in Table 1.

### Isolation and cultivation of human monocytes of the peripheral blood

Primary monocytes were isolated from healthy donor buffy coats obtained from the German Red Cross (Muenster, Germany). A modified isolation method used Ficoll gradient centrifugation followed by a magnetic-activated cell sorting using anti-CD14-coated beads (Miltenyi Biotec, Bergisch Gladbach, Germany) was applied. Enrichment of CD14-positive CD80-negative cells was routinely verified by monoclonal antibodies against CD14 and CD80, whereas the CD14-positive fraction had to be >90% and the CD80-positive fraction <10%. The cells were cultured in McCoy’s 5A modified medium with 15% fetal bovine serum (FBS), 1X nonessential amino acids, 20 mM L-glutamine, and 1 mM sodium pyruvate (Biochrom GmbH, Berlin, Germany) at 37°C and 5% CO2.

### Cell culture of the MM6 cell line

The MM6 cell line was acquired from the “Deutsche Sammlung für Mikroorganismen und Zellkulturen” (Braunschweig, Germany). Cell culture medium was Rosewell Park Memorial Institute 1640 supplemented with 10% FBS, 2 mM L-glutamine, 1X nonessential amino acids, 1 mM sodium pyruvate (Biochrom), and 10 µg/mL human insulin (Sigma-Aldrich Co., St Louis, MO, USA). The cells were subcultured every 5 days and seeded at a concentration of 3x10^5 cells/mL in 12 mL medium in a 75 cm² cell culture flask (Greiner Bio-One, Kremsmünster, Austria) and kept in a humidified incubator at 37°C and 5% CO2.

### Cytotoxicity assay

The cytotoxicity was determined by using the CytoTox-Glo assay kit from Promega Corporation (Fitchburg, WI, USA) according to Niles et al. and manufacturer’s protocol. Shortly, 2.5x10^5 cells were seeded in black µClear 96-well plates (Greiner Bio-One), and incubated overnight prior to adding controls and samples to the cells. The exposure time to the substances was 4 hours. Digitonin (50 µg/mL) was used as cytotoxicity standard (positive control), cell culture medium as negative control, and water to exclude toxic effects of the solvent. The measured data were blank-corrected and normalized to the negative control.

### Cytokine detection via ELISA

Leukocytes were incubated at a concentration of 5x10^5 cells with 500 ng/mL nanoparticles, 1 µg/mL lipopolysaccharide (LPS), and water or cell culture media for 12 hours. The suspension was filled into vials and centrifuged for 10 minutes at 13,000 rpm. The supernatant was used as samples for the enzyme-linked immunosorbent assay. Assays were done with commercially available enzyme-linked immunosorbent assay detection kit for IL-1β, IL-6, and IL-10 (Thermo Fisher Scientific, Waltham, MA, USA) according to the manufacturer’s protocols. For the experiments, 96-well Nunc Maxisorp plates (Thermo Fisher Scientific) were used. The detection of the colorimetric reaction was performed within 30 minutes in a plate photometer at 450 nm.

### Protein corona formation

Nanoparticles were incubated at a concentration of 500 ng/mL in 4 mL cell culture medium for 4 hours. All experiments were performed with cell culture medium containing the same charge of FBS to get comparable results. The nanoparticles were spun down for 15 minutes at 13,000 rpm, washed twice with phosphate-buffered saline (PBS), and resuspended in 20 µL water. A 20 µL aliquot sodium dodecyl sulfate (SDS) polyacrylamide gel electrophoresis sample buffer (0.5 M Tris, 5.2 mM SDS, 15% [v/v] glycerol, 65 mM dithiothreitol, 14 µM bromophenol blue; pH 6.8) was added, and the samples were boiled for 5 minutes at 95°C. SDS polyacrylamide gel electrophoresis was performed on a 10% resolution gel stacked with a 3% [w/v] stacking gel. The measured data were blank-corrected and normalized to the negative control.

