The role of high-intensity focused ultrasound in ablation of atrial fibrillation and other cardiac arrhythmias

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Abstract: Atrial fibrillation is the most prevalent arrhythmia of the heart, originating usually from ectopic atrial activity of the pulmonary veins. Therefore, one of the treatment options is pulmonary vein isolation. Among the novel approaches to pulmonary vein isolation, high-intensity focused ultrasound (HIFU) has been developed. The ultrasound energy can be focused on a specific area and would result in the formation of a lesion similar to that formed with radiofrequency (RF) ablation. Although preclinical studies were promising, clinical studies in patients resulted in lower efficacy and high complication rates in comparison to the standard ablation method, due to collateral damage. Using HIFU for epicardial approach during cardiac surgery and for extracorporeal ablation does seem to have a future role. In this review, we present the mechanism of HIFU lesion formation and the principal studies.

Keywords: atrial fibrillation, HIFU, high-intensity focused ultrasound, pulmonary vein isolation, epicardial ablation

Background
Atrial fibrillation (AF) is the most prevalent and sustained arrhythmia worldwide. The incidence of AF has been increasing due to the increasing elderly population. Antiarrhythmic medications are only moderately effective in controlling AF, and their use is often limited by their side effects. Seminal work from Haissaguerre et al demonstrated that the predominant trigger for AF is ectopic activity originating in the pulmonary veins (PVs). Hence, strategies to electrically isolate the PVs from the remainder of the left atrium have evolved as the dominant nonpharmacologic strategy to treat AF.

The most commonly performed method for achieving electrical pulmonary vein isolation (PVI) involves the use of radiofrequency (RF) energy. Surgical methods utilizing RF energy have been used long probes, many fashioned as a clamp, to allow for the placement of contiguous lesions around the PV. Current percutaneous methods of isolation, however, require ablation in a point-by-point fashion along the ostium of the PVs. This procedure is operator-dependent, time-consuming, and results in a significant complication rate of 4%–5%. Among the serious complications, stroke (up to 1%), tamponade (1%), atrial-esophageal fistula (AEF) (0.1%), and PV stenosis (<0.5%) are the most significant. Furthermore, clinical success is ~70%–80% in 12 months. Therefore, a search for ablation strategy that may allow for easier PVI is ongoing.

Current novel approaches for PVI, frequently referred to as single-shot approaches, capitalize on the circular nature of the PV ostium. In essence, new approaches – both RF-based and non–RF-based – allow the delivery of energy sources using a circular or
balloon-based catheter design. Some of the catheters that are currently used include cryoballoon (Medtronic, Minneapolis, MN, USA), which freezes the tissue; high-intensity focused ultrasound (HIFU; ProRhythm, Ronkonkoma, NY, USA), which delivers ultrasound (US) energy; the HeartLight laser balloon (CardioFocus, Marlborough, MA, USA); nMARK, which delivers RF energy (Biosense Webster Inc., Diamond Bar, CA, USA). It is proposed that the circular catheter-based strategy may allow for easy isolation of the PVs in relatively short time by allowing for the placement of contiguous lesions around the circumference of the PV. Furthermore, it is thought that these approaches would be less operator-dependent.

HIFU is one of the several approaches available for PVI (Figure 1). The first ablation using this technology in humans was reported in 2000. This article will review the mechanism and clinical use of HIFU for the management of arrhythmia, with special attention to AF.

**The mechanism of HIFU lesion formation**

US is a form of vibration energy that can cause thermal tissue injury. The vibration wave propagates and creates mechanical movement of particles within a medium, which is then converted to heat. Thus, tissue damage is due to thermal injury. Further tissue damage also results from the acoustic cavitation, a process of formation of microbubbles by the propagated US wave. The formation of bubbles might enhance the effect of HIFU by creating a nonabsorbable medium (raising the acoustic impedance). This effect may also result in reflection of the US wave and heating of the prefocused area. Engel et al used a wedge preparation of dog heart to investigate the ability of HIFU to create lesions. Thermal damage results in protein denaturation, vacuoles formation, mitochondrial fragmentation, and clamping and fragmentation of Z-band of myocytes. Of note, this damage is also seen in lesions caused by RF as well, except for intramyocardial vacuolization.

