Assessing the axonal translocation of CeO$_2$ and SiO$_2$ nanoparticles in the sciatic nerve fibers of the frog: an ex vivo electrophysiological study

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Abstract: The axonal translocation of two commonly used nanoparticles in medicine, namely CeO$_2$ and SiO$_2$, is investigated. The study was conducted on frog sciatic nerve fibers in an ex vivo preparation. Nanoparticles were applied at the proximal end of the excised nerve. A nerve stimulation protocol was followed for over 35 hours. Nerve vitality curve comparison between control and exposed nerves showed that CeO$_2$ has no neurotoxic effect at the concentrations tested. After exposure, specimens were fixed and then screen scanned every 1 mm along their length for nanoparticle presence by means of Fourier transform infrared microscopy. We demonstrated that both nanoparticles translocate within the nerve by formation of narrow bands in the Fourier transform infrared spectrum. For the CeO$_2$, we also demonstrated that the translocation depends on both axonal integrity and electrical activity. The speed of translocation for the two species was estimated in the range of 0.45–0.58 mm/h, close to slow axonal transportation rate. Transmission electron microscopy provided direct evidence for the presence of SiO$_2$ in the treated nerves.

Keywords: CeO$_2$, SiO$_2$, FTIR, nanoparticles, ex vivo electrophysiology, frog sciatic nerve, translocation

Introduction

Nanoscience, the study of nanoscale materials and their applications, is a modern, multidisciplinary approach with promising results across several scientific fields including the catalytic and energy sector$^{1-4}$ and is gradually established in many commercial products. In medicine, drug delivery with nanoparticles (NPs) is one of most dynamically evolving research areas.$^5$ However, fundamental understanding of issues related to toxicity and environmental impact of nanoscale materials is still under investigation.$^6$

During the past several years, there have been numerous toxicological investigations of airborne NPs and their impact on occupational health and the environment.$^7,8$ Experimental models have provided clear evidence that NPs can only translocate to organs after inhalation,$^9,10$ but can also cause disruption of the blood–brain barrier through different administration routes, including the intravenous, the intraperitoneal, and the intracerebral route.$^{11,12}$ Inhaled NPs either translocate directly into the brain or exit the lungs and enter the circulation as shown in rat experiments.$^8$

The nerve fibers of the olfactory nerve is the route of entry of NPs to the brain.$^{13}$ Silver,$^{14}$ ultrafine carbon black,$^{15}$ manganese oxide,$^{16}$ and titanium dioxide (TiO$_2$)$^{17,18}$ NPs have all been found to translocate into the brain via the olfactory nerve in rodents. These NPs are reported to cause inflammation and impair neural function in the hippocampus. It has been suggested that, despite differences between rodent and...
human olfactory systems, this pathway may be relevant in humans.\textsuperscript{10} It has also been suggested that nanogold particles cross into the cerebrospinal fluid space after axonal transport to the olfactory bulb and are distributed to different brain areas.\textsuperscript{19} Deregulation of axonal transport mechanisms is involved in a number of neurodegenerative diseases. It is therefore imperative to further investigate the effects and mechanisms of NP transportation in nerve fibers. Studying NP’s mobility in nerve fibers is essential for reasons beyond neurotoxicity, since NPs can be used as possible drug carriers. Furthermore, they can provide information about the quality of axonal transport and are also a significant parameter to assess proper function of nerve fibers.

Silicon-based particles have been long approved for medical use,\textsuperscript{20} by employing SiO\textsubscript{2} matrices as delivery systems\textsuperscript{21–27} for protein, enzymes, drugs, and genes. CeO\textsubscript{2} (ceria) NPs on the other hand were recently studied for their pharmacological potential\textsuperscript{28} as drug delivery carriers by exploiting their multienzyme antioxidant mimetic properties.\textsuperscript{29} Divergent studies though have shown both beneficial and toxic effects,\textsuperscript{30–33} requiring additional studies for biocompatible standardization.

