

# Non-invasive imaging of microcirculation: a technology review

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**Abstract:** Microcirculation plays a crucial role in physiological processes of tissue oxygenation and nutritional exchange. Measurement of microcirculation can be applied on many organs in various pathologies. In this paper we aim to review the technique of non-invasive methods for imaging of the microcirculation. Methods covered are: videomicroscopy techniques, laser Doppler perfusion imaging, and laser speckle contrast imaging. Videomicroscopy techniques, such as orthogonal polarization spectral imaging and sidestream dark-field imaging, provide a plentitude of information and offer direct visualization of the microcirculation but have the major drawback that they may give pressure artifacts. Both laser Doppler perfusion imaging and laser speckle contrast imaging allow non-contact measurements but have the disadvantage of their sensitivity to motion artifacts and that they are confined to relative measurement comparisons. Ideal would be a non-contact videomicroscopy method with fully automatic analysis software.

**Keywords:** laser speckle contrast imaging, sidestream dark-field, orthogonal polarization spectral imaging, laser Doppler imaging

## Introduction

Microcirculation is usually defined as small arteries ( $<150\ \mu\text{m}$  in diameter), arterioles, capillaries, and venules.<sup>1,2</sup> It plays a crucial role in physiological processes of tissue oxygenation and nutritional exchange. In addition, studies of microcirculation have shown its involvement in a number of pathological processes, which have increased the interest in studying microcirculation in recent years.

There are several ways to measure microcirculation. Both morphological and functional studies are possible. Morphological parameters measurable with imaging methods include vessel density, rate of perfused vessels and vessel diameter in addition to dynamic measurements of microcirculatory blood flow velocity and blood cell concentration.<sup>3</sup>

Functional studies, especially targeting microcirculatory endothelial function, include pharmacological tests with vasoactive drugs and post-occlusive reactive hyperemia test.<sup>1,4</sup> Post-occlusive hyperemia test is performed by measuring distal flow of microcirculation after a period of proximal vascular occlusion using a cuff with a pressure exceeding the systolic pressure. This is typically used to study forearm microcirculation. Further, microvascular evaluation can be performed with both single-point measurements and imaging methods, giving a full-field image of the microcirculation of a tissue surface. The use of imaging methods is preferable due to the spatial heterogeneity of perfusion seen in microvascular beds. This leads to a

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better reproducibility using imaging methods which measure larger areas as compared to methods with single-point measurements.<sup>5,6</sup> In addition, imaging methods have also been shown to have good inter-day reproducibility.<sup>5</sup>

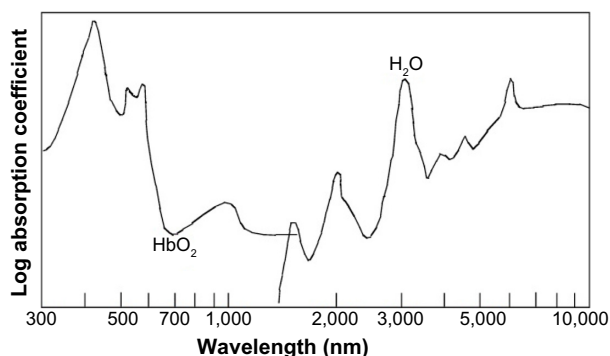
One example of the use of microvascular assessment in pathophysiology is in the field of cardiovascular disease. Studies of patients with hypertension and normotensive patients with obesity have shown structural changes in small resistance arteries by an increased tunica media to vessel lumen diameter ratio.<sup>7,8</sup> And as for hypertension, these structural changes have been correlated to a higher risk of developing stroke and myocardial infarction.<sup>7</sup> Using the post-occlusive reactive hyperemia test, a decrease in post-occlusive flow has been shown in patients with atherosclerosis.<sup>9</sup> Thus, as in this model disease, microcirculatory assessment could potentially be used to stage, monitor, and even predict pathological processes and be a useful tool in the assessment of diseases.

In this paper we aim to review the technique of non-invasive methods for imaging the microcirculation and give an overview of their clinical applications. Methods covered in this review include: videomicroscopy techniques, laser Doppler perfusion imaging (LDPI), and laser speckle contrast imaging (LSCI).