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### Table 1: Properties of the PLGA nanoparticles and the SPIONs

<table>
<thead>
<tr>
<th>Property</th>
<th>PLGA nanoparticles</th>
<th>SPIONs</th>
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<tbody>
<tr>
<td>Core</td>
<td>–</td>
<td>Iron(II, III)oxide</td>
</tr>
<tr>
<td>Shell</td>
<td>–</td>
<td>Starch</td>
</tr>
<tr>
<td>Matrix</td>
<td>PLGA</td>
<td>–</td>
</tr>
<tr>
<td>Active agent</td>
<td>mTHPP</td>
<td>–</td>
</tr>
<tr>
<td>Label</td>
<td>–</td>
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<td>Functional groups</td>
<td>Carboxyl groups</td>
<td>Hydroxyl groups</td>
</tr>
<tr>
<td>Zeta potential (mV)</td>
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<td>Negative</td>
</tr>
<tr>
<td>Hydrodynamic diameter (nm)</td>
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<td>200</td>
</tr>
<tr>
<td>Density (g/cm³)</td>
<td>-1.18</td>
<td>-1.25</td>
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**Abbreviations:** PLGA, poly(lactic-co-glycolic acid); SPIONs, starch-coated superparamagnetic iron oxides nanoparticles; mTHPP, 5,10,15,20-Tetrakis-(3-hydroxyphenyl)-porphyrin.
(25 mM Tris, 192 mM glycine, 20% [v/v] methanol; pH 8.3) for 1 hour with 56 mA per 7x8 cm gel. Membranes were stained with Coomassie G-250 solution (40% [v/v] ethanol, 10% [v/v] acetic acid, 0.1% [w/v] Coomassie G-250) for the protein pattern. The membrane was visualized via specific immuno-staining. For the specific immuno-staining, the membrane was blocked overnight with 5% casein in Tris-buffered saline (TBS) (50 mM Tris, 150 mM NaCl; pH 7.6), washed with TBS, and incubated for 2 hours with a mixture of 200 ng/mL rabbit anti-bovine serum albumin (BSA) antibody (Abcam, Cambridge, UK) and 50 ng/mL goat anti-rabbit immunoglobulin G (IgG) antibody, coupled to alkaline phosphatase (Abcam) in 1% casein in TBS with 0.1% (v/v) Tween-20. Subsequently, the membranes were washed with TBS with Tween-20 prior to developing the protein pattern via nitro-blue tetrazolium chloride/5-bromo-4-chloro-3-indolylphosphate p-toluidine salt staining technique (Sigma-Aldrich Co.). A stained protein ladder for the range 10–180 kDa (Abcam) was used to determine the molecular weight of the proteins.

**Cellular uptake of nanoparticles**

Cells were seeded at a density of 2.5×10⁵ cells/mL in 1 mL medium on coated glass coverslips and grown overnight. For the primary monocytes, 250 µg/mL fibronectin was used, and for the MM6 cell line, 100 µg/mL collagen was used. The cells were incubated with 500 ng/mL nanoparticles for 4 hours. Subsequently, the coverslips were washed twice with PBS, fixed with 4% paraformaldehyde in PBS for 15 minutes at 37°C, and mounted with a non-hardening APO VC ×100 oil-immersion objective (Nikon Corporation, Tokyo, Japan) with a Plan Apo VC ×100 oil-immersion objective (Nikon Corporation) and Type F immersion liquid (Leica Microsystems).

**Western blot of potassium channels**

Samples were prepared from the same charge of cells to get comparable results by collecting 1×10⁷ cells in a tube and centrifuged for 10 minutes at 13,000 rpm. The pellet was washed twice with PBS and incubated with lysis buffer (150 mM NaCl, 50 mM Tris, 1% [v/v] Triton X-100; pH 8) with protease inhibitor cocktail (Sigma-Aldrich Co.) 1:10 (v/v) for 30 minutes on ice. The aqueous solution was sonicated with UP400S (Hielscher, Berlin, Germany) for 10 seconds with 0.5 cycles and 20% amplitude. To determine the protein content, a bicinchoninic acid assay (Thermo Fisher Scientific) was performed. Samples were brought to a concentration of 1 µg/mL with sample buffer (described earlier). Western blot was performed according to the aforementioned method.

**Fluorescence staining of potassium channels**

Cells from the same charge as used for the Western blot were seeded as described for the uptake experiments. After 15-minute fixation with 4% paraformaldehyde in PBS and 5-minute permeabilization with 0.1% Triton X-100 in PBS, free binding sites were blocked with 1% BSA in PBS for 30 minutes. Samples were incubated with rabbit anti-Kv1.3 (3 µg/mL), rabbit anti-Kv7.1 (4 µg/mL), or unspecific rabbit IgG (4 µg/mL) antibody, washed, and then incubated with goat anti-rabbit IgG coupled to Alexa Fluor 594 (10 µg/mL) prior to mounting them with Fluoromount. The used antibodies were anti-Kv1.3 (APC-002) (Alomone Labs, Jerusalem, Israel), anti-Kv7.1 (AB5932) (Merck Millipore), unspecific rabbit IgG (ab27478) (Abcam), and goat anti-rabbit IgG (A11012) (Thermo Fisher Scientific). Imaging was performed with the fluorescence microscope mentioned earlier.

