Magnetic localization and orientation of the capsule endoscope based on a random complex algorithm

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Abstract: The development of the capsule endoscope has made possible the examination of the whole gastrointestinal tract without much pain. However, there are still some important problems to be solved, among which, one important problem is the localization of the capsule. Currently, magnetic positioning technology is a suitable method for capsule localization, and this depends on a reliable system and algorithm. In this paper, based on the magnetic dipole model as well as magnetic sensor array, we propose nonlinear optimization algorithms using a random complex algorithm, applied to the optimization calculation for the nonlinear function of the dipole, to determine the three-dimensional position parameters and two-dimensional direction parameters. The stability and the antinoise ability of the algorithm is compared with the Levenberg–Marquart algorithm. The simulation and experiment results show that in terms of the error level of the initial guess of magnet location, the random complex algorithm is more accurate, more stable, and has a higher “denoise” capacity, with a larger range for initial guess values.

Keywords: wireless capsule endoscope, magnet, optimization

Introduction

With the development of science and technology, capsule endoscopy is becoming a preferred method for examination of the gastrointestinal tract, especially for the diagnosis of intestinal disease.1 The movement of the capsule in the gastrointestinal tract of human body depends on gastrointestinal peristalsis, so it is important for the doctor to acquire precise positioning information of the capsule to observe some specific areas of the tissues. Currently, a widely used positioning technique is the magnetic method, which detects the change of the magnetic intensity generated by a magnet attached to the capsule. The magnet signal are changes as a function of the static magnetic field and is not affected by the human body, so this positioning method can obtain high positioning accuracy. Also, it can directly determine the parameters for the position and direction of the capsule, for real-time location tracking. Based on the model of magnetic field positioning, researchers have proposed many positioning methods for the localization and orientation of the magnet.2–11 For instance, Golden and Silverstein have developed a medical tube that can be positioned in the body of patients. This medical tube can be located by a detection instrument, based on the magnetic intensity generated by the magnets inside the tube. The detection instrument moves around the body until the maximum magnetic intensity is detected, and then, the position of the magnet is calculated. However, this method cannot determine the direction of the magnet and has no real-time tracking system.2 Prakash and Spelman proposed a method for localizing a single magnetic dipole has been implemented in vitro using a magnetic marker. This uses
an eight fluxgate magnetic sensor to measure the magnetic intensity of the magnetic marker, where the Newton algorithm is applied as the positioning algorithm to calculate the position and direction of the target, but the positioning precision of this method is not very high. Yang et al used swarm intelligence algorithms, including genetic algorithms and particle swarm algorithms, to optimize the function of the magnetic positioning model. Their results showed that particle swarm optimization was more accurate to meet the requirement of localization. But for real-time tracking of the magnet, the algorithm is complex, and the speed of the algorithm did not meet the requirement for localization. Hu et al put forward a new localization algorithm. First, they used an improved linear algorithm to obtain the localization parameters, by finding the eigenvector corresponding to the minimum eigenvalue of the objective matrix. Then, these parameters were used as the initial guess values for the positioning parameters of a nonlinear location algorithm so that the algorithm had better robustness and more precise positioning results.

To find a more efficient algorithm, a hybrid algorithm combining different algorithms might be a suitable method to meet the need for high positioning precision and fast speed. Based on the magnetic dipole model, some nonlinear localization methods have been tested, such as Powell’s, Downhill Simplex, DIRECT, multilevel coordinate search, and the Levenberg–Marquardt (LM) algorithm. Hu et al concluded that the LM algorithm is better than other nonlinear algorithms. However, the LM algorithm easily gets into local optimality, so when the positioning range becomes larger, it has insufficient stability and antinoise ability. Therefore, we tested some hybrid methods and obtained better results. In this paper, we put forward a new nonlinear positioning algorithm based on the random complex method. In terms of accuracy and stability, for the three-dimensional position parameters and two-dimensional direction optimization calculation, the random complex algorithm (RCA) is superior to the LM algorithm and other algorithms because of its greater error level of the initial guess of magnet location and “denoising” capacity.

The organization of this paper is as follows: In the following section, we present a magnetic positioning system for the capsule endoscope. After this, we present the nonlinear magnetic positioning algorithm. Then, we present the performance and evaluation, followed by our conclusions.

**Magnetic positioning structure of the capsule endoscope**

As shown in Figure 1, the capsule endoscope has an enclosed thin, annular magnetic tube that builds the magnetic field and which does not take up very much of the internal space.

