Novel electrosprayed nanospherules for enhanced aqueous solubility and oral bioavailability of poorly water-soluble fenofibrate

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Purpose: The purpose of the present research was to develop a novel electrosprayed nanospherule providing the most optimized aqueous solubility and oral bioavailability for poorly water-soluble fenofibrate.

Methods: Numerous fenofibrate-loaded electrosprayed nanospherules were prepared with polyvinylpyrrolidone (PVP) and Labrafil® M 2125 as carriers using the electrospray technique, and the effect of the carriers on drug solubility and solvation was assessed. The solid state characterization of an optimized formulation was conducted by scanning electron microscopy, powder X-ray diffraction, differential scanning calorimetry, and Fourier transform infrared spectroscopic analyses. Oral bioavailability in rats was also evaluated for the formulation of an optimized nanospherule in comparison with free drug and a conventional fenofibrate-loaded solid dispersion.

Results: All of the electrosprayed nanospherule formulations had remarkably enhanced aqueous solubility and dissolution compared with free drug. Moreover, Labrafil M 2125, a surfactant, had a positive influence on the solubility and dissolution of the drug in the electrosprayed nanospherule. Increases were observed as the PVP:drug ratio increased to 4:1, but higher ratios gave no significant increases. In particular, an electrosprayed nanospherule composed of fenofibrate, PVP, and Labrafil M 2125 at the weight ratio of 1:4:0.5 resulted in a particle size of ~<200 nm with the drug present in the amorphous state. It demonstrated the highest solubility (32.5±2.41 μg/mL), an excellent dissolution (~85% in 10 minutes), and an oral bioavailability ~2.5-fold better than that of the free drug. It showed similar oral bioavailability compared to the conventional solid dispersion.

Conclusion: Electrosprayed nanospherules, which provide improved solubility and bioavailability, are promising drug delivery tools for oral administration of poorly water-soluble fenofibrate.

Keywords: fenofibrate, electrospray technique, nanospherule, enhanced bioavailability

Introduction
Fenofibrate, a Biopharmaceutics Classification System class II drug, is a therapeutic agent used for the treatment of hypercholesterolemia and hypertriglyceridemia.1,2 It is a very lipophilic entity (logP =5.24) that is practically insoluble in aqueous gastrointestinal fluids (<100 μg/mL);5,6 therefore, it exhibits very poor absorption5 and bioavailability after oral administration.1 Thus, an enhancement in bioavailability is dependent upon an improvement in aqueous solubility.

Nanotechnology is an elegant science with the capability to resolve aqueous solubility, dissolution, and absorption problems of poorly water-soluble active pharmaceutical agents.6,7 A pharmaceutical nanoparticle is a particle having a
Nanoparticles can be fabricated using polymeric compounds. Natural polymers confer outstanding protection, effectiveness, biocompatibility, and biodegradation characteristics; accordingly, they are very popular matrices for pharmaceutical nanoparticle formation. There are several methods to develop pharmaceutical nanoparticles, such as solvent evaporation, emulsification, spray drying, phase inversion, self-assembly, and solvent displacement. Electrospaying is a promising technique for the preparation of pharmaceutical nanoparticles. In the preparation of a nanosphere via this technique, all of the constituents are comprehensively dissolved and the final transparent solution is subjected to electrospaying. The resulting nanosphere is a spherical nanoparticle containing evenly scattered drug molecules in the polymeric matrix.

The electrospaying approach has been successfully used to produce polymeric nanoparticles for several drug classes, such as antibiotics, anti-inflammatories, and hormones, among others. In this technique, a syringe is filled with a transparent solution of drug and other excipients such as polymeric components. Then, the loaded syringe is secured with the specified holder in the instrument. The pump, used for regulating the flow rate of the feed, is positioned so that it touches the open end of the plunger. An electrode (usually anode) is attached to the capillary nozzle of the syringe, while the other electrode (usually cathode) is attached to the product-collecting metallic sheet. At a specific high voltage, a Taylor cone is formed at the tip of the capillary nozzle, and the flowing liquid atomizes into minute droplets bearing the same charges on their surfaces; therefore, maximal scatter is achieved as a result of Coulombic repulsion. These charged droplets are directed to the collector due to gravity and Coulombic attraction. Evaporation takes place during the journey from ejector to collector.

