Effects of *Caryota mitis* profilin-loaded PLGA nanoparticles in a murine model of allergic asthma

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**Background:** Pollen allergy is the most common allergic disease. However, tropical pollens, such as those of Palmae, have seldom been investigated compared with the specific immunotherapy studies done on hyperallergenic birch, olive, and ragweed pollens. Although poly(lactic-co-glycolic acid) (PLGA) has been extensively applied as a biodegradable polymer in medical devices, it has rarely been utilized as a vaccine adjuvant to prevent and treat allergic disease. In this study, we investigated the immunotherapeutic effects of recombinant *Caryota mitis* profilin (rCmP)-loaded PLGA nanoparticles and the underlying mechanisms involved.

**Methods:** A mouse model of allergic asthma was established for specific immunotherapy using rCmP-loaded PLGA nanoparticles as the adjuvant. The model was evaluated by determining airway hyperresponsiveness and levels of serum-specific antibodies (IgE, IgG, and IgG2a) and cytokines, and observing histologic sections of lung tissue.

**Results:** The rCmP-loaded PLGA nanoparticles effectively inhibited generation of specific IgE and secretion of the Th2 cytokine interleukin-4, facilitated generation of specific IgG2a and secretion of the Th1 cytokine interferon-gamma, converted the Th2 response to Th1, and evidently alleviated allergic symptoms.

**Conclusion:** PLGA functions more appropriately as a specific immunotherapy adjuvant for allergen vaccines than does conventional Al(OH)3 due to its superior efficacy, longer potency, and markedly fewer side effects. The rCmP-loaded PLGA nanoparticles developed herein offer a promising avenue for specific immunotherapy in allergic asthma.

**Keywords:** nanoparticles, *Caryota mitis* profilin, PLGA, allergic asthma, adjuvant

**Introduction**

Allergic disease is frequently encountered, is classified as one of the four common noncommunicable diseases by the World Health Organization,1 and significantly jeopardizes human health. The incidence of allergic disease is 30%–40% worldwide, has doubled in the last 30 years, and is still increasing at a rate higher than 1% annually.2,3 Patients effectively treated by allopny, including hormones and antihistamines, are at risk of side effects, aggravated metabolic burden, and disease recurrence in the event of termination of medication, that leads to a vicious cycle.4,5 As a sole treatment for allergic disease, specific immunotherapy functions to regulate the Th1/Th2 equilibrium, but has short-term efficacy,6,7 poor stability, and discernible side effects that limit its clinical use.8 Therefore, it is important to identify other secure and more stable treatment methods, the mechanisms of which are of crucial theoretical and practical significance.

Vaccination is among the most important medical interventions that have helped to reduce and eliminate a number of diseases. The development of nanoparticles has
started to receive a lot of attention in order to provide effective immunization through better targeting and by triggering an antibody response at the cellular level. Nanotechnology has also helped to formulate efficient vaccine delivery systems that can prevent the encapsulated antigen from damage in the in vivo environment and can maintain sustained release that helps to induce the immunostimulatory properties of the vaccine. With very few adjuvants currently being used in marketed human vaccines, a critical need exists for novel immunopotentiators and delivery vehicles capable of eliciting humoral and cellular immunity. Poly(lactic-co-glycolic acid) (PLGA), a biocompatible degradable material approved by the US Food and Drug Administration, has been used extensively in bioabsorbable sutures, orthopedic fixation and tissue repair materials, and controlled drug delivery systems. PLGA and its derivatives have been spotlighted as carriers for in vitro and in vivo allergy tests are helpful in the diagnosis, allowing it to be applied as an adjuvant in antiallergic, hepatitis B, and human immunodeficiency virus vaccines. Scholl et al verified that the allergen slowly released from PLGA microcapsules effectively induced generation of antibody IgG. Profilins are ubiquitous proteins, present in all eukaryotic cells and identified as allergens in pollen, latex, and plant foods. Purified natural and recombinant profilins for in vitro and in vivo allergy tests are helpful in the diagnostic work-up. Recombinant birch profilin, as well as natural profilins from birch, timothy grass, and mugwort elicited IgE-mediated histamine release from basophils of pollen-allergic patients which cause type I allergy symptoms. However, there has been no report on the use of recombinant Caryota mitis profilin (rCmP) in the treatment of asthma. Thus, in this study, we encapsulated rCmP into PLGA nanoparticles. The immune protective, preventive, and treatment effects of rCmP-loaded PLGA nanoparticles in mouse asthma as well as the relevant mechanisms were investigated, which will be innovative in immunotherapy for allergic asthma.