To detect the capsule endoscope in the body, a magnetic sensor array (Figure 2), which is situated outside of the human body, is designed to measure the magnetic field strength generated by the magnetic tube as the capsule moves inside the human body.

Obviously, the signal received by the magnetic field sensor array is related to the magnet tube position and direction with respect to the sensors. After sampling the sensor data, the position and direction parameters of the tube can be computed by the corresponding algorithm.

**Nonlinear magnetic positioning algorithm**

**Model description**

When a capsule moves in the gastrointestinal tract of human body, the position and direction of the capsule change. Therefore, we define a fixed coordinate system (as shown in Figure 3), and under the coordinate system, the magnet’s position is represented by \((a,b,c)^T\), and the magnet orientation is represented by \(H_0 = (m,n,p)^T\).

Assume that there are \(N\) sensors, with \(l\)th sensor located at \((x_l,y_l,z_l)^T\) (serial number \(l\), \(l=1, 2, \ldots, N\)). We denote three unit coordinate vectors as \(i, j, k\) corresponding to the axes...
Figure 3 Axial circular magnet (magnetic dipole) model.

Notes: (a, b, c) is the magnet position; (X, Y, Z) is a spatial point; H₀ is the normalized vector; Rᵢ is the distance between the magnet and the spatial point.

$x$, $y$, and $z$ respectively. The magnetic flux density at the $l$th sensor location can be represented by:

$$B_l = B_{i_l} + B_{j_l} + B_{k_l} = \frac{\mu_0}{4\pi} \left( \frac{3(H_0 \cdot P_l)P_l}{R_l^3} - \frac{H_0}{R_l^3} \right)$$

(1)

where $B_{i_l}$, $B_{j_l}$, and $B_{k_l}$ are the three orthogonal components of $B_l$; $N$ is the total number of sensors; $\mu_0$ is the relative permeability ($\mu_r = 1$ in the air); $\mu_0$ is the vacuum permeability ($\mu_r = 4\pi \times 10^{-7} T \cdot m/A$); $M_l$ is the constant (related to the volume and intensity of magnetization) that characterizes the magnetic field intensity of magnets; the vectors $P_l$ connecting the $l$th sensor and the magnet can be represented by $(x_i - a, y_j - b, z_k - c)^T$; and $R_l$ is the module of $P_l$, namely, $R_l = \sqrt{(x_i - a)^2 + (y_j - b)^2 + (z_k - c)^2}$.

The $H_0$ vector is characterizing the direction of the magnetic field of magnets, and we can add the constraints:

$$m^2 + n^2 + p^2 = 1$$

(2)

Expanding Equation 1, we have:

$$B_{i_l} = B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(x_i - a)}{R_l^5} - \frac{m}{R_l^3} \right\}$$

(3)

$$B_{j_l} = B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(y_j - b)}{R_l^5} - \frac{n}{R_l^3} \right\}$$

(4)

$$B_{k_l} = B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(z_k - c)}{R_l^5} - \frac{p}{R_l^3} \right\}$$

(5)

If we detect $B_{i_l}$, $B_{j_l}$, and $B_{k_l}$ ($l \geq 2$), by using Equations 2–5, the location parameter $(a, b, c)^T$ and direction parameter $(m, n, p)^T$ can be determined.

According to the magnetic positioning model, there are five unknown parameters that must be solved, and the number of sensors needs to be $N \geq 2$. But due to the presence of noise, the solution is not unique. We define a target error function (E) as follows:

$$E = E_x + E_y + E_z,$$

(6)

for which

$$E_x = \sum_{l=1}^{N} B_{i_l} - B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(x_i - a)}{R_l^5} - \frac{m}{R_l^3} \right\}^2$$

(7)

$$E_y = \sum_{l=1}^{N} B_{j_l} - B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(y_j - b)}{R_l^5} - \frac{n}{R_l^3} \right\}^2$$

(8)

and

$$E_z = \sum_{l=1}^{N} B_{k_l} - B_l \left\{ \frac{3(m(x_i - a) + n(y_j - b) + p(z_k - c))(z_k - c)}{R_l^5} - \frac{p}{R_l^3} \right\}^2$$

(9)

