Controllable drug uptake and nongenomic response through estrogen-anchored cyclodextrin drug complex

Abstract: Breast cancer is a leading killer of women worldwide. Cyclodextrin-based estrogen receptor-targeting drug-delivery systems represent a promising direction in cancer therapy but have rarely been investigated. To seek new targeting therapies for membrane estrogen receptor-positive breast cancer, an estrogen-anchored cyclodextrin encapsulating a doxorubicin derivative Ada-DOX (CDE₁-Ada-DOX) has been synthesized and evaluated in human breast cancer MCF-7 cells. First, we synthesized estrone-conjugated cyclodextrin (CDE₁), which formed the complex CDE₁-Ada-DOX via molecular recognition with the derivative adamantane-doxorubicin (Ada-DOX) (Kd=1.617 M⁻¹). The structure of the targeting vector CDE₁ was fully characterized using ¹H- and ¹³C-nuclear magnetic resonance, mass spectrometry, and electron microscopy. CDE₁-Ada-DOX showed two-phase drug-release kinetics with much slower release than Ada-DOX. The fluorescence polarization analysis reveals that CDE₁-Ada-DOX binds to recombinant human estrogen receptor α fragments with a Kd of 0.027 µM. Competition assay of the drug complex with estrogen ligands demonstrated that estrone and tamoxifen competed with CDE₁-Ada-DOX for membrane estrogen receptor binding in MCF-7 cells. Intermolecular self-assembly of CDE₁ molecules were observed, showing tail-in-bucket and wire-like structures confirmed by transmission electronic microscopy. CDE₁-Ada-DOX had an unexpected lower drug uptake (when the host–guest ratio was >1) than non-targeting drugs in MCF-7 cells due to enсlosed ligands in cyclodextrins cavities resulting from the intermolecular self-assembly. The uptake of CDE₁-Ada-DOX was significantly increased when the host–guest ratio was adjusted to be less than half at the concentration of CDE₁ over 5 µM due to the release of the estrone residues. CDE₁ elicited rapid activation of mitogen-activated protein kinases (p44/42 MAPK, Erk1/2) in minutes through phosphorylation of Thr202/Tyr204 in MCF-7 cells. These results demonstrate a targeted therapeutics delivery of CDE₁-Ada-DOX to breast cancer cells in a controlled manner and that the drug vector CDE₁ can potentially be employed as a molecular tool to differentiate nongenomic from genomic mechanism.

Keywords: breast cancer, drug vector, functionalized, membrane estrogen receptor, polysaccharide, targeted drug delivery

Introduction

The targeted drug-delivery systems formed through various types of intermolecular forces have attracted great interest because of their therapeutic potential in drug development and cancer treatment.² Many elegant drug-delivery systems based on such non-bonding host–guest interactions have been developed.³–⁶ Cyclodextrins (CDs) are among the best nonimmunogenic vector candidates for self-assembly of targeted drug-delivery systems³ due to their unique hydrophobic hollow-cavity-containing structure, excellent biocompatibility, chemical modifiability of hydroxyl groups in the primary face, and strong ability to entrap drug molecules through molecular

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This article was published in the following Dove Press journal:
International Journal of Nanomedicine
27 July 2015
Number of times this article has been viewed

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DOI: http://dx.doi.org/10.2147/IJN.S82255

Running head recto: Estrogen-anchored cyclodextrin drug complex

Running head verso: Yin et al

Year: 2015
Journal name: International Journal of Nanomedicine

International Journal of Nanomedicine 2015:10 4717–4730

4717

Open Access Full Text Article

ORIGINAL RESEARCH

International Journal of Nanomedicine downloaded from https://www.dovepress.com/ by 54.70.40.11 on 28-Dec-2018
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Ligand-attached CDs facilitate drug delivery to tumor cells that often express abundant target receptors on the tumor cell membrane. For example, multivalent CD-based glyoclusters specifically target clinically relevant sugar receptors; recently synthesized series of drug complexes based on CDs functionalized with folic acid, arginylglycylaspartic acid (RGD tripeptide), and hyaluronic acid, in which hydrophobic therapeutics were entrapped, have been found to possess higher targeting efficiency and better drug affinity to target receptor-positive cancer cells (data from arginylglycylaspartic acid- and hyaluronic acid-conjugated CDs are unpublished).

Ligand-attached CDs represent promising multimodal drug-delivery vectors.

However, CD-based estrogen-anchored therapeutic delivery systems have never been investigated, even though estrogens are crucial in the initiation, development, and progression of human breast cancer. Overexpression of estrogen receptors (ERs) is observed in approximately 70% of human breast cancers. In addition to residing in the nucleus (“nuclear ERs” [nERs], ie, ERα and ERβ), ERs can also reside on the membrane and endoplasmic reticulum (so-called “membrane ERs” [mERs]).

Targeting the overexpressed mERs for the delivery of therapeutics represents a promising and effectual strategy for breast cancer therapy. In addition, the estrogen-conjugated CD vector is expected to preserve and elicit the estrogen response and act as a new antiestrogen for additional adjuvant endocrine treatments of ER-dependent breast cancer via targeting the ER-dependent pathways besides the targeting drug-delivery modality.