Experimental studies have demonstrated that the lesion size with HIFU appears to be dose-dependent – that is, increasing the application time and the acoustic power results in deeper lesions. The lesion created by HIFU can be deep (up to 11 mm) and wide. Unlike RF lesions, HIFU lesions are well demarked with a histologically normal tissue surrounding the ablated tissue (Figure 2). Remarkably, it has been demonstrated that one can target a certain location with the application of HIFU energy. For example, Engel et al were able to create midmyocardial lesions in cardiac tissue while ensuring that the epicardium and endocardium were intact. This property is in contrast to the RF lesions that decrease in efficacy with distance from the catheter. This property of HIFU may specifically be advantageous when ablating within the thick-walled left ventricle in patients with ventricular tachycardia, particularly those with mid- or epicardial circuits for ventricular tachycardia.

Another property of US energy that makes it advantageous for cardiac ablation is its ability to easily penetrate soft tissue. As such, US energy can produce focal lesions without the need to be in contact with the tissue. This property of HIFU makes it advantageous to other methods of ablating cardiac tissue. For example, proper contact is necessary for tissue injury to occur when RF or cryoablation energy

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**Figure 1** Schematic representation and photograph of the HIFU balloon.

**Notes:** (A) The noncompliant balloon, optimal for pulmonary vein ablation, is attached to a steerable catheter. An ultrasound crystal is located at the proximal part of the balloon. The balloon is filled with carbon dioxide and forms an interface allowing the reflection of the ultrasound beam. The acoustic power of the balloon is 45 W. (B) The HIFU catheter with the inflated balloon. Reproduced from Schmidt B, Chun KRJ, Kuck KH, Antz M. Pulmonary vein isolation by high intensity focused ultrasound. *Indian Pacing and Electrophysiology Journal*. 2006;7(2):126–133. Copyright © 2007 Schmidt et al.

**Abbreviation:** HIFU, high-intensity focused ultrasound.
is utilized. This property – produce lesions without the need to be in contact with the tissue – of HIFU makes it particularly advantageous in situations where challenging anatomy, based on the location of the tissue, and cardiac and respiratory motion impact the stability and consistency of catheter–tissue contact.

Studies in animal models
Zheng et al investigated the efficacy of HIFU in the canine heart. Lesion size was smaller than in in vivo model, suggesting that temperature cooling through blood flow is important in HIFU, similar to RF ablation. Okumura et al studied HIFU ablation of the right superior pulmonary vein (RSPV) in eight dogs using a steerable HIFU catheter (10 Fr balloon, diameter 24 mm; ProRhythm Inc.). Electrical PVI was confirmed in seven of eight PVs. The HIFU effect was inversely related to the distance, similar to RF energy. However, contact-independent lesion formation was demonstrated with HIFU, whereas this was not possible with RF energy. In addition, it was shown the HIFU lesions are much larger than RF lesions. Therefore, it was proposed that HIFU may result in faster and more effective tissue damage.

One disadvantage of large rapid lesion formation is the potential for collateral injury (Figure 3). In the study by Zheng et al, phrenic nerve palsy was purposely induced. The authors proposed that a distance of >7.5 mm between the HIFU exit and important structures is needed to prevent collateral damage. As we will explore in the following section, collateral injury may occur despite best intentions with HIFU.

Safety and efficacy in human studies
Several small, nonrandomized studies evaluated HIFU for PVI in humans. In 2006, Wong et al reported on the first patient undergoing PVI using the steerable HIFU balloon. Subsequently, Schmidt et al reported on the use of a steerable HIFU balloon in a cohort of 15 patients – the success rate at 1 year with this approach was 75%. However, the safety of this approach was questioned with two of the 15 patients (13%) having permanent phrenic nerve palsy. Phrenic nerve injury occurred despite high-output pacing at the site of ablation to verify the absence of phrenic nerve capture, as well as pacing the phrenic nerve during ablation to observe loss of phrenic capture – strategies currently employed to protect the phrenic nerve during ablation procedure.

Schmidt et al went on to describe their experience 2 years later with the steerable HIFU balloon. Acute success was improved and procedure time was shortened dramatically. However, concerns about the high rate of procedural complications was again apparent with nearly one-third of all patients (four out of 15) suffering a major complication.
The group also described a safety algorithm aimed at minimizing complications. This algorithm included ≤3 complete HIFU applications per PV, early abortion when no effect was seen after 50% of programmed time or when esophageal temperature (ET) was >40.0°C, and the use of power modulation when an ET of 39.0°C was observed in order to reduce ablation temperature in the surrounding tissue. Touch-up RF ablation was used when PVI failed. ET monitoring and endoscopy were performed 2 days after ablation. Twenty-eight patients were included in the study. Of the 109 PVs, 84 were isolated with HIFU only. HIFU was aborted in nine due to high ETs. After a median follow-up of more than 2 years, 79% of the patients were free of AF without antiarrhythmic drugs or repeat ablation. However, this was achieved with the combination of HIFU and touch-up RF ablation or RF alone in 23% of the cases. Postprocedural endoscopy demonstrated a thermal lesion in two patients.