This is a nonlinear least squares problem, so the positioning problem becomes a nonlinear optimization problem. We find $(a, b, c)^T$ and $(m, n, p)^T$ to get the minimum error of the target through the optimization algorithm, namely:

$$\arg\min_{a,b,c,m,n,p} E_x + E_y + E_z \quad s.t. \quad m^2 + n^2 + p^2 = 1$$

(10)

In order to measure the effectiveness of the algorithm, positioning and orientation errors are defined as:

$$E_p = \sqrt{(a_i - a_j)^2 + (b_i - b_j)^2 + (c_i - c_j)^2}$$

(11)

and

$$E_o = \sqrt{(m_i - m_j)^2 + (n_i - n_j)^2 + (p_i - p_j)^2},$$

(12)

where $(a_i, b_i, c_i, m_i, n_i, p_i)$ and $(a_j, b_j, c_j, m_j, n_j, p_j)$ represent the setting and calculated parameters of the position and orientation.
Random complex algorithm

For the localization of the capsule endoscope, the accuracy and execution time are very important, and the nonlinear algorithm should be of high speed and precision. There are some widely used nonlinear algorithms, such as Powell’s, downhill, simplex, DIRECT, multilevel coordinate search, and the LM algorithm. We tried these algorithms and found some defects with the efficiency, so a nonlinear optimization algorithm, RCA, is introduced.

RCA was proposed by Andersson on the basis of the complex method.\(^\text{(13)}\) In this method, the complex is constituted in the constrained space; then the function values of the complex vertices are compared one by one so that the worst vertex will be replaced by a new vertex whose function values are improved and satisfy the constraints. Repeating this process, the result gradually approaches the most accurate one.

The step of computing the optimization of RCA is described in Figure 4.

Performance evaluation

In a real system, there will be noise due to the influences of the human body and the environmental factors. So the nonlinear optimization algorithms were tested for their ability to denoise and with the initial setting range of the positioning parameters. In this section, we compare RCA with the LM algorithm in terms of positioning error, direction error, and the execution time of the algorithm. Also, the effects of initial setting errors are used to test the stability of each RCA and LM algorithm.

Although it requires at least five sensors to solve a function for the five unknown positioning and orientation parameters, the greater the number of sensors, the higher is the positioning

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The random complex algorithm

Assume that the discussed issue is described as:

\[
\underset{x \text{ s.t. } g_i(x) \leq 0, \ i = 1, 2, \ldots, n}{\text{argmin }} f(x)
\]  

\[\text{(13)}\]

**Step 1** Randomly generate k vertices in the feasible region and set Genmax (the maximum number of iterations)

**Step 2** Determining the termination criterion.

If the number of iterations \( gen > genmax \), output \( x^* = x_g, f^* = f(x^*) \) and stop; otherwise, do Step 3

**Step 3** Obtain function values and coordinates of the best point and the worst point, and calculate the centroid point.

Obtain function values of k vertices and order these from small to large so as to obtain the best point, \( x_g \) and the worst point, \( x_\text{min} \), and calculate the centroid point \( x_0 \),

\[
f(x_g) = \max_{1 \leq m \leq k} \{f(x_m)\} \\
f(x_\text{min}) = \min_{1 \leq m \leq k} \{f(x_m)\}
\]  

\[\text{(14)}\]  

\[\text{(15)}\]

\[
x_0 = \frac{1}{k-1} \sum_{m=1, m \neq g}^{k} x_m
\]  

\[\text{(16)}\]
Step 4 Obtain the coordinate and function value of reflection point and for comparison with that of the worst point.

Calculate the centroid point \( x_c \) according to formula (16) and obtain the function value \( f' \)

\[
x_c = x_0 + \alpha(x_n - x_0)
\]  \( (17) \)

Generally, \( \alpha = 1.2 \) (\( \alpha \) is the reflection coefficient)

If \( x_{(j)} < \text{bounds} (1, j) \), \( \text{bounds} (1, j) \) replaces of \( x_{(j)} \)

If \( x_{(j)} > \text{bounds} (2, j) \), \( \text{bounds} (2, j) \) replaces of \( x_{(j)} \)

\( \text{gen} = \text{gen} + 1 \)

If \( f' < f(x_0) \), do Step 5; if \( f' \geq f(x_0) \), do Step 6

Step 5 The contraction phase

When the number of iterations is less than the maximum number of iterations, the reflection point is improved with the formula:

\[
x^{(\text{new})} = \frac{1}{2+\sum_{i=1}^{n} c_i} \left[ x^{(\text{old})} + c x = \frac{1}{2+\sum_{i=1}^{n} c_i} \left[ x^{(\text{old})} + c x_0 + (1-c)x_p \right)(1-c)(2R-1) \right]
\]  \( (18) \)

where \( c = \left( \frac{n_r}{n_r + k} \right)^{-1} \), \( k \), represents the contractive cycles when the contractive point as the worst point, \( n_r \) is a constant), \( R \) is a random number in \( [0,1] \).