**Materials and methods**

**Animals and materials**

Female BALB/c mice (specific pathogen-free grade, aged 5–6 weeks, weight 16–20 g) were purchased from the Animal Center of Guangdong Province and fed in a specific pathogen-free grade breeding room. rCmP, PLGA (lactide:glycolide 50:50, molecular weight 24,000–38,000) and polyvinyl alcohol (80% hydrolyzed) were obtained from Sigma-Aldrich (St Louis, MO, USA). Analytical grade dichloromethane obtained from J&K Chemical Co, Ltd (Beijing, People’s Republic of China) was used without any further purification. Al(OH)₃ and methacholine were also purchased from Sigma-Aldrich. Biotin-labeled goat anti-mouse IgE and horseradish peroxidase (HPR)-labeled goat anti-mouse IgG and IgG2a were from eBioscience (San Diego, CA, USA). Mouse interleukin (IL)-4, IL-10, and interferon gamma (IFN-γ) enzyme-linked immunosorbent assay (ELISA) kits were obtained from BioLegend (San Diego, CA, USA).

**Expression and purification of rCmP**

The strain was expressed by the gene sequences BL21 of rCmP at 37°C in a shaking water bath with a shaking speed of 120 rpm, which has been described previously. The protein was purified with a Ni²⁺ affinity chromatography column. The elution, which including resultant protein was dialyzed and lyophilized.

**Formation of rCmP-loaded nanoparticles**

rCmP-loaded PLGA nanoparticles were prepared by a w/o/w double emulsion solvent evaporation method as reported by Jain et al with slight modifications. Briefly, aqueous phase (0.5 mL) containing 10 mg of rCmP was added to organic phase (2 mL/dichloromethane and acetone at a volume ratio 9:1) including copolymer PLGA (5% w/v). The primary emulsion (w/o) was obtained by probe sonication in an ice bath for 120 seconds. The primary emulsion was then added to 100 mL of aqueous solution containing polyvinyl alcohol (1% w/v) as an emulsifier and sonicated in an ice bath for 60 seconds to form the secondary emulsion (w/o/w). The resulting emulsion was stirred vigorously overnight to evaporate the organic phase. The nanoparticles were collected by centrifugation (20,000 rpm, 15 minutes, 4°C), washed twice with distilled water to remove residual polyvinyl alcohol, and subjected to lyophilization. The final nanoparticles were stored at 4°C in a refrigerator.

**Characterization of rCmP-loaded nanoparticles**

**Size and zeta potential**

The nanoparticle size and size distribution were measured by dynamic light scattering using a Mastersizer 2000 (Malvern Instruments Ltd, Malvern, UK). Before measurement, approximately 0.2 mg of freshly prepared nanoparticles were diluted in 1 mL of distilled water and sonicated in an ice bath.
for 30 seconds. The data obtained represent the average of three measurements.

Surface morphology
The surface morphology of the nanoparticles was examined by field emission scanning electron microscopy (FESEM) using a JSM-6700F system (JEOL, Tokyo, Japan) operated at a 5.0 kV accelerating voltage. To prepare samples for FESEM, the particles were fixed on the stub by double-sided sticky tape and then coated with a platinum layer using an automatic fine platinum coater (JFC-1300, JEOL) for 60 seconds.