In this study, to develop a novel electrospayed nanoparticles conferring the most optimized aqueous solubility, dissolution, and oral bioavailability to poorly water-soluble fenofibrate, numerous fenofibrate-loaded electrospayed nanoparticles were prepared with polyvinylpyrrolidone (PVP) and Labrafil M 2125 as carriers using the electrospaying technique. Then, the effect of the carriers on the solubility and dissolution of the drug present in them was assessed. The solid state characterization of an optimized formulation was conducted by powder X-ray diffraction (PXRD), differential scanning calorimetry (DSC), scanning electron microscopy (SEM), and Fourier transform infrared (FTIR) spectroscopic analyses. Oral bioavailability in rats was evaluated in comparison with free drug and a conventional fenofibrate-loaded solid dispersion for the formulation of an optimized preparation.

Materials and methods
Materials
Fenofibrate and fenofibric acid were provided by Hanmi Pharmaceutical Co (Suwon, South Korea). PVP K30 was procured from BASF (Ludwigshafen, Germany). Labrafal M 2125 was purchased from Gattefosse (Saint Priest Cedex, Lyon, France). Clofibric acid was obtained from Sigma-Aldrich (St Louis, MO, USA). All other chemical substances were of reagent grade.

Preparation of nanospherules
Each nanospherule formulation was prepared using ESR 100 electrospaying equipment (NanoNC, Seoul, South Korea). All the components, including nonmicronized fenofibrate, were completely dissolved in dichloromethane. This clear solution was filled in a gas-tight glass syringe (Hamilton Co, Reno, NV, USA) equipped with a polytetrafluoroethylene plunger tip (Figure 1). Subsequently, electrospaying was performed at a flow rate of 0.5 mL/h under an optimized voltage of 8.5 kV. The dried product was carefully collected and preserved in dry microtubes.

Aqueous solubility test
An ample quantity of each nanospherule formulation (~10 mg) was added to 500 μL of distilled water in a 2 mL microtube and vortex-mixed (~1 minute). Subsequently, the tubes were agitated at 100 rpm for 7 days in a water bath at 25°C. Then, after vortex-mixing again, centrifugation was performed at 10,000 × g for 10 minutes (Smart 15; Hanil Science Industrial Co, Gangneung, South Korea). A 300 μL aliquot of supernatant was diluted with 300 μL of acetonitrile in another clean microtube. The diluted was filtered through a syringe filter (0.45 μm, number 6789–1304; Whatmann Co, Shrewsbury, MA, USA) and the concentration of fenofibrate in the filtrate (50 μL) was quantified by high-performance liquid chromatography (HPLC) (Agilent 1260 Infinity; Agilent Technologies, Santa Clara, CA, USA). The HPLC system was equipped with a Capcell Pak C18 column (4.6 mm inner diameter × 250 mm, 5 μm particle size; Shiseido, Tokyo, Japan). The column temperature was set at 30°C. The mobile phase, consisting of acetonitrile and 0.1% (v/v) aqueous phosphoric acid at a volume ratio of 75:25, was eluted at a flow rate of 2 mL/minutes. The eluent was monitored at 286 nm for the quantification of fenofibrate.
Dissolution test
The dissolution test was performed using the basket apparatus (Vision® Classic 6™; Hanson Research Co, Los Angeles, CA, USA). Each nanospherule formulation, equivalent to 15 mg of fenofibrate, was properly enclosed in a dialysis bag (Spectra/Por® dialysis membrane, molecular weight cutoff: 3,500 Da; Spectrum Laboratories, Rancho Dominguez, CA, USA) and the loaded bag was placed in the basket. The basket was immersed in 500 mL of 2% (w/v) aqueous Tween 80 at 37°C ± 0.5°C. The rotation speed of the basket was set to 100 rpm. At preset time intervals, 1 mL of the dissolution medium was sampled, filtered (0.45 μm), and analyzed using the HPLC method described earlier. After each sampling, the medium was replenished by the addition of 1 mL of fresh dissolution medium.