Herein, we report an mER targeting estrone (E1)-conjugated CD vector CDE1 and prepared drug-delivery complex CDE1-Ada-DOX (Figure 1A) through molecular recognition of a doxorubicin derivative adamantane-doxorubicin (Ada-DOX) and CDE1. In this system, E1 was first conjugated to CDs (CDE1) to vectorize the encapsulated drug Ada-DOX which comprises an adamantane (Ada) molecule covalently linked to doxorubicin. The molecular moiety of adamantine

Figure 1 Schematic of estrone targeting vector based on cyclodextrin.

Notes: (A) The chemical structure of the CDE1-Ada-DOX inclusion complex. (B) Reaction scheme for the synthesis of ligand-attached cyclodextrin vectors (CDEi and CDPg), intermediates (CDOTs, CDN1), and mER-targeting supramolecule CDE1-Ada-DOX. (a) Dissolve β-CD in H2O at the presence of NaOH (3eq) followed by adding acetonitrile solution of p-TsCl (1eq), react for 6 hours at rt. (b) (1) Neutralized by adding 2 eq of HCl, followed by recrystallization with cold acetone; (2) React in NH3·H2O for 3–7 days at 70°C. (c) (1) React in pyridine (or DMF) for 48 hours with ligand (2) excess NaBH4 in methanol solution. (d) React in anhydrous CH2Cl2 at presence of Et3N and N2 overnight at rt. (e) Molecular recognition with CDEi or CDPg. L* interpreted as: ligand as estrone (E1); progesterone (Pg). The CDE1-Ada-DOX inclusion complex is a supramolecule generated through hydrophobic interaction and molecular recognition.

Abbreviations: CDE1, estrone-conjugated cyclodextrin; CDN1, mono-6-deoxy-6-aminocyclodextrin; CDOTs, mono-6-deoxy-6-(p-tolysulfonyl)-b-cyclodextrin; CDPg, progesterone-conjugated cyclodextrin; mER, membrane estrogen receptor; Ada-DOX, adamantane-doxorubicin; rt, room temperature.
forms stable drug inclusion with CDs with high affinity and low cytotoxicity.\textsuperscript{23,24} The drug uptake of CDE\textsubscript{1}\textendashAda-DOX and non-targeting CD-Ada-DOX have been examined in time course altered with host\textendash;guest ratios; notably, the drug release and uptake of Ada-DOX from CDE\textsubscript{1}\textendashAda-DOX in MCF-7 cells was in a controllable manner due to the unique intermolecular self-assembly of and the resulting stealth or release of the E\textsubscript{1} residues in CDE\textsubscript{1}. Finally, we investigated whether the synthesized “estrogen-like” CDE\textsubscript{1} could activate nonclassical rapid response through activated ER-mediated pathway in MCF-7 cells, and the potential application in differentiation of genomic and nongenomic pathways.\textsuperscript{25–27}

**Methods**

For chemical synthesis, characterization, drug release, TEM microscopy, drug uptake, and Western blot, see Supplementary materials.

**Binding affinity of CDE\textsubscript{1} with Ada-DOX in aqueous solution determined using the fluorescence titration method**

We next determined how strong the host molecule CDE\textsubscript{1} interacted with the guest molecule Ada-DOX using the fluorescence titration method as described previously.\textsuperscript{29} The effect of varying CDE\textsubscript{1} concentrations on the fluorescence intensity of Ada-DOX was examined in order to determine the association constant ($K_d$) between CDE\textsubscript{1} and Ada-DOX. The concentration of Ada-DOX was set at 50 \(\mu\text{M}\) in the presence of CDE\textsubscript{1} at escalating concentrations of 0, 0.17, 0.26, 0.35, 0.44, 0.53, 0.62, 0.71, 0.79, and 0.88 \(\mu\text{M}\), and the fluorescence intensity was monitored using a Synergy\textsuperscript{TM} H4 Hybrid Microplate Reader (BioTek Inc., Winooski, VT, USA). The solvent used was dimethylformamide:H\textsubscript{2}O (50/50, v/v). The fluorescence of Ada-DOX was measured with \(\lambda_\text{ex}=490\text{ nm}\) and \(\lambda_\text{em}\) ranging from 500 to 700 nm with an escalating step of 2 nm. The $K_d$ value was calculated using the above-mentioned approach by nonlinear fitting for various models.

**Effects of the phosphorylation of p44/42 mitogen-activated protein kinase (Erk1/2) at Thr202/Tyr204 in MCF-7 cells**

To examine whether CDE\textsubscript{1} elicited nongenomic events in MCF-7 cells, the cells were treated with CDE\textsubscript{1} or other drugs at 1 \(\mu\text{M}\) for 5, 10, 15, 30, and 60 minutes to detect p44/42 mitogen-activated protein kinase (MAPK) (Erk1/2) phosphorylation at Thr202/Tyr204 using Western blotting analysis in MCF-7 cells. The experiments were repeated in triplicate.

