Transmyocardial revascularization devices: technology update

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Abstract: Transmyocardial laser revascularization (TMR) emerged as treatment modality for patients with diffuse coronary artery disease not amendable to percutaneous or surgical revascularization. The procedure entails the creation of laser channels within ischemic myocardium in an effort to better perfuse these areas. Currently, two laser devices are approved by the US Food and Drug Administration for TMR – holmium:yttrium–aluminum–garnet and CO₂. The two devices differ in regard to energy outputs, wavelengths, ability to synchronize with the heart cycle, and laser–tissue interactions. These differences have led to studies showing different efficacies between the two laser devices. Over 50,000 procedures have been performed worldwide using TMR. Improvements in angina stages, quality of life, and perfusion of the myocardium have been demonstrated with TMR. Although several mechanisms for these improvements have been suggested, evidence points to new blood vessel formation, or angiogenesis, within the treated myocardium, as the major contributory factor. TMR has been used as sole therapy and in combination with coronary artery bypass grafting. Clinical studies have demonstrated that TMR is both safe and effective in angina relief long term. The objective of this review is to present the two approved laser devices and evidence for the safety and efficacy of TMR, along with future directions with this technology.

Keywords: laser, revascularization, angiogenesis, coronary artery disease

Introduction

As life expectancy and coronary-event survival rates rise, an increasing number of patients with severe coronary artery disease experience angina that is not amenable to percutaneous coronary intervention or surgical revascularization.1–3 Moreover, up to 25% of coronary artery bypass grafting (CABG) patients have incomplete revascularization, a strong independent predictor of operative mortality and morbidity.4,5 Therefore, a great deal of interest in alternative strategies to traditional revascularization has been pursued. These experimental approaches include pharmacologic interventions,6 enhanced external counterpulsation,7,8 spinal cord stimulation,9 protein,10 gene,11 or stem cell therapy12,13 to promote angiogenesis (the formation of new blood vessels), and the topic of this discussion – transmyocardial laser revascularization (TMR).

TMR is a US Food and Drug Administration (FDA)-approved intervention utilizing a laser device intended to treat ischemic myocardium. This procedure was approved by the FDA in 1998 to treat moderate to severe angina (class 3–4 based on the Canadian Cardiovascular Society Classification System14 – Table 1) as a result of diffuse coronary artery disease not amendable to conventional medical therapy, percutaneous coronary intervention, or surgical revascularization via CABG. Over 50,000 TMR procedures

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have been performed worldwide in more than 38 countries, with over 20,000 performed in the United States to date. Over the past two decades, results from prospective and retrospective studies on TMR have been reported. A few meta-analyses have also been reported, along with an FDA review on short-term and long-term outcomes with the use of TMR. This review covers two different FDA-approved devices for TMR, evidence-based practice, and future directions aimed at utilizing a combined TMR and stem cell therapy approach.

**Proposed mechanism**

TMR is an approved surgical procedure that induces transmural laser channels within ischemic myocardium. The thought behind direct perfusion to the myocardium was based on descriptions of reptilian heart sinusoids that allowed blood to flow directly from the ventricles into the myocardium, perfusing the heart muscle. TMR creates channels that are 1 mm in diameter, with the number of channels depending on heart size and ischemic territory (Figure 1). The exact mechanism of angina relief is debated.

Patent channels that allow perfusion from the ventricle to the myocardium may provide a potential mechanism for TMR and angina relief. Clinical and experimental work have shown evidence of long-term patency. However, several autopsy case reports and reviews have demonstrated that channels created by TMR in humans do not remain patent. Therefore, it is believed that patency of channels providing perfusion to the ischemic myocardium is not the mechanism of action for TMR.

Denervation of the sympathetic nerve fibers innervating the heart is another proposed mechanism of angina relief following TMR. Afferent, sympathetic efferent postganglionic, and parasympathetic efferent postganglionic neurons all innervate the heart. Conflicting experimental evidence has been reported regarding denervation playing a role in angina relief. These experiments only focused on short-term results. Furthermore, it is difficult to assess and isolate the afferent nerves involved in pain signaling. A study by Al-Sheikh et al utilizing positron emission tomography scanning demonstrated that sympathetic denervation occurs following TMR. Nevertheless, evidence indicating that denervation is the primary cause of angina relief is lacking.

Angiogenesis has shown the strongest experimental and clinical evidence for being the primary basis of angina relief after TMR. Several independent groups have provided concrete histological evidence of increased angiogenesis and neovascularization as a direct result of TMR channel creation. Additionally, upregulation of proangiogenic factors, such as vascular endothelial growth factor, fibroblast growth factor 2, and platelet-derived endothelial cell growth factor, was demonstrated in myocardial tissue following TMR. This neovascularization process is not specific to laser only, but can also be seen with other means of myocardial channel formation, such as hot and cold needles and radiofrequency ablation. However, TMR minimizes scar formation, which allows optimal functional contribution of the new blood vessels. Therefore, the evidence from a histological and molecular standpoint supports the notion of angiogenesis promotion in the ischemic heart following TMR, with the minimization of scar tissue following channel creation.