Protein loading and encapsulation efficiency
The protein loading content (LC) and encapsulation efficiency (EE) of the nanoparticles were determined by bicinchoninic acid protein assay. In summary, 5 mg of nanoparticles were dissolved in 2 mL of aqueous phase containing 1% sodium dodecyl sulfate and 0.05 M sodium hydroxide (NaOH). Each batch was performed in triplicate. The protein LC and the EE of the rCmP-loaded nanoparticles were calculated using the following equations:

\[
\text{LC} (\%) = \frac{\text{Weight of protein in the nanoparticles}}{\text{Weight of the nanoparticles}} \times 100\%
\]

\[
\text{EE} (\%) = \frac{\text{Weight of protein in the nanoparticles}}{\text{Weight of the feeding protein}} \times 100\%
\]

In vitro release study
To perform the in vitro release study, 20 mg of rCmP-loaded nanoparticles was dispersed in 5 mL of phosphate-buffered saline (PBS, pH 7.4) to form a suspension. The suspension was incubated at 37°C in a shaking water bath at a shaking frequency of 120 rpm. At appropriate time intervals, a 1 mL sample was collected following centrifugation at 20,000 rpm for 30 minutes and replaced with fresh PBS. Samples were detected using the bicinchoninic acid assay method to determine the fraction of protein released. Each batch was repeated in triplicate.

SDS-PAGE and Western blotting of rCmP-loaded nanoparticles
The protein components in rCmP and in the rCmP-loaded PLGA nanoparticles (PLGA-rCmP) were subjected to sodium dodecyl sulfate polyacrylamide gel electrophoresis (SDS-PAGE) identification and electrobotted onto nitrocellulose membranes. The membranes were blocked with 3% bovine serum albumin (BSA) overnight at 4°C and then incubated in diluted (1:5) positive serum of allergic patients at 37°C for 2 hours.

Biotin-labeled goat anti-human IgE diluted (1:3,000) by TBST (TBS/0.05% Tween-20) was added to the resulting membranes, which were then incubated at 37°C for 2 hours. After adding HRP-labeled streptavidin diluted (1:1,000) by TBST, the membranes were incubated at 37°C for another 1.5 hours. The membranes were washed three times after each step (5 minutes). They were then visualized in freshly prepared diaminobenzidine substrate solution and observed after being washed in double-distilled water.

Animal sensitization and specific immunotherapy
The administrative committee on animal research at the Graduate School of Shenzhen, Tsinghua University, approved all the protocols used for the animal experiments. The animal sensitization model and specific immunotherapy were designed (Figure 1) by combining the previous literature and the requirements herein.21–24 The mice were randomly divided into five groups (n=8), ie, a normal group, a model group, a PLGA-rCmP group, a rCmP/Al(OH)₃ (ie, rCmP) vaccine group, and a blank PLGA nanoparticle control group. Mice in the normal group were sensitized and treated with normal saline, and the other groups were sensitized three times every

![Figure 1](https://www.dovepress.com/)

**Figure 1** Experimental design. Five groups of mice (n=8 per group) were used in the experiment.

**Abbreviations:** AHR, airway hyperresponsiveness; PLGA, poly(lactic-co-glycolic acid); rCmP, recombinant Caryota mitis profilin; SIT, specific immunotherapy; ip, intraperitoneal injection; sc, subcutaneous injection; in, nasal inhalation.
3 weeks by intraperitoneal injection of 50 µg Caryota mitis (Cm) pollen crude proteins adsorbed on 2 mg of Al(OH)₃. The treatment was initiated on day 36. The PLGA-rCmP group was subcutaneously injected with nanoparticles containing 50 µg rCmP, the rCmP group was injected with rCmP adsorbed on 2 mg of Al(OH)₃, and the PLGA group was injected with an equivalent amount of PLGA. The mice were treated three times every 4 weeks. The mice were intranasally challenged three times daily with 200 µg of crude proteins one week after the final treatment. The mice were subjected to an airway hyperresponsiveness (AHR) test 24 hours after the final challenge and were then euthanized.

