

# An in silico analysis of oxygen uptake of a mild COPD patient during rest and exercise using a portable oxygen concentrator

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**Abstract:** Oxygen treatment based on intermittent-flow devices with pulse delivery modes available from portable oxygen concentrators (POCs) depends on the characteristics of the delivered pulse such as volume, pulse width (the time of the pulse to be delivered), and pulse delay (the time for the pulse to be initiated from the start of inhalation) as well as a patient's breathing characteristics, disease state, and respiratory morphology. This article presents a physiological-based analysis of the performance, in terms of blood oxygenation, of a commercial POC at different settings using an in silico model of a COPD patient at rest and during exercise. The analysis encompasses experimental measurements of pulse volume, width, and time delay of the POC at three different settings and two breathing rates related to rest and exercise. These experimental data of device performance are inputs to a physiological-based model of oxygen uptake that takes into account the real dynamic nature of gas exchange to illustrate how device- and patient-specific factors can affect patient oxygenation. This type of physiological analysis that considers the true effectiveness of oxygen transfer to the blood, as opposed to delivery to the nose (or mouth), can be instructive in applying therapies and designing new devices.

**Keywords:** efficiency, respiratory physiology, respiratory disease, pulsed delivery

## Introduction

A recent review<sup>1</sup> of home-based long-term oxygen treatment makes several pertinent points regarding the proper selection and use of intermittent-flow devices such as pulse delivery modes available from portable oxygen concentrators (POCs). Intermittent-flow devices, introduced in the 1980s, addressed the need to improve the efficiency of oxygen delivery by providing flows only when the patient was inhaling, thereby eliminating the supply, and therefore the waste, of gas during exhalation. POCs depend on these efficiency gains to reduce size and extend operating times to achieve ambulatory systems that are patient friendly, thereby improving adherence. However, these devices have also created confusion related to oxygen delivery, prescriptions, device selection, understanding patient versus product capabilities, and reimbursement for long-term oxygen treatment. In particular, health care professionals and patients alike do not have the theoretical or practical tools to compare intermittent-flow devices, commonly characterized by the pulse bolus sized in milliliters of oxygen, with the better understood continuous-flow administration of supplemental oxygen, prescribed in liters per minute. In fact, the equivalence of intermittent-flow delivery to continuous-flow delivery is dependent on a number of variables, yet when one or more of these variables change, the equivalence

of an intermittent-flow delivery method to continuous-flow delivery cannot be achieved. Furthermore, the timing of the oxygen pulse is also a key design feature and setting, as the pulses can be administered at a fixed frequency independent of the patient's breathing or triggered, usually based on a negative pressure threshold that is fixed by the manufacturer or set by the user. Thus, McCoy<sup>1</sup> shows that the shape of the oxygen flow curve, as the dose is delivered, may also impact patient comfort and adherence, and we would add, also potentially, the level of oxygenation.

Recognizing that oxygenation using a POC with intermittent-flow setting depends on the characteristics of the delivered pulse such as volume, pulse width (the time of the pulse to be delivered), and pulse delay (the time for the pulse to be initiated from the start of inhalation) as well as on a patient's breathing characteristics, disease state, and respiratory morphology, McCoy<sup>1</sup> shows that there is a lack of research on new home oxygen therapies to ensure that the patient is provided adequate oxygenation at all activity levels.

In appreciation of this need, we have performed a physiological-based analysis of the performance, in terms of blood oxygenation, of a popular commercial POC at different settings using an *in silico* model of a COPD patient at rest and during exercise. This analysis encompasses experimental measurements of pulse volume, width, and time delay of the POC at three different settings and two breathing rates related to rest and exercise. These experimental data of device performance are inputs to a physiological-based model of oxygen uptake<sup>2</sup> that takes into account the real dynamic nature of gas exchange to illustrate how device- and patient-specific factors can affect patient oxygenation. The COPD model used represents a relatively mild case of the disease that is normoxic at rest. The specific aim is to illustrate and quantify the complex interaction of the medical device and patient functional parameters during oxygen uptake to give guidance on making POC therapy more effective.