**Table 1** Canadian Cardiovascular Society Angina Classification System

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<th>Class</th>
<th>Description</th>
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<tr>
<td>I</td>
<td>Ordinary physical activity, such as walking and climbing stairs, does not cause angina. Angina occurs with strenuous, rapid, or prolonged exertion at work or recreation.</td>
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<tr>
<td>II</td>
<td>Slight limitation of ordinary activity. Angina occurs on walking or climbing stairs rapidly; walking uphill; walking or stair climbing after meals, in cold, in wind, or under emotional stress; or only during the few hours after awakening. Angina occurs on walking more than two blocks on the level and climbing more than one flight of ordinary stairs at a normal pace and in normal conditions.</td>
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<tr>
<td>III</td>
<td>Marked limitations of ordinary physical activity. Angina occurs on walking one to two blocks on the level and climbing one flight of stairs in normal conditions and at a normal pace.</td>
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<tr>
<td>IV</td>
<td>Inability to carry on any physical activity without discomfort; anginal symptoms may be present at rest.</td>
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Another critical issue explored by several studies is the notion that angiogenesis following TMR may lead to improvement in heart function. Improvement in subjective quality of life was shown following TMR. Moreover, objective improvements were demonstrated based on dobutamine stress echocardiography, positron emission tomography scanning, and cardiac magnetic resonance imaging (MRI). Improvements in perfusion and myocardial function were noted in animal models of chronic myocardial ischemia as well, supporting the proangiogenic basis of improvement. The role of angiogenesis was further supported by a study that showed emergence of small vessels perfusing the heart on follow-up angiography 10 years after TMR. These secondary blood vessels were not present prior to TMR. Thus, neovascularization and angiogenesis seem to be the predominant driving force for angina improvement and increased myocardial perfusion.

**Devices**

Many different wavelengths of laser light have been studied experimentally, including xenon--chloride, neodymium:yttrium--aluminum--garnet (YAG), erbium:YAG, thulium--holmium--chromium:YAG, holmium:YAG (Ho:YAG), and CO2. Two different laser devices are currently FDA-approved and utilized for TMR (Figure 2) – the Heart Laser CO2 Transmyocardial Revascularization System (Novadaq Technologies Inc., BC, Canada) and the SolarGen TMR Ho:YAG Laser System (CardioGenesis Corporation, Foothill Ranch, CA, USA). In addition to different wavelengths, these lasers employ different energy outputs and require slightly different surgical approaches.

The CO2 laser has a wavelength of 10,600 nm and uses an energy level of 15–20 J per pulse with a pulse duration of 25–40 ms. A single pulse is used, and the pulse beam is directed within the device to the myocardium using a system of mirrors (Figure 3). Using this level of energy and single pulses, the laser photons do not create tissue explosions, limiting the total structural damage (Figure 4). The CO2 laser is also synchronized with the R-wave (maximal ventricular filling) of the electrocardiogram cycle. Transesophageal echocardiography can be used to confirm accurate transmural channel formation, as a result of vaporization of blood within the ventricle. This characteristic acoustic response is helpful in assessing whether proper laser pulse delivery was achieved.

In contrast to the CO2 laser, the Ho:YAG laser system has a wavelength of 2,120 nm and uses pulsed laser beam sequences of 1–2 J and 6–8 W per pulse. This laser beam is projected through a 1 mm fiberoptic bundle at a rate of five pulses per second. The arrival of the sequential pulses must be separated by time in order to allow for proper thermal dissipation to avoid excess heat accumulation. If the pulses are incorrectly timed, this can lead to tissue explosions and subsequent structural trauma, along with thermocoagulation. Even with the pulsed low sequences, high levels of peak...
power are delivered to the tissue, causing small explosions (Figure 4). During the procedure using the Ho:YAG laser, the laser fiber is advanced manually through the myocardium. Due to this physical manipulation, it is not possible to decipher whether the channel in the myocardium is being created as a result of the mechanical effects of the fiber or whether there has been enough time for thermal dissipation to occur prior to the next initiated pulse. Furthermore, the Ho:YAG laser is unsynchronized to the cardiac cycle and is prone to producing ventricular arrhythmias.

**TMR sole therapy**

TMR has been performed solely or in combination with other procedures, such as CABG. Sole TMR may be done without the use of cardiopulmonary bypass or anticoagulation. The procedure requires general anesthesia, generally done via a double-lumen endotracheal tube or bronchial blocker to isolate the left lung. Exposure to the left ventricle is obtained via a left anterolateral thoracotomy performed on the fifth intercostal space. Upon laser activation, transesophageal echocardiography is used to monitor whether a successful channel was created with the CO₂ laser. Channel formation using the Ho:YAG laser is monitored by tactile and auditory feedback. Upon completion, a chest tube is placed and the thoracotomy is closed. In most cases, the patient is extubated in the operating room.