The purpose of this work was to use an ex vivo nerve preparation based on the isolated frog sciatic nerve in order to study in detail the movement of CeO\textsubscript{2} and SiO\textsubscript{2} NPs in the nerve fibers of the peripheral nervous system.

**Material and methods**

**The sciatic nerve preparation**

Frogs (*Rana ridibunda*) of either sex and of the same age (ranging from 12 to 15 months), weighing 40–60 g, were used. The frogs were euthanatized (decapitated and pithed), and the sciatic nerves were dissected from the spinal cord to the knee, immersed in standard physiological saline solution, and cleaned under a dissection microscope. All experimental procedures were conducted in accordance with the protocols outlined by the Aristotle University of Thessaloniki, Greece, regarding the recommended standard practices for Biological Investigations. When required, the epineurial sheath was removed. The composition of the saline was (in mmol/L): NaCl 135, KCl 4.7, CaCl\textsubscript{2} 2.4, MgCl\textsubscript{2} 1.1, NaHCO\textsubscript{3} 1.0, HEPES 10, glucose 11 (pH 7.4). The nerve was mounted across a three-chambered recording bath, made of Plexiglas, a diagram of which is shown in Figure 1A. The recording bath has been used in a variety of ex vivo neurotoxicological studies and it is fully described elsewhere,\textsuperscript{34–36} but a short description will be given below in order to clarify the protocol for the exposure of the nerve to NPs. The recording bath consists of three chambers: 1) the stimulating chamber (S in Figure 1A) where the proximal cut end of the nerve (Figure 1B) and the active stimulating electrode were placed. The stimulating electrode was connected to a constant voltage stimulator (Digitimer, DS9A; Digitimer Ltd, Welwyn Garden City, UK); 2) the perfusion chamber (n in Figure 1A), where the middle of the nerve was immersed and the grounds of the recording and stimulating electrodes were placed; and 3) the recording chamber (R in Figure 1A), where the distal end of the nerve and the active electrode of an AC (alternating current) differentiate amplifier (Neurolog, NL822; Digitimer Ltd) were placed. Gold electrodes of 24 carat were used. The dimensions of each chamber were 22×22×10 mm (length, width, depth), allowing a solution volume of 10 mL. The three chambers were next to each other, separated by two partitions of 2 mm width (part in Figure 1A).

**Sciatic nerve electrophysiology**

For the electrophysiological experiments and the application of NPs, a waterproof insulation between the three parts of the nerve (proximal, middle, and distal) was required. This was necessary to obtain a constant amplitude in nerve compound action potential (CAP) for a long period of time and to eliminate the possibility of any transport of NPs from one chamber to another.\textsuperscript{37} For this purpose, the top of each partition, including a part of the nerve at the top, approximately 2 mm long, was smeared with a layer of 1–2 mm thick impression paste Xantopren, Heraeus Kulzer, Germany (Xanth in Figure 1A), while a glass cover (c in Figure 1A) was placed on top of the nerve and the impression paste. Thus, the part of the nerve on the partition and the impression paste were sandwiched between the glass cover (c) and the top of the partition. The impression paste Xantopren, used extensively in dentistry, was found to have the smallest impact on the vitality of the nerve compared to other similar materials.\textsuperscript{35} When the impression paste solidified, the three chambers were filled once to cover the part of the nerve in each chamber with oxygenated saline (O\textsubscript{2}, 100%). The saline was stagnant in the three chambers for the rest of the experiment. The temperature of the saline was constantly maintained at 24°C±1°C using a cooling–heating system of water running below the perfusion chamber. To record nerve activity, we generated CAP (Figure 1C) using continuous electrical stimulation of 1 Hz. The constant-voltage stimuli were supramaximal (duration: 0.05 milliseconds and amplitude: 2–3 V), 2–3 times higher than the stimulus intensity required to generate the maximum CAP. Throughout the text, the term CAP refers to maximum CAP recorded using the AC amplifier.
The output of the amplifier was fed to a computer through a data acquisition card interface (Keithley KPCI 3102; Keithley Instruments, Cleveland, OH, USA). The software was designed using Labview (Labview 5.1, National Instruments, Austin, TX, USA).