## Methods

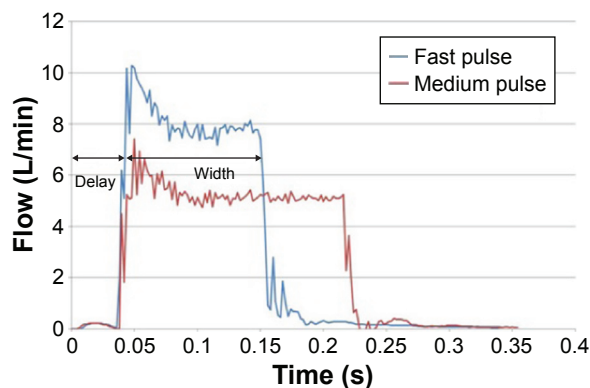
### POC pulse characterization experiments

Measurements of pulse volume (mL of oxygen), pulse width (ms), and pulse delay (ms) of a POC shown in Figure 1 (Eclipse 5; Caire Inc., Ball Ground, GA, USA) are performed using a test system designed specifically to evaluate intermittent-flow devices (Series 1130, O<sub>2</sub> Conserver Testing System; Hans Rudolph Inc., Shawnee, KS, USA). The POC was connected to the test system through the standard 2.1 m of cannula tubing. The test system trigger was set to 2 cm H<sub>2</sub>O. The POC had nine (1–9) possible



**Figure 1** Eclipse 5 portable oxygen concentrator connected to the test system.

pulse bolus volume settings and three rise time options – fast, medium, and slow for delivery of the specified 90% oxygen. The low settings nominally represent the equivalent continuous flow: for setting 1, the pulse volume is specified as 16 mL provided during an inspiration of 1 second. Thus, nominally the pulsed delivery relative to the equivalent continuous delivery is  $0.016 \text{ L} \times 60 \text{ s/min} = 0.96 \approx 1 \text{ L/min}$ . Figure 2 shows examples of flow versus time pulses for



**Figure 2** Output flow curves for setting 1, fast and medium pulse, obtained from the test system for the Eclipse 5 POC.

**Notes:** The nominal delay and width times are indicated by the arrows; measured times are defined as the time from the beginning of the negative pressure signal until the flow begins and the time measured from the beginning of the pulse to the time that the flow falls  $<0.2 \text{ L/min}$ , respectively.

**Abbreviation:** POC, portable oxygen concentrator.

setting 1, indicating two different rise times with the pulse width and time delay. The pulse volume can be found by integrating the flow versus time curve. Tests were performed at settings 1, 5, and 9 (specified pulse volumes of 16 mL, 80 mL, and 192 mL, respectively) at the fast and medium rise times and two different breathing conditions (described later). Data were collected for ten successive pulses in each condition/setting.

## Gas uptake model

An oxygen uptake model developed by Kang et al<sup>2</sup> solves a system of partial differential equations for 1D convection along the airway and diffusion and permeation across the peripheral alveolar surface to the blood within a realistic acinus morphology. The two key equations that are the basis of the model are as follows:

$$\frac{\partial C(x,t)}{\partial t} = D \frac{\partial^2 C}{\partial x^2} - \frac{\partial}{\partial x}(C \cdot U) - \Omega \frac{S}{V}(C - C_v/\alpha) \quad (1)$$

$$\frac{dC_{RBC}(t)}{dt} + \frac{1}{\delta_{Hb} + \alpha' \delta_{Ext}} C_{RBC}(t) = \frac{\alpha' \alpha C}{\delta_{Hb} + \alpha' \delta_{Ext}} \quad (2)$$