PXRD analysis
The crystallinity of the samples was examined using a Rigaku X-ray diffractometer (D/MAX-2500 PC; Rigaku Corporation, Tokyo, Japan). The analysis was carried out using a Cu Kα, monochromatic radiation source with 40 mA of current and 40 kV voltage. The X-ray diffraction patterns were recorded in the range of 10°C–80°C, with a 2θ scanning mode, a step size of 0.02°/second, and a scan speed of 5°/minute.

DSC analysis
The thermograms of samples were recorded using a DSC (DSC Q20; TA Instruments, New Castle, DE, USA). Each sample was enclosed in an aluminum pan and scanned over a range of 30°C–130°C, at a heating rate of 10°C/minutes and a nitrogen flow of 25 mL/minutes.

FTIR spectroscopic analysis
The FTIR spectroscopic analysis was executed to determine the potential interaction between the drug and the excipients. The FTIR spectra of samples were recorded using an FTIR spectrophotometer-430 (Shimadzu Corporation, Tokyo, Japan). Each sample, thoroughly triturated with potassium bromide and subsequently compressed to make a disk, was scanned over a range of 400–4,000 cm⁻¹ with 2 cm⁻¹ resolution.

SEM analysis
The shape and surface attributes of free drug and nanospherule were observed using a scanning electron microscope (S-4800; Hitachi Ltd., Tokyo, Japan). The samples, attached on the exposed side of double-sided adhesive tape affixed on a metallic disk, were coated with platinum using an EMI Teck Ion Sputter (K575K). Coating was continued for 4 minutes under a pressure of 8×10⁻³ mbar, 15 mA current, and 100% turbo speed with the intention of making the samples electrically conductive for imaging.

Pharmacokinetic studies
Care of animals
Eighteen male Sprague Dawley rats (each 270–300 g) were placed under a controlled environment at 22°C–25°C,
with 50%–60% relative humidity, and ad libitum access to food and water. Access to food was discontinued 36 hours prior to the start of the pharmacokinetic procedures because food intake greatly affected the oral absorption of fenofibrate; nevertheless, free access to drinking water was continued. The procedures for the animal studies were consistent with National Institutes of Health Policy and the Animal Welfare Act under the approval of the Institutional Animal Care and Use Committee at Hanyang University.

**Dose administration and periodic blood sampling**

Before compound administration, each fasted rat was surgically cannulized in the right carotid artery. Then, it was placed in a separate restraining box, in which it was sufficiently free to move and drink water. The cannulized rats were divided into three groups, each comprising six rats. Each treatment, whether the nonmicronized free drug, the fenofibrate-loaded solid dispersion, or the nanospherule formulation, was equivalent to 20 mg/kg fenofibrate and was enclosed in tiny, hard gelatin capsules (#9; Suheung Capsule Co, Seoul, Korea). The capsules were administered via the oral route to the corresponding rat. The electrospayed nanospherules and the solid dispersion were composed of fenofibrate, PVP, and Labrafil M 2125 at a weight ratio of 1:4:0.5. This fenofibrate-loaded conventional solid dispersion was prepared by dissolving nonmicronized fenofibrate in ethanol and then spray-drying it with a Büchi B-290 mini spray dryer (Büchi Co, Flawil, Switzerland). Blood samples were collected at the following preset time intervals: 0.25, 0.5, 1, 1.5, 2, 4, 6, 10, 14, 24, and 36 hours using heparinized syringes. Plasma was immediately isolated from each blood sample (400 μL) by centrifugation (Hanil Science Industrial Co) at 10,000×g for 10 minutes. Subsequently, plasma samples were refrigerated at −20°C until further experimentation.

