Functional respiratory imaging to assess the interaction between systemic roflumilast and inhaled ICS/LABA/LAMA

Wim Vos¹
 Bitaj Hajian²
 Jan De Backer¹
 Cedric Van Holsbeke¹
 Samir Vinchurkar¹
 Rita Claes²
 Annemie Hufkens²
 Paul M Parizel³
 Lieven Bedert⁴
 Wilfried De Backer²

¹FLUIDDA nv, Groeningenlei, Kontich,

²Department of Respiratory Medicine,

³Department of Radiology, University Hospital Antwerp, Wilrijkstraat, Edegem, ⁴Department of Respiratory Medicine, ZNA Middelheim Hospital, Antwerp, Belgium

Background: Patients with COPD show a significant reduction of the lobar hyperinflation at the functional residual capacity level in the patients who improved >120 mL in forced expiratory volume in 1 second (FEV₁) after 6 months of treatment with roflumilast in addition to inhaled corticosteroids (ICSs)/long-acting beta-2 agonists (LABAs)/long-acting muscarinic antagonists (LAMAs).

Methods: Functional respiratory imaging was used to quantify lobar hyperinflation, blood vessel density, ventilation, aerosol deposition, and bronchodilation. To investigate the exact mode of action of roflumilast, correlations between lobar and global measures have been tested using a mixed-model approach with nested random factors and Pearson correlation, respectively.

Results: The reduction in lobar hyperinflation appears to be associated with a larger blood vessel density in the respective lobes ($t=-2.154$, $P=0.040$); lobes with a higher percentage of blood vessels reduce more in hyperinflation in the responder group. Subsequently, it can be observed that lobes that reduce in hyperinflation after treatment are better ventilated ($t=-5.368$, $P<0.001$). Functional respiratory imaging (FRI)-based aerosol deposition showed that enhanced ventilation leads to more peripheral particle deposition of ICS/LABA/LAMA in the better-ventilated areas ($t=2.407$, $P=0.024$). Finally, the study showed that areas receiving more particles have increased FRI-based bronchodilation ($t=2.564$, $P=0.017$), leading to an increase in FEV₁ ($R=0.348$, $P=0.029$).

Conclusion: The study demonstrated that orally administered roflumilast supports the reduction of regional hyperinflation in areas previously undertreated by inhalation medication. The local reduction in hyperinflation induces a redistribution of ventilation and aerosol deposition, leading to enhanced efficacy of the concomitant ICS/LABA/LAMA therapy. FRI appears to be a sensitive tool to describe the mode of action of novel compounds in chronic obstructive pulmonary disease. Future studies need to confirm the enhanced sensitivity and the potential of FRI parameters to act as surrogates for clinically relevant, but more difficult to measure, end points such as exacerbations.

Keywords: modeling, physiology, ventilation, aerosol distribution, FRI

Introduction

Today, the standard of care for patients suffering from chronic obstructive pulmonary disease (COPD) usually consists of long-acting beta-2 agonists (LABAs), long-acting muscarinic antagonists (LAMAs), inhaled corticosteroids (ICSs), or a combination of these. Recently, a phosphodiesterase type 4 (PDE4) inhibitor has been added as a therapeutic option, but some open questions remain. While LABAs and LAMAs relax the smooth muscle, the ICS component and PDE4 inhibitor are targeted at reducing the chronic inflammation associated with COPD. While ICS combined with LABA remains an established standard, several monoclonal antibodies, a new

Correspondence: Wim Vos
 FLUIDDA nv, Groeningenlei 132,
 2550 Kontich, Belgium
 Tel +32 3 450 87 20
 Fax +32 3 450 87 29
 Email wim.vos@fluidda.com