**Binding determination of the CDE\textsubscript{1}\textendashAda-DOX inclusion complex to recombinant human ER\textalpha\ fragments using the fluorescence polarization method**

Fluorescence polarization (also called fluorescence anisotropy) is a versatile solution-based technique that has been widely used to investigate molecular interactions (eg, ligand\textendash;receptor binding), enzymatic activity, and nucleic acid hybridization.\textsuperscript{48} Quantitatively, fluorescence polarization (mP) is defined as the difference of the emission light intensity parallel and perpendicular to the excitation light plane normalized by the total fluorescence emission intensity. The binding of the CDE\textsubscript{1}\textendashAda-DOX inclusion complex to recombinant human ER\textalpha\ fragments consisting of amino acid residues 1–116 at the C-terminus (His tag C-terminus, Molecular Mass =12,200 Da) (catalogue number: ab153776; Abcam Plc, Cambridge, UK) was investigated using the fluorescence polarization method as described previously.\textsuperscript{31} Briefly, human ER\textalpha\ fragments were reconstituted in phosphate-buffered saline to the final concentration of 0.8 \(\mu\text{M}\), and CDE\textsubscript{1}\textendashAda-DOX complex samples at concentrations from 0.04 \(\mu\text{M}\) to 1.26 \(\mu\text{M}\) were added to the protein solution. The samples were mixed well at room temperature and subject to analysis immediately. mP was measured using the Synergy H4 Hybrid Multi-Mode Microplate reader at \(\lambda_\text{ex}=485/20\text{ nm}\) and \(\lambda_\text{em}=620/10\text{ nm}\) with xenon flash as the light source. The acquisition parameters were set as follows: 200 flashes and positioning delay 100 msec. The experiment was repeated in triplicate. The mP values were plotted against an increasing concentration of CDE\textsubscript{1}\textendashAda-DOX and the equilibrium binding constant ($K_d$) was calculated using nonlinear least squares that fit the curve data by Prism 6.03 program (GraphPad Software, Inc., La Jolla, CA, USA).

**Results and discussion**

In this study, E\textsubscript{1} was successfully conjugated with \(\beta\)-CD to generate CDE\textsubscript{1} as a new drug vector to target mERs of breast cancer cells. At the same time, progesterone, having a similar structure to E\textsubscript{1}, was also conjugated to CDs as the substrate extension of the conjugation reaction (Figure 1B). CDE\textsubscript{1} accommodates the hydrophobic Ada-DOX through host\textendash;guest interactions to form the CDE\textsubscript{1}\textendashAda-DOX supramolecule for drug delivery since the geometry and hydrophobicity of the adamantyl group allows an excellent fit into the CD’s torus inner cavity. The structures of the synthetic compounds have been confirmed using multiple spectral methods which include \(\textsuperscript{1}H\) nuclear magnetic resonance, \(\textsuperscript{13}C\) nuclear magnetic resonance, high-resolution...
matrix-assisted laser desorption/ionization-time of flight mass spectroscopy, fluorescence spectroscopy, and circular dichroism spectroscopy (Figure 2). The 1:1 stoichiometric inclusion complex CDE\textsubscript{1}-Ada-DOX was readily prepared by the coprecipitation method through molecular recognition.

The host–guest binding affinity of CDE\textsubscript{1} with Ada-DOX ($K_d$) was measured using the fluorescence titration method as described previously.\textsuperscript{29} With an increasing amount of CDE\textsubscript{1} added to the dimethylformamide and H\textsubscript{2}O (1:1) solution containing Ada-DOX, the fluorescence intensity was measured at varying emission wavelengths from 500 to 700 nm with 600 nm as the maximum peak, which decreased in a concentration-dependent manner (Figure 2C). The $K_d$ values were calculated using the fluorescence intensity versus CDE\textsubscript{1} concentration curve. This data showed that the one-phase and two-phase exponential decay models were the best fit. The calculated $K_d$ was 0.93, 1.09, 0.77, and 0.73 mM when the emission wavelengths were 550, 574, 600, and 634 nm, respectively. The fluorescence quenching effect during the titration of CDE\textsubscript{1} to Ada-DOX indicated that host–guest binding occurs.

