

Ongoing studies of cell-based therapies for articular cartilage defects in Japan

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Abstract: Recently, cell-based therapies have generated great interest in the repair of articular cartilage defects and degeneration. Surgical treatments for these indications have multiple options, including marrow stimulation, osteochondral autograft transplant, and autologous chondrocyte implantation. The autologous chondrocyte implantation technique has been improved using a cell scaffold and other devices. Meanwhile, advanced cell-based therapies, including cultured stem cell treatment, have been studied in clinical trials. Most studies have been designed and authorized by institutional review boards and/or the regulatory agencies of the investigators' countries. For cellular products in regenerative medicine, regulations of many countries are amenable to expedited approval. This paper aims to provide an update on ongoing and prospective cell-based therapies, focusing on articular cartilage injury at designated institutions authorized by the Japanese Pharmaceutical and Medical Device Agency.

Keywords: autologous chondrocyte implantation, mesenchymal stem cell, knee joint

Introduction

The number of articular cartilage defects is greatly increasing, particularly in the young and middle-aged populations. When the defect is symptomatic, it causes joint disability followed by progressive osteoarthritis.¹ Ultimate treatment results in total joint replacement, as articular cartilage has been recognized as being nonregenerative tissue in the orthopedic arena.²⁻⁵ Surgical treatments for cartilage defects include debridement,⁶ bone marrow stimulation, osteochondral autograft transplant (OAT), and autologous chondrocyte implantation (ACI, Figure 1). ACI in particular has attracted great interest as a cell-based therapy in younger populations. ACI aims to avoid total joint replacement and the associated limitations in prosthetic material durability. Using expanded populations of a patient's own cells, this technique has extended the treatment options and overcome some of the limitations of bone marrow stimulation and OAT. Moreover, the latest treatments have been developed using biomaterials or adult tissue-derived mesenchymal stem cells (MSCs). Although various cell therapies are in development elsewhere, we focus on new methods that are either in clinical trials or in clinical research, and approved by their own country's regulatory agency. In this review, we focus on the latest commercially available cell therapy and ongoing trials with cells conducted in Japan.

Bone marrow stimulation and OAT

The most popular treatments for cartilage defects are recognized to be bone marrow stimulation and OAT. Bone marrow stimulation includes drilling,⁷ abrasion,⁸ and

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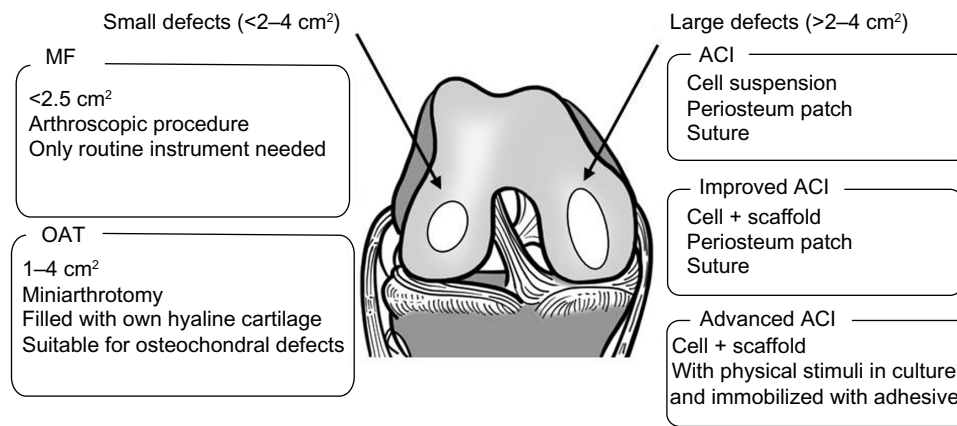


Figure 1 Treatment criteria, technical significance, and benefits.