**Fluorescence imaging of F-actin**

For F-actin staining, cells were seeded as described for the uptake experiments. Cells were fixed in 4% paraformaldehyde in PBS for 15 minutes at 37°C and permeabilized for 10 minutes with 0.1% Triton X-100. F-actin was stained with Alexa Fluor 555-conjugated phalloidin (Thermo Fisher Scientific). Cells were also stained with DAPI for the identification of nuclei. All steps during the staining process were conducted at room temperature in a dark room. After staining, cells were sandwiched between the glass coverslip and a glass slide and mounted with Fluormount (Sigma-Aldrich Co.). Images were obtained with an Eclipse TE2000-U fluorescent microscope (Nikon Corporation, Tokyo, Japan) with a Plan Apo VC ×100 oil-immersion objective (Nikon Corporation) and Type F immersion liquid (Leica Microsystems).

**TEVC technique**

For these experiments, X. laevis oocytes (EcoCyte Bioscience, Austin, TX, USA) were cultured in Barth’s media (EcoCyte Bioscience) and measured in ND96 solution (96 mM NaCl, 4 mM KCl, 1.8 mM MgCl₂, 1 mM CaCl₂, 5 mM 4-(2-hydroxyethyl)-1-piperazineethanesulfonic acid [HEPES]; pH 7.6). The oocytes were microinjected with 1 ng Kv1.3.
cRNA or 6 ng Kv7.1 plus 1.2 ng KCNE1 cRNA. The cRNA was kindly provided by the working group of Professor Seebohm from the Department of Cardiovascular Medicine of the Institute for Genetics of Heart Diseases of the University Hospital Muenster. The oocytes were incubated for 72 hours at 19°C for the protein expression of the injected RNA. Both nanoparticles were coated with a 250 µg/mL BSA solution in a 1:5 ratio for at least 24 hours on a rocking shaker. Prior to measuring, oocytes expressing the ion channels and uninjected control oocytes were incubated for 4 hours in ND96 media with 500 ng/mL nanoparticles, protected from light, and kept at 19°C. The measurement was done with a TEC-10 CX Amplifier (NPI Electronics, Tamm, Germany) and a Digidata 2000 Acquisition System (Molecular Devices LLC, Sunnyvale, CA, USA) connected to a computer with the ClampEx 9.2 software (Molecular Devices LLC). For measuring the Kv1.3 channel beginning from a holding potential of −80 mV, 2,000 ms square pulses from −70 to 60 mV with increments of 10 mV were used, and for the Kv7.1 channel, 3,000 ms square pulses from −100 to 60 mV with increments of 20 mV were used.

**Patch clamp technique**

Whole-cell currents were recorded with the patch clamp technique. An EPC 10 USB Amplifier (HEKA, Lambrecht, Germany) connected to a computer with the PatchMaster software (HEKA) was used for data acquisition. Patch electrodes with a resistance of 8–11 MΩ were produced in a DMZ Universal Puller (Zeitz, Martinsried, Germany) from borosilicate glass capillaries (Harvard Apparatus, Holliston, MA, USA) with an outer diameter of 1.5 mm and an inner diameter of 0.86 mm. The extracellular solution was composed of 120 mM NaCl, 5.4 mM KCl, 2 mM CaCl₂, 1 mM MgCl₂, 10 mM HEPES, and 25 mM D-glucose with a pH of 7.4 adjusted with NaOH. The capillaries were filled with 120 mM KCl, 1 mM CaCl₂, 2 mM MgCl₂, 10 mM HEPES, 11 mM ethylene glycol tetraacetic acid, and 20 mM D-glucose adjusted to pH 7.3 with KOH. After establishing a high-resistance seal, the leak current was set to zero. To measure voltage-gated potassium currents, from the −60 mV holding potential, a 0 mV square pulse of 200 ms was generated.