Moreover, we examined the releasing kinetics of Ada-DOX from the CDE\textsubscript{1}-Ada-DOX inclusion complex in phosphate-buffered saline against 50% fetal bovine serum solution using a validated fluorescence method.\textsuperscript{31} The release kinetics of Ada-DOX and CDE\textsubscript{1}-Ada-DOX from the formulations clearly demonstrated that the drug released from CDE\textsubscript{1}-Ada-DOX was significantly slower (>50%) than Ada-DOX within the incubation time period (Figure 3). Detachment of Ada-DOX from the CDE\textsubscript{1}-Ada-DOX inclusion complex showed sustained releasing kinetics. By fitting the released drug data versus time, the kinetic parameters were calculated. For Ada-DOX, the $K_{d_{1/2}}$ and $K_{d_{2/3}}$ were 1.04 and 0.015 hours\textsuperscript{-1}, with elimination half-life ($t_{1/2a}$) and $t_{1/2b}$ of 0.67 and 45.02 hours, respectively. For CDE\textsubscript{1}-Ada-DOX, the $K_{d_{1/2}}$ and $K_{d_{2/3}}$ were 0.02 and 0.02 hours\textsuperscript{-1}, with $t_{1/2a}$ and $t_{1/2b}$ of 35.40 and 35.30 hours, respectively. The accumulation and absolute released drug for Ada-DOX and CDE\textsubscript{1}-Ada-DOX were also compared using two-way analysis of variance. At 2 hours, the cumulated drug release was 6.5% and 20.5% for CDE\textsubscript{1}-Ada-DOX and Ada-DOX, respectively ($P>0.05$). At 4 hours, the values were almost unchanged (6.6% versus 23.5%, $P<0.05$). At 6 hours, the values were increased to 11.1% and 28.4%, respectively ($P<0.05$). At 21 hours, drug-release values were increased to 20.9% and 49.1%, respectively ($P<0.001$). The measured drug released was 46.1% for CDE\textsubscript{1}-Ada-DOX and 99.0% for Ada-DOX over 75 hours of dialysis ($P<0.001$). These data clearly show that the release of Ada-DOX from CDE\textsubscript{1}-Ada-DOX is sustained compared with Ada-DOX over 75 hours. The sustained release of Ada-DOX from the inclusion complex would facilitate continuous drug uptake and long-term proliferation inhibition of the cancer cells.

In addition to the sustained drug release of CDE\textsubscript{1}-Ada-DOX, it has been clearly demonstrated that anchored ligands in the drug-delivery systems providing specific drug–cell surface interactions are crucial in determining the ultimate drug internalization by cancer cells.\textsuperscript{8} The cellular uptake of the mER-targeting drug complex CDE\textsubscript{1}-Ada-DOX and non-targeting compound CD-Ada-DOX was investigated to check for the targeting efficiency; flow cytometric analysis was performed in MCF-7 cells by taking advantage of intrinsic fluorescence emission from Ada-DOX. MCF-7 cells were treated with CDE\textsubscript{1}-Ada-DOX and non-targeting drug CD-Ada-DOX at different host–guest molecular molar ratios and drug concentrations in time course (Figure 4). The control (MCF-7 cells with no drug treated) and CDE\textsubscript{1} itself did not elicit obvious fluorescence and showed very low levels of autofluorescence. The addition of CDE\textsubscript{1} at 1, 3, or 5 µM to the MCF-7 cells slightly increased the fluorescence. Interestingly, excess CDE\textsubscript{1} quenched the fluorescence intensity of Ada-DOX at 1 µM when formulated in ratios of 1:1, 1:3, and 1:5 (Ada-DOX:CDE\textsubscript{1}) with 12.5% and 27.2% decrease for 1:3 and 1:5, respectively, in comparison to 1:1 CDE\textsubscript{1}-Ada-DOX complex (Figure 4A). CDE\textsubscript{1}-Ada-DOX had an unexpected lower cellular uptake than non-targeting CD-Ada-DOX complex in MCF-7 cells at 1 µM with a 1:1 host–guest molar ratio (Figure 4B), while the uptake of CDE\textsubscript{1}-Ada-DOX was enhanced when the host–guest molecule molar ratio and total concentration were altered. The cells were exposed to different CD or CDE\textsubscript{1} inclusion complexes for 2, 4, and 6 hours, respectively, with host and guest molar ratio set at 1:1. The drug uptake in MCF-7 cells treated with CD-Ada-DOX with host–guest ratio of 1:1 (CD\textsubscript{1} concentration =1 µM) for 2, 4, and 6 hours was 3.34-, 3.55-, and 3.61-fold of that in cells treated with CDE\textsubscript{1}-Ada-DOX with host–guest ratio of 1:1 with CD\textsubscript{1} concentration at 1 µM, respectively ($P<0.001$). The internalization efficacy of the targeting complex CDE\textsubscript{1}-Ada-DOX rebounded greatly compared with the drug without ligand attached (CD-Ada-DOX) as the host–guest molecular molar ratio increased to 1:2 with CDE\textsubscript{1} concentration of 1 µM (Figure 4C). The drug uptake in MCF-7 cells treated with CD-Ada-DOX with host–guest ratio of 1:2 at 1 µM of CDE\textsubscript{1} for 2, 4, and 6 hours was 1.62-, 1.36-, and 1.57-fold of that in cells treated with CDE\textsubscript{1}-Ada-DOX with host–guest ratio of
Figure 2 Characterization of CDE.

Notes: (A) The 1H-NMR spectrum of CDE, (800 MHz, d4-DMSO, temperature = 298 K). (B) The HR-MALDI-TOF spectrum of CDE-Ada-DOX. (C) Fluorescence emission spectra of CDE-Ada-DOX (Coneq = 50 µM) in DMSO at different CDE concentrations of 0.17, 0.26, 0.35, 0.44, 0.53, 0.62, 0.71, 0.79, and 0.88 mM, with increasing step of 0.08 mM. (D) Circular dichroism spectra of CDE-Ada-DOX. Samples in fluorescence measurements are excited at λex = 485 nm.

