#### ORIGINAL RESEARCH

# Investigation of a cuboidal permanent magnet's force exerted on a robotic capsule

#### Wan'an Yang<sup>1</sup> Chengbing Tang<sup>2</sup> Fengqing Qin<sup>1</sup>

<sup>1</sup>School of Computer and Information Engineering, Yibin University, Yibin, <sup>2</sup>CNPC Chuanqing Geophysical Prospecting Company Research Center Computer Department, Chengdu, Sichuan, People's Republic of China

Correspondence: Wan'an Yang School of Computer and Information Engineering, Yibin University, 8 Wuliangye Avenue, East Jiusheng Road, Yibin, Sichuan 644000, People's Republic of China Email ywaly@126.com **Abstract:** To control and drive a robotic capsule accurately from outside a patient's body, we present a schema in which the capsule enclosing the imaging device, circuits, batteries, etc is looped by a permanent magnet ring that acts as an actuator. A cuboidal permanent magnet situated outside the patient's body attracts or pushes the magnet ring from different directions to make the capsule move or rotate. A mathematic model of attractive or repulsive force that the cuboidal magnet exerts on the magnet ring is presented for accurate calculation of force. The experiments showed that the measuring force was in agreement with the theoretical one, and the relations between the dimensions of the cuboidal magnet and force are useful to produce a cuboidal magnet with optimal shape to get appropriate force.

**Keywords:** control and drive, robotic capsule, permanent magnet ring, optimal dimension, force model

#### Introduction

Wireless capsule endoscopy is advantageous because it provides clear pictures of the gastrointestinal (GI) tract.<sup>1-4</sup> Based on these pictures, it is easier for doctors to diagnose specific diseases, such as stomach ulcers, colon cancers, Crohn's disease, ulcerative colitis, etc, in the whole GI tract. However, the clinical products currently available are passive devices whose locomotion is driven by natural peristalsis, with the drawback of failing to capture the images of important GI-tract regions, since the doctor is unable to control the capsule's motion and orientation.<sup>5</sup> To address these limitations, many research groups are working to develop active locomotion devices that allow capsule endoscopy to be performed in a totally controlled manner. This would enable the doctor to steer the capsule toward interesting pathological areas and to accomplish medical tasks.

There are principally two strategies for providing a swallowable capsule with active locomotion.<sup>6</sup> One is pursuing the miniaturization of locomotion systems to be integrated onboard the capsule. The main limit of this approach is the high amount of energy needed to be stored on board in order to actuate the mechanism.<sup>7</sup> The alternative relies on an external approach, where actuation, generally based on magnetic fields, is outside the capsule.

For instance, Ciuti et al described an approach to guide capsular endoscopy by using an internal cylindrical permanent magnet with a diameter of 3 mm, a length of 10 mm, and an external permanent magnet with a diameter of 60 mm and a length of 70 mm.<sup>7</sup> Also, Ciuti et al deployed an endoscopic capsule prototype incorporating a permanent magnet with a length of 19.1 mm and a diameter of 3.2 mm. Ex vivo

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© 2014 Yang et al. This work is published by Dove Medical Press Limited, and licensed under Creative Commons Attribution — Non Commercial (unported, v3.0) permission from Dove Medical Press Limited, provided the work is properly attributed. Permissions beyond the scope of the License are administered by Dove Medical Press Limited, Information on how to request permission may be found at: http://www.dovepress.com/permissions.pp and in vivo experiments stated capsular endoscopy was successfully maneuvered.<sup>8</sup> Mahoney and Abbott showed 5 degrees-of-freedom manipulation of a magnetic capsule in fluid. The capsule contained a cube neodymium magnet arranged parallel to the capsule's principal axis; the remainder of the capsule's volume was filled with air. A feedback controller, using the triangulated capsule position obtained from the vision system, was used to move the capsule to any desired position in the workspace.<sup>9</sup> Keller et al also reported a system for remote magnetic control of a wireless capsule endoscope in the esophagus. The results showed that remote control of the magnetic maneuverable capsule in the esophagus of healthy volunteers was safe and feasible.<sup>10</sup> Other scholars investigated the feasibility and safety of magnetically guided capsule endoscopy in the human stomach.<sup>11–13</sup>

In summary, these magnetically controlled systems consist of capsule endoscopy incorporating a magnet, a guidance magnet robot, a data recorder, and a computer workstation with software for real-time view and control. The guidance magnet robot provides 5 or 6 degrees of control freedom.