If \( x_{(j)} < \text{bounds} (1, j) \), \( \text{bounds} (1, j) \) replaces of \( x_{(j)} \)

If \( x_{(j)} > \text{bounds} (2, j) \), \( \text{bounds} (2, j) \) replaces of \( x_{(j)} \)

\( \text{gen} = \text{gen} + 1 \)

Step 6 Coordinate and the function value of the worst point are replaced by the newly obtained point

Return to Step 2

**Figure 4** The calculation steps for the random complex algorithm (RCA).

accuracy. The simulation is based on the layout for 16 three-dimensional magnetic sensors evenly arranged on the 240 \( \times \) 240 mm square area X-Y plane, as shown in Figure 5.\(^3\)

In the simulation, the RCA and the LM algorithms are compared for algorithm characteristics, based on the nonlinear magnetic positioning model.

**Tolerance of the initial guess of the parameters and stability of the algorithm**

The nonlinear optimization algorithms usually require an initial guess of the parameters, or their bounds, to search for the optimal value. If the initial parameters (or bounds) are chosen with large error, the algorithms may fail to give the

**Figure 5** Arrangement of sensors.
correct (global optimization) solution because there might be many local optima. Therefore, the chosen optimization algorithm should have large tolerance for the initial guess of the parameters.

For all the test vectors, the vector \( \mathbf{v}_r = [-0.05, -0.00, 0.97, 0.00, -1.00, 0.00] \) is the most representative when the error levels of the initial location guess is 100 cm. The simulation results of RCA and the LM algorithm are shown in Figure 6.

For Figure 6, we observe that if the location error is 5 mm and direction error is 5%, the LM algorithm lapses when the initial guess of location is 15 cm, and RCA lapses when the initial guess of location is 36 cm.

For all the 32 test vectors, when the initial guess of localization is in the range of 10–100 cm, if the location error is 5 mm and direction error is 5%, the simulation results of the proportion of successful points of the RCA and the LM algorithm are shown in Figure 7.

The simulation results show that when the limit for the initial guess of localization is 10 cm for the RCA and the LM algorithm, all test points are successful. But when the limit for the initial guess of localization is extended to 30 cm, 37.5% of test points of the LM algorithm lapse, while the RCA can still successfully and accurately calculate the optimal position and direction. So the tolerance of the initial guess for RCA is higher than that for the LM algorithm. In Figure 9, with the increase in error level of the initial guess for magnet location, the proportion of successful points in the RCA and the LM algorithm will decrease, but the RCA is better than the LM algorithm. Thus, the stability of the RCA is better than that of the LM algorithm.

**Denoise capacity**

The algorithm and system implementation should be robust with regard to the noise in the sensor data. In a practical system, there is always some noise due to the influences of the human body and the environment. In this section, we present the simulation results for the denoising ability of the LM algorithm and RCA, and the results obtained by a real sensor array system with sixteen three-axis Hall effect sensor.

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**Figure 6** Position and orientation errors for the error levels of the initial guess of location.

**Abbreviation:** LM, Levenberg–Marquart.
For all the 32 test vectors, when the initial guess of localization is 10 cm, under different noise levels (0.1–1,000, where 1,000 is approximately 40% full sensing range) of random noises, the average and maximum localization and orientation errors of the LM algorithm and RCA are shown in Table 1.

According to Table 1, when the noise level is from 0.1 to 1,000, the RCA has smaller fluctuation, and the average value of localization and orientation error of the RCA is smaller than that of the LM algorithm.

For the real vectors $V_r=[0.0853, -0.0956, 0.0520, 0.9183, 0.3958, 0.0000]$ and $V_r=[-0.815, 0.070, 0.097, 0.2169, 0.9762, 0.0000]$, when the initial guess of localization is 10 cm and the noise level, $dl$, is in the range of 0 to 1,000, the simulation results of the RCA and the LM algorithm are shown in Figures 8 and 9.