*10^3 indicates the y-axis value needs to be multiplied by 1,000.

Abbreviations: CDE, estrone-conjugated cyclodextrin; DMSO, dimethyl sulfoxide; HR-MALDI-TOF, high-resolution matrix-assisted laser desorption/ionization-time of flight; NMR, nuclear magnetic resonance; Ada-Dox, adamantane-doxorubicin.
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The drug uptake of CDE

Ada-DOX exceeded that of CD-

Ada-DOX when the concentration of the guest drug was

continually raised. When the host–guest molecular ratio

was altered to 1:2 with a CDE

concentration of 5 μM, the drug uptake of MCF-7 cells treated with CDE

Ada-DOX was higher (69.9%) than cells treated with CD-Ada-DOX

(P<0.01) (Figure 4D and E). These results suggest that the

targeted CDE

Ada-DOX inclusion complex improved the

uptake of Ada-DOX in comparison to the non-targeted CD-

Ada-DOX inclusion complex when CDE

and Ada-DOX

were formulated in appropriate ratios and drug concentrations

to release ample E

ligands from CDE

With higher guest drug concentrations or altered host–

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eties from the complex CDE

Ada-DOX have been enhanced

through binding to the mERs and have consequently facil

tated the drug internalization process in a controlled manner.

These interesting findings led us to propose that estrogen

residues covalently bonded with the CD are stealthy under

certain circumstances. In order to further substantiate the

presence of stealthy ligands in CDE

and CDE

Ada-DOX, transmission electronic microscopy (TEM) and scanning

electronic microscopy (SEM) examinations were conducted.

Representative TEM and SEM images of CDE

and CDE

Ada-DOX are shown in Figure 5. The intermolecular assem

bly of CDE

exhibited a tail-in-bucket structure and wire-like

morphology for CDE

, which shows the conjugated estrogen

residing inside the CD cavity of the adjacent CDE

molecule.

Figure 5A–C illustrate the long, tangled, uniform CDE

wires. The estrogen residues in CDE

act as linkers of CDE

molecules due to intermolecular recognition. Figure 5D–F

show the TEM images of CDE

Ada-DOX under the same

experimental conditions as CDE

. CDE

Ada-DOX particles

showed an unorganized structure under the same prepara

tion conditions compared with the CDE

containing no drug

payload. The observation was consistent and reproducible

in the TEM/SEM examinations. These findings indicate that
Figure 4 Flow cytometric analysis of the drug uptake by MCF-7 cells after incubation with various drug formulations for 2–6 hours.

Notes: (A) The fluorescence intensity of various samples of CDE$_{1}$ and CDE$_{2}$-Ada-DOX with host–guest molar concentration ratio of 1:1, 3:1, and 5:1 at 1 µM of Ada-DOX in MCF-7 cells. The control is obtained by the autofluorescence from the MCF-7 cells without any drug exposure. (B–E) The drug uptake indicated as the fluorescence intensity of various samples of CDE$_{1}$-Ada-DOX and the non-targeting drug complex CDE$_{2}$-ADA-DOX with 1:1, 1:2, or 1:5 of host–guest molar concentration ratio in MCF-7 cells under CDE$_{1}$ concentration of 1 or 5 µM. Data are presented as the mean ± standard deviation from three independent experiments. **P<0.01; ***P<0.001. The fluorescence is tested with E$_{x}$ of 490 nm and E$_{m}$ of 600 nm.

Abbreviations: CD, cyclodextrin; CDE, estrone-conjugated cyclodextrin; Ctrl, control; h, hours; Ada-DOX, adamantane-doxorubicin.
the conjugated E1 residues of CDE1 were entrapped in the CD cavities of CDE1 in the absence of a guest molecule. Furthermore, when the guest molecule such as Ada-DOX was added into CDE1, the competition between exogenous and the intermolecular recognition with the CD cavity resulted in the consequent release of a certain amount of E1 residues, in turn disrupting intramolecular self-assembling, disassembling the wire-like and tail-in-bucket structure of CDE1. Moreover, circular dichroism analysis indicated that Ada-DOX interacted with CDE1 (Figure 2D) and caused conformational changes at the CD cavity binding site followed by chiral microenvironment changes for the whole

Figure 5 The TEM/SEM characterization of CDE, and CDE-Ada-DOX.

Notes: A solution of CDE, or CDE-Ada-DOX at 1.8 mM in water:dimethylformamide (1:1, v/v) was dried in vacuum oven at 35°C overnight and then subject to TEM/SEM analysis. (A and B) The TEM image of CDE, (magnification: ×10,000 for A, ×40,000 for B) shows the wire-like morphology for CDE, due to self-assembly. The estrogen residue in CDE, acts as the linker in intermolecular recognition. (C) The SEM image of CDE, (magnification: ×40,000) shows the long, tangled, and uniform CDE, wires resulting from self-assembly. (D–F) The TEM image of CDE-Ada-DOX (magnification: ×4,000 for D; ×10,000 for E; ×30,000 for F). (G) The structure of CDE-Ada-DOX. (H and I) Presumable structures of CDE, which do not exist. (J) The tail-in-bucket and wire-like structure of CDE, resulting from self-assembly, which were confirmed by TEM and SEM examinations.

