The application of EDTA in drug delivery systems: doxorubicin liposomes loaded via NH$_4$EDTA gradient

Yanzhi Song¹
Zhenjun Huang¹
Yang Song²
Qingjing Tian¹
Xinrong Liu¹
Zhennan She¹
Jiao Jiao¹
Eliza Lu³
Yihui Deng¹

¹College of Pharmacy, Shenyang Pharmaceutical University, Shenyang, People’s Republic of China; ²Jiangsu Hansoh Pharmaceutical Co., Ltd., Lianyungang, People’s Republic of China; ³Livzon Mabpharm Inc., Zhuhai, People’s Republic of China

Abstract: The applications of ethylenediaminetetraacetic acid (EDTA) have been expanded from the treatment of heavy metal poisoning to chelation therapies for atherosclerosis, heart disease, and cancers, in which EDTA reduces morbidity and mortality by chelating toxic metal ions. In this study, EDTA was used in a drug delivery system by adopting an NH$_4$EDTA gradient method to load doxorubicin into liposomes with the goal of increasing therapeutic effects and decreasing drug-related cytotoxicity. The particle size of the optimum NH$_4$EDTA gradient liposomes was 79.4±1.87 nm, and the entrapment efficiency was 95.54±0.59%. In vitro studies revealed that liposomes prepared using an NH$_4$EDTA gradient possessed long-term stability and delayed drug release. The in vivo studies also showed the superiority of the new doxorubicin formulation. Compared with an equivalent drug dose (5 mg/kg) prepared by (NH$_4$)$_2$SO$_4$ gradient, NH$_4$EDTA gradient liposomes showed no significant differences in tumor inhibition ratio, but cardiotoxicity and liposome-related immune organ damage were lower, and no drug-related deaths were observed. These results show that use of the NH$_4$EDTA gradient method to load doxorubicin into liposomes could significantly reduce drug toxicity without influencing antitumor activity.

Keywords: NH$_4$EDTA, liposome, doxorubicin, ion gradient, antitumor activity, toxicity

Introduction

Ethylenediaminetetraacetic acid (EDTA) is a general chelating agent that was approved by the US Food and Drug Administration for the treatment of heavy metal poisoning in the early 1950s, and remains the first choice for such treatment.¹⁻⁴ From the earliest clinical trials, EDTA-mediated chelation therapy has consistently demonstrated a remarkable ability to cleanse the organism of metals and other deposits that are responsible for atherosclerosis, heart disease, and cancers.⁷⁻¹² It has been reported that EDTA can reduce radical reactions and oxidation processes by chelating toxic metals that are responsible for cell membrane injury.¹³ EDTA and its analogs are inhibitors of calcium/calmodulin-dependent protein kinase II and protein kinase C, which play important roles in the occurrence and development of numerous diseases.¹⁴ EDTA can mitigate hypercalcemia, soften arteries, and reduce the incidence of osteoporosis by chelating calcium ions,¹⁵,¹⁶ and it can also reduce cancer mortality by inhibiting suppression of the immune system.¹⁰,¹⁷,¹⁸ Furthermore, EDTA can improve the stability of preparations by inhibiting bacterial contamination via chelating divalent metal ions, which are essential for germs.¹⁹

Doxorubicin (DOX) is one of the best-known members of the anthracycline family of antibiotics. It was first introduced in the 1960s and was widely utilized against...
hematological and solid tumors. However, the antitumor
effects of DOX were often followed by numerous undesired
side effects, in particular serious cardiotoxicity, which
led to research devoted to investigating the mechanisms of
its antitumor and cardiotoxic effects, and the relationship
between them. Although the mechanisms might overlap
to some extent, it is generally thought that DOX exerts
its antitumor effects and cardiotoxicity by distinct mecha-
nisms: the former is associated with DNA intercalation,
topo Isomerase-II inhibition, and apoptosis, while the latter is
mainly mediated by oxidative stress. Trace element research
also showed that the antitumor effects of DOX generally do
not require the participation of transition metal ions, while
its cardiotoxic effects do. Therefore, it is believed that
the antitumor effects of DOX will not be influenced by a
decreased concentration of transition metal ions in vivo,
but that cardiotoxicity will be weakened by the reduction in
reactive oxygen species (ROS).