Abbreviations: ACI, autologous chondrocyte implantation; MF, microfracture; OAT, osteochondral autograft transplant.

microfracture.⁹ The indication for this treatment is generally a lesion area of less than 2.5 cm². As this technique can be conducted minimally invasively and with routine surgical instruments, it is widely used for cartilage defects. This technique involves penetration into the subchondral bone to release bone marrow elements, including stem cells and growth factors, which form a clot and stimulate cartilage repair.¹⁰ However, histologic follow-up studies of microfracture indicated that cartilage defects were filled with fibrous tissue between 1 and 2 years post surgery.^{11,12} Moreover, the regenerated tissue was biomechanically suboptimal and eventually failed.¹³ In randomized studies of microfracture, the early revision rate was 2.5% before 2 years, 23% at year 2, and 31% thereafter by year 5.¹⁴

Another intervention is OAT, or so-called “mosaicplasty”. The indication for this treatment is generally a lesion area within approximately 2–4 cm². This technique involves harvesting autologous osteochondral plugs from the femoral condyle and/or trochlea and transplanting them into the cartilage defect. Ultimately, the defect is filled with pieces of harvested hyaline cartilage and the underlying subchondral bone.¹⁵ However, OAT has concerns regarding donor tissue morbidity, unmatched shape of the host and donor cartilage surfaces, and a limitation of defect size. Randomized studies for the same indication regarding the superiority of OAT compared with microfracture have been somewhat controversial. Patients treated with OAT had significantly better clinical outcomes according to the International Cartilage Repair Society (ICRS) score 10 years postoperatively than microfracture ($P < 0.001$).¹⁶ In addition, OAT maintained a significantly higher activity level according to Marx Activity Rating Scale scores than microfracture by 5 years ($P = 0.02$).¹⁷ On the other hand, a follow-up study with a median of

9.8 years indicated no significant difference between OAT and microfracture based on Lysholm scores, Knee Injury and Osteoarthritis Outcome Score (KOOS), muscle strength, and radiographic outcome.¹⁸ Therefore, microfracture and OAT still require more information for appropriate indications and outcomes.

ACI

ACI was developed in the early 1990s to treat focal defects in the knee joint.¹⁹ Since then, over 15,000 ACI procedures have been performed in the USA, and over 20,000 had been performed in Europe by 2010.²⁰ Briefly, ACI requires two surgeries. First, cartilage fragments are harvested from the nonweight-bearing site in the patellofemoral condyle. The fragments are enzymatically digested for isolation of chondrocytes followed by cell number expansion in monolayer culture. At the second surgery several weeks after cartilage harvest, a suspension of the chondrocytes is injected into the defect, and covered with the harvested periosteum flap from the tibia of the same leg.

Proof of concept of ACI was demonstrated using a rabbit model prior to clinical study.²¹ In this animal model, synovitis and osteophyte formation are markedly decreased in the joint treated with ACI compared to the nontreated joint. In addition, the articular cartilage surface was smooth and glistening white, similar to normal hyaline cartilage. Histologically, the defect was filled with a cartilage matrix that was similar to adjacent tissue at 6 weeks following cell implantation. After achieving successful results in a rabbit model, Brittberg et al addressed the usefulness of ACI clinically and histologically.¹⁹ At an average of 2 years post ACI, 14 of 16 patients showed good to excellent clinical outcomes and histologic appearance of hyaline cartilage. Recently, the extended

follow-up study indicated significant improvement in joint function, reduction of symptoms, and regeneration of hyaline-like cartilage.²² Arthroscopic findings were normal or nearly normal in 87.7%–93% according to the ICRS scale.²³ In addition, the other study conducted by Minas et al showed that at a minimum of 10 years post ACI, there was a survivorship of ACI grafts in 71% and improved function in 75% of patients with symptomatic cartilage defects.²⁴

Although ACI has become popular, several concerns have been raised. ACI requires two surgeries, resulting in inconvenience to the patient, a longer period of rehabilitation, and higher cost. Harvesting a periosteum flap is also a rather painful intervention²⁵ and the regenerating cartilage increases the risks of hypertrophy,^{26,27} catching, and swelling.^{28,29} Moreover, expansion of chondrocytes in monolayer culture risks losing the chondrocytic phenotypes. From a technical standpoint, the injected cell suspension has risks of leaking out from the pocket after resuming normal joint-loading, as well as moving around within the pocket.^{28,30,31} Therefore, these concerns motivated the development of improved ACI using a cell scaffold and medium supplements.