Abbreviations: CDE, estrone-conjugated cyclodextrin; SEM, scanning electron microscope; TEM, transmission electron microscope; Ada-DOx, adamantane-doxorubicin.
drug complex supramolecule. The circular dichroism spectra provide supportive evidence for the morphology differences of CDE, and CDE$_1$-Ada-DOX complexes.

Herein, we consider that targeting mERs expressed on MCF-7 cells is an effective means of affecting the uptake of the drug complex into these cells since the drug complex is taken up by ER-mediated endocytosis. Our results showed that CDE$_1$ preserved the binding ability after E$_1$ conjugated to CD. More importantly, drug uptake can be augmented significantly if the estrogen molecules in the complex are released to ensure the estrogen residue tailed outside the CD cavity. The intermolecular recognition between the covalent attached estrogen residue of one CDE$_1$ and the CD cavity of another CDE$_1$ molecule results in the host–guest molar ratio-dependent difference in drug uptake since the targeting moiety has been entrapped, and in turn reduces or loses its affinity to mERs. When an appropriate guest molecule approaches the CDE$_1$, the estrogen residues are pushed out and released. The competition between complexation of the drug and intermolecular inclusion of the estrogen in the CD cavity leads to altered drug uptake. In other words, the equilibrium of the host–guest molecules and the complex is the critical factor for controlling and optimizing the release kinetics of the targeting and drug moieties, mER binding, drug uptake efficiency, dissimilarity, and biological responses.

Furthermore, the cholesterol levels have been monitored in both cancerous cells (MCF-7 and A549 cells) and normal cells (MCF-10A and T80 cells) to investigate cholesterol depletion of lipid rafts on the cell membrane after drug exposure of CDE$_1$ and the drug complexes, since CD derivatives have been reported to be able to extract cholesterol from bilayer membrane by the CDs cavity, and modulate the activity of multiple signaling pathways. Cholesterol and estrogens have structural similarity. It was shown that the cholesterol level was not significantly affected after CDE$_1$, treatment due to the preoccupation of the CD cavity by E$_1$ residues from the intramolecular self-assembly (Figure 6).

Therefore, the magnitude of drug binding and internalization in cancer cells could be modulated by disrupting the intramolecular self-assembly of CDE$_1$, and changing the drug exposure levels and composition (eg, host–guest molecular molar ratio) in a controllable manner based on our findings.

To confirm the binding ability of CDE$_1$-Ada-DOX to mERs in breast cancer cells, we performed the competition assay with CDE$_1$-Ada-DOX using E$_1$ and a selective ER modulator, tamoxifen, as the inhibitors in MCF-7 cells. The results are shown in Figure 7A. The flow cytometric analysis showed that E$_1$ at 5−50 µM inhibited CDE$_1$-Ada-DOX uptake in a concentration-dependent manner in MCF-7 cells. E$_1$ at 5, 10, and 50 µM diminished the uptake of CDE$_1$-Ada-DOX by 5.1%, 4.3%, and 8.3%, respectively, in MCF-7 cells ($P<0.001$). Furthermore, tamoxifen also concentration-dependently reduced the uptake of CDE$_1$-Ada-DOX in MCF-7 cells. Tamoxifen at 1, 5, and 10 µM inhibited the uptake of CDE$_1$-Ada-DOX by 7.0%, 20.5%, and 19.2%, respectively, in MCF-7 cells ($P<0.001$). The results demonstrate that both E$_1$ and tamoxifen competed with CDE$_1$-Ada-DOX for mER binding in MCF-7 cells in a concentration-dependent manner with higher competing potency for tamoxifen compared to E$_1$.

Binding to mERs on tumor cells by tamoxifen or E$_1$, prevented the entry of other ER ligands such as CDE$_1$-Ada-DOX targeting complex to the binding pocket. These findings provide further evidence that estrogen residues from CDE$_1$-Ada-DOX complex recognize and bind to mER/mERs on MCF-7 cells.

Additionally, we used a fragment of human ERα containing the ligand binding domain (recombinant human ERα fragments consisting of amino acid residues 1–116 at the C-terminus, His tag C-terminus, Mr =12,200 Da; Abcam Plc) to examine whether CDE$_1$-Ada-DOX could bind to it using the fluorescence polarization approach. The polarization (mP) data over the concentration of the CDE$_1$-Ada-DOX inclusion complex in the absence or presence of human ERα fragments at a fixed concentration of 0.08 µM are shown in Figure 7B–D. The mP values were increased when the concentration of the CDE$_1$-Ada-DOX inclusion complex was increased without adding the ERα fragments, with a $K_d$ of 0.018 µM.

When the CDE$_1$-Ada-DOX inclusion complex at escalating concentrations from 0.04 to 1.26 µM was mixed with human ERα fragments, the mP values were increased with a $K_d$ of 0.027 µM. These results demonstrate the interaction of CDE$_1$-Ada-DOX with human ERα fragments containing the ligand-binding domain.