Thus far, a common approach to prevent DOX-related
cardiotoxicity has been to employ drug carriers that utilize
an enhanced permeation and retention effect to alter tissue
distribution and pharmacokinetics of the drug. The loading
of DOX into liposomes by the application of a trans-
membrane NH$_4$EDTA gradient method should maintain the
advantages of liposomes and also afford several other known
and potential benefits. First, intraliposomal EDTA should
increase the stability of liposomal formulations by inhibiting
bacterial contamination and the catalytic effect of metal ions
on lipids. Second, EDTA reduces the generation of ROS
by chelating transition metal ions, which should decrease
damage to the cardiomyocyte membrane and reduce the
risk of DOX-related cardiomyopathy. Previous studies
have shown that liposomes prepared by a transmembrane
NH$_4$EDTA gradient method can significantly increase
drug retention and decrease liposome-related damage to
the immune system compared with liposomes prepared by
other gradient methods. Finally, EDTA binds to calcium,
which should lead to a decreased incidence rate of
hypercalcemia and improve the quality of life of advanced
cancer patients.

In this paper, EDTA was used in a drug delivery sys-
tem to encapsulate doxorubicin into liposomes using a
transmembrane NH$_4$EDTA gradient. Through comparison
with the classic ammonium sulfate gradient method, it was
investigated whether liposomes prepared via an NH$_4$EDTA
gradient show superior therapeutic efficacy and decreased
toxicity as well as the potential advantages of EDTA men-
tioned above.

Materials and methods

Materials

DOX hydrochloride was provided by Huafeng Lianbo
Technology Co. Ltd. (Beijing, People’s Republic of China).
Hydrogenated soy phosphatidylincholine (HSPC; MW 785)
was obtained from Lucas Meyer GmbH (Düsseldorf,
Germany). Cholesterol (CH) was supplied by Nanjing Xinbai
Pharmaceutical Co. Ltd. (Nanjing, People’s Republic of
China). 1,2-Distearoyl-sn-glycero-3-phosphoethanolamine-
N-(methoxy[polyethylene glycol]-2000) (mPEG$_{2000}$-DSPE)
was purchased from J&K Scientific (Beijing, People’s
Republic of China). Sephadex$^\text{TM}$ G-50 (medium) was obtained
from Sigma-Aldrich (St Louis, MO, USA). All other reagents
were of analytical grade.

Animals

Male Kunming mice weighing 18–22 g were purchased from the
Experimental Animal Center of Shenyang Pharmaceutical
University (Shenyang, People’s Republic of China). All mice had free access to food and water and all animal
experiments were in accordance with the guidelines for the
Care and Use of Laboratory Animals at Shenyang Pharmaceutical
University.

Preparation of liposomes

Liposomes were prepared using a modified ethanol injection
method. Briefly, a lipid mixture containing HSPC/CH/
mPEG$_{2000}$-DSPE (3:1:1, w/w/w) was dissolved in ethanol at
65°C, and the solvent was subsequently removed by stirring.
The resulting lipid film was hydrated in 200 mM NH$_4$EDTA
solution (pH 5.5) under magnetic agitation at an appropriate
rate. Liposomes containing an inner aqueous medium of
200 mM (NH$_4$)$_2$SO$_4$ (pH 5.5) were also prepared for the
in vitro release assays, long-term stability tests, and animal
experiments.

The initially produced bulk liposome suspension was
transformed into small unilamellar vesicles by sonication
using a JY92-2D Vibra-cell probe sonicator (Ningbo Xinzhi
Biological Technology Co. Ltd., Zhejiang, People’s Republic
of China) for an initial 6-minute cycle (400 W; 3 seconds
on, 3 seconds off) followed by a 2-minute cycle (200 W).
The resulting vesicles were extruded through polycarbonate
membranes with gradually decreasing pore sizes (0.8, 0.45,
and 0.22 μm) to remove large particles.