Assessment of AHR to methacholine challenge
Twenty-four hours after the final challenge, AHR was measured using unrestrained whole-body plethysmography with a four-chamber system (Buxco Research Systems, Wilmington, NC, USA). The baseline response was recorded for 5 minutes in the event of stabilized respiration after 10 minutes of adaptation. The responses of the mice were then recorded every 5 minutes after inhaling different concentrations of atomized methacholine solutions (0, 6.25, 12.5, 25, 50, and 100 mg/mL PBS). Tests at two different concentrations were separated temporarily to allow the respiratory intensity to drop back to baseline. The percentage curves for Penh values at different methacholine concentrations were plotted based on that of PBS.

Determination of allergen-specific IgE, IgG, and IgG2a antibodies in serum
Blood was sampled from mouse eyes 24 hours after the AHR test, left undisturbed for 2 hours, and stored overnight at 4°C. The blood was then centrifuged at 4°C and 3,000 rpm for 10 minutes, and the supernatant serum was collected. Next, the responses of C. mitis pollen-specific IgE, IgG, and IgG2a were detected in serum using the indirect ELISA protocol. The antibodies were coated with 1 ng/µg rCmP and stored overnight at 4°C. The plates, which were washed with PBST and blocked with 3% BSA/PBS (200 µL/well), were incubated at 37°C for 2 hours. Mouse serum diluted (IgG, 1:2,000; IgG2a, 1:1,000; IgE, 1:5) by 1% BSA-PBST and 1% BSA-PBST was added to the test wells and the control well (100 µL/well) after the plates were washed with PBST, and incubated at 37°C for one hour. Next, 100 µL of biotin-labeled goat anti-mouse secondary antibodies diluted (HRP-IgG, 1:2,000; HRP-IgG2a, 1:2,000; biotin-IgE, 1:20,000) with 1% BSA/PBST were added after the plates were washed with PBST, and incubated at 37°C for a further hour. The plates were subjected to color development in the dark at 37°C for 10 minutes utilizing 3,3',5,5'-tetramethylbenzidine solution after being washed with PBST, and the reactions were terminated by 1 M H₂SO₄. The absorbances at 450 nm were then measured on a microplate reader.

Bronchoalveolar lavage and inflammatory cell differential counting
Immediately after being euthanized, the mice were subjected to bronchoalveolar lavage. The lung was immediately lavaged via the trachea cannula with 0.8 ml of PBS. The bronchoalveolar lavage fluid was collected after five bouts of pumping. Each mouse underwent bronchoalveolar lavage three times, yielding approximately 2 mL of bronchoalveolar lavage fluid each time (recovery rate >80%). The combined bronchoalveolar lavage fluid was centrifuged at 4°C for 10 minutes, and the supernatant was then sampled to determine cytokine levels. The precipitate was resuspended with 100 µL of PBS, which was utilized for cell counting (10 µL) and cell differential counting (90 µL). The stained cells were then classified and counted using Liu’s stain. At least 200 cells were counted and classified as neutrophils, eosinophils, lymphocytes, or macrophages according to their morphologic characteristics.

Cytokine assay
Mouse spleen tissue was ground and filtered through a 200-mesh screen. The splenocytes, which were then resuspended by Roswell Park Memorial Institute 1640 medium (100 mg/L fetal bovine serum, 100 U/L penicillin, and 100 mg/L streptomycin) and erythrocyte lysate were collected by centrifugation. The cells were cultured in Roswell Park Memorial Institute 1640 medium in 24-well plates at a density of 5 × 10⁶/well, stimulated with C. mitis pollen crude proteins (200 µg/well), and incubated at 37°C for 72 hours. The culture medium was then collected and centrifuged at 4°C and 1,500 rpm. The supernatant was then collected and stored at −80°C for cytokine determination. The IL-4, IL-10, and INF-γ levels in the supernatants of the splenocyte culture medium and bronchoalveolar lavage fluid were measured strictly according to the instructions of the ELISA kit (Biolegend, San Diego, CA, USA).