**Cell elasticity measurements by AFM**

Force spectroscopy experiments on the cells were done with an atomic force microscope MFP-3D Stand Alone (Asylum Research, Santa Barbara, CA, USA). PNPL-SiO colloidal cantilevers (sQube) with 6 µm spherical tips, 200 µm length, and a force constant of 0.08 N/m (NanoAndMore GmbH, Darmstadt, Germany) were used in the experiments and changed after each experiment. Spring constant values were measured via the thermal tuning method. One-day-old cells were seeded on 250 µg/mL fibronectin-coated glass coverslips at a density of 5x10⁴ cells/mL in 1 mL medium and attached overnight. The samples were incubated with 5 ng/mL tumor necrosis factor-α (TNF-α), 2 µg/mL LPS, 1 µM latrunculin A, 500 ng/mL SPIONs, or 500 ng/mL PLGA nanoparticles for 4 hours at 37°C and 5% CO₂. Cells treated with TNF-α or LPS were taken as positive control, and cells treated with latrunculin A as negative control. Latrunculin A will increase the elasticity by preventing polymerization of G-actin to F-actin,³⁶,³⁷ and LPS as well as TNF-α will decrease the cell elasticity by triggering inflammatory processes in the cells.³⁸ Cell viability was checked before starting measurement by adding Trypan blue (Biochrom) to the cell culture media for 3 minutes. Only living cells were used for measurements. All experiments were performed in Rosewell Park Memorial Institute 1640 culture medium (without phenol red) with 20 mM HEPES at room temperature. Force curves were acquired at the cytoplasmic area avoiding the nucleus. Measurements were done within 1 hour. To avoid any influence from cell–cell interactions, only cells without any contact to neighboring cells were measured. At least 150 independent measurements were performed for each designed experimental condition. In each treatment, at least 20 healthy cells were chosen to measure three times at three different positions. The indentation depth was controlled to be within 300 nm in order to better simulate cytoskeleton deformations which occur beneath the cell membrane. The force-versus-indentation curves from each measurement were analyzed using a Hertz model¹⁹ to obtain the Young’s modulus of each cell. Measurements on the cells with complete actin skeleton and destroyed actin skeleton were displayed comparatively. Young’s moduli were calculated as average values ± standard error of the mean.

**Statistical analysis**

Data are shown as mean value ± standard error of the mean. Statistical analysis was done with Prism 6 (GraphPad Software, Inc., La Jolla, CA, USA) using one-way analysis of variance followed by a Kruskal–Wallis test.

**Results**

**Toxicity of nanoparticles**

In order to use doses of investigated nanoparticles close to in vivo conditions, we chose a particle concentration of 500 ng/mL. Neither the PLGA nanoparticles nor the SPIONs showed any toxic effects on primary monocytes (Figure 1A) and the MM6 cell line (Figure 1B) at this concentration.
Protein corona

Nanoparticles incubated in cell culture medium with FBS as an additive formed a protein corona. BSA, an abundant protein in FBS, was visualized using Western blot followed by Coomassie G-250 or specific immuno-staining (Figure 2). The three parts of each subfigure originated from one gel. Just the relevant lanes are presented. The unspecific Coomassie G-250 staining (Figure 2A and B) revealed more proteins in the samples than the specific antibody staining (Figure 2C and D) indicating that the nanoparticles absorb other proteins in addition to BSA. BSA was detected for both types of nanoparticles in the FBS-containing cell culture medium (Figure 2C), whereas in the serum-free media (Figure 2D), no bands were detected. BSA, FBS, and cell culture media with FBS and without FBS served as markers. These results showed that BSA is part of the protein corona developed around the nanoparticles used for these experiments.

Uptake of nanoparticles

Experiments for uptake of nanoparticles were performed with primary monocytes and the MM6 cell line. Uptake of nanoparticles was visualized by confocal laser scanning microscopy. During imaging, one layer within the cell was visualized. The images for primary monocytes (Figure 3A and B) and MM6 cells (Figure 3C and D), respectively, show an enrichment of PLGA particles in the endosomal cell compartment. In case of SPIONs, neither for the primary monocytes (Figure 3E and F) nor for the MM6 cell line (Figure 3G and H), any red fluorescence indicative of nanoparticle accumulation was observed. Thus, there is obviously no indication for an enrichment or directed uptake of the nanoparticles.

Secretion of cytokines

For the MM6 cell line and the primary monocytes, PLGA nanoparticles and SPIONs did not affect the secretion of IL-1β or IL-10 compared to a negative control without nanoparticles (data not shown). For IL-6, secretion was reduced in primary monocytes but not in MM6 cells (Figure 4). IL-6 secretion of primary monocytes was reduced to approximately 20% compared to the negative control.