The mean diameters and size distributions of the lipos-
omes were estimated using a dynamic laser light scattering
instrument (Nicomp$^\text{TM}$ 380 Submicron Particle Sizer;
Particle Sizing Systems, Port Richey, FL, USA) operated at
a wavelength of 632.8 nm. All samples were diluted with 5% glucose solution and measurements were conducted at 25°C in triplicate.

**Preparation of the ammonium gradient for drug encapsulation**

The ammonium gradients of the liposomes were established using a dialysis method monitored by ion pair high-performance liquid chromatography (IP-HPLC). Liposome suspensions (2 mL) consisting of HSPC/CH/mPEG\textsubscript{2000}-DSPE (3:1:1, w/w/w) were placed in dialysis tubing with a molecular weight cutoff of 10 kDa and dialyzed against 500 mL of 5% glucose solution. The glucose solution was changed at 0°C half an hour, and the dialysis was ceased when the IP-HPLC results stayed constant. The dialyzed liposomes were diluted with the glucose solution to a final lipid concentration of 20 mg/mL. Subsequently, DOX solution (2 mg/mL) was added to the liposomal suspension to achieve a drug/lipid ratio of 1:10 (w/w). The loading process was carried out at 60°C for 30 minutes, and then the mixture was cooled rapidly in an ice/water bath (0°C–2°C) for 5 minutes.

**Determination of encapsulation efficiency**

Non-entrapped drug was removed by using size exclusion chromatography to pass the DOX-loaded vesicle dispersions through a Sephadex G-50 mini-column (10×70 mm). The separation of 0.2 mL liposomes from free DOX was carried out by eluting with distilled water (0.4 mL, four times), and the concentration of DOX was determined by an ultraviolet spectrophotometer (UV-1801 UV/VIS Spectrophotometer, Beijing Rayleigh Analytical Instrument Co., Ltd, People’s Republic of China) at a wavelength of 480 nm after lysis of the liposomes with 90% (v/v) isopropyl alcohol containing 0.75 M hydrochloric acid. The encapsulation efficiency was calculated as the percentage of DOX remaining in the liposomes after elution, and DOX concentration was calculated using the lipid concentration.

**Solubility of DOX in different mediums**

The solubility of DOX was investigated in NH\textsubscript{2}EDTA (200 mM) and (NH\textsubscript{4})\textsubscript{2}SO\textsubscript{4} (200 mM) solutions. The pH values of these salt solutions were adjusted with aqueous ammonia solution or hydrochloric acid. In brief, 100 mg of lyophilized DOX powder was dissolved with diluted water to a concentration of 10 mg/mL, and 0.2 mL of this solution was added to 0.8 mL of 250 mM NH\textsubscript{2}EDTA or (NH\textsubscript{4})\textsubscript{2}SO\textsubscript{4} solutions to obtain final drug concentrations in each solution of 2 mg/mL. Each sample was vortexed for 2 minutes and incubated at 25°C for 48 hours in a homeothermic oscillator with a velocity of 100 rpm under low-light conditions. The drug precipitate was separated from the supernatant by centrifugation (10,000 rpm for 15 minutes) and the DOX concentration in the supernatant was measured photometrically at a wavelength of 480 nm.

**Release experiments in vitro for DOX-loaded liposomes**

Two types of release medium were used in the release assays: a conventional phosphate-buffered saline (PBS) and a special PBS buffer containing ammonium chloride (80 mM), histidine (10 mM), penicillin (100 μg/mL), and streptomycin (100 μg/mL). The pH values of both PBS buffers were adjusted to 7.4 with hydrochloric acid and osmotic pressure was adjusted to 280–320 mOsm with glucose. Briefly, 2 mL of HSPC/CH/mPEG\textsubscript{2000}-DSPE (3:1:1, w/w/w) liposomes containing DOX (drug/lipid ratio 1:10, w/w) were placed in dialysis tubing with a molecular weight cutoff of 10 kDa and dialyzed against 198 mL release buffer. The dialysis process was performed at 37°C with a velocity of 75 rpm under low-light conditions. At indicated time points, aliquots were withdrawn and analyzed using a fluorescence spectrophotometer (650-60; Hitachi Ltd., Tokyo, Japan) with excitation and emission wavelengths set at 472 nm and 591 nm, respectively.