Lung histology and inflammation scoring
The mouse lungs were immediately removed and fixed in cold formalin solution for 24 hours, and then dehydrated by different concentrations of ethanol. The lung tissues
were embedded in paraffin and cut into approximately 5 mm × 5 mm blocks, which were sliced using a slicing machine (4 µm thick). The slices were then stained with hematoxylin and eosin and sealed to observe any histologic changes under an optical microscope.

**Statistical analysis**

The data are expressed as the mean ± standard deviation. Statistical comparisons between two groups were made using the two-tailed, unpaired Student’s t-test with Statistical Package for the Social Sciences version 16 software (SPSS Inc, Chicago, IL, USA). P<0.05 was considered to be statistically significant.

**Results**

**Characterization of nanoparticles**

The size and size distribution of the rCmP-loaded PLGA nanoparticles were investigated by dynamic light scattering. Physicochemical characteristics, such as particle size and surface properties, play an important role in vitro and in vivo. Therefore, they affect the therapeutic efficacy of specific immunotherapy. The mean diameter of the rCmP-loaded PLGA nanoparticles was approximately 180 nm, which is in the excellent size range for cellular uptake of nanoparticles. The nanoparticles exhibited a relatively narrow polydispersity index (≈ 0.135), which is useful for treatment effects. The zeta potential of nanoparticles is a crucial factor for stability in a suspension through the electrostatic repulsion between the nanoparticles, interaction with the cell membrane in vivo, and judgment of component onto the nanoparticle surface. The rCmP-loaded PLGA nanoparticles showed a negative surface charge of around −10 mV which was stable in vivo. The protein LC and EE of the rCmP-loaded PLGA nanoparticles was 9.79% and 63.56%, respectively.

The surface morphology of the rCmP-loaded PLGA nanoparticles was investigated by FESEM. Figure 2A shows an FESEM image for rCmP-loaded PLGA nanoparticles. The nanoparticles seemed to be about 180 nm in diameter and

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**Figure 2** (A) Field emission scanning electron microscopic image, (B) dynamic light scattering spectra, and (C) in vitro cumulative protein release of rCmP-loaded PLGA nanoparticles.

**Abbreviations:** PLGA, poly(lactic-co-glycolic acid); rCmP, recombinant Caryota mitis profilin; NPs, nanoparticles.
have a smooth surface within the resolution level. Further, the FESEM images demonstrated the particle size detected using a Mastersizer based on dynamic light scattering (Figure 2B).

The in vitro release research was carried out in PBS (pH 7.4). The release profile of rCmP-loaded PLGA nanoparticles showed a typical biphasic release pattern (Figure 2C). The first phase was a rapid burst release in the initial 24 hours (approximately 28.3%). This could be attributed to the amount of rCmP adherent to or just beneath the surface of the nanoparticles. This type of release is advantageous in terms of vaccine delivery, because it offers a primary immunization effect. The second phase consisted of constant continuous release of rCmP driven by diffusion through the rigid PLGA core. Release of rCmP reached a plateau in the following 192 hours (8 days), with a cumulative release of 65.2%. Further, we found that the cumulative protein release was 69.3% within 336 hours (14 days) and no further obvious release was observed. This may be due to degradation of the encapsulated protein because of the harsh conditions formed by PLGA. A similar result was reported by Jain et al.19

SDS-PAGE and Western blotting of rCmP-loaded PLGA nanoparticles

We used SDS-PAGE to detect changes in rCmP after coating with nanoparticles. The bands of PLGA-rCmP and rCmP are almost identical, indicating that rCmP and PLGA were bound without alterations (Figure 3). In addition, the Western blotting results (Figure 4) show that PLGA-rCmP binds to specific IgE in serum, suggesting that the activity of profilin in rCmP-loaded PLGA nanoparticles maintained intact after being bound physically to PLGA.