class of anti-inflammatory agents, are under development to treat respiratory diseases.^{1,2} Often, these products are administered systemically either orally or intravenously. During the clinical trials investigating the efficacy of these novel compounds, it is of paramount importance to understand the interaction between the systemic and the inhaled drugs as it is expected that the systemic drugs will only gradually replace the inhaled therapy, if at all. This implies that patients in clinical practice will be treated with both inhaled and systemic drugs, which is already often the case. So far, traditional end points, such as the forced expiratory volume in 1 second (FEV₁), and exacerbations have been typically used to assess the efficacy of novel drugs. However, for both of these end points, significant challenges arise when applied to the study of anti-inflammatory drugs. The FEV₁ alone lacks the sensitivity to describe regional effects of the novel therapy, which for an anti-inflammatory product is a crucial aspect of the mechanism of action. While exacerbations are clinically relevant end points, the lack of a specific definition introduces significant variability, especially in multicenter trials. In addition, to detect a beneficial effect on exacerbations, the investigators first have to establish a baseline exacerbation rate to assess potential improvements by the new drug. Both establishing the baseline and assessing the therapeutic effect require long and large clinical trials. Therefore, the development of novel drugs would benefit from additional end points that yield regional information and that could potentially act as surrogates for exacerbations in early Phase II trials. The latter would increase the probability of success of the, often-expensive, Phase III trials. Functional respiratory imaging (FRI) is a novel tool consisting of a combination of high-resolution computed tomography (HRCT) and computational fluid dynamics (CFD). The [Supplementary video](#) gives a short summary of how functional respiratory imaging works. The HRCT provides regional information on the lung, airway, and vascular structures, while the CFD subsequently provides the functional component in terms of airway resistance and aerosol deposition characteristics. The regional ventilation and deposition were previously validated on a lobar basis using single-photon emission computed tomography (SPECT),³ gamma scintigraphy,⁴ and hyperpolarized gases.⁵ Subsequently, the method has been used to investigate the mechanism of action of LABAs,⁶ LABAs/ICSs,⁷ short-acting beta-2 agonists/short-acting muscarinic antagonists,⁸ and antioxidant therapy.⁹

In a recent study,¹⁰ our group assessed the effect of the PDE4 inhibitor roflumilast as add-on therapy to ICSs/LABAs/LAMAs in Global initiative for chronic Obstructive

Lung Disease (GOLD) stages III and IV COPD patients. Roflumilast is a selective PDE4 inhibitor.¹¹ PDE4 regulates cyclic adenosine monophosphate (cAMP) in most of the cell types that are involved in inflammatory processes. Inhibition of PDE4 reduces the breakdown of cAMP, which in turn downregulates the inflammatory process. Earlier studies^{12,13} have confirmed the anti-inflammatory capabilities of the compound in terms of reducing the level of circulating tumor necrosis factor (TNF)- α , reducing the level of TNF- α in bronchoalveolar lavage (which acts as a proinflammatory mediator), and increasing the level of interleukin-10, an anti-inflammatory mediator. Two large-scale clinical trials^{14,15} have assessed the clinical efficacy of roflumilast in terms of improving or stabilizing FEV₁ and reducing exacerbations. The present study used a combination of classical end points and FRI demonstrated a superior effect of roflumilast relative to placebo. At the same time, the trial demonstrated that especially patients suffering from dynamic hyperinflation at baseline (eight out of 23 patients, 35%), determined using the 6-minute walk test, benefited from roflumilast, with a posttreatment improvement in FEV₁ >120 mL. In the discussion of that manuscript, we speculated that this was caused by the fact that the orally administered roflumilast reached areas in the lung previously undertreated by ICS. This study aims to extend the research by further investigating this hypothesis in the responder group. Specifically, the regional vasculature and the deposition patterns of the inhaled triple therapy are analyzed in more detail using FRI. The hypothesis for the mode of action of roflumilast as outlined in Figure 1 will be assessed. This study therefore focuses on assessing regional hyperinflation, internal airflow distribution, regional aerosol deposition patterns, and image-based bronchodilation.

Figure 1 Hypothesis for the mode of action of roflumilast.

Abbreviations: FEV₁, forced expiratory volume in 1 second; ICS, inhaled corticosteroid; LABA, long-acting beta-2 agonist; LAMA, long-acting muscarinic antagonist.

Materials and methods

The study design can be found in De Backer et al.¹⁰ and is summarized in the CONSolidated Standards Of Reporting Trials (CONSORT) diagram in Figure 2. Baseline measurement consisted of spirometry, body plethysmography, 6-minute walk test, patient reported outcome parameters, and FRI. All measurements were repeated after 6 months of treatment. Both baseline and 6-month measurements were performed after bronchodilation. The remainder of this article will mainly discuss the parameter FEV₁, which is measured using spirometry and a set of FRI-based parameters, which are extensively described in the following sections. FRI parameters are derived from HRCT scans taken at functional residual capacity (FRC) and total lung capacity (TLC) at baseline and after 6 months of treatment. Patient characteristics and demographics can be found in Table 1. The study was approved by the ethical committee of the University Hospital of Antwerp, and written informed consent was obtained from each participant. [ClinicalTrials.gov](https://clinicaltrials.gov/ct2/show/study/NCT01480661) Identifier: NCT01480661.