Identification of voltage-gated potassium channels in different cell systems

In these experiments, the effects of nanoparticles on two selected voltage-gated potassium channels, Kv1.3 and Kv7.1, were examined. To validate the existence of these channels, Western blots and immunocytochemistry were done with primary monocytes and the MM6 cell line. The Western blots (Figure 5) show selected bands of one gel. These indicate that in the leukemic monocyte cell line MM6, for the Kv1.3 ion channel, no protein of 63 kDa but a fragment of 35 kDa was observed (Figure 5A), which could be the Kvβ2 subunit of 39 kDa, whereas for the Kv7.1 ion channel, only unspecific staining and no protein of 75 kDa was identified (Figure 5B). For the primary monocytes (M0), no expression of Kv1.3 (Figure 5A) or Kv7.1 (Figure 5B) was detected.

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Figure 1 Induction of necrosis.

Notes: Toxicity experiments with (A) 2.5×10⁵ primary monocytes and (B) the MM6 cell line after 4-hour incubation with 500 ng/mL nanoparticles. For the assays, the commercial test system CytoTox-Glo (G9291) from Promega was used. Digitonin (60 µg/mL) was used for the positive control, cell culture media for the negative control, and water for the solvent control. Shown is the mean value ± SEM (n=3). Significance intervals are indicated by asterisks with the following intervals: P<0.0001 (**). Abbreviations: SEM, standard error of the mean; PLGA, poly(lactic-co-glycolic acid); SPIONs, superparamagnetic iron oxide nanoparticles.
To verify the results of the Western blot experiments, immunocytochemistry was performed. In the fluorescent pictures (Figure 6) for the primary cells no signal of the Kv1.3 channel could be detected (Figure 6A) while a brighter fluorescence for the MM6 cell line can be observed (Figure 6B). For the Kv7.1 channel (Figure 6C and D) and the unspecific IgG staining (Figure 6E and F) no significant difference in fluorescence can be observed.

**Ion channel function**

To investigate the effects of the nanoparticles on these voltage-gated potassium channels, two different experimental setups were used. First, we performed patch clamp experiments with primary monocytes and the MM6 cell line. In the “Supplementary materials” section, an example measurement (Figure S1) is presented, together with an inhibition experiment with tetraethylammonium (Figure S2) to ensure that the measured ion currents result from the activation of voltage-gated potassium channels.

In primary monocytes, no channel activity was measured (data not shown). This is in agreement with the negative results for protein expression. In the MM6 cell line that has been shown to express at least a subunit of Kv1.3, currents were detected (Figure 7). These currents were not reduced after preincubation with PLGA nanoparticles or SPIONs. To investigate the impact of nanoparticles on one channel at a time, we used the TEVC setup with oocytes overexpressing Kv1.3 or 7.1. The TEVC experiments (Figure 8) indicated that the currents of both voltage-gated potassium channels were downregulated after incubation with nanoparticles. This is visible by comparing the curve of the control cells (Figure 8, black curve), which were injected with ion channel inhibitors, to the curves of the nanoparticles-treated cells (Figure 8, colored curves).
cRNA but not incubated with any substances, with the curve of ion channel expressing cells preincubated with PLGA nanoparticles (Figure 8, blue curve) or SPIONs (Figure 8, red curve). The current was clearly lowered by both nanoparticles but to a different extent. Whereas the SPIONs had a high impact on the ion currents, the PLGA nanoparticles showed a smaller effect. This observation was made for both voltage-gated potassium channels. The untransfected oocytes (Figure 8, green curve) showed no currents during the measurement. In this study, only the curve for the uninjected oocytes without nanoparticle incubation is shown as an example; the uninjected oocytes with nanoparticle incubation also

Figure 3 Uptake of nanoparticles.
Notes: (A, C, E, and G) Bright field and (B, D, F, and H) fluorescent microscopic pictures of (A, B, E, and F) primary monocytes and (C, D, G, and H) the MM6 cell line made with confocal laser scanning microscopy. The cells were incubated for 4 hours with (A–D) 500 ng/mL PLGA nanoparticles or (E–H) SPIONs. The bright spots (B and D) indicate an agglomeration of particles. Nuclei are stained in blue with DAPI; red color indicates fluorescence of mTHPP-loaded nanoparticles or SPIONs.
Abbreviations: PLGA, poly(lactic-co-glycolic acid); SPIONs, starch-coated superparamagnetic iron oxide nanoparticles; DAPI, 4′,6-diamidino-2-phenylindole; mTHPP, 5,10,15,20-Tetrakis-(3-hydroxyphenyl)-porphyrin.