Improved ACI

Cell scaffolds are being widely developed elsewhere using extracellular matrix extracted from animals, then synthesized with biodegradable polymers for constructing a scaffold with chondrocytes. A hyaluronan-based scaffold would also improve maintenance of chondrocyte phenotypes.³² In Japan, atelocollagen gel (acid-soluble, pepsin-digested collagen) has been widely used for three-dimensional cell culture. Proof of concept of this improved ACI using the atelocollagen gel scaffold revealed that the histologic quality of regenerative tissue was significantly higher than using classic ACI, and higher than the periosteum flap and no treatment control in rabbits.^{33–36} Moreover, human articular chondrocytes in the gel efficiently promoted the production of cartilage-specific matrices and avoided an increase of predominantly collagen type I in vitro.³⁴ A leading clinical study of the improved ACI using this gel construct was conducted by Ochi et al.³⁷ They reported that the clinical outcome by Lysholm score was significantly improved at 2 years after implantation ($P < 0.001$). Most recently, the improved ACI showed a good Lysholm score at a mean 8 years (range 5.0–11.3 years), and a significant correlation between arthroscopic ICRS grade at 2 years and final Lysholm scores ($P < 0.01$). Histologically, hyaline-like cartilage was seen (ICRS-2 histologic scale 70.4 ± 20.8 , $n = 40$), although a normal layered structure was not seen at 1 year after implantation.

In addition, other improvements have been made for manufacturing improved ACI. Tohyama et al changed the serum source from patient serum 15% to fetal bovine serum (FBS) 10%, as chondrocytes with 10% FBS proliferated six times faster than those with patient serum. They also changed the starting time of enzymatic chondrocyte isolation from 2 hours to 1 day after harvest (Table 1).^{30,38} Although the manufacturing processes were changed for practical reasons, clinical evaluations using those methods have not yet been completed. If the methods do not cause any significant changes, those culture protocols will be useful for consistent and convenient processes.

Regarding complications, the overall incidence was 11%–30% in these studies and hypertrophy of the transplant was most common. Neimeyer reported that the incidence of hypertrophy by periosteum-covered ACI was 15.4%.²⁷ Using a periosteum patch is still problematic in improved ACI and further development of stabilizing the transplant without a periosteum flap is required to reduce these complications.

Advanced ACI for cartilage defects

Beyond improvement of ACI, various methods of ACI have been developed using biological, chemical, and physical methods. Conceptually, these methods are used by mimicking physiologic changes in chondrocytes. Mizuno et al have developed a novel cell culture method with hydrostatic pressure for promoting chondrogenesis by autologous chondrocytes.^{39,40} The rationale for using hydrostatic pressure, which is a passively loaded stress on articular cartilage similar to joint-loading and weight-bearing, was that hydrostatic pressure-loaded chondrocytes produced and accumulated more cartilage extracellular matrix within a collagen gel/sponge scaffold.^{41,42} Moreover, the cell gel/sponge construct, Neocart[®], was implanted into the cartilage defect using a novel collagen/polyethylene glycol-based glue. The clinical results of Neocart (ie, International Knee Documentation Committee score, KOOS, visual analog scale scores) were significantly superior compared with microfracture 2 years after implantation ($P < 0.05$).⁴³ An advantage of using hydrostatic pressure is that physical stimuli on chondrogenesis needs less safety concern than biological and chemical stimuli. Globally, other improved ACIs have been developing and are voluntarily registered at ClinicalTrials.gov, supported by the US National Institutes of Health. From these lists, two cell-based therapies should be known based on their level of clinical study and support by scientific reports. Matrix-associated cartilage implantation (MACI[®]) has been developed using type I/III bilayer collagen membranes.^{44,45} Autologous chondrocytes