## Videomicroscopy techniques Technology

Videomicroscopy techniques can be used for direct visualization of microcirculation and involve orthogonal polarization spectral (OPS) imaging and its successor sidestream dark-field (SDF) imaging. Both techniques are based on the same underlying principles that were developed many years ago.<sup>10</sup> However, it was first in 1999 that Groner et al used OPS in a handheld device measuring microcirculation.<sup>11</sup>

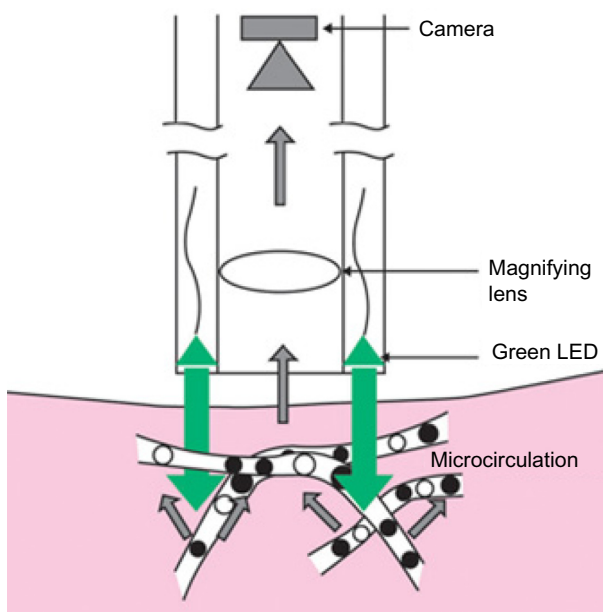
The underlying technique of OPS is described in detail by Groner et al.<sup>11</sup> Summarily, polarized light is illuminating the tissue to be examined. Only light that penetrates the tissue more deeply becomes depolarized and by sending the reflected light through a orthogonal polarizer this enables only depolarized light to be passed, thus excluding direct reflections. The collected light then forms an image of the illuminated area and can be recorded with a charge coupled device (CCD) video camera. By polarizing the light from the light source with a wavelength that is absorbed by hemoglobin (548 nm), red blood cells (RBC) will appear dark, thus forming an image of the microcirculation. This results in vessels only being visible if they contain RBC. In Figure 1, the absorption spectrum of oxygenated hemoglobin



**Figure 1** Absorption spectra in tissue of oxygenated hemoglobin ( $\text{HbO}_2$ ) and water. **Note:** The absorption of hemoglobin decreases at approximately 650 nm.

is shown. OPS imaging has been validated against intravital fluorescence microscopy and conventional capillary microscopy.<sup>12–14</sup>

Driven by the fact that a relatively strong external light source is needed in OPS imaging and the limited visualization of the capillaries due to blurring, SDF imaging was developed.<sup>15,16</sup> In SDF imaging, the light source is made up of concentrically placed light emitting diodes surrounding the optics (see Figure 2). The light emitting diodes provide pulsed green light in synchrony with the CCD frame rate, thus preventing smearing of moving objects. The whole microscope including optics and light source is housed in one handheld device. Like in OPS imaging, the light wavelength is chosen so that the RBC appear dark (530 nm). SDF imaging has been validated by comparison to OPS imaging.<sup>16</sup>



**Figure 2** Sidestream dark-field (SDF) imaging technique.

**Note:** Courtesy of MicroVision Medical <http://www.microvisionmedical.com/>.<sup>17</sup>  
**Abbreviation:** LED, light emitting diodes.

These methods allow direct visualization of the microcirculation and vessel diameter, vessel density and red blood cell velocity can be measured. Microcirculatory analysis is made with semi-automatic analysis software. Yet, some manual intervention is still needed. According to Micro-Vision Medical web page, they are working on a new software package which requires less manual intervention.<sup>17</sup> Different analyses scores of microcirculation have been developed and De Backer et al propose the use of proportion of perfused vessels (PPV), perfused vessel density, microvascular flow index (MFI), and heterogeneity index.<sup>3</sup> PPV is calculated after manually identifying the amount of vessels that have continuous or intermittent flow. Perfused vessel density is calculated by multiplying vessel density by PPV. MFI score is based on flow characterization (absent, intermittent, sluggish or normal) in the four quadrants of the recorded images of the microcirculation. Finally, heterogeneity index can be calculated by measuring the MFI in three to five sites and then taking the difference between highest MFI minus the lowest MFI divided by the mean flow velocity.