Some scholars also proposed that a small cylindrical permanent magnet was enclosed in the capsule to obtain three-dimensional localization and two-dimensional orientation parameters.<sup>14,15</sup> Other scholars also suggest that a small cuboidal magnet be enclosed in the capsule to obtain whole six-dimensional parameters.<sup>16,17</sup>

However, the limited volume available for both the locomotion and localization mechanisms makes system integration quite challenging. The PillCam<sup>®</sup> (Given Imaging, Yoqneam, Israel)<sup>18</sup> is 11 mm in diameter and 26 mm long, with such components as circuits, imaging device, and batteries enclosed in the capsule. The addition of an extra magnet would make the final device hard to swallow. Therefore, we present an approach in which the capsule is looped by a permanent magnet ring of 1 mm thickness, which only increases the dimension of the robotic capsule a little. In this paper, we investigate the force that the cuboidal permanent magnet exerts on the permanent magnet ring when maneuvering the capsule.

# Mathematical model of the force produced by the permanent magnet

The incremental magnetic force,  $d\vec{F}$ , acting on an infinitesimal element (dV) of a magnet is given by Kelvin's formula<sup>19</sup>:

$$d\vec{F} = \mu_0 \nabla(\vec{M} \cdot \vec{H}), \tag{1}$$

where  $\vec{M}$  is the magnetization and  $\vec{H}$  is the external magnetic field strength. The total force acting on the magnet ring is

obtained by integrating the differential force over the magnet ring volume -V:

$$\vec{F}_{magnet} = \int_{V} d\vec{F} dV.$$
 (2)

Provided that the permanent magnet is uniformly magnetized with constant magnetization,  $M_0$ , in the z-direction (ie,  $\vec{M} = M_0 \vec{z}$ ), according to Equation 2, the gradient of the dot product  $\vec{M} \cdot \vec{H}_{ext}$  is integrated over the magnet volume to obtain the vector force acting on the magnet. This resultant vector force has both axial and lateral components. The axial component is computed based on the z-component of the gradient, and the lateral components based on the x- and y-components. The external magnetic field strength,  $\vec{H}$ , also has x-, y- and z-components:  $H_x$ ,  $H_y$ , and  $H_z$ . Although a certain component of magnetic field strength is the main contributor to the same component of force, the other two components of magnetic field strength cannot be ignored in the mathematic model. Therefore, the complete force expressions are given by:

$$\vec{F}_{x} = \int_{V} d\vec{F}_{x} = \mu_{0} M_{0} \int_{V} \frac{\partial}{\partial x} (H_{x}) + \frac{\partial}{\partial x} (H_{y}) + \frac{\partial}{\partial x} (H_{z}),$$
(3)

$$\vec{F}_{y} = \int_{V} d\vec{F}_{y} = \mu_{0} M_{0} \int_{V} \frac{\partial}{\partial y} (H_{x}) + \frac{\partial}{\partial y} (H_{y}) + \frac{\partial}{\partial y} (H_{z}),$$
(4)

and

$$\vec{F}_{z} = \int_{V} d\vec{F}_{z} = \mu_{0} M_{0} \int_{V} \frac{\partial}{\partial z} (H_{x}) + \frac{\partial}{\partial z} (H_{y}) + \frac{\partial}{\partial z} (H_{z}).$$
(5)

#### H-field strength of the permanent magnet

According to Equations 3-5, the magnetic field strength produced by the second magnet must be explicitly known to calculate the force. In the case of the magnetic field strength acting on the magnet being produced by a second permanent magnet, the method of equivalent magnetizing current (amperian current) is used to investigate the *H*-field established by the second permanent magnet.<sup>20,21</sup> The approach is valid only for uniform media; therefore, the relative permeability of the magnets must be assumed to be uniform.