Here,  $C$  is the concentration of oxygen at a position  $x$  in the acinus airway at time  $t$ ,  $D$  is the diffusion coefficient of oxygen in air,  $U$  is gas convection velocity in the airway,  $\Omega$  is the oxygen integrative permeability of all the elements between the gas phase and venous blood,  $\alpha$  is the Ostwald partition ratio,  $C_v$  is the oxygen concentration in the venous blood,  $C_{RBC}$  is the oxygen concentration in the red blood cells,  $\delta_{Hb}$  is a characteristic time for oxygen trapping by hemoglobin molecules,  $\alpha'$  is the partition ratio of oxygen concentration between plasma and red blood cells, and  $\delta_{Ext}$  is the characteristic time for oxygen diffusion from the alveolar space to a red blood cell surface. Also of fundamental importance to this work is a calculation of the arrival time of inhaled gas to the acinus that is a function of the trachea–bronchial dead volume and the inhalation flow rate. The system of equations is solved via time integration to provide the instantaneous oxygen flux from the gas phase to the blood and all of the other functional parameters over time. Of interest here is the total oxygen flux integrated over a single breath.

The model was validated by comparing in silico results to functional data for healthy lungs at rest and during exercise found in the literature.<sup>3</sup> The general approach of the model allows many applications that have included a mapping of oxygen uptake over a wide range of ventilation

and perfusion combinations and to illustrate the influence of altitude. Furthermore, the model (using the same equations as for oxygen) was able to predict the transport and trapping of carbon monoxide and nitric oxide used in single-breath lung function testing consistent with experiments. While the complete mathematical description of the gas uptake model is beyond the scope of this article, the key point to recognize is its ability to illustrate the importance of time, that is, ventilation and perfusion dynamics, in the process of oxygen capture. Thus, the model can include the effect of the arrival time of the enriched oxygen pulse from the POC to the acinus region in the oxygen capture process. The form of the pulse itself is simplified to be a square wave in the model and added to the inhalation flow. The details of this model are beyond the scope of this article but can be found in the cited reference.<sup>2</sup>

## COPD model

Input parameters to the in silico oxygen uptake model for normal, healthy individuals at rest are taken from Kang et al<sup>2</sup> (Table 1). These parameters have been adjusted to complete a normal, healthy model for moderate exercise, where moderate exercise is taken to be walking upstairs, 4.7 metabolic equivalents to rest.<sup>4</sup> The COPD parameters at rest and exercise were taken from the study reported by Agusti et al<sup>5</sup> (Table 1). In that study, eight patients (all male, 62±1 years) were confirmed to have COPD using standard clinical criteria and with previous functional confirmation of nonreversible chronic airflow limitation (FEV<sub>1</sub> 1.15±0.12 L; 36%±3% predicted). None of them had clinical evidence of overt right heart failure. Type B COPD was present in five patients, whereas the three remaining patients had predominantly type

**Table 1** Characteristics of the in silico healthy and the COPD disease models

	Normal rest	Normal exercise	COPD rest	COPD exercise
Tidal volume (mL)	625	1,666	495	834
Frequency (bpm)	12	30	19	29
Minute ventilation (L/min)	7.5	50	9.4	24.2
Total lung capacity (mL)	6,200	6,200	7,690	7,690
Functional residual capacity (mL)	2,480	2,480	3,845	3,845
Anatomical dead space (mL)	170	170	170	170
Inhalation time (s)	2	1	1.05	1.03
Oxygen partial pressure in the mixed venous blood (Pv in mmHg)	40	25	38	30
Cardiac output (L/min)	5	10	5.4	10.6

**Note:** Data from Kang et al<sup>2</sup> and Agusti et al.<sup>5</sup>

A COPD. Type A patients are characterized by the presence of anatomical emphysema or an increased total lung capacity (TLC), while type B patients are characterized by evidence of chronic inflammation or smaller TLC.<sup>6</sup> Minute ventilation and respiratory rate were recorded minute by minute using a calibrated Wright spirometer. Low dead space, low resistance, and nonbreathing valves were used to collect the expired gas through a heated-mixing box, at rest (no 1,500; Hans Rudolph Inc.) or during exercise (E Jaeger, Wurzburg, Germany) to measure oxygen uptake. Tidal volume is calculated by dividing the minute ventilation by the breathing frequency. Functional residual capacity (FRC) is 40% of TLC for normal healthy subjects and 50% for COPD subjects.<sup>7</sup> TLC for COPD is based on data from Wagner et al.<sup>8</sup> The inhalation time is obtained from the breathing frequency by assuming an inhalation/exhalation ratio of 0.5 at rest and 1 during exercise. Based on these morphological, ventilatory, and cardiac output parameters, the model, that is, the inputs to the oxygen uptake model, a COPD model has been defined.