**Synthesis, application, and observation of CeO$_2$ and SiO$_2$ NPs**

NPs were synthesized by an aerosol spray pyrolysis unit used for the synthesis of tailor-made NPs. In aerosol spray pyrolysis, a precursor solution is atomized into fine droplets, which undergo evaporation of solvent and gradual precipitation of the precursor as they pass through a tubular heated reactor. A quartz fiber filter at the exit of the reactor collects the synthesized particles. The precursor solution for the CeO$_2$ particles was an aqueous 6 M solution of CeCl$_3$·7H$_2$O (ACROS Organics, New Jersey, NJ, USA). The synthesis temperature of the tubular reactor was 500°C, and the gas flow rate was 7 L/min, while the collected particles were calcined at 700°C for 2 hours. The particles were
characterized by transmission electron microscopy (TEM, JEOL JEM 2010; JEOL USA, Inc, Peabody, MA, USA) for their morphology, which was spherical and dense with a diameter size distribution from 110 to 250 nm. Their structure was polycrystalline.

SiO$_2$ particles were synthesized from a precursor solution of TEOS (Fluka)/EtOH/H$_2$O in molar ratios of 1/9.9/63.3. The synthesis temperature was 500°C in 7 L/min flow rate, while the particles were calcined at 550°C/4 hours. The SiO$_2$ NPs were characterized by TEM (JEOL JEM 2010) for their morphology. The TEM image also depicts spherical dense particle morphology with diameter size distribution between 30 and 120 nm, while their crystallinity is amorphous.

In order to study the transport of CeO$_2$ and SiO$_2$ NPs in the axons of the peripheral nerve, the NPs were diluted in saline and placed in the stimulating chamber, where the proximal end of the nerve was immersed. Before application, the edge of the proximal part was cut again using sharp fine microscissors, and the cut end was exposed to double distilled water for 3 minutes in order to open the cut ends of the nerve fibers. The CeO$_2$ or SiO$_2$ NPs were supplied at the final concentration of an aqueous distilled water pH = 7 solution of 1.7 g/L concentration and were diluted eight times when applied in the stimulating chamber, where the proximal cut end of the nerve was placed (final concentration: 0.21 g/L). The particles were not charged by surface treatment in order to avoid particle movement by stimulation voltage. Under these conditions, the nerve was continuously stimulated. When the amplitude of CAP reached values below 20% of its original amplitude, usually after 36 hours, the experiment was terminated, the nerve was washed with distilled water and fixed using 20% glutaraldehyde for 12 hours.

For the observation with Fourier transform infrared (FTIR) microscopy, the fixed nerves were cut in three parts, the proximal, middle, and distal (Figure 1B), and dried in 100°C for 2 days in 100% ethanol for dropping it on the TEM carbon holder. The holder was left to dry under ambient conditions before loading it in the vacuum chamber.

Data analysis – statistics
As an indication of the proper physiological function of the nerve fibers of the isolated sciatic nerve, samples of the evoked CAP were digitized and stored in a computer every 30 minutes throughout the experiment, usually lasting over 36 hours. The amplitude of the CAP was measured from baseline to peak and expressed as a percentage of the amplitude of the CAP after 1 hour equilibration of the nerve. The percentage values were expressed as mean and standard error mean. The outcomes of many trials using different nerves were averaged and plotted against time as the vitality curve, or the time–response curve. For the eight experiments in which the nerves were exposed to CeO$_2$, the values of the CAP, measured every 30 minutes, were expressed as means and standard error mean and were used to plot the time–response curve. When required, data were analyzed by one-way analysis of variance (ANOVA) and Bonferroni’s post hoc tests. We determined significance using Student’s $t$-test or ANOVA, as appropriate ($P<0.05$).