**Sample preparation**

Separated plasma samples were acidified by the addition of 200 μL of 1 M HCl. Subsequently, 40 μL of clofibric acid solution, at a concentration of 400 μg/mL in acetonitrile, was added and mixed. Then, liquid–liquid extraction was performed twice with 2 mL of diethyl ether by vigorous, thorough mixing for 5 minutes and centrifuging at 10,000×g for 10 minutes (Hanil Science Industrial Co). The transparent supernatant was evaporated in another clean microtube at 40°C. Samples were reconstituted in 200 μL of acetonitrile. Each reconstituted sample was placed in a small-volume HPLC vial and subjected to HPLC analysis.

**HPLC analysis**

Fenofibrate is a prodrug. After oral administration, it is completely metabolized to fenofibric acid by biological esterases. Thus, an evaluation of the bioavailability of fenofibrate is dependent upon the measurement of fenofibric acid in the blood stream. A 100 μL aliquot of the prepared sample was analyzed for fenofibric acid content. An Agilent 1260 Infinity HPLC system (Agilent Technologies) was used for this purpose. A Capcell Pak C18 column (4.6 mm inner diameter ×250 mm, 5 μm particle size), with temperature set to 30°C, was used for reverse-phase HPLC analysis. The mobile phase consisted of acetonitrile and 0.1% (v/v) phosphoric acid (54:46, v/v). The flow rate of the mobile phase was 2 mL/minutes. Fenofibric acid quantification was accomplished at 285 nm.

**Results and discussion**

Electrospraying is a promising technique for the preparation of pharmaceutical polymeric nanoparticles. In this study, fenofibrate, PVP, and Labrafil M 2125 were entirely dissolved in volatile dichloromethane (boiling point: 39.6°C) and subjected to electrospraying via the solvent evaporation method, leading to the novel fenofibrate-loaded nanospherules. PVP and Labrafil M 2125 were selected as the most suitable excipients owing to their excellent fenofibrate solubilization ability and their complete solubility in dichloromethane to form an absolutely clear solution for electrospraying.

To determine the effect of Labrafil M 2125 concentration on the aqueous solubility and dissolution of fenofibrate, nanospherule formulations I–VI (Table 1) were prepared with gradually increasing amounts of Labrafil M 2125 while maintaining the fenofibrate/PVP ratio constant at 1:2. All of the electrospayed nanospherule formulations had remarkably enhanced aqueous solubility and dissolution compared with the free drug. With increasing amounts of Labrafil M 2125, solubility (Figure 2A) and dissolution (Figure 2B) were enhanced further. Labrafil M 2125, a surfactant, improved

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**Table 1** Compositions of electrosprayed nanospherules

<table>
<thead>
<tr>
<th>Constituents (g)</th>
<th>I</th>
<th>II</th>
<th>III</th>
<th>IV</th>
<th>V</th>
<th>VI</th>
<th>VII</th>
<th>VIII</th>
<th>IX</th>
<th>X</th>
<th>XI</th>
</tr>
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<tbody>
<tr>
<td>Fenofibrate</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
<td>1</td>
</tr>
<tr>
<td>PVP</td>
<td>2</td>
<td>2</td>
<td>2</td>
<td>2</td>
<td>2</td>
<td>2</td>
<td>1</td>
<td>4</td>
<td>6</td>
<td>8</td>
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<tr>
<td>Labrafil M 2125</td>
<td>0</td>
<td>0.1</td>
<td>0.2</td>
<td>0.3</td>
<td>0.4</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
<td>0.5</td>
</tr>
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</table>

**Abbreviation:** PVP, polyvinylpyrrolidone.
the drug solubility and dissolution due to its high solubilization ability. Among the nanospherule formulations I–VI, formulation VI, containing fenofibrate/PVP/Labrafil M 2125 at the weight ratio of 1:2:0.5, showed the highest apparent aqueous solubility (21.23±2.54 μg/mL) and dissolution (~70% at 1 hour) of fenofibrate. Therefore, this formulation was selected for further study.