## Results

### Pulse characterization

The results of the pulse characterization experiments, performed at rest (19 bpm) and during exercise (29 bpm) with the breathing frequencies for the COPD model, are given in Table 2. At rest, there is no degradation at settings 1 and 5 of the pulse volume as per the manufacturer's nominal specification<sup>9</sup> of 16 mL and 80 mL, respectively. However, for setting 9, the specified pulse volume is 192 mL, which was not achieved for the breathing patterns tested. For exercise,

**Table 2** Average values of pulse volume, pulse width, and pulse delay of ten measurements

Condition/ setting	Pulse volume (mL)	Pulse width (ms)	Pulse delay (ms)
Rest (19 bpm)			
1 (medium)	16.2 (0.2)	226.5 (1.9)	38.2 (4.4)
1 (fast)	16.3 (0.3)	189.4 (2.7)	35.0 (1.9)
5 (medium)	79.4 (0.8)	678.6 (5.0)	36.3 (1.8)
5 (fast)	79.5 (0.5)	541.7 (9.9)	35.2 (1.9)
9 (medium)	157.2 (1.0)	876.6 (4.6)	35.1 (2.2)
9 (fast)	156.4 (0.7)	742.8 (12.7)	35.3 (1.8)
Exercise (29 bpm)			
1 (medium)	16.3 (0.2)	227.0 (3.1)	36.2 (1.5)
1 (fast)	16.3 (0.2)	187.6 (2.6)	36.1 (3.7)
5 (medium)	79.4 (0.8)	678.6 (5.0)	36.3 (1.8)
5 (fast)	80.1 (0.4)	533.6 (3.0)	34.8 (1.6)
9 (medium)	104.9 (0.7)	627.6 (2.4)	35.4 (2.0)
9 (fast)	104.0 (0.7)	542.0 (7.7)	35.0 (1.6)

**Notes:** Standard deviations are in parentheses. The pulse volumes specified by the manufacturer are 16 mL, 80 mL, and 192 mL for settings 1, 5, and 9, respectively.

settings 1 and 5 again meet the specifications, while for setting 9, the pulse volume is only 54% of that specified. In terms of rise time options, there were no differences in pulse volume between medium and fast rise time under all of the conditions tested. For all the tests, the 90% specified oxygen concentration was met.

### Oxygenation

The oxygenation results obtained using the in silico oxygen uptake model are given in Table 3. The first column of Condition/setting defines the set of simulation input parameters taken from Tables 1 and 2 that were used to obtain the uptake results. Column 2 provides the delivered dose volume of 90% oxygen from the POC. This is not applicable for the two baseline cases (normal for a typical adult male and a representative COPD patient) where there is no delivered dose. For continuous oxygen treatment, the delivered dose volume from the POC for 1 L/min, 5 L/min, or 9 L/min is simply 1,000 mL/min, 5,000 mL/min, or 9,000 mL/min. Pulsed delivery per minute is calculated from the pulse volume delivered by the POC per breath given in Table 1 multiplied by the breathing frequency given in Table 2. Columns 3 and 4 are oxygen uptake (mL/min) and the arterial partial pressure (mmHg), respectively, which are outputs from the model. The uptake here is the time average because the instantaneous rate is variable and only occurs during inhalation. Derivative results are presented in columns 5 and 6. The uptake over a single breath (mL) is obtained by multiplying column 3 by the breathing frequency. Another output of the model is the percentage of saturation as calculated using the oxygen disassociation curve<sup>6</sup> with the input of the calculated arterial pressure. Columns 7 and 8 are measures of the effectiveness and efficiency of the oxygen treatment, respectively. The percentage of the normal uptake gives an indication of the relative severity of the COPD model and the extent that the therapy can return the COPD patient to *normal*. The efficiency (the increased uptake divided by the delivered dose) is a measure of the effectiveness of a therapy to provide longer time for ambulatory activity and is shown in Figure 3. In more precise terms, it is a measure of how much of the supplementary oxygen is actually used (uptake to blood) as opposed to the delivery to the nose (or mouth).