Chemicals
We purchased KCl, NaCl, and MgCl$_2$ from Panreac (Barcelona, Spain), HEPES from BiochemicaFluka (Fluka, Switzerland), glucose from Riedel-de Haen (Seelze, Germany) and NaHCO$_3$ from Merck (Darmstadt, Germany), and CeCl$_3$.7H$_2$O from ACROS Organics.

Results
The nerve preparation
In normal solution, CAP amplitude remained constant for nearly 12 hours and then gradually declined (Figure 1C). The gradual decrease in amplitude is due to an accumulating number of axons losing the ability to conduct action potentials over time. On average, CAPs reached 20% of their initial amplitude in 36 hours (n=6) as shown in the vitality curve, in Figure 1D (filled squares). For NP mobility evaluation, the stimulating bath with the proximal nerve was filled with physiological solution with CeO$_2$ NPs at a concentration of 0.21 g/L. To exclude the possibility of any toxic effects of CeO$_2$ NPs on the exposed part of the nerves, the vitality curve for the particular case was plotted (Figure 1D, open squares). This curve (n=8) displayed similar characteristics with the control, and no statistically significant difference was seen ($P>0.05$), although a small protective trend can be observed for CeO$_2$. This is an indication that at the relatively
small concentrations used in our study (0.21 g/L), there is no toxic effect on the proximal part of the nerve.

**CeO$_2$ NPs translocate in the sciatic nerve fibers**

In this study, eight nerves were exposed to CeO$_2$ NPs and screen scanned using the FTIR microscope, as described. The FTIR absorption spectrums of a nonexposed nerve and of the pure CeO$_2$ NPs were used as negative and positive controls, respectively. No traces of CeO$_2$ NPs were detected in the untreated nerves.

In six out of eight treated nerves, CeO$_2$ NPs translocated within the nerves. CeO$_2$ was observed mainly in the middle and distal regions of the nerve. In all six nerves, no NPs were observed in the proximal region. In the other two nerves, there was no transport. In Figure 2, exemplary FTIR traces are shown from such an experiment. The bottom trace is the negative control (control nerve, free of NPs) and the trace at the top (CeO$_2$ NPs) the positive. CeO$_2$ NPs presence is indicated with arrows. The nerve was screened scanned every 1 mm. The middle FTIR trace (Figure 2, no CeO$_2$) is indicative of the proximal, distal, and of the first 13 mm of the middle part, where no NPs were detected, (compare traces marked with no CeO$_2$ and CeO$_2$). It is worth mentioning that the absorption spectrum indicating the presence of CeO$_2$ NPs appeared only in a short region as a bundle at the middle part of the nerve (insert at the right of Figure 2). In this particular case, NPs were located between 14 and 15 mm of the middle part (according to Figure 1B). The difference in size of the CeO$_2$ characteristic peak at 600–800 cm$^{-1}$ indicates that at 14 mm (low CeO$_2$, trace), the concentration of CeO$_2$ NPs is lower than at 15 mm (high CeO$_2$ trace). Although the exact terminal positioning of the NPs differed among the six nerves examined between 14 and 20 mm, a constant observation was that CeO$_2$ NPs tended to cluster and travel together as a bundle.

Another less typical set of recordings is demonstrated in Figure 3, where it seems that NPs reached the beginning of the distal region (1–2 m, according to Figure 1B), far from their usual position at the 15–20 mm region of the middle part, while a bundle of NPs is also located at the far distal part (at 4–5 mm).

All the aforementioned experiments were terminated when the CAP reached a value of 20% of its initial value in 36–40 hours, and the nerves were fixed eliminating any further translocation. Thus, the appearance of NPs at the far end of the middle part allowed us an approximate estimation of the speed of their movement inside the nerve fibers. Our results indicate an average NPs translocation speed of 0.45–0.58 mm/h.