Preliminary nonrandomized trials showed benefit for sole TMR in patients with diffuse coronary artery disease and no other options to alleviate severe angina.¹⁵⁻¹⁷ This symptomatic improvement led to prospective randomized controlled trials, which were designed to test TMR plus optimal medical management versus optimal medical management alone.²²⁻²⁶ Over 1,200 patients were enrolled in these trials. In order to fit inclusion and exclusion criteria, all patients had refractory angina that was not amenable to percutaneous coronary intervention or CABG (confirmed on recent angiogram), evidence of reversible ischemia upon myocardial perfusion scanning, and a left ventricular ejection fraction greater than 25%. Three of the five trials used the CO₂ laser,²⁴⁻²⁶ and two trials used the Ho:YAG laser.²²⁻²³ The major subjective endpoint investigated entailed a change in angina symptoms. Other study endpoints included: operative mortality, 1-year survival, myocardial perfusion, exercise tolerance, quality of life, cardiac-related hospitalizations, and major adverse events. Patients were evaluated and assessed at 3 months, 6 months, and 12 months following randomization.

Significant angina improvement was seen in all studies (Figure 5). Based on all five clinical trials, a summary odds ratio of 9.3 (95% confidence interval =4.6–18.5; \( P<0.001 \)) for angina reduction was calculated. Moreover, quality of life, freedom from rehospitalization at 1 year, exercise tolerance, and decreased need for nitrates were significantly improved.

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**Figure 4** Stop-action photography of laser pulses.

Notes: (A) Stop-action photography of laser pulses created with the CO₂ laser. The CO₂ laser creates a clean and straight channel within the tissue. (B) Stop-action photography of laser pulses created with the Ho:YAG laser. The Ho:YAG laser creates wider explosive ablations within the tissue.


**Figure 5** Angina relief at 12 months.

Notes: Summary of angina relief in five randomized controlled trials at 1-year follow-up as defined by a decrease of two or more angina classes. Column graph illustrates differences between medical management and transmyocardial revascularization plus medical management groups. Corresponding \( P \)-values are shown below the bars.

Abbreviations: MM, medical management; TMR, transmyocardial revascularization.
in patients who received laser treatment. A meta-analysis looking at 1-year survival in randomized patients showed similar survival between patients treated with laser and those managed with medical therapy alone. Functional analysis looking at myocardial perfusion showed some evidence of improvement in reversible ischemic defects and perfusion of ischemic territories with the CO$_2$ laser.

Long-term follow-up of the prospective randomized controlled trials showed continued angina relief in the TMR group. Specifically, intention-to-treat analyses showed that at a mean of 5 years, 88% of patients who received TMR experienced at least a 2-level reduction in angina class, compared with 44% of patients managed medically ($P<0.001$). Furthermore, long-term analysis of a trial that did not allow crossover between groups showed an improvement in angina symptoms ($P<0.001$) and reduction in unstable angina hospitalizations in the TMR group ($P<0.05$) at 43 months of follow-up. A long-term outcome analysis conducted by the FDA, Society of Thoracic Surgeons, and Duke Clinical Research Institute showed that there were no differences in long-term morbidity or mortality between CO$_2$ and Ho:YAG lasers used for sole TMR. On the basis of the evidence demonstrated by the randomized clinical trials, both the American College of Cardiology/American Heart Association and the Society of Thoracic Surgeons have provided practice guidelines favoring the use of TMR in patients with medically refractive angina not amenable to revascularization procedures.

**CABG plus adjuvant TMR**

TMR plus CABG is reserved for patients who have ischemia that is able to be bypassed coupled with ischemic zones not amenable to bypass grafting. This combined procedure may be performed with or without the use of cardiopulmonary bypass. Both CO$_2$ and Ho:YAG lasers have been used with this hybrid approach. The efficacy of CABG plus TMR has been challenging to assess, due to the inability to delineate the influence of coronary bypass grafts and also the lack of randomized controlled arms in several studies.