Two patients had persistent phrenic nerve palsies, one patient had an ischemic stroke, one patient experienced a pericardial effusion 48 days after ablation, one patient had fatal AEF 31 days after ablation, and one patient had an unexplained death 49 days after ablation. The study was prematurely stopped after the lethal case of AEF. The high complication rate (in all, 23% experienced major complications) led the authors to conclude that the safety algorithm failed to prevent lethal complications.

Improving the safety algorithm suggested by Neven et al is difficult to perform. One may use power management (PM) in advance regardless of the esophageal power, which is not considered to be an ideal predictor of AEF. However, given the reduced efficacy with the current protocol, it is expected that further power reduction will decrease the rate of successful PVI much below the rates achieved by RF ablation and other methods. The same is expected with
reduced power. Another option could be cover all but the US focus area (Figure 1) with a gas-filled balloon that will prevent energy delivery toward the phrenic nerve and other structures. However, the efficacy may be decreased, and it may still result in significant collateral damage.

**The HIFU balloon catheter**

The first-generation HIFU balloon was a nonsteerable over-the-wire device. The energy delivery was circumferential around the balloon equator. Saliba et al reported on 33 cases treated with HIFU balloon catheters. Success rate was only 40%. Large or funnel-shaped PV ostium and early branching accounted for the low success rate. A second-generation balloon was developed with a steerable catheter and a forward-projecting focused US beam. The catheter design has two balloons—the distal balloon containing the US crystal while the proximal balloon is filled with carbon dioxide and thus enables the forward projection of US wave (Figure 1). This design was thought to be more suitable for antral PVI rather than ablation within the vein itself, which may result in PV stenosis and phrenic nerve injury.

For PV ablation using HIFU, a double transeptal puncture is required, including 16.5 F sheath for the HIFU catheter. A second 8F sheath for the circular (lasso) catheter is positioned inside the PV to be ablated. Additional electrodes are positioned at the discretion of the operator but usually include at least a decapolar catheter in the coronary sinus. Different sizes of HIFU, including diameters of 24, 27, and 32 mm, balloons are available. The choice is made according to the size of the PVs, measured usually in preoperative cardiac tomography (CT). HIFU application time varies between 40 and 90 seconds and depends on the balloon size (40, 60, and 90 seconds for balloon size of 24, 27, and 32 mm, respectively). Ideally, the balloon should be aligned with the axis of the PV.

**Limitations of balloon technique**

A major limitation of any balloon-based ablation strategy is variability of the PV anatomy. For example, a large common left PV has been reported in up to 20% of patients undergoing AF ablation and right middle PV in ~15% of patients. These variations create a major technical difficulty for the operator. Another limitation is collateral, and in particular permanent, injury to extracardiac tissue such as the phrenic nerve and esophagus. Phrenic nerve palsy may result in dyspnea and is difficult to overcome. Phrenic nerve injury may result from placing the HIFU balloon too distal in the vein. Although methods to minimize phrenic nerve injury have been proposed, phrenic nerve palsy remains significant with the use of the HIFU balloon. In contrast to ablation using cryoballoon, the phrenic nerve palsy caused by HIFU is rarely reversible. Esophageal injury may be fatal as was noted in early clinical studies.

**Noninvasive ablation using HIFU**

Given the ability to direct the focus of US energy, it may be possible to utilize HIFU outside the vascular system. Indeed, extracorporeal HIFU ablation is widely used in oncology (prostate cancer, uterine fibroids, breast, and kidney tumors) and has been used for this purpose for more than 15 years. The US beam may be focused to a distant point without damaging the tissue between the transducer and the ablated tissue. Thus, extracorporeal ablation using HIFU may be advantageous by avoiding complications associated with vascular access and placement of catheters within the vascular system, such as cardiac perforation or stroke related to thrombus formation on the ablation equipment.