Figure 4 Interleukin-6 secretion of 5x10^5 primary monocytes after overnight incubation with 500 ng/mL nanoparticles.
Notes: The values are normalized with respect to the negative control; 1 μg/mL LPS was used as positive control. The mean value ± SEM (n=3) is presented. Significance intervals are indicated by asterisks with the following intervals: *P<0.01 (**).
Abbreviations: LPS, lipopolysaccharide; SEM, standard error of the mean; PLGA, poly(lactic-co-glycolic acid); SPIONs, starch-coated superparamagnetic iron oxide nanoparticles.

Figure 5 Demonstration of voltage-gated potassium channels in primary cells and the MM6 cells.
Notes: Western blot of voltage-gated potassium channels (A) Kv1.3 and (B) Kv7.1 in the leukemic monocyte cell line MM6 and primary monocytes (M0). Primary antibodies used were rabbit anti-Kv1.3 (3 μg/mL; APC-002; Alomone Labs) or rabbit anti-Kv7.1 (4 μg/mL; A58932; Millipore, Billerica, MA, USA) and a goat anti-rabbit IgG coupled to alkaline phosphatase (50 ng/mL; Abcam). Bound antibody was stained by the NBT/BCIP technique (Sigma-Aldrich Co.).
Abbreviations: IgG, immunoglobulin G; NBT/BCIP, nitro-blue tetrazolium chloride/5-bromo-4-chloro-3-indolylphosphate p-toluidine salt.
showed no currents. Example measurements are presented in the “Supplementary materials” section (Figure S3).

Elasticity measurements
The terms elasticity and stiffness are reciprocally connected; that is, if the cell stiffness is increased, the elasticity decreases and vice versa. By comparing primary monocytes or the MM6 cell line incubated with nanoparticles to cells incubated with reagents with known effects on cell elasticity, it was possible to analyze the influence of the nanoparticles on cell stiffness. Experimental data are shown in Figure 9A for primary monocytes and Figure 9B for the MM6 cell line. An example measurement can be found in the “Supplementary materials” section (Figure S4). As expected, incubation of the cells with latrunculin A increased the elasticity of the cells, and induction of inflammatory processes via LPS or TNF-α decreased it. In comparison to these substances with known effects, the PLGA nanoparticles did not show an alteration of the elasticity, whereas the SPIONs increased it in an amount comparable to the latrunculin A.

Figure 6 Validation of voltage-gated potassium channels.
Notes: Fluorescent staining of the voltage-gated potassium channel proteins (A and B) Kv1.3 and (C and D) Kv7.1 in (A, C, and E) primary monocytes or (B, D, and F) the MM6 cell line with an (E and F) unspecific IgG control. Cells were stained with either rabbit anti-Kv1.3 (3 µg/mL; APC-002; Alomone Labs) or rabbit anti-Kv7.1 (4 µg/mL; AB5932; Millipore) or unspecific rabbit IgG (4 µg/mL; ab27478; Abcam) and goat anti-rabbit IgG (10 µg/mL; A11012; Thermo Fisher Scientific) coupled to Alexa Fluor 594.
Abbreviation: IgG, immunoglobulin G.
control. To visualize and confirm the changes of the actin cytoskeleton, measured by AFM, staining experiments with phalloidin were done.

Visualization of changes in the actin cytoskeleton
The experiments with the AFM indicated that both the primary monocytes and the MM6 cell line responded in the same way to the nanoparticles. The SPIONs had an effect on the cells, whereas the PLGA nanoparticles did not. Consequently, we visualized the actin cytoskeleton by phalloidin staining. The actin cytoskeleton was examined after exposure to the different nanoparticles and compared to a control without any treatment. In Figure 10, the results for primary monocytes and MM6 cells are shown. By comparing the F-actin cytoskeleton of untreated controls and cells incubated with PLGA nanoparticles, no differences were observed which correlates with the results of the AFM experiments. Between the control and cells incubated with SPIIONs, significant changes in the cytoskeleton were found. For both cell systems, the control cells and the PLGA-treated samples showed a widespread filamentous network, whereas the SPIIONs-incubated samples lacked these filamentous spread of actin fibers. These results support our hypothesis that altered elasticity is linked to impairment of the actin cytoskeleton.