**Long-term stability experiments**

The liposomal formulations were assessed for stability over a period. HSPC/CH/mPEG\textsubscript{2000}-DSPE (3:1:1, w/w/w) liposomal formulations (10 mg/mL) containing DOX (drug/lipid ratio 1:10, w/w) and driven by NH\textsubscript{2}EDTA (200 mM) or (NH\textsubscript{4})\textsubscript{2}SO\textsubscript{4} gradient (200 mM) (which is marked as NH\textsubscript{2}EDTA-L and (NH\textsubscript{4})\textsubscript{2}SO\textsubscript{4}-L in the following texts, respectively) were stored at 4°C±2°C for a period of 3 months. Stability was evaluated in terms of appearance, particle size, and encapsulation efficiency at selected time intervals during the storage period by methods described above.

**Antitumor activity tests**

Antitumor activities of DOX preparations were investigated by a xenograft mouse model of liver cancer (H\textsubscript{22}). In brief, tumors were established in 6–8 weeks old Kunming male mice on Day 0 by injecting H\textsubscript{22} tumor cells (provided by the Cancer Institute of Liaoning Province, Shenyang, People’s Republic of China) subcutaneously at the right axillary flank. Treatments consisted of multiple dosing on Days 6, 9, 12, and 15, and the animals were sacrificed on
Day 16. Sixty tumor-bearing mice were randomly divided into six groups (n=10 per group). For the treatment groups, drug dosages are listed in Table 1, and the control group received injections of normal saline. During this period, mice had free access to food and water and their weights were recorded from the day of tumor injection to the day of execution. Necropsies were conducted to obtain the tumor, spleen, thymus gland, and heart. Tumor inhibition ratio, spleen index, and thymus gland index were calculated and served as indicators for the evaluation of antitumor activity and immunotoxicity.

Tissue distribution by repeated injection
Mice bearing H22 tumors were randomly divided into six groups (n=10 per group) for tissue distribution studies. The formulations administered were DOX solution, NH4EDTA-L, and (NH4)2SO4-L, and doses were the same as those used in the antitumor activity tests. Treatments consisted of multiple dosing on Days 6, 9, 12, and 15 after inoculation with H22 cells. Blood samples were collected at 24 hours after the last drug administration via the retroorbital collection method. Briefly, 0.1 mL blood samples were diluted to 5 mL with methanol/water (50:50, v/v) containing 0.3 M HCl and centrifuged immediately at 10,000 rpm for 10 minutes, and the supernatants were kept for analysis. The heart, liver, spleen, lungs, kidneys, and brain of each mouse were rapidly excised following blood collection and weighed. Tissue samples of 0.05 g were excised and all tissue samples were homogenized. The homogenates were diluted to 5 mL with methanol/water (50:50, v/v) containing 0.3 M HCl and centrifuged immediately at 10,000 rpm for 10 minutes, and the supernatants were kept for analysis. After DOX extraction from the serum and tissue-based samples, DOX levels were determined by fluorescence.

Histopathological studies of cardiotoxicity
Cardiac tissue from ventricles was excised from the mice used in the tissue distribution experiments, washed by normal saline, fixed in 10% formalin solution, cleaned by ethanol, and embedded in paraffin wax. The embedded samples were placed into the tissue slicer to make ultra-thin slices. After heating at 70°C, the slices were stained with hematoxylin and eosin and observed under a fluorescence microscope (IX71; Olympus Corporation, Tokyo, USA).