Strickberger et al created a model of extracardiac atrioventricular (AV) junction ablation. The ablation US transducer was attached to an imaging transducer and positioned within the thorax in a liquid medium. The AV junction area was identified with the US and a focused US ablation energy was applied during the diastole for only 30 seconds. All procedures resulted in AV block. Histologic sections showed a well-demarcated area of acute inflammation with normal adjacent tissue. Otsuka et al similarly performed ventricular septal ablation, and suggested that this approach may be considered for treatment of hypertrophic obstructive cardiomyopathy. In these two studies, the ablation was performed through a thoracotomy due to attenuation of the US energy by the bony structures of the chest and the gas-rich lungs. However, extracorporeal HIFU can be used in the thorax as was shown for oncological states, mainly sub-diaphragmatic liver cancer. The most popular method is creating an artificial pleural effusion to displace the lung and improve the acoustic window. Wu et al created a pleural effusion by infusing saline and performed AV junction ablation successfully in all the 21 dogs. Rong et al used the same method to create ventricular septal lesions. In their study, 300 mL of saline was injected into the left pleura of 21 canines prior to the ablation, displacing the lung parenchyma and improving the acoustic window. During each HIFU application, lasting 20 seconds, mechanical ventilation was held to decrease the cardiac motion. In addition, meticulous care of the skin was needed, since any hair or dirt may cause US beam deflection and skin burns.
Epicardial ablation using HIFU

Epicardial AF ablation has been used at the time of cardiac surgery as well as during percutaneous epicardial procedures. The original Maze-Cox procedure or its modification is currently used with reasonable outcomes.28 Davies et al recently reported on the use of the Epicor ablation system (St Jude Medical, Minneapolis, MN, USA; Figure 4) during surgical AF ablation procedures29 and confirmed its utility for surgical AF ablation with a 2-year freedom from AF of 81% for paroxysmal AF and 56% for persistent AF. Another group enrolled patients undergoing HIFU PVI during cardiac surgery.30 Each patient underwent electrophysiogical study with mapping 6 months after the HIFU ablation. Although 60% of the patients were free of AF at 6 months, only 38% had evidence of durable PVI.

The safety of epicardial HIFU application for ventricular tachycardia ablation (Figure 5) was studied by Koruth et al using a swine model.31 In particular, the ability to focus the US beam and to avoid injury of adjacent structures was capitalized on, as HIFU application performed on top of coronary arteries did not result in significant coronary artery injury. Indeed, epicardial approaches to HIFU application may be important to consider for future use, as it may avoid collateral injury described with endocardial approaches and allow one to focus ablation to deeper sites. This approach may indeed prove beneficial for ablation of mid-myocardial and septal foci of ventricular tachycardia.

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Figure 4 The Epicor epicardial HiFU system.
Notes: The epicardial HiFU system is placed around the four pulmonary veins to create the “box” lesion at the time of a cardiac surgical procedure for AF ablation. St Jude Medical is a trademark of St Jude Medical, Inc. and its related companies. Reprinted with permission of St Jude Medical, © 2015. All rights reserved.
Abbreviations: HIFU, high-intensity focused ultrasound; AF, atrial fibrillation.

Figure 5 Epicardial ventricular ablation over a coronary artery.
Notes: (A) HiFU application on the epicardial aspect of the left ventricle over the left anterior descending artery. Note the absence of coronary artery injury. (B) Image (4×, Masson’s trichrome [MA]) shows transition from viable myocytes (left) to fibrotic border with inflammation (middle) to necrotic myocytes (right); (C) image (4×, hematoxylin-eosin [HE]) shows LAD with adventitial fibrosis (yellow arrow); (D) image (40×, HE) shows calcification of necrotic myocytes with giant cell (yellow arrow); (E) image (40×, HE) shows necrotic myocytes with nuclear loss (yellow arrow). Adapted from Koruth JS, Dukkipati S, Carrillo RG, et al. Safety and efficacy of high-intensity focused ultrasound atop coronary arteries during epicardial catheter ablation. Journal of Cardiovascular Electrophysiology. 2011;22:1274–1280.31 Copyright © 2011 Wiley Periodicals, Inc.
Abbreviations: HIFU, high-intensity focused ultrasound; LAD, left anterior descending artery.
Summary and future perspective

Current transvenous HIFU ablation for AT carries a high complication rate. With the availability of other techniques (cryoballoon, circular RF catheters), it seems unlikely that this procedure will regain popularity. However, the utility of this approach may not be lost due to its potential for extracorporeal and epicardial ablation.

Disclosure

The authors report no conflicts of interest in this work.

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