Next, the influence of the quantity of polymeric matrix on the solubility and dissolution of the drug were investigated. The nanospherule formulations VII–XI (Table 1) were prepared with varying amounts of PVP while keeping the fenofibrate/Labrafil M 2125 ratio fixed at 1:0.5. As the PVP/drug ratio increased to 4:1, the solubility (Figure 3A) and dissolution (Figure 3B) increased. Further increasing the quantity of PVP in formulations IX, X, and XI did not significantly change the solubility or dissolution. Thus, on the basis of the highest apparent solubility (32.51±2.41 μg/mL) and dissolution (~97% in 20 minutes) behavior of the drug, the formulation IX, containing fenofibrate/PVP/Labrafil M 2125 at the optimized weight ratio of 1:4:0.5, was chosen as an optimal formulation of electrosprayed nanospherule.

The X-ray diffraction patterns of the samples are displayed in Figure 4A. The free drug pattern was characterized by sharp spikes, representing its typical crystalline nature (Figure 4A-a). The diffraction for PVP did not show any peaks, suggesting that it was amorphous in nature (Figure 4A-b). The main distinguishing peaks attributed to crystalline fenofibrate were also seen in the physical mixture (Figure 4A-c). However, the drug was present in the amorphous state in the electrosprayed nanospherule (Figure 4A-d).11,12
Figure 4B shows the thermal properties of the samples. The free drug gave a sharp endothermic peak at the melting point of fenofibrate at ~81.5°C (Figure 4B-a). This confirmed that the drug was typically crystalline in nature. PVP did not generate any endothermic peaks (Figure 4B-b); however, a broad downward curve was observed due to moisture evaporation. Fenofibrate also generated an endothermic peak (Figure 4B-c) in the physical mixture, suggesting that the drug was present in the crystalline form in the physical mixture. On the other hand, the drug was completely transformed into the amorphous state in the nanospherules (Figure 4B-d).

The SEM outcomes of the study of fenofibrate powder and electrosprayed nanospherules are presented in Figure 5. The free drug showed crystals of irregular shape and surface (Figure 5A). The electrosprayed nanospherules appeared as tiny spherical nanoparticles (Figure 5B). The SEM image indicated that these electrosprayed nanospherules had a particle size <200 nm. In general, a pharmaceutical nanoparticle is a particle having a diameter <1,000 nm.

Figure 6 shows the mean fenofibric acid concentration–time profiles after oral administration of the free drug, the solid dispersion, and the electrosprayed nanospherules; each dose was equivalent to 20 mg/kg fenofibrate. Fenofibrate, a prodrug, is completely bio-transformed after oral administration to fenofibric acid, an active metabolite, by blood and tissue esterases. There is no fenofibrate detectable in plasma following oral administration; therefore, a bioavailability assessment relies upon quantification of its metabolite. The nanospherules and solid dispersion gave higher mean plasma concentrations of fenofibric acid than did the free drug at all time points.
with particularly significant differences from 1 to 12 hours ($P<0.05$). Moreover, the plasma titers of fenofibric acid in the nanospherule group were not significantly different from those in the solid dispersion group, even if the former showed lower values than did the latter. The pharmacokinetic parameters are displayed in Table 2. The area under the curve (AUC) and maximum plasma concentration ($C_{\text{max}}$) of the nanospherule and solid dispersion was remarkably improved as compared to the AUC and $C_{\text{max}}$ of the free drug ($P<0.05$). Similar to the plasma concentration, there were no significant differences in AUC and $C_{\text{max}}$ values between the nanospherule and the solid dispersion. The AUC values of the free drug and the novel nanospherule formulation were $17.72\pm1.52$ and $41.01\pm10.60$ h $\mu g/mL$, respectively. Similarly, the $C_{\text{max}}$ values of the free drug and the novel nanospherule formulation were $2.36\pm0.34$ and $5.12\pm1.61$ $\mu g/mL$, respectively. On the other hand, the half-lives did not show significant variation from one another. With similar bioavailability as the conventional solid dispersion, the nanospherule improved bioavailability by ~2.5-fold as compared with the free drug. This enhancement might be attributed to the remarkable improvement in the aqueous solubility and dissolution resulting from particle size reduction and conversion of the crystalline drug to the amorphous state. Generally, improvement in aqueous solubility and bioavailability of poorly water-soluble drugs by conventional solid dispersion systems is due to wetting enhancement, particle size reduction, and/or a change of the crystalline drug to the amorphous form. Thus, in this study, the electrosprayed nanospherule may have improved the aqueous solubility and bioavailability of poorly water-soluble fenofibrate by the same mechanisms, except through wetting enhancement. On the other hand, unlike other microcapsules