Results
Solubility of DOX in different mediums
As shown in Figure 1, the solubility of DOX in (NH4)2SO4 and NH4EDTA solutions at 25°C was dependent on pH. The solubility of DOX in 200 mM (NH4)2SO4 solution was almost invariable from pH 4 to pH 7 (approximately 0.23 mg/mL) and decreased gradually as pH was raised above pH 7. In 200 mM NH4EDTA solution, the solubility of DOX decreased sharply from 1.92 mg/mL (at pH 4) to 0.23 mg/mL (at pH 5), and the variation in solubility was comparable to that of (NH4)2SO4 solution above pH 5. The solubility of DOX in (NH4)2SO4 and NH4 EDTA solutions at pH 4 was further examined by dilution with distilled water. As shown in Figure 2, DOX formed a precipitate in (NH4)2SO4 solution after centrifugation, while it was well dispersed in the NH4EDTA solution. However, when diluted with isochoric distilled

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Abbreviations: DOX, doxorubicin; EDTA, ethylenediaminetetraacetic acid; L, doxorubicin-loaded liposomes.

Statistical analysis
Statistical comparisons were performed using Student’s t-test for two groups and one-way analysis of variance for multiple groups. The significance threshold was set such that P-values less than 0.05 were considered to be statistically significant, and P-values less than 0.01 were considered to be extremely significant.

Figure 1 A comparison of the solubilities of DOX in different salt solutions as a function of pH. The solubilities of DOX were quantified after a 24-hour incubation of 2 mg DOX within 1 mL of 200 mM salt solutions of different pH at 25°C. **P<0.01 versus (NH4)2SO4 group. Abbreviations: DOX, doxorubicin; EDTA, ethylenediaminetetraacetic acid.
water, the supernatant of the (NH₄)₂SO₄ solution appeared to be homogeneous, while that of the NH₄EDTA solution appeared layered.

Release experiments in vitro for DOX-loaded liposomes

Drug release experiments were performed for the quantitative comparison of the release kinetics of DOX from NH₄EDTA-L and (NH₄)₂SO₄-L, and the results are shown in Figure 3.

When the release medium was conventional PBS (pH 7.4), the drug release rates from both liposomes over 24 hours were less than 5% with no significant difference between them (P>0.05). When the release medium was a special PBS buffer (pH 7.4) with ammonium chloride (80 mM), the release of encapsulated drug from NH₄EDTA-L was much slower than (NH₄)₂SO₄-L, and the total amounts of released DOX were 11.4% and 23.7%, respectively. Furthermore, it was noted that there was a small difference between the release profiles of the two DOX liposomes. For the NH₄EDTA-L preparation, release occurred at a constant slow and steady rate, while release from the (NH₄)₂SO₄-L preparation followed a biphasic pattern, in which the first phase of drug release was a rapid response that lasted nearly 5 hours, which was followed by a slow and prolonged second phase.

Long-term stability experiments

The long-term stability of the liposomal formulations was determined during 90 days of storage at 4°C±2°C, and changes in particle sizes and entrapment efficiencies are shown in Table 2. When stored at 4°C±2°C for 1 month, neither formulation showed obvious changes in entrapment efficiency (P>0.05), but both showed a slight increase in particle size (P<0.05). Precipitation was observed at Day 60 in the (NH₄)₂SO₄-L preparation, but not in the NH₄EDTA-L preparation. Over the 3-month study period, the NH₄EDTA-L preparation showed constant entrapment efficiency and an increase in particle size from 79.4±1.87 nm to 106.2±3.55 nm.
Antitumor activity tests

Antitumor activities of DOX solution, NH₄EDTA-L DOX preparations (different concentrations), and the (NH₄)₂SO₄-L preparation were evaluated in a rapidly growing H₂₂ liver cancer xenograft model in mice. As shown in Figure 4A, all of the DOX preparations (solution and liposomes) produced extremely significant antitumor effects (P<0.01 versus saline). The antitumor effects observed in all liposome groups were greater than those of the free DOX solution group (P<0.05). There was no significant difference (P>0.05) among the groups that received different doses (low, medium, and high) of the NH₄EDTA-L preparation. Tumor inhibition was comparable for equivalent doses of the NH₄EDTA-L and (NH₄)₂SO₄-L preparations, but the numbers of deaths in these groups were zero and two, respectively.