Table 1 Clinical research showing improved autologous chondrocyte implantation

Reference	Patients n	Age, years	F/U, years	Etiology	Defect size (cm ²) and location	Cell number (×10 ⁶)	Lysholm score before and after surgery	Histologic/biomechanical findings	Graft failure rate (type)/clinical complication
Ochi et al ³⁰	28	26	2	Trauma 57% OCD 32% OA 7% Chondromalacia patella 4%	3.0 (0.7–16.0) MFC 46% LFC 46% Patella 8%	2.75 (0.4–42)	71±12/97±5 (P<0.001), 2 years	Hyaline-like cartilage with integration 1 year (n=1), 6 months (n=1) Hardness: similar to that of the surrounding cartilage (1 year, 2 years) N/A	25% Hypertrophy (n=3); partial periosteum detachment (n=3); partial graft ossification (n=1)/crepitus and occasional discomfort (n=3) 7.4% Hypertrophy and detachment (n=1); partial detachment (n=1)/restricted range of motion (n=1) 30%
Tohyama ³⁸	27	N/A	2	Trauma 70% OCD 11% OA 19%	3.2 (1.2–9.4) MFC 59% LFC 19% Patella 6%	N/A	60.0±13.7/89.8±9.5 (P<0.001), 2 years	ICRS II scale: 70.4±20.8, ECM: strongly stained with safranin O Not normal layer (1 year; n=40) Hardness: femoral condyle, similar to surrounding cartilage; patellar lesion, significantly decreased compared with femoral condyle (2 years)	Hypertrophy was most common/N/A
Adachi et al ³⁷	73	25	1, 2, >5	Trauma 56% OCD 33% Recurrent patella dislocation 5% OA 3%	3.6 (2.0–16.0) MFC 45% LFC 34% Patella 21%	2.2 (0.4–42)	N/A		

Note: ^aAverage age at the time of surgery.

Abbreviations: F/U, follow-up; OCD, osteochondritis dissecans; OA, osteoarthritis; MFC, medial femoral condyle; LFC, lateral femoral condyle; N/A, not applicable; ICRS, International Cartilage Repair Society; ECM, extracellular matrix.

expanded in number were seeded onto the membrane, incubated, and implanted into the cartilage lesion. This method allowed implantation without a periosteum flap and reduced hypertrophy of the graft. This membrane alone was also utilized for improving the ACI instead of a periosteum flap, and showed a similar reduction of hypertrophy. These clinical studies strongly suggest that refraining from the use of periosteum could be one strategy for preventing adverse events. Another therapy was that particulate juvenile articular cartilage (DeNovo NT[®]) harvested from allogeneic juvenile cadaveric cartilage was implanted into lesions with fibrin glue.⁴⁶ In addition, allogeneic engineered chondrocyte implantation (DeNovo ET[®]) is undergoing clinical trials.⁴⁷ These methods are advantageous when compared with ACI, as both implant techniques do not require two surgeries. If a smaller number of donors are sufficient, using allogeneic cartilage can be useful. Clinical outcomes are still incomplete, as the dataset is not enough to provide statistical power yet. This technique still needs more time and information before routine implementation of ACI.

Overall, methodologies for cell-based therapy have been improved for in vitro cell culture and implantation techniques. Clinical outcomes following improved and advanced ACIs are adding up long-term. However, the only way to obtain histologic data is from failure cases that undergo total joint replacement. Improved and advanced ACI will continue to provide functional recovery and impact other treatment strategies in regenerative medicine. Meanwhile, some meta-analyses were conducted between ACI and bone marrow stimulation and between ACI and OAT.^{48,49} These analyses showed no significant difference between treatments. Although they were performed by matching demographic background and lesion size, each study was designed with other varied indications (eg, lesion location, lesion number, preoperative duration of symptoms, previous treatment, and desired physical activity). Thus, other indications have a chance to influence interpretation of these analyses. Concerning indications, well-designed and long-term follow-up studies will provide more comparable data sets for clinical guidelines.