### Discussion

This study follows the fundamental understanding that exercise is critical to reduce patient's morbidity<sup>10-15</sup> and that portable oxygen may allow patients the potential to increase their exercise capacity. However, clinical studies that tested



**Table 3** Oxygenation results

Condition/ setting	Dose delivered (mL/min)	Oxygen uptake (mL/min)	Arterial partial pressure (mmHg)	Oxygen uptake per breath (mL)	Oxygen saturation (%)	Normal uptake (%)	Efficiency of therapy (%)
Rest							
Normal	NA	210.6	101.4	17.6	97.6	100	NA
COPD	NA	255.3	101.6	13.4	97.6	76.1	NA
1 continuous	1,000	266.8	126.4	14.0	98.5	79.5	1.15
5 continuous	5,000	276.5	189.4	14.6	99.3	82.7	0.42
9 continuous	9,000	278.6	232.5	14.7	99.5	83.5	0.26
1 (medium)	309	268.6	132.9	14.1	98.6	80.1	4.30
1 (fast)	310	269.7	137.2	14.2	98.7	80.7	4.65
5 (medium)	1,510	276.7	192.6	14.6	99.3	82.8	1.42
5 (fast)	1,510	276.4	187.8	14.6	99.3	82.7	1.40
9 (medium)	2,990	278.4	226.0	14.7	99.5	83.3	0.77
9 (fast)	2,970	278.9	240.3	14.7	99.6	83.4	0.79
Exercise							
Normal	NA	993.8	104.4	33.1	97.7	100	NA
COPD	NA	721.8	72.2	24.9	94.0	75.2	NA
1 continuous	1,000	765.3	85.4	26.4	96.1	79.7	4.35
5 continuous	5,000	817.4	126.1	28.2	98.6	85.1	1.91
9 continuous	9,000	830.6	158.0	28.6	99.2	86.5	1.21
1 (medium)	470	780.5	92.4	26.9	96.9	81.3	12.5
1 (fast)	470	782.9	93.8	27.0	97.0	81.6	13.0
5 (medium)	2,300	816.2	124.1	28.1	98.6	85.0	4.10
5 (fast)	2,330	821.1	132.8	28.3	98.8	85.5	4.26
9 (medium)	3,040	825.2	141.7	28.5	99.0	86.0	3.40
9 (fast)	3,020	827.3	147.3	28.5	99.1	86.2	3.49

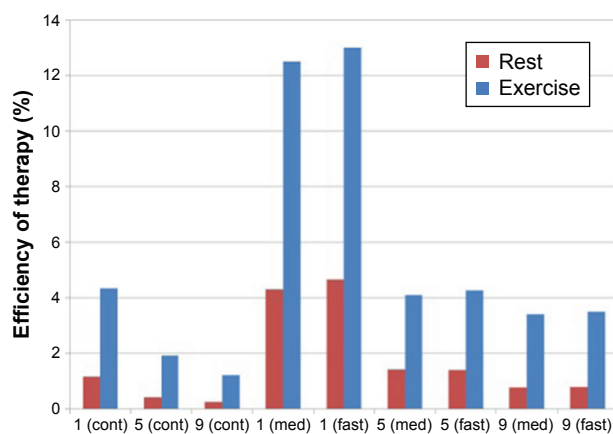
**Abbreviation:** NA, not applicable.

this concept have not been definitive. For example, Casaburi et al<sup>16</sup> followed 22 COPD patients for 6 months, with a control group and one using 3.6 lb. cylinders on cart to provide the portable oxygen. Activity monitoring revealed low activity levels prior to randomization and no significant increase over time in either group. In another study, POCs alone did not supply the same levels of oxygenation as the combination of

fixed and portable systems.<sup>17</sup> Furthermore, as described by McCoy<sup>1</sup> and others,<sup>18</sup> it is not clear how the wide variety of models and setting available on modern POCs affect patient oxygenation and adherence. Thus, we believed that a fundamental study of the interaction of patient physiology with the output of a real POC could provide guidance for future developments in device design and patient management.