Discussion
With this work, we present a comparative study of the effects of two different nontoxic nanoparticles, their influence on ion channels, and alteration of cell elasticity caused by interactions with the actin cytoskeleton in primary monocytes and the MM6 cell line.

Prior to our investigation on cellular effects, we demonstrated the presence of a protein corona on the surface of our two nanoparticle systems. It is well known that nanoparticles form protein coronas after contact with biological fluids, a process that depends on nanoparticle characteristics.8–10 The effect of the commonly used nanoparticles on cells
Comparison of nanoparticle effects on human monocytes

Figure 9: Atomic force spectroscopy measurements of the cell stiffness after incubation with different reagents or nanoparticles.

Notes: The measured cells were (A) primary monocytes and (B) the MM6 cell line. Controls were without treatment (n=139/151) or incubated with 1 µM latrunculin A (n=169/133) to increase the elasticity and 2 µg/mL lipopolysaccharide (n=225/217) to decrease the elasticity. The investigated nanoparticles were 500 ng/mL SPIIONs (n=171/215) or Plga nanoparticles (n=171/215). Values are shown as mean ± SEM. Significance intervals are indicated by asterisks with the following intervals: $P<0.01$ (**), $P<0.0001$ (****).

Abbreviations: Plga, poly(lactic-co-glycolic acid); SPIIONs, starch-coated superparamagnetic iron oxide nanoparticles; SEM, standard error of the mean.

Figure 10: Fluorescence staining of the F-actin cytoskeleton of MM6 cells and primary monocytes with and without incubation with nanoparticles.

Notes: F-actin staining of the (A, C, and E) MM6 cell line or (B, D, and F) primary monocytes. Cells were stained with Alexa Fluor 555-coupled phalloidin (red) to visualize the actin cytoskeleton and DAPI (blue) for the nucleus. Cells not incubated with nanoparticles are shown in (A) and (B), whereas cells incubated with 500 ng/mL PLGA nanoparticles are shown in (C) and (D) and those incubated with the same amount of SPIIONs for 4 hours are shown in (E) and (F).

Abbreviations: DAPI, 4',6-diamidino-2-phenylindole; PLGA, poly(lactic-co-glycolic acid); SPIIONs, starch-coated superparamagnetic iron oxide nanoparticles.
presented in this study is due to such a protein layer. PLGA nanoparticles and SPIONs are reported to be highly biocompatible and nontoxic. These findings are confirmed by our results that the nanoparticles in our experiments had no effects on primary monocytes or on the leukemic monocyte cell line MM6 in terms of necrosis. To describe their immunogenicity, we investigated the secretion of different ILs in both cell systems. As a result, secretion of neither IL-1β nor IL-10 was affected by the selected nanoparticles. This was supported by an experimental setup where the induction of IL-1β secretion was exclusively achieved by embedding LPS into the outer particle structure. Generally, PLGA is known to be a non-immunogenic material. Interestingly, IL-6 secretion was reduced in primary monocytes by both types of nanoparticles but not in MM6 cells, which fortifies again that biocompatibility and immunology studies with cancerous cells are not necessarily close to the response of a patient with a healthy immune system. This effect is described for macrophages after TiO₂/protein corona contact, indicating a central role of this cytokine during interaction of specific nanoparticles with cells. The downregulation of IL-6 by the nanoparticles used for these experiments is a clear indication of their biocompatibility.