MSC-based therapy

Recently, MSCs have attracted much interest in the field of tissue regeneration because of their relative ease of isolation and their amenability to ex vivo expansion while retaining the potential to differentiate into a variety of connective tissues, including bone, cartilage, tendon, muscle, and adipose tissue.^{50–52} MSCs have been identified and isolated from bone marrow,^{53–55} synovial membrane,⁵⁶ periosteum,⁵⁷

skeletal muscle,⁵⁸ adipose tissue,⁵⁹ trabecular bone,⁶⁰ and umbilical cord blood cells.⁶¹ Bone marrow-derived MSCs and synovium-derived MSCs (S-MSCs) have been used for cartilage regeneration, particularly in Japan (Table 2).⁶²⁻⁶⁵

Bone marrow-derived MSCs

It has been reported that MSCs from human bone marrow are capable of chondrogenesis, osteogenesis, and adipogenesis in vitro.^{52,55} Using a rabbit injury model, Wakitani et al transplanted autologous bone marrow-derived MSCs embedded in collagen gel into an osteochondral defect (3×6 mm, 3 mm in depth) in medial femoral condyles, and cover the defects with a periosteum flap. The defect was mostly replaced with hyaline cartilage at 2 weeks after transplantation, and was followed by subchondral bone formation at 4 weeks. Ultimately, the defect was completely repaired by 24 weeks.⁶⁶ After proof of concept using rabbits, these investigators performed bone marrow-derived MSC transplants in three indications: traumatic cartilage defects in the patella alone, the patellofemoral joint, and osteoarthritic lesions in the medial femoral condyle. Bone marrow-derived MSCs were harvested from the anterior iliac crest, expanded for 3 weeks, and embedded in collagen gel. This construct was then transplanted with periosteum. In the traumatic defect cases, clinical symptoms were improved significantly by 8 months and the defects were filled histologically with fibrocartilage by 1 year.^{62,63} In the osteoarthritis cases, they compared the bone marrow-derived MSC construct (cells within a scaffold) and the scaffold alone in 24 patients who were concomitantly treated with high tibial osteotomy.⁶⁴ By a mean follow-up of 16 months, the clinical outcome was not different between the bone marrow-derived MSC construct and the scaffold alone using the Hospital for Special Surgery knee rating scale. Moreover, the longer follow-up of 64 months also indicated the same trend.⁶⁷ However, arthroscopic and histologic evaluations were significantly better in the bone marrow-derived MSC construct than in the scaffold alone, with appearance of fibrocartilage in almost all areas of the repair ($P<0.05$).^{66,68} Overall, bone marrow-derived MSC/collagen gel transplantation can be clinically effective and is one of the options for traumatic defects. However, well-designed studies are still needed to draw conclusions regarding effectiveness, because both the existing reports are case studies with no controls.

Synovium membrane-derived MSCs

The rationale for using S-MSCs comes from the idea that S-MSCs represent a more natural strategy to promote spontaneous healing of articular cartilage in the joint space.

Table 2 Clinical study of cartilage regeneration with bone marrow-derived MSCs

Reference	Study	n	F/U	Mean age, years	Etiology	Rehabilitation	Clinical outcomes	Macroscopic findings	Histologic findings	MRI findings
Wakitani et al ⁶⁴	Case control + HTO with/without cells	12/12	16 months	63	OA	4 days, CPM 6 weeks, PWB 8 weeks, FWB	HSS not significantly different	Greater score in MSC	MSC > no-cell	None
Wakitani et al ⁶²	Prospective case	2	5 years, 9 months, 4 years	26 44	Trauma (chronic)	3 days, CPM 3 weeks, PWB 6 weeks, FWB	Satisfied but show slightly limited knee motion score (-)	Cartilage-like tissue	Fibrocartilage (1 year)	None
Wakitani et al ⁶³	Prospective case	3	17-27 months	31	Chronic cartilage lesions	3 days, CPM 3 weeks, FWB	IKDC improved	Cartilage-like tissue	Cartilaginous matrix (11 months)	Complete coverage/less intensity than normal
Kuroda ⁶⁵	Case report (athlete)	1	1 year	31	Trauma	11 days, CPM 4 weeks, PWB 8 weeks, FWB	Return to preinjury level activities with no pain	Smooth tissues (7 months)	Hyaline-like cartilage + collagen type 2 (7 months)	Focal chondral/subchondral irregularities

Abbreviations: F/U, follow-up; HTO, high tibial osteotomy; OA, osteoarthritis; CPM, continuous passive motion; PWB, partial weight bearing; HSS, Hospital for Special Surgery; IKDC, International Knee Documentation Committee; MRI, magnetic resonance imaging; MSC, mesenchymal stem cell.