AHR assessment

AHR changes were assessed by methacholine challenge 24 hours after the last allergen challenge. The results (Figure 5) show that AHR in the model group was significantly greater ($P<0.01$) than in the normal group, and that in animals challenged by 25 mg/mL, 50 mg/mL, and 100 mg/mL methacholine was particularly high. AHR in the PLGA-rCmP group was significantly lower than in the model group ($P<0.01$), whereas the Penth value did not differ significantly from that of the normal group. The similar AHR of the Al(OH)$_3$-containing rCmP group and the model group indicates that the rCmP-loaded PLGA nanoparticles performed better than the individual rCmP. The blank PLGA nanoparticle control group performed similarly to the model group.
Determination of serum IgE, IgG, and IgG2a

Serum IgE, IgG, and IgG2a levels were measured by ELISA to evaluate the efficacy of the vaccine. The results (Figure 6) show that serum IgE levels in the model group were significantly higher than those in the normal group ($P<0.001$). Compared with the model group, PLGA-rCmP inhibited the immune response of serum IgE to a greater extent than did rCmP, given the significantly lower serum IgE levels of the two groups ($P<0.05$). Serum IgE levels in the PLGA and model groups did not differ significantly. PLGA-rCmP and rCmP both elevated serum IgG and IgG2a levels significantly compared with the model group, and PLGA-rCmP induced serum IgG2a more obviously than did rCmP. Serum IgG and IgG2a levels in the PLGA and model groups did not differ significantly. In general, PLGA-rCmP facilitated the Th1 immune response while suppressing the Th2 response.

Bronchoalveolar lavage and inflammatory cell differential counting

Figure 7 shows that the total counts of cells and inflammatory cells in the bronchoalveolar lavage fluid sampled from the model group were significantly higher than those in the normal group ($P<0.01$). The inflammatory cells mainly comprised neutrophils and eosinophils. The total counts for cells and inflammatory cells were significantly lower after being treated with rCmP-loaded PLGA nanoparticles and rCmP compared with the model group. In particular, considerably fewer cells, eosinophils, and lymphocytes were observed in the PLGA-rCmP group. In contrast, the total counts of cells and inflammatory cells in the PLGA control group do not differ from those in the model group.

Cytokine assay

IL-4, IL-10, and IFN-γ concentrations in the splenocyte culture medium supernatant and bronchoalveolar lavage fluid detected by ELISA (Figure 8A and B) show that the model group had allergen-specific Th2 immune responses, ie, IL-4 and IFN-γ levels, that were evidently upregulated and downregulated, respectively, compared with the normal group. After being treated with rCmP-loaded PLGA nanoparticles and rCmP, IL-4 and IFN-γ levels were dramatically downregulated and upregulated, respectively, suggesting that treatment with the nanoparticles promoted the Th1 immune response and inhibited the Th2 immune response by excreting...
more IFN-γ. In addition, IL-10 levels in the PLGA-rCmP and rCmP groups were higher than in the model group, which boosted anti-inflammatory and immunosuppressive functioning more effectively. The Th1/Th2 imbalance in the PLGA group was not restored, based on the concentrations of IL-4, IL-10, and IFN-γ in the splenocyte culture medium supernatant and bronchoalveolar lavage fluid that were almost identical to those in the model group.

**Lung histologic analysis**

As shown in Figure 9, lung tissue structures in the normal group were well defined without discernible damage or edema, and the trachea and blood vessels were not infiltrated peripherally by inflammatory cells. However, lung tissue and bronchial structures in the model group were disturbed by internal hemorrhage and edema. The bronchial and vascular walls were thickened and infiltrated by a considerable number of inflammatory cells. Lung tissue in the PLGA-rCmP group showed histologic changes with occasional inflammatory cell infiltration similar to that seen in the normal group. Although lung tissue in the rCmP group was free from edema and damage, there was markedly irregular architecture and inflammatory cell infiltration. Regardless, the histologic results of the rCmP group generally improved relative to those of the model group.