## Performance of the POC

The performance of the Eclipse 5 POC as provided in Table 1 indicates that only at setting 9, is there a decrease in the pulse volume compared to the equivalent continuous dose and the nominal pulse volume quoted in the device specifications.<sup>9</sup> However, it should be noted that the User's Manual clearly states that under certain conditions the output volumes can be reduced. For example, when the Eclipse 5 is connected to the DC supply in a vehicle a maximum of only 3.0 L/min of continuous flow is available. Furthermore, it is stated that Bolus (or pulse) volume decreases as the breath rate exceeds the published range (15–40 bpm based on the setting) and that the pulse dose setting is not necessarily equal to the continuous flow rate in L/min. Finally regarding the Eclipse 5 specifically, note that it can be classified as ambulatory (comparable to rolling carry-on luggage, 8.2 kg,



**Figure 3** The percentage efficiency of therapy under each condition/setting combination, where the efficiency is the percentage of oxygen provided by the device that is taken up by the blood.

**Abbreviations:** cont, continuous; med, medium.

45.5×29.0×18.0 cm<sup>3</sup>) but not portable in the sense of fitting into a shoulder bag or smaller.

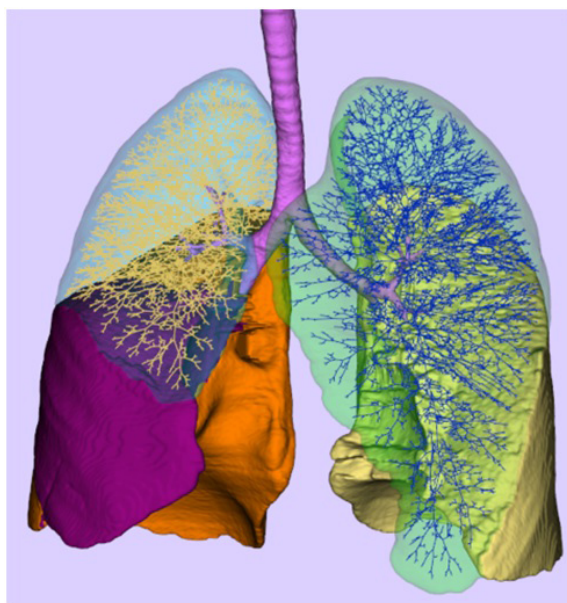
## Oxygen uptake

Oxygen uptake results are provided in Table 2 for a normal (healthy) case as well as for a single COPD model at rest and during light exercise, similar to walking up stairs. These comparative *in silico* results between normal and COPD, at rest and during exercise, are similar to previous *in vivo* results.<sup>19</sup> The oxygen uptake of a healthy adult gives a control comparison to the COPD model. At rest, arterial pressure and saturation are maintained, but at the cost of higher breathing frequency. The overall uptake is actually greater (more energy is needed for breathing) but the uptake per breath is reduced (76.1% of normal). During exercise, the diseased lung is no longer able to maintain oxygenation so the uptake in mL/min and per breath (75.2% of normal) are less than normal and partial desaturation occurs (94.0% versus 97.7% normal). However, this COPD model clearly represents a mild case of the disease. The application of supplementary oxygen during exercise for normoxic patients at rest has been suggested because oxygen reduces dyspnea by a reduction in minute ventilation during exercise and would have a beneficial effect on oxidative metabolism in peripheral muscle, leading to an increase in exercise capacity.<sup>20</sup> On the other hand, more recent clinical results recommend that supplemental oxygen during exercise for these patients is not indicated.<sup>21</sup> This limitation in our study model is discussed later.