Sekiya et al reported that chondrogenesis of S-MSCs from humans and various animals was superior to, or at least comparable with, bone marrow-derived MSCs with regard to the gene expression profile *in vitro*,⁶⁹ and superior to MSCs from periosteum, adipose tissue, and muscle with regard to proliferation and chondrogenesis *in vitro*.⁷⁰⁻⁷² An animal study showed that S-MSCs and bone marrow-derived MSCs had greater chondrogenic potential histologically⁶⁶ than MSCs from adipose tissue and skeletal muscle in the rabbit.⁷³ In addition, delivery methods for MSCs were also explored because the regeneration processes (resurfacing) would be different from ACI. Placing a suspension of S-MSCs in the cartilage defect for 10 minutes resulted in more than 60% of S-MSCs adhering within the defect, and promotion of cartilage regeneration *ex vivo* in human and rabbit cartilage.⁷⁴

Based on the *ex vivo* study by Koga et al, S-MSC transplantation was approved for clinical study in the treatment of articular cartilage defects.⁷⁵ Briefly, S-MSCs were harvested arthroscopically, expanded for 2 weeks, and suspended in phosphate-buffered saline. Then, the S-MSCs suspension was implanted to the defect arthroscopically. They reported regeneration of cartilage, reduction in defect size, and symptomatic improvement in most patients for 3 years. Further investigation is needed to evaluate the effectiveness of S-MSC transplantation.

Cell processing and innovative technologies

Conceptually, cell-based cartilage regeneration has been conducted by implanting autologous chondrocytes, chondro-induced stem cells, or nontreated stem cells. To make treatment more convenient and reliable, isolation of cells from patients and their expansion are critical processes *in vitro*. Minimizing passage numbers is necessary to avoid the risk of declining their phenotypes. However, a certain number of chondrocytes is necessary to fill a cell construct with newly synthesized cartilage matrix. Using a three-dimensional scaffold has the advantage of maintaining chondrocytic phenotypes while implanting a cell construct securely.^{30,40,44-46}

Without inducing MSCs to chondrocytes, MSCs were implanted into a defect. A higher cell density of MSCs in the defect appears to be necessary for cartilage regeneration and differentiation into chondrocytes *in situ* without a cell construct and differentiation factors, eg, transforming growth factor- β .⁷⁵⁻⁷⁹ Koga et al embedded MSCs in collagen gel and incubated the cell/gel construct in medium including FBS, bone morphogenetic protein, transforming growth factor- β , dexamethasone, ascorbate-2-phosphate, pyruvate, proline,

and insulin, transferrin, and selenious acid to differentiate into chondrocytes *in vitro*. Next, 5×10^7 chondro-induced MSCs/mL successfully promoted cartilage regeneration in the rabbit, but a concentration of 1×10^6 cells/mL failed.⁷³ The relevance of these two distinct culture processes using MSCs is unclear in the clinical setting.

An appropriate serum source was a concern due to not only the quality of the serum components, but also because of potential immune rejection of the xenograft. Autologous chondrocyte culture could switch from patient serum to FBS due to consistent quality and higher proliferation rate. However, serum for MSC culture is still under consideration. Motility and growth of bone marrow-derived MSCs were higher in autologous serum than in FBS.^{80,81} Human S-MSCs with autologous serum had a higher proliferation rate than those with FBS; however bone marrow-derived MSCs with FBS had a higher proliferation rate than those with autologous serum.⁸² Moreover, the chondrogenic potential of bone marrow-derived MSCs and S-MSCs with human serum was lower than that with FBS. These various studies suggest that the serum source should be chosen depending on the cell proliferation and differentiation of MSCs.