# Analytical expression of *H*-field strength of the cuboidal magnet

The cuboidal magnet is shown in Figure 1. P(x, y, z) is an external spatial point around the magnet. The magnetization is in the *z*-direction, and the surface current lays on the four planes, which are parallel with the x - z and y - z planes, respectively. Supposing that the magnetization of air is zero, the three-dimensional magnetic field strengths at point *P* are shown by Equations 6–8:

$$H_{x} = -\frac{k}{2} [\Gamma(L-x, y, z) + \Gamma(L-x, W-y, z) - \Gamma(x, y, z) - \Gamma(x, W-y, z)],$$
(6)

$$H_{y} = -\frac{k}{2} [\Gamma(W - y, x, z) + \Gamma(W - y, L - x, z) - \Gamma(y, x, z) - \Gamma(y, L - x, z)],$$
(7)

$$\begin{split} H_z = -k[\Phi(y,L-x,z) + \Phi(W-y,L-x,z) + \Phi(x,W-y,z) \\ &+ \Phi(L-x,W-y,z) + \Phi(W-y,x,z) + \Phi(y,x,z) \\ &+ \Phi(L-x,y,z) + \Phi(x,y,z)], \end{split}$$

where  $k = J/4\pi$ , *J* is the surface-current density on the planes being parallel to the plane XOY, and

$$\Gamma(r_1, r_2, r_3) = \ln \frac{\sqrt{r_1^2 + r_2^2 + (r_3 - \hat{z})^2} - r_2}{\sqrt{r_1^2 + r_2^2 + (r_3 - \hat{z})^2} + r_2} \Big|_{\hat{z}=0}^{\hat{z}=H}$$
(9)

$$\Phi(\phi_1,\phi_2,\phi_3) = \begin{cases} tg^{-1} & \left[ \frac{\phi_1}{\phi_2} \frac{\phi_3 \hat{z}}{\sqrt{\phi_1^2 + \phi_2^2 + (\phi_3 - \hat{z})^2}} \right]_{\hat{z}=0}^{\hat{z}=H} (y \neq 0) \\ 0 & (y=0) \end{cases}$$
(10)

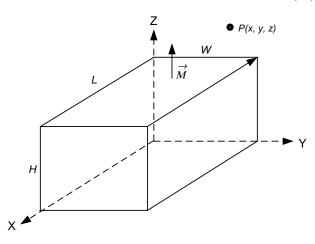


Figure I Cuboidal magnet coordinate schema.

# Calculation of force $\vec{F}_z$

The forces in the *x*- and *y*-directions approximate to zero, and thus the force in the *z*-direction,  $\vec{F_z}$ , was used to drive the robotic capsule. It is important to calculate the partial derivative of the cuboidal magnet's *H*-field strength before calculating  $\vec{F_z}$ . The expressions of the cuboidal magnet's *H*-field strengths shown by Equations 6–8 are analytical, so the partial derivatives of the magnet's *H*-field strengths should be analytical.  $\partial/\partial z(H_x)$ ,  $\partial/\partial z(H_y)$ ,  $\partial/\partial z(H_z)$  are as follows:

$$\frac{\partial}{\partial z}(H_x) = -\frac{k}{2} [\Gamma'_{r_3}(L-x,y,z) + \Gamma'_{r_3}(L-x,W-y,z) - \Gamma'_{r_3}(x,y,z) - \Gamma'_{r_3}(x,W-y,z)], \quad (11)$$

$$\frac{\partial}{\partial z}(H_{y}) = -\frac{k}{2} [\Gamma'_{r_{3}}(W - y, x, z) + \Gamma'_{r_{3}}(W - y, L - x, z) - \Gamma'_{r_{3}}(y, x, z) - \Gamma'_{r_{3}}(y, L - x, z)], \quad (12)$$

$$\frac{\partial}{\partial z}(H_z) = -k[\Phi'_{r_3}(y, L-x, z) + \Phi'_{r_3}(W-y, L-x, z) + \Phi'_{r_3}(x, W-y, z) + \Phi'_{r_3}(L-x, W-y, z) + \Phi'_{r_3}(W-y, x, z) + \Phi'_{r_3}(y, x, z) + \Phi'_{r_3}(L-x, y, z) + \Phi'_{r_3}(x, y, z)],$$
(13)

where:

$$\Gamma_{r_{5}}'(r_{1}, r_{2}, r_{3}) = \frac{\omega(r_{1}, r_{2}, r_{3}) + r_{2}}{\omega(r_{1}, r_{2}, r_{3}) - r_{2}} \\
\cdot \frac{(\omega(r_{1}, r_{2}, r_{3}) + r_{2}) \cdot (r_{3} - \hat{z}) - (\omega(r_{1}, r_{2}, r_{3}) - r_{2})(r_{3} - \hat{z})}{(\omega(r_{1}, r_{2}, r_{3}) + r_{2})^{2} \cdot \omega(r_{1}, r_{2}, r_{3})} |_{\hat{z}=0}^{\hat{z}=H},$$
(14)