Computed tomography image acquisition

The level of inspiration during computed tomography (CT) was monitored with a commercially available spirometry system (Spirostik; Geratherm Respiratory GmbH, Kissingen,

Germany) that enables real-time monitoring of the breathing cycle. This ensured that the examinations were performed at the correct lung volume. The CT settings were as follows: tube voltage, 100 kV; tube current, 10–200 mAs; noise factor, 45; collimation, 0.625 mm; rotation time, 0.6 seconds; and pitch factor, 1.375.

FRI assessment of blood vessel density

Blood vessel density can be determined through segmentation and three-dimensional reconstruction of the blood vessels. The segmentation is based on a Hounsfield unit (HU) threshold of [−600; 600] and is performed on the TLC scan. The blood vessel density can be considered a surrogate for perfusion, as outlined in the study by De Backer et al.¹⁰ Because roflumilast is orally administered, the regional perfusion determines the regional delivery of the PDE4 inhibitor.

FRI assessment of regional hyperinflation

The FRI process includes segmentation of the lung volumes at FRC and TLC from the HRCT images by using an HU threshold of [−1,024; −400]. In addition, the fissures that separate the individual lung lobes are identified. By using the fissure lines as cutting planes, the individual lobe volumes can be determined and expressed as percentages of predicted values (Figure 3).

Figure 2 CONSORT diagram of the clinical trial.

Abbreviations: CONSORT, CONSolidated Standards Of Reporting Trials; qd, once daily.

Table 1 Patient characteristics and demographics after randomization

	Roflumilast			Placebo
	Total	Responders	Nonresponders	
Length (cm)	166.2±6.44	166.75±7.77	165.90±5.90	170.06±10.56
Pack-years smoking (years)	53.13±35.57	73.94±46.99	42.03±22.48	54.83±30.24
Age (years)	63.61±7.38	62.12±6.94	64.40±7.73	70±6.76
Weight (kg)	84.08±28.58	87.90±35.45	82.04±25.35	92.81±26.18
FVC (%pred)	79.76±21.08	82.24±23.62	78.44±20.35	79.97±13.43
FEV ₁ (%pred)	41.3±12.17	46.91±11.04	38.31±12.01	47.28±11.19
FEV ₁ /FVC (%)	42.5±12.62	47.64±12.33	39.77±12.29	46.61±10.41
RV (%pred)	171.32±35.31	168.21±24.48	172.97±40.64	146.36±28.26
TLC (%pred)	114.44±21.39	112.26±20.69	115.61±22.39	106.22±11.02
FRC (%pred)	147.22±33.72	144.88±26.69	148.47±37.76	130.94±25.07
Raw (kPas/L)	0.77±0.3	0.71±0.24	0.80±0.33	0.67±0.35
sRaw (kPas)	3.97±1.96	3.43±0.91	4.24±2.30	3±1.26
LCI (units)	8.87±1.33	8.63±1.21	9.02±1.44	9.16±1.94
Nitrogen washout time (min)	5.48±2.51	5.22±2.66	5.64±2.56	3.46±1.16
6MWT (m)	357.53±90.02	393.83±84.48	340.77±90.66	403.88±148.84

Note: Data presented as mean ± standard deviation.

Abbreviations: 6MWT, 6-minute walk test; %pred, percentage of predicted; FEV₁, forced expiratory volume in 1 second; FRC, functional residual capacity; FVC, forced vital capacity; LCI, lung clearance index; Raw, airways resistance; RV, residual volume; sRaw, specific airways resistance; TLC, total lung capacity.

FRI assessment of internal airflow distribution

The patient's specific internal airflow distribution can be determined by subtracting the FRC lobe volume from the TLC lobe volume.

FRI assessment of regional aerosol deposition

Regional aerosol deposition is determined by simulating the flow in the patient-specific geometries using patient-specific boundary conditions by means of CFD. CFD essentially solves the Navier–Stokes equations numerically on a computational grid. While solving the flow equations particles

are released simultaneously in the flow, and the force mass balance of the individual particles is determined through additional discrete phase computations. More information on the method can be found in the study by De Backer et al.¹⁶ The patient-specific HRCT-based airway geometries constitute the basis for the aerosol deposition assessments. The three-dimensionally reconstructed airway geometries were transformed into computational grids using TGrid 14.0 (Ansys Inc., Canonsburg, PA, USA). High-quality, unstructured grids consisting of tetrahedral elements were created. Several grids were tested to assess the mesh sensitivity, and a typical grid of 3×10⁶ cells was selected for the analyses to ensure good resolution at all high-gradient regions.