## Applications

The most studied area with these techniques is the sublingual mucosa in patients with sepsis where it has been shown that alterations in microvascular blood flow are frequent in patients with sepsis and more severe alterations have been associated with severe disease and a higher mortality rate.<sup>18,19</sup> However, several other organs have been studied such as skin, gingiva, conjunctiva, brain, lungs, tongue, liver, gut, ileostomies or colostomies, and rectal mucosa.<sup>13,20–30</sup> In liver transplants, assessment of hepatic microcirculation is reported to be predictive of early graft postoperative function and in liver resections, hepatic microcirculation parameters have been used to distinguish histologically damaged livers.<sup>27,30</sup> Figure 3 shows a typical SDF image of rat liver parenchyma.

## Advantages and limitations

The greatest advantage with videomicroscopic techniques is their direct visualization of the microcirculation. Yet, there are limitations as well. These methods are sensitive to motion and pressure artifacts.<sup>16,27,31</sup> Motion can result in movement artifacts and pressure can disturb vessel blood flow. Analysis software has a built-in image stabilization that partly deals with movement artifacts and the use of a stabilization attachment has been suggested.<sup>32,33</sup> Also, inability to measure high blood flow velocities has been reported.<sup>32,34</sup> Moreover, when using these methods on solid organs, the organ capsule has to be thin.<sup>31</sup> Otherwise, the capsule has to be removed before



**Figure 3** Sidestream dark-field (SDF) image of rat liver parenchyma.

**Note:** The wider vessel is a post-sinusoidal venule and the narrower vessels are sinusoids.

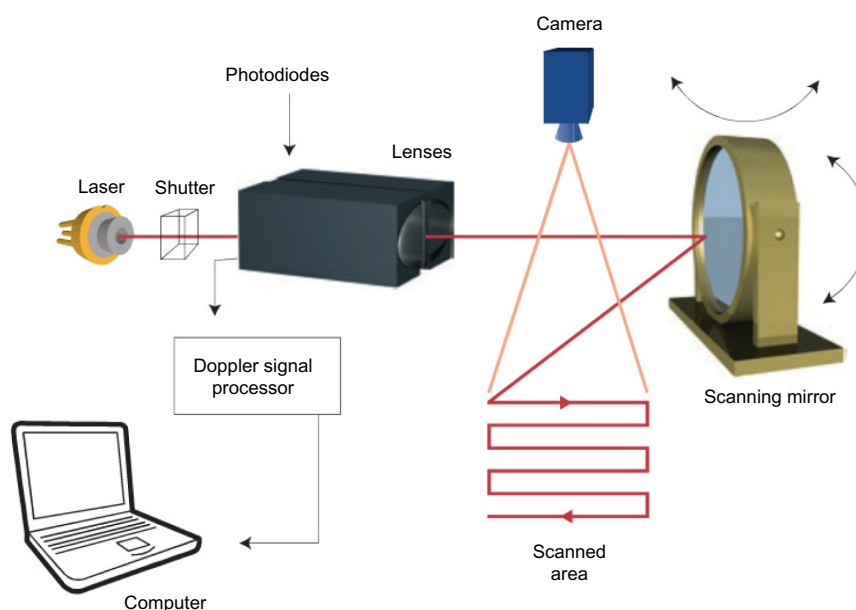
measuring.<sup>27</sup> Also, the offline analysis is time consuming, for liver analysis approximately 5 minutes per measurement point.<sup>27</sup>

## LDPI Technology

Studying retinal perfusion, Riva et al were the first to describe flow measurements in microvascular vessels using laser Doppler flowmetry.<sup>35</sup> The technique uses coherent laser light which undergoes a small shift in frequency due to the Doppler effect when striking moving particles such as RBC.<sup>36</sup> This only appears when light is reflected on moving objects and reflected light from static tissue surrounding the RBC returns with unchanged frequency. The average amount of change in frequency, called Doppler shift, in the reflected light is proportional to the product of average speed and concentration of RBC. The Doppler shift is the output of laser Doppler flowmetry.