Prospective treatments and evaluation for cartilage injury

In this update on the latest cell-based therapies conducted in Japan, we focus on various treatment options for articular cartilage injury. None of the new treatments reported direct adverse events in registered clinical research. In particular, it was proven that autologous chondrocytes and adult tissue-derived stem cells are safe after implantation. Prior to cell implantation, cellular characteristics can be determined regardless of the cell source and cell culture method. However, the fate of the implanted cells is still unclear. Although an animal study partially reproduces the regenerative process of articular cartilage *in vivo*, we must recognize that the long-term failure cases were not available from these animal studies. The behavior of stem cells in animals is different from that in humans. Therefore, in order to establish reliable regenerative treatments, it is necessary to gain more information about the mechanisms of resurfacing cartilage defects. Due to the inherent limitations of tracking and imaging implanted cells, clinical symptoms, such as joint pain and decreased range of motion (using the ICRS, KOOS, Lysholm grading systems) are the only way to compare cell-based therapies. Thus, clinical evaluation requires extended study durations, resulting in the slow development of new treatments. The development of an efficient evaluation system

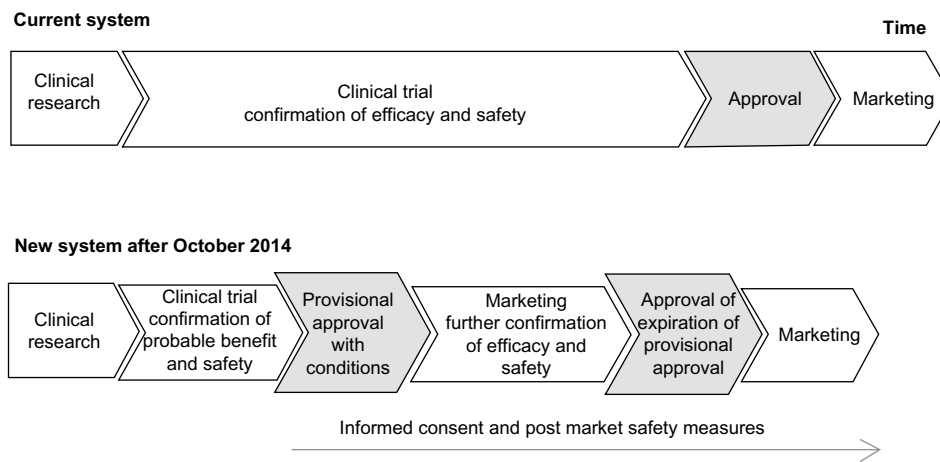


Figure 2 New approval system for commercialization of cell therapy products.

would therefore take on a role equally important to that of successful cell therapy.

All clinical research on cell-based therapy in Japan has been carried out using single-arm studies due to ethical issues. However, microfracture has been used as a control arm for test treatment in the USA because microfracture and OAT are conducted for indications similar to ACI. Moreover, some ACI, stem cell implantation, and OAT procedures were conducted with high tibial osteotomy in order to reduce stress at the injured site by changing the weight-bearing alignment of the knee joint. Although this is beneficial for patients, an evaluation of outcomes is rather complex. Thus, data from each study are less interchangeable. If a database of the same or similar indications for microfracture and OAT is established, it will be of great benefit for developing future cell-based therapies. A nationwide joint registry for indications and treatments in Japan will be helpful for collecting comprehensive relevant data about cell-based therapy in order to provide an early warning of issues relating to patient safety. In fact, this type of joint registry for artificial joint implantation was previously organized for the continuous improvement of outcome quality and ensuring the quality and cost-effectiveness of joint replacement surgery.

New Japanese regulations for clinical research and trials will be implemented in November 2014 (Figure 2).⁸³ The concept of the new regulations will be to bring new treatments to patients as rapidly as possible. Under the previous regulatory system, the approval process was long and tedious. However, under the upcoming regulations, provisional approval will be made for commercialization if probable benefit and safety are confirmed, although certain conditions may apply. Early provisional approval will greatly benefit patients, although patients will be required to cover the full or partial cost of

treatment. It could, however, cover tissues with difficult regeneration, including cases with a potential threat to life and loss of tissue/organ function, for which there are currently no available treatments. Regenerative medicine includes cure of life-threatening disease, functional recovery of damaged tissues, and reconstruction of tissue shapes. Being able to evaluate study designs and outcomes with an internationally recognized system would greatly aid the research process.

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Disclosure

The authors report no conflicts of interest in this work.

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