$$\begin{split} \Phi_{r_{3}}'(\phi_{1},\phi_{2},\phi_{3}) &= \frac{1}{1 + \left(\frac{\phi_{1}}{\phi_{2}} \cdot \frac{\phi_{3} - \hat{z}}{\omega(\phi_{1},\phi_{2},\phi_{3})}\right)^{2}} \cdot \frac{\phi_{1}}{\phi_{2}} \\ \cdot \frac{\omega(\phi_{1},\phi_{2},\phi_{3}) - (\phi_{3} - \hat{z})^{2} \omega^{-1}(\phi_{1},\phi_{2},\phi_{3})}{\omega^{2}(\phi_{1},\phi_{2},\phi_{3})} |_{\hat{z}=0}^{\hat{z}=H} (y \neq 0), \end{split}$$

$$(15)$$

and

 $\omega(\xi_1,\xi_2,\xi_3) = \sqrt{\xi_1^2 + \xi_2^2 + (\xi_3 - \hat{z})^2}.$  (16)

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After substituting Equations 11–16 into Equation 5, the force  $\vec{F}_z$  can be calculated by the triple integral over the magnet-ring volume. With MatLab 7.0 (MathWorks, Natick, MA, USA), the double integral is calculated by the function quad2d, and then the integral is obtained by using the function quad1.

### Methods and results Force $(\vec{F}_z)$ that the cuboidal magnet exerts on the magnet ring

In order to validate the mathematic model of the force, we measured the attractive force of a cuboidal permanent magnet (regarded as the source magnet) with length 5 cm, width 1 cm, and height 0.3 cm exerted on the magnet ring (regarded as the target magnet), whose outer radius, inner radius, and H were 0.95, 0.75, and 0.9 cm, respectively, using a Sundoo force gauge (Wenzhou Sundoo Instruments, Wenzhou, People's Republic of China). The parameter k of the cuboidal magnet in Equations 11-13 equaled 49,677, and the magnetization,  $M_0$ , of the magnet ring in Equations 3–5 was  $1.21 \times 10^6$  (A/m). The force gauge's capacity was 2 N and its resolution was 0.001 N. The measurement was carried out in an unshielded room at normal temperature. The magnet ring was over the cuboidal magnet (see Figure 2). Their magnetizations were in the z-direction (upward). The magnet ring and force gauge were connected through a rigid thread. To prevent force-gauge damage when the force exceeded the maximum capacity, organic glass was put between the magnet ring and cuboidal magnet. The measured forces and locations of the magnet ring are listed in Table 1. The results showed that the measured forces agreed with the theoretical values, as shown in Figure 3.

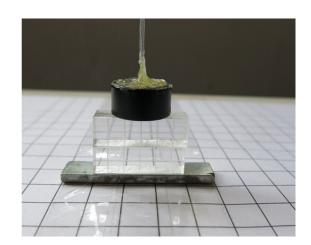


Figure 2 Cuboidal magnet and magnet ring.

 
 Table I Measured forces that the cuboidal magnet exerted on the magnet ring

Bottom center of the magnet ring			Measured
X (cm)	Y (cm)	Z (cm)	force (N)
2.5	0.5	1.3	1.028
2.5	0.5	1.8	0.656
2.5	0.5	2.3	0.426
2.5	0.5	2.8	0.277
2.5	0.5	3.3	0.184
2.5	0.5	3.9	0.126

### Shape's effect on force $(\vec{F}_z)$

It is meaningful to find relationships between each shape parameter and the force  $-\vec{F}_z$ . If the relations are known in advance, a magnet of optimal shape can be made to obtain appropriate force. A cuboidal magnet has three shape parameters: length, width, and height. As any parameter may vary arbitrarily, it is inconvenient to investigate how the three parameters affect force at the same time. Therefore, we fixed the other two parameters while investigating one parameter's effects on force variation.

Firstly, the length or width of the cuboidal magnet is fixed, and the height changes. The force  $\vec{F_z}$  variation trends with the cuboidal magnet's height are shown in Figure 4. It can be seen from Figure 4 that the force always increased with the increasing height of the cuboidal magnet, no matter what the width or length of the magnet was. An interesting thing that should be noted is that the magnitude of force  $\vec{F_z}$  increased slowly with increasing width or length of the cuboidal magnet.