### Table 1: The average and maximum of localization and orientation errors

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<th>Number</th>
<th>The average of localization error (mm)</th>
<th>The maximum of localization error (mm)</th>
<th>The average of orientation error (%)</th>
<th>The maximum of orientation error (%)</th>
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<td>RCA</td>
<td>LM algorithm</td>
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**Note:** The values with asterisks represent the better values of two algorithms.  
**Abbreviations:** RCA, random complex algorithm; LM, Levenberg–Marquardt.
Figure 8 Position and orientation errors via noise level; vector Vr1. Abbreviation: LM, Levenberg–Marquart.

Figure 9 Position and orientation errors via noise level; vector Vr2. Abbreviation: LM, Levenberg–Marquart.
From the simulation results, the average of the position error for the RCA is 0.76 mm, and the maximum value is 4.60 mm; the mean value of the orientation error is 2.22%, and the maximum value is 12.99%. The average of the position error for the LM algorithm is 592.59 mm, and the maximum value is 4.34×10^4 mm; the mean value of the orientation error is 9.75%, and the maximum value is 236.93%.

From the simulation results, the average of the position error for RCA is 4.91 mm, and the maximum value is 34.50 mm; the mean value of the orientation error is 7.32%, and the maximum value is 33.74%. The average of the position error for the LM algorithm is 11.82 mm, and the maximum value is 55.92 mm; the mean value of the orientation error is 23.09%, and the maximum value is 168.41%.

From the above figure, when the noise level dl ranges from 0 to 1,000, the condition of failure may occur for the LM algorithm but does not happen for the RCA; comparing with the LM algorithm, the noise immunity of the RCA is stronger.

**Real experiment and comparison with testing results**

We built an actual experimental system, which consists of magnetic sensors, amplifiers, an analog-to-digital (A/D) converter, and a computer. The 16 magnetic sensors (Figure 7) are made of three-axis Hall sensors. In the system, the magnetic sensors receive the magnetic signals and convert them to electrical signals. The amplifiers amplify (or adjust) the signal magnitude until suitable to the range for A/D conversion. Then, the computer selects the particular signal channel and samples the signal using a 12-bit A/D converter (we tried a 16-channel, ISA bus data acquisition card [PCL-818L; Advantech Co, Ltd, Taipei, Taiwan]). In the experimental process, 32 positions of magnet are selected and the corresponding data of magnetic induction intensities in each position is obtained. Based on the data, the RCA compares with the LM algorithm in terms of the position and direction error, and the execution time of the algorithm, and the result is shown in Figure 10.

In Figure 10, in each position among 32 positions, when the algorithms (RCA and LM) were run, we obtained the average values for positioning and direction errors and the running time of the algorithms, with error bars (95% confidence interval) for all of the mean values. The error bars specify the size of the uncertainty of the measurement data. For the LM algorithm, the position error is less than 12.51 mm, and the average value is 4.86 mm; the direction error is less than 10.56%, and the average value is 5.71%; and the execution
time of the algorithm is less than 0.24 seconds, and the average value is 0.22 seconds. Alternately, for the RCA, the position error is less than 8.34 mm, and the average value is 3.70 mm; the direction error is less than 10.80%, and the average value is 3.27%; and the execution time of the algorithm is less than 0.21 seconds, and the average value is 0.20 seconds. Obviously, for the 32 positions in the actual measured data, the RCA performs better than the LM algorithm for the position, the direction, and the execution time.

Summary
As mentioned above, the positioning and tracking technology of the capsule is the key technology for capsule endoscopy. To realize stable and accurate localization, we must find appropriate algorithms. Based on the magnetic positioning model of the capsule endoscope with an embedded permanent magnet, we propose a new localization algorithm – the RCA. Simulation results show that the RCA is better than the LM algorithm with regard to the stability, the initial guess setting range, and noise immunity. We have tested and compared actual experimental data, based on an actual test system, and find that the RCA is better than the LM algorithm with regard to the position accuracy and the execution time of the algorithm. For the actual localization system, we can design a hybrid algorithm combining the RCA nonlinear algorithm with other algorithms, by first using other algorithms to find a initial position of the capsule and then using the RCA to track it in a real system.

Acknowledgments
This work was supported by the National Natural Science Foundation of China (grant number 61273332) and Ningbo Science and Technology (Innovation Team) plan project (grant number 2014B82015).

Disclosure
The authors report no conflicts of interest in this work.

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