Laser Doppler flowmetry is a single-point technique measuring an average of the microcirculation in about 1 mm<sup>3</sup> of tissue. By combining several single measurements over a tissue surface one can create an image of microcirculation of the tissue. This technique is called LDPI.<sup>37–39</sup> The standard LDPI apparatus uses a movable mirror that directs the laser beam on the different measurement points, scanning the tissue surface of an area up to 50×50 cm<sup>2</sup>.<sup>40</sup> Figure 4 illustrates a principal model of the LDPI technique.

Using this approach of mapping with subsequent measuring points is both time consuming and produces large amounts of raw data requiring long processing times. Classically, this has impeded imaging of dynamic processes



**Figure 4** Laser Doppler perfusion imaging technique.

**Note:** Courtesy of Moor Instruments <http://gb.moor.co.uk/>.<sup>70</sup>

such as functional tests and increased the susceptibility to motion artifacts.<sup>5,36,40</sup> However, in recent years, the introductions of high-speed complementary metal-oxide semiconductor cameras in combination with new ways of mapping algorithms, have shortened measurement times for LDPI substantially.<sup>41–43</sup> The experience of these high-speed detectors in clinical settings is still small as compared to the standard mapping techniques.

Measurement depth with LDPI is dependent on laser wavelength and tissue properties but ranges from 1 to 1.5 mm.<sup>44</sup> This is deeper than for LSCI (described in the LSCI section) and has to be accounted for when choosing a method for the specific tissue to be studied.

## Applications

LDPI has been tested on a large range of organs, skin being the most frequent because of its easy accessibility. One dermatologic application is the use of LDPI for differentiation between malignant and benign skin lesions.<sup>45</sup> Further, several studies have been conducted studying different kinds of wounds, including ischemic ulcers, diabetic foot ulcers, and skin burn wounds.<sup>46</sup> Studying healing wounds, Gschwandtner et al, have shown increased perfusion in areas of granulation as a marker of angiogenesis, indicating that areas with low perfusion have diminished healing potential.<sup>47</sup>

Equally, in evaluation of perfusion in skin burns, LDPI can be used to grade the severity of damage of the burnt tissue.<sup>48</sup> A high flux indicates superficial damage and low flux

a deeper injury. This knowledge has been used to develop a prognostic tool for healing time and helping to decide which patients are in need of surgical treatment.<sup>49</sup> In general, prognostic information about healing potential may be used to assist in the choice of wound therapy.

In the pathogenesis of diabetic foot ulcers both micro-angiopathy and autonomous neuropathy contribute to development of ulcers. Besides studying the angiogenesis of the wound healing process, LDPI has been used to study the neural component of the pathogenesis. By using a functional test, using heating and cooling of fingers, the autonomous nerve function have shown to be impaired in the vessels of diabetic patients.<sup>50</sup>

In addition, application on internal organs has been made in intra-operative settings. Hajivassiliou et al used LDPI on patients undergoing colectomies for inflammatory bowel disease and found inflammatory bowels to have an increased blood flow as compared to normal.<sup>51</sup> Studies implementing LDPI in neurosurgery have been carried out in animal models. In a model of cerebral ischemia, Liu et al used LDPI to monitor an increase in cerebral perfusion as a response to albumin infusion.<sup>52</sup>

## Advantages and limitations

On the contrary to videomicroscopy techniques, LDPI has the advantage of being a non-contact method, avoiding interaction with the studied tissue and thus avoiding the generation of pressure artifacts. Furthermore, the possibility

of measuring large areas with a good spatial resolution gives LDPI a good reproducibility.<sup>5,53</sup> However, measuring average Doppler shift, LDPI cannot evaluate absolute flow properties in eg, mL/s but rather measure relative comparisons of flux which are based on a normalized baseline value and presented as arbitrary flux units.<sup>54</sup>