Voltage-gated potassium channels play a crucial role in the differentiation processes of monocytes and other cells of the immune system. Surprisingly, we could not confirm the existence of Kv1.3 channels in primary monocytes with any of the performed experiments, though they are described in the literature for their descendants, the macrophages. Nonetheless, it is also known that the expression levels of these tightly regulated proteins can differ depending on origin and differentiation status of the cells. On the other hand, the positive results for the leukemic monocyte cell line MM6 have proven that our experimental setups were working properly. While we were not able to show any regulatory effects of the nanoparticles in the patch clamp system, we could show that they have an impact on two voltage-gated potassium channels in a heterologous expression system. Unfortunately, the leukemic monocyte cell line MM6 is not yet characterized in terms of the expression of ion channels, though it is known that potassium channels, and especially the Kv1.3 and Kv1.5 channel complex, play a crucial role in the process of differentiation from monocytes to macrophages. Most likely, the effect of the nanoparticles depends on the type of Kv channel so that the cell might start to compensate the lack of function of one channel by increasing expression or upregulation of another channel. Another model would be that a certain amount of channels needs to be expressed before the regulatory effects of the nanoparticles can be measured. Whereas the patch clamp system is better used to investigate effects on whole-cell systems, the TEVC system is better for investigating the effects on single channels. That nanoparticles can have a regulatory impact on ion channels was shown for SiO₂ nanoparticles on TRP4 channels in a neuronal cell line. Ion channels are tightly connected to the cytoskeleton, especially to the actin fibers, either through bindings between specialized proteins and the fibers or through interaction between fibers and lipid rafts, in which the channels can be located. These connections allow the channels to maintain their function in the fluidic environment of the membrane. Next to these tasks, the investigation of cell elasticity is important as a marker of the healthiness of cells, since many processes are regulated by mechanical changes. For macrophages, the integrity of the cytoskeleton is of special interest, since the phagocytic activity is linked to the intact cytoskeleton. Alterations of cell elasticity can be associated with a variety of diseases, especially tumorous transformation of tissue or cells. Reorganization of the actin cytoskeleton is important for the migration of leukocytes into the tissue. Therefore, the increase of elasticity, as shown by the cells incubated with SPIONs, may have physiological impact such as reduced transmigration of monocytes through endothelial cells. Though the influence of nanoparticles on the F-actin network was already described, no information to align these effects to structure, size, material, or other properties of the nanoparticles exists. It is well known that the actin cytoskeleton is the part of the cytoskeleton which is mostly responsible for cell stiffness, while the microtubule network only has a small effect on this parameter.

As the actin cytoskeleton is important for the functionality and regulation of ion channels via the connection by proteins like cortactin, disruption can modulate the activity of different channels. Such an effect was, however, not observed in our patch clamp experiments with the MM6 cells. One explanation may be that expression and regulation of ion channels is so complex that the cell alters its expression pattern to maintain a working condition even with a disrupted actin cytoskeleton. Nevertheless, the disruptive effects of the SPIONs on the actin cytoskeleton alongside with the downregulating effect proven by the TEVC experiments could be connected. The PLGA nanoparticles on the other hand showed no alteration of the actin cytoskeleton but a downregulating effect on the ion channels. This could be the outcome of two different mechanisms of impact on the cell with the SPIONs altering the actin cytoskeleton via
disruption of the actin network where the PLGA nanoparticles may work via disturbance of the membrane or the ion channels directly. How far this effect is caused by cellular uptake remains unclear. Though a high uptake of the PLGA nanoparticles was shown for two bide duct cancer cell lines, the little uptake of the SPIONs used in this work was shown for a comparable starch-coated magnetite nanoparticle.

The effect of these findings is not obvious and has to be in focus of further investigations. In our systematic comparative study, we demonstrated that nanoparticles exposed to living system, for example, for medical purposes, alter the cellular processes at different levels.

**Conclusion**

In summary, our work demonstrates the alteration of selected potassium ion channels and the actin cytoskeleton by specific nanomaterials. The results show that in biological systems, nanomaterials may have more subtle effects than interference with cell death or inflammation. If these modifications are supporting or inhibiting, specific medical applications has to be investigated for each particle. We conclude that there are still more aspects to consider to open the opportunities of medical application of nanoparticles but also with respect to nanoparticle safety.

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**Disclosure**

The authors report no conflicts of interest in this work.

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Supplementary materials

Figure S1 Patch clamp measurement of an MM6 cell.
Notes: Shown is the current against the time. Each measuring cycle takes 13 seconds to complete and generates 17 points.

Figure S2 Patch clamp measurement of an MM6 cell with addition of TEA in different concentrations to block voltage-gated potassium channels.
Notes: Shown is the current against the time. Each measuring cycle takes 13 seconds to complete and generates 17 points.
Abbreviation: TEA, tetraethylammonium.

Figure S3 Example currents of Kv channels with their corresponding pulse protocol.
Notes: Two-electrode voltage clamp example currents of (A) Kv1.3 and (C) Kv7.1 with the (B and D) corresponding pulse protocols.
Figure S4 Example curve for the atomic force microscopy measurements of a primary monocyte.

Note: The curve approaching the cell is indicated in red, and the one retracting from the cell in blue.