The body weights of tumor-bearing mice were also determined. For the saline-treated group, body weights increased from Day 0–12 as the tumor grew. After Day 12, the tumors in several mice progressed to a degree that resulted in loss of life quality and weight loss. For the DOX solution group, persistent weight loss was observed from the first treatment (6 days after inoculation), and four deaths occurred before the group was sacrificed. For the DOX-loaded liposome groups, low- and medium-dose NH₄EDTA-L groups showed similar body weight changes; weight loss was observed from the second drug administration and there were no deaths during the observation period. Body weights at sacrifice were similar to those recorded on the first treatment day. For (NH₄)₂SO₄-L and high-dose NH₄EDTA-L groups, significant weight loss occurred after the second administration and two and three deaths were observed, respectively, after the third treatment.

Spleen index and thymus gland index were taken as indicators (weight of the spleen or thymus gland/body weight of
the mouse, expressed in mg/g) to evaluate liposome-related damage to immune organs. As described in Figure 4B, compared with the saline-treated group, no significant weight loss was observed in the spleens or the thymus glands from low-dose and medium-dose NH$_4$EDTA-L groups ($P>0.05$), but significant weight loss was observed in organs collected from the DOX solution, high-dose NH$_4$EDTA-L, and (NH$_4$)$_2$SO$_4$-L groups ($P<0.05$). Compared with an equivalent dose of the NH$_4$EDTA-L preparation, spleen weight loss was significantly greater in mice treated with the (NH$_4$)$_2$SO$_4$-L preparation ($P<0.05$).

**Tissue distribution studies**

In the in vivo distribution studies, the disposition of DOX after intravenous administration of each preparation was investigated. As seen in Figure 5A, the distribution of DOX in the tumor and all measured tissues was very low after intravenous administration of DOX solution, which was owing to its short half-life and the rapid elimination that occurred without the protection of vehicles. In the case of liposomal preparations, NH$_4$EDTA-L (low, medium, and high doses) and (NH$_4$)$_2$SO$_4$-L showed excellent targeting to the tumor, as indicated by a significant difference in disposition compared to tumor tissue from the free DOX solution-treated group ($P<0.01$). Compared with the equivalent dose of (NH$_4$)$_2$SO$_4$-L, tissue accumulation after NH$_4$EDTA-L administration was lower in the heart (by 45%), the liver (by 16%), and the spleen (by 72%), but higher in tumors (by 28%). Variation in dosage of each preparation also affected tissue distribution; as shown in Figure 5B, the drug concentrations
measured in all tissues increased at various rates as the administered dosage increased. For example, when the dose was increased from 5 mg/kg to 10 mg/kg, measured DOX increased by 92% in tumors, 258% in the liver, 2,323% in the spleen, and 55% in the heart. In addition, the damage that was caused by drug administration to the liver and spleen increased sharply.

**Histopathological studies of cardiotoxicity**

Slice samples of ventricles were observed under a fluorescence microscope using a 40× objective. Vacuolization, edema, and inflammatory cell infiltration were not observed in any tested cardiac tissue samples. However, all of the experimental groups showed fragmentation of the myocardium to different degrees, which were markedly different from normal Henle’s fissures. Typical images are shown in Figure 6, and the myofibrillary damage sites are indicated by black circles.

![Figure 6](image)

**Figure 6** Typical images of pathological classification of myocardium injury of different DOX formulations: (A) NS; (B) DOX solution; (C) NH$_4$EDTA-L (low-dose); (D) NH$_4$EDTA-L (medium-dose); (E) NH$_4$EDTA-L (high-dose); and (F) (NH$_4$)$_2$SO$_4$-L.

**Notes:** Photographs were obtained under a fluorescence microscope (IX71; Olympus Corporation, Tokyo, Japan) using a 40× objective. The black circles point out the damaged sites of myocardium fragmentation.