The LDPI apparatus requires calibration before measurement due to the presence of a biological zero signal. Even during complete flow occlusion, the LDPI output signal would not be zero due to noise in the Doppler signal, denoted as the biological zero. The noise has been suggested to consist of local redistribution of blood cells within the vessels and Brownian motions of molecules.<sup>40</sup> How to interpret and handle the biological zero is under debate and needs to be investigated further.<sup>55,56</sup>

In addition, the standard LDPI setting using a scanning technique requires measurement times of about a minute, which gives the method a low temporal resolution, unsuitable for functional tests. The new high-speed methods may provide a solution to the problem, but currently the clinical experience is low.

## LSCI Technology

Another laser based technique for microvascular imaging is LSCI. Laser light illuminating biological tissue gives rise to a light phenomenon called laser speckle.<sup>57</sup> Laser speckle arises from the irregularities in the structure of the tissue, which backscatter the laser light irregularly, creating dark and light interference patterns. These patterns can be detected by a CCD camera. The speckle pattern of tissue changes with movement within the tissue such as blood flow,<sup>58</sup> creating blurring of the image on the capturing camera. Speckle contrast is a quantification of the blurring at a given exposure time of the camera. Increased blood flow will increase image blurring thus lowering the contrast which is measured as the ratio of the standard deviation to the mean grayscale intensity in a square of pixels (eg, 5×5 pixels), thus representing the average velocity and concentration of moving particles in that square.<sup>44</sup> LDPI and LSCI are related methods but rely on different physical theories and have different ways of data sampling. LSCI does not use a scanning technique as LDPI but instead measures nearly instantly the whole tissue under study enabling fast measurements with a high sampling rate. As for LDPI, LSCI measures average velocity and data are presented in an arbitrary unit.

A correlation of perfusion results between the two methods at different perfusion rates has been made showing LSCI to have a non-linear relation to blood flow and to LDPI,

especially at low blood flows.<sup>59</sup> The need for a new algorithm for comparison of the methods has been suggested.<sup>60</sup> However, LSCI measuring depth is more superficial at about 300 µm as compared to the measuring depth of 1–1.5 mm of LDPI, which has to be accounted for when choosing a measuring technique for specific organs.<sup>40</sup> On skin, for example, LSCI measures the more superficial slower flowing vessels while LDPI measures deeper, faster flowing vessels hence giving different results.

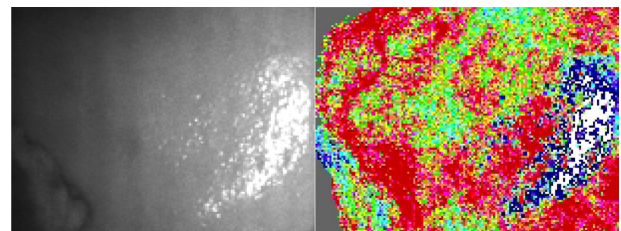
## Applications

Briers and Fercher made the first clinical measurements with laser speckle photography on retinal perfusion in the 1980s<sup>61</sup> and later developments of the technique led to real-time perfusion imaging with LSCI.<sup>62,63</sup> Having faster temporal resolution than standard LDPI setups, LSCI has proven a useful method in functional tests of skin microcirculation.<sup>1</sup> For instance, studies of burn injuries have correlated faster healing times with increased perfusion in the first week post-injury assessed with LSCI.<sup>64</sup> Further, LSCI has been of interest in the assessment of intraoperative cerebral microcirculation where local cerebral blood flow has been measured after revascularization surgery.<sup>65</sup> Bezemer et al have proposed LSCI for monitoring renal cortex ischemia/reperfusion injury.<sup>6</sup> LSCI has also proven useful in the assessment of hepatic microcirculation during liver resection surgery.<sup>33,66</sup> A typical example of an LSCI measurement of human liver is shown in Figure 5.