Notably, at rest, the lack of oxygenation is not serious unless the patient's respiratory muscles would become fatigued. Thus, the addition of oxygen therapy results in very little increased uptake, although the percentage of normal uptake per breath is increased, indicating that the breathing frequency might be reduced in time. Continuous therapy is not efficient; the great majority of the oxygen provided is never used by the body. The pulsed therapies improve efficiency only slightly for the patient at rest. During exercise, the efficiency of the therapy increases, especially the pulsed delivery relative to the continuous. However, the therapy is still relatively inefficient suggesting that devices could be greatly optimized by simply providing a small and fast pulse without all of the optional settings. For example, the relatively efficient pulse setting of 1 medium could be improved by 28% (from 12.5% to 16%) if the 35 ms pulse delay were eliminated. This result implies that the timing of the pulse, in fact its arrival time at the acinus, affects the oxygen uptake and perhaps that a very small, low weight device that provided a single small volume of oxygen without a delay could be more effective for many patients.

These results show that while eliminating oxygen delivery during exhalation, relatively improves uptake efficiency, the continued overall inefficiency of the pulsed therapies is an indication of the importance of the particular respiratory physiology of the patient to obtain truly efficient uptake. The role of physiology can be explored in greater depth by considering *arrival time*. The high concentration pulse shown in Figure 2 is assumed to mix with the ambient inhalation gas stream such that the ventilation is unchanged but oxygen concentration is elevated for a fixed period during the breath. The arrival of the fresh gas stream, and then the high concentration pulse if there is a delay, to the acinus is a factor controlling the local oxygen uptake. The arrival time is dependent on the complete morphological structure upstream from the acinus and the ventilator parameters.

To illustrate the role of lung morphology in the oxygen uptake, the algorithm for the generation of an individualized 3D deterministic model of the conducting part of the human tracheo-bronchial tree developed by Montesantos et al can be considered.<sup>22</sup> Distinct initial conditions were obtained from the high-resolution computed tomography images of seven healthy volunteers from a previous study. The algorithm developed is fractal in nature and is implemented as a self-similar space subdivision procedure. The expansion process utilizes physiologically realistic relationships and thresholds to produce an anatomically consistent human airway tree that leads to thousands of separate paths unique to each acinus (Figure 4). For two subjects (H01,



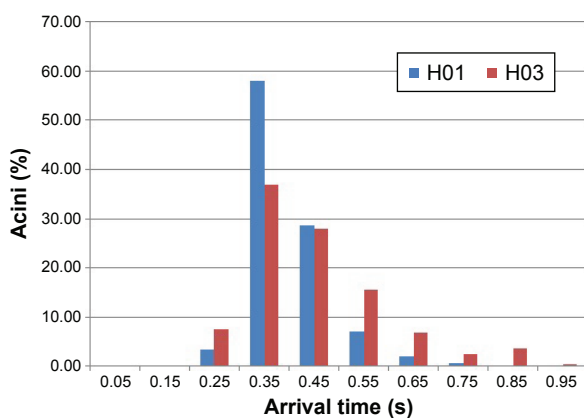
**Figure 4** Individualized, 3D deterministic model of the conducting part of the human tracheo-bronchial tree.

**Notes:** For clarity, the branching structure is only shown in the right and left upper lobes. A complete lung structure model will allow for accurate determination of the pulse arrival time at each individual acinus.