Secondly, the height or width of the cuboidal magnet was fixed, and the length varied. The force  $\vec{F}_z$  variation trends

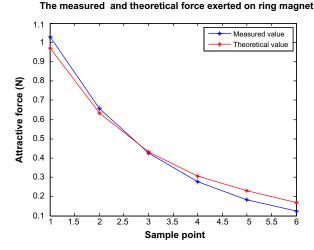
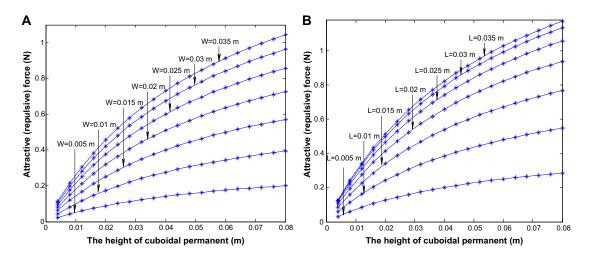
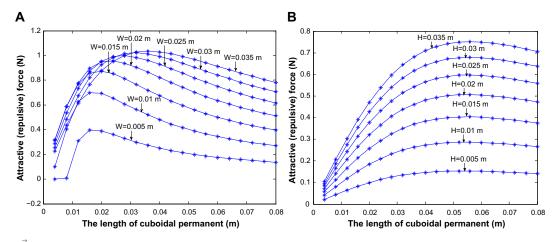


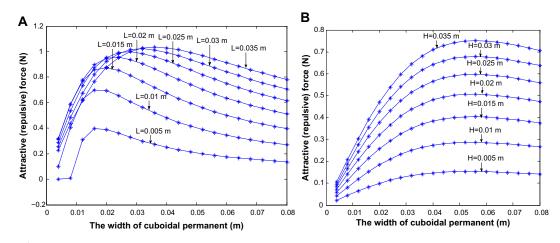
Figure 3 Measured and theoretical force  $(\,\vec{F}_{\rm z}\,)$  that the cuboidal magnet exerted on the magnet ring.



**Figure 4** Force  $(\vec{F}_{z})$  variation versus the height of the cuboidal magnet **Note:** (A) The force variation as the length is fixed; (B) the force variation as the width is fixed. **Abbreviations:** W, width; L, length.



**Figure 5** Force  $(\vec{F}_z)$  variation versus the length of the cuboidal magnet **Note:** (A) The force variation as the height is fixed; (B) the force variation as the width is fixed. **Abbreviations:** W, width; L, length.



**Figure 6** Force  $(\vec{F}_{,j})$  variation versus the width of the cuboidal magnet **Note:** (**A**) The force variation as the height is fixed; (**B**) the force variation as the length is fixed. **Abbreviations:** W, width; L, length.

with the cuboidal magnet's length are shown in Figure 5. This shows that the force increased with increasing length at the beginning, whatever the width or the height; after the force reached a maximum, it went down as the length continued to increase.

Thirdly, the height and length of the cuboidal magnet was fixed, and the width varied. The cuboidal magnet's width effects on force  $\vec{F_z}$  are shown in Figure 6. We found that the force-variation trend was the same as that in Figure 5.

According to Figures 4–6, it can be concluded that force  $\vec{F}_z$  will increase with the cuboidal magnet's height, and the force will maximize when the width and length are certain values.

#### **Conclusion and future work**

Some scholars have testified that a remote magnetic maneuver for a robotic capsule enclosing a magnet is feasible. The problem is that the volume of the robotic capsule is limited, because the batteries, circuits, camera, etc are incorporated. If an extra magnet is contained within it, system integration will be quite challenging. Expansion of the dimensions of a robotic capsule makes it hard to swallow. To address this problem, we propose that the capsule is looped by a magnet ring of 1 mm thickness, and maneuvered by a cuboidal magnet.

In this paper, we presented a mathematical model of force that a permanent magnet exerts on another permanent magnet. The experiments showed that the measurement values were in agreement with the theoretical values. The experiments also showed that the magnetic force can be adjusted by changing the dimensions of the cuboidal magnet. According to the mathematical model, the optimal cuboidal magnet can be calculated accurately in advance. In the future, we will investigate the cylindrical magnet's force on the magnet ring, and we will also study the force that the new robotic capsule needs when it moves forward in the whole GI tract.

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# Disclosure

The authors report no conflicts of interest in this work.

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