## Advantages and limitations

An advantage of LSCI is its fast measurement time, nearly instantly measuring the microcirculation over a large area. This makes LSCI suitable for dynamic functional tests requiring high temporal resolution. Comparative studies of LDPI and LSCI have been made highlighting the advantages of faster measurement time with LSCI compared to LDPI.<sup>40,67</sup> In addition, LSCI has good reproducibility.<sup>5</sup> Another advantage is that the method is non-contact, not interacting with the tissue under study.

However, LSCI is sensitive to movement artifacts.<sup>1,66</sup> Techniques of handling these artifacts have been suggested



**Figure 5** Laser speckle contrast image of human liver.  
**Note:** The color scale represents blood flow level.

**Table 1** Overview of microcirculation imaging methods

	<b>Videomicroscopy (OPS imaging, SDF imaging)</b>	<b>Laser Doppler perfusion imaging</b>	<b>Laser speckle contrast imaging</b>
Variables measured	Vessel diameter, vessel density, RBC velocity, heterogeneity of perfusion	RBC mean velocity, RBC concentration	RBC mean velocity, RBC concentration
Contact	Yes	No	No
Measuring depth	~500 $\mu$ m	~1–1.5 mm	~300 $\mu$ m
Pros	Direct visualization of microcirculation	Non-contact	Non-contact, fast
Cons	Motion artifacts, pressure artifacts, time consuming analysis	Motion artifacts, long measurement time, relative measurements	Motion artifacts, relative measurements

**Abbreviations:** OPS, orthogonal polarization spectral; SDF, sidestream dark-field; RBC, red blood cells.

by using an opaque reference area for subtraction of artifact signals.<sup>68,69</sup>

Relying on similar physical principles as LDPI, LSCI also suffers from a biological zero signal, but for LSCI it is even larger. Likewise, because the LSCI signal is based on the average velocity and concentration of RBC, values cannot be given in absolute numbers, but are limited to relative measurements.

## Conclusion and future challenges

In this paper we have reviewed three different techniques for imaging the microcirculation and presented examples of several different clinical applications. When choosing a method for study of a specific organ and pathological process it is important to consider the different properties of the methods. To measure the dynamic processes of functional tests, imaging methods with high temporal resolution have to be used, thus methods with fast measuring times are required. Differences in measurement depth have to be considered as the differences in optical properties of tissues.

The non-contact methods do not affect the tissue with pressure. However, they are more susceptible to motion artifacts, which both LDPI and LSCI cannot automatically differentiate from the movements of RBC. Further, LDPI and LSCI measures relative flow properties and are in need of calibration due to a relatively large biological zero signal, which is not the case for videomicroscopy techniques. Videomicroscopy techniques also have the benefit of offering direct visualization of microcirculation. In Table 1, the major differences between the methods are presented.

Regardless of the choice of technique, a challenge lies in the interpretation of the measurement output and its relation to physiological and pathological processes. The methods offer several output variables and careful thought has to be given to which one is of importance. In an attempt to solve this problem, expert conferences have been carried out, trying

to set standards for experimental settings and define output variables of each technique.<sup>3,54</sup>

Another challenge is to compare microcirculatory results between different methods. Several studies have been conducted, attempting to compare the results of different techniques.<sup>33,59,60</sup> These are important efforts for the understanding of the microvascular results and will make microcirculatory imaging more accessible for use in the clinical assessment of patients.

In the authors' opinion, future improvement of imaging methods should focus on developing methods which allow measurement without interaction of the studied tissue, such as a non-contact method. In addition, measurements must be fast to decrease vulnerability to motion artifacts and making it possible to study dynamic processes. To simplify the interpretation of the output, data should be given in an absolute variable, for example flow in mL/s. Finally data analysis should be automatic.

Measurement of microcirculation can be applied to many organs in various pathologies. Above, examples of clinical fields of applications have been presented. The numerous skin applications described above are an example of how imaging techniques can be used to assist the clinician in staging, monitoring, and even predicting pathological processes and be a useful tool in the assessment of patients. Still, great potential lies in the implementation of microvascular imaging systems for intraoperative assessment and future studies may outline new fields of use.

## Disclosure

The authors report no conflicts of interest in this work.

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