FRC = 2,360 mL, anatomical dead space = 123 mL, 15,952 acini; H03, FRC = 3,170 mL, anatomical dead space = 138 mL, 28,255 acini), the arrival time to each acinus was calculated for the same ventilation maneuver (tidal volume of 600 mL, inhalation time of 2 seconds, and for an inspiratory flow rate of 18 L/min). The frequency distribution of arrival times is plotted in Figure 5. It is important to note the range of arrival times present for each of these healthy individuals (in a sense intrasubject variability) and the intersubject variability between them, owing to the volume of the physiological dead space of the tracheo-bronchial region along different pathways supplying the acini. Note that with the single compartment model used herein, the single arrival times for the model cases of normal at rest, normal during exercise, COPD at rest, and COPD during exercise are 0.7 second, 0.21 second, 0.42 second, and 0.31 second, respectively. Also of importance is the heterogeneous nature of the gas uptake that can result from disease<sup>23</sup> deriving from obstruction, ventilation heterogeneity, and alveolar dead space.

## Limitations

There are many important limitations to this study. The single COPD model is not exhaustive but illustrative. Clearly, the variability of COPD will have significant effects on oxygen uptake, both in terms of severity and type.<sup>24–26</sup> The interaction of local ventilation and perfusion in the lung for COPD patients is very complex.<sup>8</sup> Perhaps, the key limitation in the COPD model is the single compartment with one arrival time for the whole lung. Indeed, it is interesting that with a single compartment lung model, it was not possible to obtain a severe COPD case using the measured ventilatory parameters from the literature that were used.<sup>5</sup> This suggests that there is an important role of heterogeneous or regional lung



**Figure 5** Arrival time at the acini in lung model for two healthy volunteers with tidal volume of 600 mL, inhalation time of 2 seconds, and for an inspiratory flow rate of 18 L/min.

**Notes:** Total number of acini were 15,952 for subject H01 and 28,255 for subject H03. The intersubject and intrasubject variabilities in arrival time to the acini will influence the efficiency oxygen uptake for a given pulse setting.

deterioration that limits oxygen uptake.<sup>27</sup> The next step in our research is to integrate the acinar oxygen uptake model with the lung morphology model to calculate the oxygen uptake for the thousands of acini individually. With this approach, regional lung morphology and localized disease can be investigated. In spite of the mild case considered, there was desaturation during exercise, and the efficiency of the uptake of the supplementary oxygen was relatively poor, although the need to consider more severe cases is clear.

The model can be considered to apply to the situation at the onset of therapy because no physiological changes with therapy are included in the model (eg, changes in cardiac output and breathing frequency that are expected benefits of the therapy).<sup>28</sup> In terms of assessing the device itself, the model does not account for the metabolic load of moving the POC. As noted, the Eclipse 5 can be called ambulatory. Thus, it is also evident that there is a need to consider many of the other smaller and more portable models where oxygen outputs would be less stable.

Palwai et al<sup>29</sup> have shown that clinical performance of devices can often be quite different than specified performance. There are a multitude of device and patient characteristics that could be considered. The testing of the device and the in silico model took no consideration for the efficiency of patient interface that can affect triggering as well as comfort and adherence. The fact that there was a direct connection of the POC to the testing device is different than loose fitting nasal cannulae that often occurs with patients is but one aspect of real patient–device interaction that may affect oxygenation.

## Conclusion

The goal of POCs is to allow patients to increase their activity. But as noted by clinical researchers, “POC recipients should be appropriately tested during all activities of daily living to ensure adequate oxygenation. The health care provider should provide information and help direct the preferences and lifestyle”.<sup>30</sup> This issue is understood by POC manufacturers, at least in the sense that they provide warnings in the user’s manual that setting must be determined for each patient at different levels of activity. We have demonstrated in this study the physiological complexity of oxygen uptake on the use of a POC, to underline the need for robust and repeated (as the patient’s condition could change over time) testing of a particular patient, at a particular level of exertion, with a particular device, at a particular setting. We have also shown that the poor efficiency of the POC in terms of oxygen uptake, at least for this mild case of COPD during exercise, implies much smaller and lighter devices that have much lower oxygen-producing capability could be more effective. Finally, this type of physiological analysis that considers the true effectiveness,

oxygen transfer to the blood as opposed to delivery to the nose (or mouth), can be instructive in applying therapies and designing new devices.

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## Disclosure

The authors report no conflicts of interest in this work.

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