**Table 2 Pharmacokinetic parameters**

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Fenofibrate powder</th>
<th>Solid dispersion</th>
<th>Electrosprayed nanospherule</th>
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</thead>
<tbody>
<tr>
<td>AUC (h $\mu g/mL$)</td>
<td>17.7±3.5</td>
<td>52.0±14.7</td>
<td>41.0±10.6</td>
</tr>
<tr>
<td>$C_{\text{max}}$ (h $\mu g/mL$)</td>
<td>2.4±0.3</td>
<td>5.7±1.8</td>
<td>5.1±1.6</td>
</tr>
<tr>
<td>$T_{\text{max}}$ (hour)</td>
<td>1.6±0.2</td>
<td>2.7±1.0</td>
<td>1.8±0.3</td>
</tr>
<tr>
<td>$t_{1/2}$ (hour)</td>
<td>6.1±0.9</td>
<td>6.7±0.3</td>
<td>5.3±1.4</td>
</tr>
</tbody>
</table>

**Notes:** Each value represents the mean ± standard deviation (n=6). The electrosprayed nanospherule and the solid dispersion were composed of fenofibrate, PVP, and Labrafil M 2125 at the weight ratio of 1:4:0.5. $^*$P<0.05 compared with free drug. **Abbreviations:** AUC, area under the curve; $C_{\text{max}}$, maximum plasma concentration; PVP, polyvinylpyrrolidone; SD, standard deviation; T $\text{max}$, time to reach maximum plasma concentration; $t_{1/2}$, half-life of drug.
and solid dispersions, the electrospayed nanospherule could be manufactured without heat, leading to production of more stable formulations compared to the former two. Moreover, the electrospayed nanospherule might greatly enhance the aqueous solubility and oral bioavailability of various poorly water-soluble drugs compared to other ones due to the greater reduction in particle size, even if they present similar oral bioavailability, as in this study. Therefore, the novel well-established electrospayed nanospherule system is a promising candidate to deliver poorly water-soluble drugs with remarkably improved oral bioavailability and excellent stability.

**Conclusion**

The novel electrospayed nanospherule, composed of fenofibrate, PVP, and Labrafil M 2125 at the weight ratio of 1:4:0.5, had a particle size <200 nm, with the drug present in the amorphous form. It improved the solubility (32.5±2.41 µg/mL), dissolution (~85% in 10 minutes), and oral bioavailability (~2.5-fold) of the drug compared with the properties of the free drug; accordingly, this formulation is a potential drug delivery system to deliver poorly water-soluble fenofibrate with greater bioavailability. Further studies on its efficacy, including measurement of serum triglycerides, will be carried out for the development of novel fenofibrate-loaded electrospayed nanospherule.

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**Disclosure**

The authors report no conflicts of interest in this work.

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