**Abbreviations:** DOX, doxorubicin; EDTA, ethylenediaminetetraacetic acid; L, doxorubicin-loaded liposomes; NS, normal saline.

Drug retention characteristics of liposomal formulations affect in vitro stability and in vivo dissolution rates, and
indirectly affect the activity and toxicity of the loaded drugs. If the loaded drug forms an insoluble complex with the hydration medium in the liposomes, and the dissolution rate of the complex is slower than that of the drug departing through the bilayer, then increased drug retention will be observed. In addition to drug properties, retention is also dependent on the anionic varieties present and concentrations of the inner aqueous medium. When citric acid and ammonium sulfate gradients were employed to load DOX into liposomes, precipitation was observed as fiber bundles by cryo-electron microscopy with no observable membrane invagination. A similar result was obtained in liposomes loaded with idarubicin by an NH$_4$EDTA gradient. In the current solubility studies, the biggest difference in DOX solubility between NH$_4$EDTA and (NH$_4$)$_2$SO$_4$ solutions appeared at pH 4. The solubility of DOX seemed ten times greater in the NH$_4$EDTA solution than in the (NH$_4$)$_2$SO$_4$ solution. In fact, DOX formed a gel-like complex that could not be precipitated by centrifugation. This difference in the solubility of DOX in different hydration mediums also resulted in differences in release rates in vitro.

Two types of media were utilized for in vitro release profile tests because conventional PBS could not differentiate the two formulations sufficiently within 24 hours. A special PBS solution with ammonium chloride, which led to the depletion of the transmembrane gradient and the release of encapsulated drugs, was employed to amplify the discrepancy between the DOX liposomes loaded by various gradients. Results showed that DOX release from the NH$_4$EDTA-L preparation was much slower than release from the (NH$_4$)$_2$SO$_4$-L preparation. For the NH$_4$EDTA-L preparation, almost all of the DOX formed a gel-like compound, which resulted in a steady and nearly linear release rate. In contrast, DOX encapsulated in the liposomes in the (NH$_4$)$_2$SO$_4$-L preparation was in the form of a saturated solution containing a DOX-(NH$_4$)$_2$SO$_4$ precipitate, and the release followed a biphasic pattern. The first phase of release involved transmembrane release of the dissolved drug, and the second phase involved drug dissolving from the precipitate, which was followed by transmembrane release.

Additionally, the long-term stability experiments showed that the NH$_4$EDTA-L preparations were highly stable when stored at 4°C±2°C for 3 months. In contrast, the (NH$_4$)$_2$SO$_4$-L preparation showed a decreased loading ability for DOX after 2 months of storage, as indicated by a precipitate at the bottom of the bottle. The outstanding stability of NH$_4$EDTA-L in the same storage conditions could be caused by the chelation of metal ions by intraliposomal EDTA, which inhibited the catalytic oxidation of phospholipids by metal ions. Furthermore, EDTA could inhibit bacterial contamination by chelating divalent metal ions that are essential for microbial growth. These advantages of EDTA are important for laboratory research, because they facilitate the production of stable lipid formulations for which long-term stability can be easily estimated.

In the clinic, repeated injections of antitumor formulations are generally used to treat cancers, so the antitumor activities and tissue distributions of the two DOX preparations after repeated administration were investigated. Compared with an equivalent dose of (NH$_4$)$_2$SO$_4$-L, the accumulation of NH$_4$EDTA-L was significantly greater in tumors, but lower in the liver, spleen, and heart. Although the tumor inhibition ratios showed no significant differences, toxicity caused by NH$_4$EDTA-L was very low and no drug-related deaths were observed during the experiments.