**Discussion**

Allergic airways disease mainly results from airborne pollens, that endanger over 100,000 people worldwide and 15%–30% of the population in developed countries. In addition to nonstandardized allergen diagnostic agents and vaccines, hypoallergenic tropical pollens have seldom been investigated, unlike the enormous studies done on hyperallergenic birch, olive, and ragweed pollens. The Palmae plant, which is widely distributed in Guangdong, Hainan, Guangxi, Fujian, and some subtropical regions in the People’s Republic of China, is the main source of pollen causing allergic disease in those regions. It was reported that positive skin test rates for *C. mitis* and *Phoenix roebelenii* pollens ranked highest for Palmae among 20 tested tropical plants. Profilin is an omnipresent panallergen in higher plants, and its highly conserved
structure accounts for the cross-reactive nature of IgE antibodies against plant pollen (and plant food) profilins and their designation as panallergens. Therefore, we prepared a novel rCmP vaccine and explored antigen specific immunotherapy to allergic asthma. Traditional vaccines that are metabolized rapidly are subject to the environment of the organism, and cannot be delivered intact to immune system targets and maintain long-term effects. On the other hand, PLGA is a biodegradable polymer approved by the US Food and Drug Administration and has been widely used, including in vaccines and medical industrial materials. Allergens encapsulated by PLGA are not exposed to environmental influences prior to being slowly released, this prolongs the therapeutic effects and stable delivery to the specific immune targets stimulating the immune responses of the host cells.

In this study, mice with allergic asthma were treated with PLGA-encapsulated rCmP utilizing a rCmP/Al(OH)₃ vaccine group and a blank PLGA nanoparticle group as controls. We confirmed that rCmP-loaded PLGA nanoparticles and rCmP both mitigated allergic inflammation, and the former treatment performed more effectively in inhibiting airway inflammation, decreasing vascular permeability, and dramatically reducing the numbers of inflammatory cells, especially eosinophils in bronchoalveolar lavage fluid. Meanwhile, rCmP-loaded PLGA nanoparticles effectively inhibited generation of serum IgE and induced serum IgG₂a, while facilitating binding between serum IgG and allergens and inhibiting binding between serum IgE and allergens. Moreover, secretion of the Th2 cytokine IL-4 and the Th1 cytokine IFN-γ were apparently suppressed and induced by rCmP-loaded PLGA nanoparticles, respectively, indicating that rCmP-loaded PLGA nanoparticles are a potent specific immunotherapy vaccine because of their ability to inhibit the Th2 response and stimulate the Th1 response. The augmented secretion of IL-10 after treatment with PLGA-rCmP indicates subsequent immune tolerance of allergen-specific T cells. Further, lung tissue in the PLGA-rCmP group showed histologic changes similar to that in the normal group in the presence of well defined structures without observable damage or edema, and the trachea and blood vessels were not infiltrated peripherally by inflammatory cells. Lung tissue in the rCmP group showed structural disturbance and mild infiltration by inflammatory cells, whereas the blank PLGA nanoparticles had no therapeutic benefit.

**Conclusion**

The rCmP-loaded PLGA nanoparticles synthesized in this study were able to prevent and treat asthma effectively by regulating Th1/Th2 equilibrium via downregulation of Th2 cytokine expression, inhibition of eosinophil differentiation, and induction of Th1 cytokine expression. PLGA acts more appropriately as a specific immunotherapy adjuvant for allergen vaccines than the conventional Al(OH)₃ adjuvant because of its superior efficacy and longer potency, and has remarkably fewer side effects. Hence, our attempt to prepare a novel and secure PLGA-allergen nanoparticle herein will innovate the immunotherapy of allergic asthma and provide theoretical evidence for the prevention and treatment of allergic disease.

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**Disclosure**

The authors report no conflicts of interest in this work.

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