Figure 3 Regional hyperinflation at the FRC level for a COPD patient from the roflumilast trial and a healthy volunteer (both female, both 170 cm in height).

Abbreviations: %p, percentage of predicted; COPD, chronic obstructive pulmonary disease; FRC, functional residual capacity.

Flow simulations were performed using Fluent 14.0 (Ansys Inc.). The air in the lower airway was considered to be homogeneous, incompressible, and Newtonian. The flow simulations use so much patient-specific information (eg, airway geometry, internal airflow distribution, inhalation profile) that they provide an accurate idea of the regional resistance and deposition patterns. These profiles were determined in the clinical center by means of a pneumotachometer. The pressure-based solver was used with a node-based Green-Gauss gradient treatment. A second-order pressure discretization scheme was selected for the pressure calculation, and a second-order upwind scheme was used for the momentum equations. The pressure-velocity coupling was solved using the Semi-Implicit Method for Pressure-Linked Equations (SIMPLE) algorithm. Turbulence was evaluated through large eddy simulations with a turbulent kinetic subgrid model to assess the possible influence of turbulence on the flow pattern and aerosol deposition. Aerosol transport was modeled by an implicit Runge-Kutta Lagrangian discrete particle model, with a one-way coupling of the forces from the flow to the particle and taking into account the Saffman lift forces. Particles were considered deposited the moment they hit the airway wall.

The aerosol characteristics used for the simulations include the mass mean aerodynamic diameter (MMAD), the geometric standard deviation (GSD), and the fine particle fraction (FPF) of the respective ICS/LABA and LAMA products. Table 2 provides an overview of the aerosol parameters. Inhalation regimens in the trial were as follows:

Table 2 Aerosol characteristics of LAMA and LABA/ICS used in the FRI deposition calculations

Inhaler	MMAD	GSD	FPF (%)
Spiriva (LAMA) ²⁶	3.9	1.8	23.21
Onbrez (LABA) ²⁶	3.2	2	39.41
Oxis (LABA) ²⁷	2.13	1.72	69.06
Pulmicort (ICS) ²⁸	1.9	2.1	48
Seretide Diskus (ICS/LABA) ²⁹			
ICS	3.54	1.49	21.6
LABA	3.57	1.46	23.34
Symbicort (ICS/LABA) ²⁹			
ICS	3.30	1.57	38.71
LABA	3.09	1.56	43.73
Inuvair MDI (ICS/LABA) ³⁰			
ICS	1.3	1.97	38.07
LABA	1.3	2.00	39.47
Seretide MDI (ICS/LABA) ³¹			
ICS	3.5	1.9	42.06
LABA	3.4	1.9	42.94

Abbreviations: FPF, fine particle fraction; FRI, functional respiratory imaging; GSD, geometric standard deviation; ICS, inhaled corticosteroid; LABA, long-acting beta-2 agonist; LAMA, long-acting muscarinic antagonist; MDI, metered dose inhaler; MMAD, mass mean aerodynamic diameter.

Spiriva 18 (100% of the patients), Seretide Diskus 50/500 and 50/250 (54% and 4%), Symbicort 9/320 and 4.5/160 (18% and 7%), Inuvair 12/200 and 6/100 (11% and 4%), Pulmicort 400 and 200, Oxis 9, Onbrez 150, and Seretide MDI 25/250 (all 4%).

FRI assessment of bronchodilation

Segmentation of the airways or image-based airway volume can be performed down to the level of the smaller airways with a diameter of 1–2 mm using an HU threshold of [–1,024; –824]. By performing airway segmentation at baseline and at 6 months, the patient-specific three-dimensional geometry of the airways can be extracted at both time points. The two geometries can be subsequently placed on top of each other, and regional measurements of changes in airway volume (ie, bronchodilation or bronchoconstriction) can be performed. FRI typically reports changes through color-coded figures.