**CeO$_2$ NPs translocate through the nerve fibers exclusively**

In order to verify that NPs were translocated only through the axons and not along the other elements of the sciatic nerve, such as the epineurium (perineural sheath), perineurium, and endoneurium, the nerve fibers were damaged by applying a slight pressure on the nerve using the tip of a fine forceps. The pressure was enough to damage the nerve fibers since the transmission of the electrically generated CAP along the sciatic nerve was completely eliminated; a CAP was never recorded from the four nerves tested even after 40 hours of continuous recordings. Care was taken so the lesion was enough to damage the nerve fibers, but not enough to cause any damage on the structures surrounding and protecting the nerve fibers. No CeO$_2$ NPs translocation was observed in all four damaged nerves tested.

To ensure that NPs enter the nerve fibers only from their cut end, the middle part of the nerve incubated in the middle

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*Figure 2* FTIR traces from different regions of CeO$_2$-treated sciatic nerve of the frog.  
**Notes:** Arrows indicate CeO$_2$ presence compared to control (CeO$_2$ NP). Peaks approximately 1,640 cm$^{-1}$ are attributed to the $\nu_2$ band of the hydrogen bond of water.  
**Abbreviations:** FTIR, Fourier transform infrared microscopy; NP, nanoparticle.

*Figure 3* FTIR traces from different regions of CeO$_2$-treated sciatic nerve of the frog.  
**Notes:** Arrows indicate CeO$_2$ presence compared to control (CeO$_2$ NP). Peaks approximately 1,640 cm$^{-1}$ are attributed to the $\nu_2$ band of the hydrogen bond of water.  
**Abbreviations:** FTIR, Fourier transform infrared microscopy; NP, nanoparticle.
chamber was exposed to 0.21 g/L CeO$_2$, while recordings were made for over 40 hours. NPs were found in none of the three nerves examined.

**CeO$_2$ translocation depends on nerve fiber electrical activity**

To demonstrate the relation between nerve fiber electrical activity and NPs translocation, we used another simple method. Four nerves were treated using CeO$_2$, as already described, but in the absence of electrical stimulation. In this case, the transportation of NPs was minimized. In two out of four cases, few traces of CeO$_2$ were detected only in the proximal region. In all four nerves, no NPs were detected in either the middle or the distal region. The results of these experiments provide a clear indication that the translocation of NPs depends not only on the integrity of the nerve axons, but also on their electrical activation.

**SiO$_2$ also translocates within the peripheral nerve**

In this study, four nerves were exposed to SiO$_2$ NPs, as already described. In three out of four nerves exposed to SiO$_2$, traces of NPs were observed in very narrow bundles of 2–3 mm of the distal region of the sciatic nerve, in accordance to the observation for CeO$_2$.

In Figure 4, the FTIR traces of a nonexposed nerve (control nerve) and of the SiO$_2$ NPs are shown as negative and positive controls, respectively. No NPs were detected in the middle and distal parts of the nerve. However, in the distal part, 5 mm before the end of the nerve, an area with high SiO$_2$ presence was detected (trace high SiO$_2$) following a low one (trace low SiO$_2$). Prior to this region, and similar to the other areas of the nerve, NPs were not detected (trace no SiO$_2$).

To provide convincing evidence that our FTIR signal was generated by SiO$_2$ NPs, parts of the nerve with strong signal were examined using TEM. A SiO$_2$ NP from these studies is shown in Figure 5. The TEM images depict spherical dense particle morphology with diameter size distribution between 30 and 120 nm and amorphous crystallinity, all concordant with SiO$_2$ presence.

**Discussion**

NPs are widely investigated as drug delivery vehicles in nanomedicine. We investigated the translocation ability of two commonly used NPs, namely CeO$_2$ and SiO$_2$, in a model peripheral nerve, the ex vivo preparation of the frog sciatic nerve. Our results indicate that CeO$_2$ and SiO$_2$ NPs, with a mean diameter of 120 and 140 nm respectively, translocate along the nerve fibers with an average speed of 0.45–0.58 mm/h. This speed is closer to the slow axonal transport rate (0.072 mm/h) than the fast one (8–10 mm/h). A similar transportation rate, of 1.9 mm/h, has been reported for the Herpes simplex virus-1 in the same preparation. It is possible is that the same transport mechanism is involved in both cases. The relatively large size of CeO$_2$ and SiO$_2$ may explain the slower speed compared to the virus.