In addition to the targeting drug-delivery modality of the novel “estrogen-like” molecule CDE$_1$, the cellular response triggered by CDE$_1$ in a manner different from the classical nER-mediated pathway was investigated by Western blotting assay (Figure 8). Estrogens bind to nuclear ERα and ERβ, triggering the classical pathway of estrogen-dependent action and finally eliciting remarkable genomic responses. The action of nuclear ERs includes binding lipophilic hormone molecule in cytoplasm, translocation of the ligand–ER complex to the nucleus, dimerization,
interaction with estrogen-specific response elements in the promoter areas of target genes, and finally initiating gene transcription.\(^{18,19,32}\) The effects of steroid hormone action dependent on ER occur within hours or even days. On the other hand, some ligands can elicit rapid nongenomic signaling cascades in a much shorter time (from seconds to minutes) upon estrogen binding.\(^{18,19,33,34}\) These rapid nongenomic effects of estrogens result in calcium mobilization, cyclic adenosine monophosphate stimulation, phospholipase C activation, inositol phosphate generation, and activation of membrane-associated signaling pathways, including protein kinase A, phosphotyidinositol-3 kinase, and MAPK (p44/42 MAPK, also called extracellular-signal-regulated kinase [Erk1/2]) signaling pathways.\(^{18,19}\) Importantly, crosstalk via second messengers between mER- and nER-initiated signaling responses can regulate transcriptional activation of multiple target genes in a coordinated manner.\(^{18,19}\) The estrogens E\(_{1}\) and E\(_{2}\), the selective ER modulator tamoxifen, and the synthetic estrogen 17\(\alpha\)-ethyl estradiol were used as positive control to trigger the rapid response of Erk1/2; adamantan and 1-adamantanol were used as structural fraction controls to the drug complex CDE\(_{1}\)-Ada-DOX. It was demonstrated that CDE\(_{1}\) resulted in rapid phosphorylation of p44/42 MAPK (p-Erk1/2) within 30 minutes in ER-positive cancerous cells such as MCF-7 cells, A549 cells, OVCAR3 cells, and even in the normal lung T80 cells.
while no significant response was observed in normal breast MCF-10A cells. Cells treated with CDE$_1$ at 1 µM showed a maximum p44/p42 MAPK phosphorylation at Thr202/Tyr204 at 15 minutes drug exposure and increases by 22.2%, 25.5%, and 59.2% at 30 minutes for MCF-7, A549 and OVCAR3 cells respectively, compared with controls ($P<0.05$). These results show that treatment of MCF-7 cells with CDE$_1$ activated the mER-mediated signaling pathway as indicated by the significantly increased phosphorylation of p44/42 MAPK (Erk1/2) rapidly within 5–30 minutes at Thr202/Tyr204 in MCF-7 cancer cells. Estrogens such as E$_2$ induce a number of rapid signaling events in cells that express mERs such as GPR30,$^{19,32}$ except in classical pathways.$^{18,39}$ Different stimuli including mitogens, growth factors, cytokines, virus infection, ligands for heterotrimeric G protein-coupled receptors, transforming agents, and carcinogens can activate the p44/42 MAPK (Erk1/2) pathway.$^{35-37}$ There is evidence that E$_2$-induced p44/42 MAPK (Erk1/2) activation requires GPR30, and occurs via transactivation of the epidermal growth factor receptor.$^{38,39}$ In the Raf–MEK–MAPK/Erk pathway, receptor tyrosine kinases and G protein-coupled receptors activate Ras, which in turn activates c-Raf.$^{35,37}$ Activation of c-Raf involves phosphorylation at multiple residues including Ser338, Tyr341 and Ser499. p21-activated protein kinase can phosphorylate c-Raf at Ser338 and the Src family phosphorylates Tyr341.
of c-Raf.\textsuperscript{35,37} Activated c-Raf activates MAPK kinase (called MKK, MEK, or MAP2K) at Ser217/221 located in the activation loop of subdomain VIII, and MEK1/2 activate p44 and p42 through phosphorylation of activation loop residues Thr202/Tyr204 and Thr185/Tyr187, respectively.\textsuperscript{37} p44/42 MAPK (Erk1/2) are negatively regulated by a family of dual-specificity (Thr/Tyr) MAPK phosphatases, along with MEK inhibitors such as U0126 and PD98059.\textsuperscript{40}

In this study, treatment of MCF-7 cells with the new synthetic CDE\textsubscript{1}, resulted in rapid phosphorylation of p44/42 MAPK (Erk1/2) in minutes. These findings suggest that CDE\textsubscript{1} can interact with and activate mERs and might be used as a probe for studying mER-mediated nongenomic events in comparison with nER-mediated genomic responses that involve DNA binding and gene expression initiation; it also needs a much longer time. It was demonstrated that adamantane and 1-adamantanol molecules do not affect p44/42 MAPK phosphorylation in tumor cells significantly, while upregulation of p-Erk1/2 from the drug complex CDE\textsubscript{1}-Ada-DOX results from CDE\textsubscript{1} and partially from the Ada-DOX since Ada-DOX treatment also cause slight pErk1/2 over-expression.