Statistics

Statistical analysis was performed using the open-source statistical environment R 3.02. Correlations between parameters that are measured on a lobar basis were assessed using a mixed-model approach, wherein the different lobes were considered to be nested random factors. Correlations between global measurements were determined using Pearson correlation. Significance level was set at $P < 0.05$. A responder group was a priori defined based on the measurement error of FEV₁, which was recently determined to be 120 mL.¹⁷

Results

De Backer et al¹⁰ previously reported a significant reduction of the lobar hyperinflation (iLobes_FRC) at the FRC level in the patients who improved >120 mL in FEV₁, the so-called responder group. The reduction in lobar hyperinflation appears to be associated with a larger blood vessel density in the respective lobes (Figure 4; $t = -2.154$, $P = 0.040$): lobes with a higher percentage of blood vessels reduce more during hyperinflation in the responder group. No correlation between blood vessel density and change in hyperinflation is found in the placebo group (Figure 5; $t = -0.760$, $P = 0.453$), indicating that the reduction in hyperinflation might be caused by PDE4 inhibition. Subsequently, it can be observed that lobes that reduce during hyperinflation after treatment are better ventilated (Figure 6; $t = -5.368$, $P < 0.001$), where ventilation is determined by the difference in TLC and FRC lobe volumes. FRI-based aerosol deposition shows that enhanced ventilation also leads to more particle deposition of ICSs/LABAs/LAMAs in the better-ventilated areas (Figure 7; $t = 2.407$,

Figure 4 Negative correlation between the lobar blood vessel density and the change in lobar hyperinflation in the roflumilast responder group after 6 months of treatment.

Note: Better-perfused lobes experience larger reduction in hyperinflation.

Abbreviation: %p, percentage of predicted.

$P=0.024$). Finally, the study shows that areas receiving more particles have increased FRI-based bronchodilation (Figure 8; $t=2.564$, $P=0.017$), leading to an increase in FEV_1 (Figure 9, $R=0.348$, $P=0.029$).

Discussion

This report provides additional analyses of the study reported by De Backer et al,¹⁰ with the main focus on regional changes in ventilation, aerosol deposition, bronchodilation, and blood vessel density. Lobes with a high percentage of blood vessels reduce more during hyperinflation in the responder group.

For the first time, HRCT data and CFD are used to understand the interaction between systemic and inhaled drugs. The study appears to support the hypothesis that roflumilast reaches, via the vasculature, areas that were

Figure 5 No correlation between the lobar blood vessel density and the change in lobar hyperinflation in the placebo group.

Abbreviation: %p, percentage of predicted.

Figure 6 Negative correlation between the change in lobar hyperinflation and the change in lobar ventilation in the Roflumilast responder group after 6 months of treatment.

Note: Lobes that experience a larger reduction in hyperinflation are better ventilated.

Abbreviation: %p, percentage of predicted.

previously undertreated by the inhaled medication. Opening smaller airways or preventing airway collapse, presumably by reducing inflammation and edema, results in a reduction of regional hyperinflation, eventually cascading into enhanced efficacy of the concomitant ICS/LAMA/LABA treatment. Even though this appears to be the mode of action of roflumilast, it is likely that the PDE4 inhibitor by itself also has a positive, but potentially smaller effect, on the larger airways in terms of bronchodilation and reduction of inflammation. This can be concluded from the differences observed between the treatment and placebo arms. The latter remains a topic of ongoing research and can be assessed by studying inhaled PDE4 inhibitors currently under development^{18,19} and

Figure 7 Positive correlation between the change in lobar ventilation and the change in lobar aerosol deposition in the roflumilast responder group after 6 months of treatment.

Note: Lobes that are better ventilated consequently experience more drug deposition.

Figure 8 Positive correlation between the change in lobar aerosol deposition and the change in lobar CT-based bronchodilation (iVaw) in the roflumilast responder group after 6 months of treatment.

Note: Lobes with higher deposition had more bronchodilation.

Abbreviations: CT, computed tomography; iVaw, image-based airway volume.

comparing the results with those from orally administered roflumilast. Overall, the results of this study raise several challenging research questions.

A previous study by Vestbo et al³² on inhaled PDE4 inhibitor showed no effect of treatment on spirometric measures and symptoms score in patients with moderate-to-severe COPD. However, we think this needs further investigation: It may have no effect on spirometric values, but we can get better insight of the local responses with functional respiratory imaging to fully evaluate the regional hyperinflation, internal airflow distribution, regional aerosol deposition patterns, and image-based bronchodilation. So, inhaled roflumilast could be a therapeutic option for COPD

Figure 9 Positive correlation between the change in CT-based bronchodilation (iVaw) and the observed changes in FEV₁.

Note: More bronchodilation leads to better FEV₁.

Abbreviations: CT, computed tomography; FEV₁, forced expiratory volume in 1 second; iVaw, image-based airway volume; %p, percentage of predicted.

patients without the systemic side effects, but it needs further investigation.