Only two randomized controlled trials assessing CABG plus adjuvant TMR versus CABG alone have been reported. In these trials, patients were blinded to treatment assignment through 1 year of follow-up. Patient characteristics and number of bypass grafts were similar between groups. Outcomes from one of the trials showed reduced postoperative mortality (1.5% versus 7.6%, $P=0.02$), increased 30-day freedom from major adverse cardiac events (97% versus 91%, $P=0.04$), and improved 1-year Kaplan–Meier survival (95% versus 89%, $P=0.05$). The other trial showed a similar trend in postoperative mortality within high-risk patients (9% versus 33%, $P=0.09$). On subsequent 4-year follow-up of these patients, survival was similar between groups; however, there was an increase in the need for revascularization in the CABG-alone group (24% versus 0%, $P<0.05$). Furthermore, a retrospective study showed no difference in survival between TMR plus CABG and CABG-alone groups, although with 4-year follow-up in the TMR plus CABG group there was a sustained improvement in New York Heart Association Classification ($P<0.001$). No differences in long-term outcomes for morbidity and mortality were noted between CO$_2$ and Ho:YAG lasers used in combination with CABG.

**Percutaneous TMR**

In an attempt to reduce perioperative morbidity, a minimally invasive percutaneous approach to myocardial revascularization has been previously pursued.77,78 This approach is carried out using a laser fiber inserted into a peripheral artery and guided into the left ventricle. Electromechanical mapping is used to verify the fiber position within the heart. The fiber utilized Ho:YAG laser to create 2–3-mm-deep divots in the subendocardial tissue.

Results with percutaneous myocardial revascularization (PMR) have been less favorable than those observed with TMR.79–81 Furthermore, a pilot study evaluating the efficacy of PMR in combination with percutaneous coronary intervention showed a high rate of periprocedural adverse events (11.5%). Given these results, the FDA has rendered PMR unapprovable. The failure associated with PMR may result from several factors. The maximal depth of channel formation is only 6 mm with PMR. This is significantly less than the full-thickness channel formation found with TMR. Additionally, fewer channels are created with PMR. The exact location of channel formation is also a critical issue within the beating ventricle. Lastly, there are inherent limitations with using the Ho:YAG laser in PMR.

**TMR plus adjuvant cell therapy**

A plethora of research has centered on cell therapy in an effort to stimulate angiogenesis and myogenesis for heart disease. Stem cells, including hematopoietic stem cells, endothelial progenitor cells, mesenchymal stem cells, myoblasts, and undifferentiated side-population cells, have been used clinically with various routes of administration for ischemic heart disease. Of the different cells studied, bone marrow stem cells have shown promise. It is believed that bone marrow stem cells
promote the paracrine secretion of growth factors and cytokines, which stimulate angiogenesis and aid in the survival of cardiomyocytes through the mobilization of progenitor cells.

The combination of cell therapy and TMR has been studied in both animal models and in several clinical studies. One group showed that TMR assisted in mesenchymal stem cell engraftment in rat hearts, with corresponding increases in expression of stem cell factor, stromal derived factor-1, c-kit, and chemokine receptor type 4, as compared to control rats who received only stem cells. Clinical studies of mesenchymal stem cells plus TMR include individual case reports or series of patients with angina refractory to CABG or percutaneous coronary intervention. The bone marrow stem cells that were transplanted were autologous and harvested on the same day of surgery. All of these studies demonstrated that injection of stem cells in addition to TMR was safe and showed an improvement in angina class. Several studies showed some evidence of improvement in perfusion and left ventricular contractility. One of the major limitations of these studies is lack of differentiation between the effects of injected autologous stem cells versus laser revascularization. Furthermore, these studies may have been limited as a result of the small number of cells being injected due to no ex vivo expansion of these stem cells prior to injection. Future investigation into the concomitant use of cell therapy and TMR is warranted.

Our group is currently working on an NIH-sponsored clinical trial (NCT01557543) to study the effects of direct injection of ex-vivo-expanded autologous mesenchymal stem cells in patients undergoing CABG or TMR using the CO₂ laser (Figure 6). The outcomes of interest include cardiac function, quality of life, and reduction of cardiac events in patients versus historical controls at 3 months and 6 months after intervention. With expansion of the autologous mesenchymal stem cells ex vivo coupled with direct injection into the myocardium, we believe this technique should provide further clinical benefit in addition to the CABG or TMR procedure.

Conclusion
TMR is a surgical procedure pioneered in the 1990s that provides angina relief to patients with diffuse coronary disease. The predominant theory behind improvement involves myocardial angiogenesis leading to increased perfusion. Both Ho:YAG and CO₂ laser devices have been approved by the FDA. TMR can be combined with CABG to target ischemic areas that cannot be readily bypassed. Safety of the procedure and long-term angina relief has been shown both with sole TMR and with CABG plus adjuvant TMR. PMR with the use of Ho:YAG has been attempted as a minimally invasive option of TMR, yet it has demonstrated less-favorable results than TMR. Finally, current efforts have been aimed at combining TMR with adjuvant stem cell therapy to better improve functional outcomes in patients.

Disclosure
The authors have no commercial associations or financial disclosures that might pose or create a conflict of interest with information presented in this manuscript (such associations include consultancies, stock ownership, or other equity interests, patent licensing arrangements, and payments...
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