It is well known that estrogens activate the rapid, non-classical signaling cascades via mERs, and there is crosstalk between mER-mediated nonclassical and nER-mediated classical pathways.\textsuperscript{39,41,42} Deregulation of both pathways plays important roles in the pathogenesis of cancer and other diseases.\textsuperscript{41} It is recognized that selective ER ligands are needed to delineate the role of extranuclear and nuclear ERs in disease development and therapeutics where ERs represent important therapeutic targets. Several estrogen conjugates, including CD–E\textsubscript{2}, E\textsubscript{2}–BSA, E\textsubscript{2}–peroxidase, and E\textsubscript{2}–dendrimers, have been reported and used to probe the nonclassical and classical cascades.\textsuperscript{44–47} CD derivatives are generally considered cell-membrane impermeable. Therefore, CDE\textsubscript{1} can be employed as a molecular tool to differentiate nongenomic response from genomic response based on the findings.

**Conclusion**

We synthesized the novel estrogen-anchored conjugate CDE\textsubscript{1} and the corresponding drug inclusion with the doxorubicin derivative Ada-DOX (CDE\textsubscript{1}-Ada-DOX). The structures

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**Figure 8** Western blot analysis of CDE\textsubscript{1}-Ada-DOX and its analogs on A549, MCF-7, OVCA-3, T-80 and MCF-10A cells.

**Notes:** Western blot analysis shows the time course (0, 5, 10, 15, 30, and 60 minutes) of p44/42 MAPK (Erk1/2) phosphorylation at Thr202/Tyr204 by tamoxifen, Ada-DOX, 17α-ethinyl estradiol, CDE\textsubscript{1}-Ada-DOX, adamantane, E\textsubscript{2}, β-cyclodextrin, E\textsubscript{1}, and CDE\textsubscript{1} at 1 µM in MCF-7, A549, and OVCA cancerous cells (A); and in T-80 and MCF-10A human normal cells (B). In the experiments, Western immunoblotting was performed using rabbit antibodies against p-p44/42 MAPK (Erk1/2) at Thr202/Tyr204 and β-actin was used as the internal control. Data are from three independent experiments. Data are presented as the mean ± SD from three independent experiments.

**Abbreviations:** CDE\textsubscript{1}, estrone-conjugated cyclodextrin; E\textsubscript{1}, estrone; E\textsubscript{2}, estradiol; Ada-DOX, adamantane-doxorubicin.
of these new compounds were confirmed with rigorous spectral methods. A tail-in-bucket and wire-like structure of CDE$_1$ via intermolecular self-assembly was observed by TEM and SEM examination; in contrast, CDE$_2$-Ada-DOX exhibited unorganized structure due to disruption of self-assembly in the presence of guest molecules. The binding of $K_d$ between CDE$_1$ and Ada-DOX through hydrophobic interactions was determined to be 0.77 mM by fluorescence titration. CDE$_1$-Ada-DOX showed sustained and two-phase exponential drug-release kinetics over 75 hours. Notably, for the mER-targeted CDE$_1$-Ada-DOX inclusion complex, the critical factor for drug uptake efficiency in MCF-7 cells relied on the equilibrium between the host–guest and drug complex. By altering the ratios between the host and the guest molecules and the breakdown of the self-assembly nanostructure, CDE$_1$-Ada-DOX delivered the anticancer drug into MCF-7 cells in a controlled manner. E$_2$ and tamoxifen suppressed the drug uptake in MCF-7 cells treated with CDE$_1$-Ada-DOX through competition for mER binding. Moreover, CDE$_2$-Ada-DOX binds to recombinant human ER$_{α}$ fragments with a $K_d$ of 0.027 μM determined by fluorescence polarization. The treatment of MCF-7 cells with CDE$_2$-Ada-DOX elicited rapid activation of MAPKs (p44/42 MAPK, Erk1/2) in minutes through phosphorylation of Thr202/Tyr204. These results demonstrate a targeted delivery of the DOX derivative Ada-DOX to mER-positive breast cancer cells using CDE$_2$ as the drug carrier vectors in a controlled manner. The estrogen conjugates elicit nongenomic (but not genomic) events in MCF-7 cells. CDE$_1$ can be used as a powerful probe to explore the classical and nonclassical steroid-mediated pathways that are critical in the initiation, development, and progression of certain type of cancer (breast and ovarian cancer).

**Acknowledgments**

The authors are grateful for the support from the National Natural Science Foundation of China (Grant No 81372383), and the startup fund from College of Pharmacy, University of South Florida. This work has been supported in part by the Florida Center of Excellence for Drug Discovery and Innovation at the University of South Florida. The authors thank Dr S Karoly and Dr A Garces at the Lisa Muma Weitz Advanced Microscopy Core Laboratory for their support in data acquisition of flow cytometry and electronic microscopy. We also thank Dr R Sprunt at Moffitt Cancer Center for the MALDI-TOF mass spectroscopy.

**Disclosure**

The authors report no conflicts of interest in this work.

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