The similar inhibition ratios observed for the NH$_4$EDTA-L and (NH$_4$)$_2$SO$_4$-L preparations, despite the high tumor accumulation produced by the former, might be associated with the controlled release of DOX. Because of this delayed DOX release, the available drug concentration produced by NH$_4$EDTA-L administration was similar to that of (NH$_4$)$_2$SO$_4$-L administration. Furthermore, the primary antitumor mechanism of DOX has been reported to be the formation of a complex with DNA by intercalation between base pairs or interaction with topoisomerase II. However, the generation of ROS, which results in DNA damage, lipid peroxidation, and apoptosis, might also have an effect on antitumor activity. Thus, when transition metal ions were chelated by EDTA, antitumor activity might be influenced by a reduction in ROS.

From the spleen index and thymus gland index results, the superiority of the NH$_4$EDTA-L preparation was quite apparent, because of lesser tissue accumulation in these organs and the chelating effect of EDTA. DOX cytoxicity generally manifests as high levels of ROS and low levels of antioxidants and protective enzymes. Transition metal ions promote free radical reactions through enzymatic and nonenzymatic pathways; in the enzymatic pathway, the metal ions accept or donate single electrons to cellular oxidoreductases (eg, cytochrome P450 reductase, nicotinamide adenine dinucleotide dehydrogenase of complex I, xanthine oxidase), while in nonenzymatic pathways metal ions form compounds with DOX and thus generate superoxide anions, singlet oxygen, and hydrogen peroxide. Thus, it was presumed that the lower toxicity of NH$_4$EDTA-L was
owing to its chelation of metal ions, which inhibited and/or deregulated the immune system, and resulted in binding of receptor sites, suppression of proper enzyme functions, reduced antibody response, disordered hormone functions, undesirable upregulation of the immune system, and auto-immune diseases.⁴⁰

Tissue distributions and histopathological studies of cardiototoxicity indicated that liposomal formulations show a lower risk of DOX-induced cardiototoxicity. Furthermore, NH₄EDTA-L possessed a clear advantage over (NH₄)₂SO₄-L at equivalent drug concentrations. A concentration dependent trend of toxicity among the three NH₄EDTA-L groups was also observed. Due to the slow release rate of the liposomes, liposomal preparations could achieve high accumulation in targeted tissues because of the enhanced permeation and retention effect. Thus, the drug would reach relatively low levels in other tissues, and lessen the risk of drug-related toxicity. Within the two liposomal formulations in this study, NH₄EDTA-L presented a notable advantage over (NH₄)₂SO₄-L with respect to DOX-induced cardiototoxicity when an equivalent dose was administered. The primary reason for this result may have been that EDTA reduced the generation of ROS by chelating transition metal ions, which led to cardiomyocyte membrane damage and the occurrence and development of DOX-related cardiomyopathy. Additionally, as described above, excessive calcium in vivo can cause hypercalcinemia and promote the migration of cancer cells to the bones. Therefore, when EDTA is employed in a drug formulation extra calcium might be eliminated owing to its chelating effect, and suffering of associated off-target complications may be reduced.

The most valuable clinical implication of these studies on NH₄EDTA-L is that it can reduce the cardiototoxicity induced by DOX without affecting the antitumor activity of the drug. However, the primary limitation of these novel liposomes is that drug accumulation in the spleen and liver remains high, and thus the risk of damage to these organs increases with the dose of the drug. To date, the authors have encapsulated several other amphiphilic weak bases, such as topotecan and huperzine A, via a transmembrane NH₄ EDTA gradient method. All tested drugs showed rapid accumulation in the vesicles, good long-term stability, considerable antitumor activity, and low cytotoxic activity, compared with drugs encapsulated by ammonium sulfate gradient or citric acid gradient. These findings led to the conclusion that this particular method could provide new opportunities for the clinical use of many chemotherapy drugs that have been limited by their severe side effects.

Conclusion

Use of the NH₄EDTA gradient method to load doxorubicin into liposomes produced rapid and efficient drug encapsulation, and the liposomes showed slow drug release and good long-term stability. Furthermore, compared with liposomes prepared by (NH₄)₂SO₄ gradient, doxorubicin loaded into liposomes via an NH₄EDTA gradient produced significantly reduced toxicity and mortality without altered antitumor effects.

Disclosure

The authors report no conflicts of interest in this work.

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