First of all, one can wonder whether inhalation medication by itself adequately treats COPD patients. Today's standard of care in lung diseases is usually LABA, LAMA, ICS, or a combination thereof. However, if it is really true that areas in the lungs are chronically undertreated due to either ineffective deposition (insufficient amount of particles) or ineffective exposure (insufficient dose), then even the most potent compounds will not be able to demonstrate high efficacy. Gienbycz and Newton²⁰ recently argued that roflumilast is beneficial in severe COPD patients who frequently show exacerbation because these patients are prone to bacterial colonization, infection, and a high level of inflammation. Moreover, Yu et al²¹ concluded that patients at high risk of severe exacerbations have a net benefit from roflumilast. On the basis of these findings and the results of our study, we would suggest that frequent exacerbations in patients are a result of inadequate control of the disease using inhalation medication due to low regional exposure of the drug in poorly ventilated areas. The systemic delivery route of roflumilast, and particularly earlier start of the treatment, therefore could mitigate this undertreatment and provide a benefit to these severe patients. While the results of this study provide initial evidence of the hypothesis, additional confirmatory trials are needed. Considering this, the recent publication of the REACT trial results²² strengthens the belief of the authors that the proposed hypothesis might indeed be correct.

The second interesting research topic relates to the pathophysiology of COPD exacerbations. The label of roflumilast currently indicates that the product can be used to reduce exacerbations, and the studies mentioned herein also support this indication. Our trial demonstrated that the mode of action of roflumilast is probably related to regional hyperinflation. This finding triggers the following hypothesis: COPD exacerbations are associated with regional hyperinflation. The association of exacerbations with overall hyperinflation measured using body plethysmography has been described in recent studies.^{23,24} However, these aggregate measures might not fully reflect the changes in hyperinflation due to the interdependence between the lobes. It could be that certain lobes are hyperinflated, but when an intervention reduces the hyperinflation in that lobe, the neighboring lobe(s) might reinflate, thereby reducing the overall signal in the conventional black box parameters. Imaging, and in particular FRI, provides highly detailed, quantifiable information, which makes it a valuable tool in early clinical development of novel compounds. The fact

that FRI end points can be assessed on a lobar level already provides higher statistical power because one patient now yields five measurement points, compared to conventional outcome parameters such as FEV₁, whereby one patient only yields one black box measure. However, a correction for the lobe interdependence needs to be included in the statistical analysis (as described in the preceding text, via the generalized estimating equation with an autoregressive covariance). In a recent review, Coxson et al²⁵ confirmed the potential of imaging to go beyond FEV₁ in COPD.

Especially in early clinical phases, it is particularly useful to have a surrogate for exacerbations. Having a surrogate would allow the researcher to assess the effect of the novel drug on this surrogate, thereby de-risking the late phase of drug development.

At present, the usefulness of FRI to better characterize COPD exacerbations is speculative, and additional studies using FRI need to be performed to confirm the correlation between regional hyperinflation and exacerbations. A clinical trial with the latter topic (NCT01684384) has been recently concluded, and the results will be available shortly.

Often, in clinical trials with FRI and spirometry, one raises the following question: which end points are “measurements” and which end points are “calculations”. While the easy answer is to state that all parameters derived from the HRCT are calculated, the topic becomes more complex when we take one step back and realize that virtually all measurements are in fact calculations. The FEV₁, for instance, is a calculation of a pressure drop over a known resistance integrated between 0 second and 1 second; the HRCT is regarded as a measurement or even a picture, while it is inherently a calculation (the C stands for computed). The problem we experienced using terms such as calculation, model, simulation etc is that these end points are often dismissed as not real or idealized, while the opposite is true. FRI parameters are advanced quantifications of patient-specific measures. In our view, the difference between a “measurement” and a “calculation” is merely the level of general acceptance of the method used to obtain the parameter.

The study demonstrated that orally administered roflumilast supports the reduction of regional hyperinflation in areas previously undertreated by inhalation medication. The local reduction in hyperinflation induces a redistribution of ventilation and aerosol deposition, leading to enhanced efficacy of the concomitant ICS/LABA/LAMA therapy. FRI appears to be a sensitive tool to describe the mode of action of novel compounds in COPD. Future studies need to confirm the enhanced sensitivity and the potential of FRI parameters to act as surrogates for clinically relevant, but more difficult to measure, end points such as exacerbations.

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Disclosure

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