A key observation of our study has been the detection of a narrow band in the FTIR spectrum, indicating the presence of NP aggregates usually within one of the 1 mm segments in the distal or middle regions of the nerve. The absence of NPs, as characterized by FTIR, can also be defined as low NP quantity in other regions. FTIR spectroscopy characterizes a sample by the absorption peaks of its asymmetric molecular vibrations. The nerve sample exhibits its characteristic control FTIR spectrum, while on the other hand in the NPs case, the collective spectrum of the control and the NPs incorporated in the nerve matrix is presented; thus, the resolution capability for NP presence is limited to

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**Figure 4** FTIR traces of different SiO$_2$ treated nerve regions.  
**Notes:** Arrows indicate SiO$_2$ presence. Peaks approximately 1,640 cm$^{-1}$ are attributed to the $\nu_2$ band of the hydrogen bond of water.  
**Abbreviations:** FTIR, Fourier transform infrared microscopy; NP, nanoparticle.
NP quantities that can distinct from the control background. There may be at least two explanations for the narrow band formation. One possibility is that the anterograde transport mechanism requires an aggregate, in other words a “critical NP mass”, to operate. If this hypothesis is true, NPs should be present, but below the detection threshold in the proximal segment, absent until the detection site, and the aggregation rate should be slow enough to allow a second, observable band within our 36-hour protocol. Another possibility is that there is a block at the site where the band is detected, and translocated NPs merely aggregate at that point. In this case, NPs should be present, at concentrations below detection, along the length of the nerve up to the detection site. Time and concentration dependence experiments will help to shed light on this interesting phenomenon.

The route of NPs translocation has also been investigated in our study. NPs are transported through the axon and not by other structures of the nerve as the damaged axon experiments have demonstrated. Evidence toward this conclusion has been also provided by the results of the experiments where the whole middle part of the desheathed nerve was exposed to 0.21 g/L CeO₂ with no observed penetration or transportation through either myelin or nodes of Ranvier. The same experiment also demonstrated that the application of NPs at this concentration has no toxic effect on the nerve at the concentration. In other in vitro studies, it has been shown that the number of NPs impacts cytotoxicity.⁵⁹

We have also demonstrated that electrical activation is required for effective transportation. In similar ex vivo frog sciatic nerve experiments, repetitive action potentials have been shown to retard mitochondrial motility through nodes of Ranvier by reducing the number of mobile mitochondria, reducing the velocity, and increasing the pause duration in a Ca²⁺-dependent manner.³⁵ Apparently, NP translocation depends on a different mechanism which is facilitated by electrical activation. Further studies are required to investigate this interesting phenomenon.

Our ex vivo nerve preparation constitutes a valuable tool for studying a number of important questions regarding axonal transportation of NPs. The study can be easily extended to other types of NPs, and it can also be used to investigate the relation of NPs size with speed of axonal transport and further to estimate the optimum diameter for maximum speed. The size is an important issue because it may determine the transportation rate of the maximum load. Our methodology is also a useful tool for the pharmacological study of various parameters, eg, drugs diluted in the perfusion chamber, ionizing radiation, and temperature, which may affect the axonal transport of NPs. Furthermore, an investigation is in preparation to assess the movement of NPs in the nerve fibers of mammals, and more specifically in rats. Results from mammalian tissues will provide mechanism insights closer to the human conditions.

Conclusion
Using an ex vivo preparation of the frog sciatic nerve, we have demonstrated that two commonly used NPs, CeO₂ and SiO₂, are transported through the nerve with a speed in the range of the slow transportation rate. The movement depends on axonal integrity and electrical activity. No neurotoxic effects were shown for the CeO₂ concentration tested even after long hours of exposure. Our preparation is advantageous for studying various aspects of axonal transportation of NPs.

Disclosure
The authors report no conflicts of interest in this work.

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