Background: To establish a potential gene-delivery system with the ability to deliver plasmid DNA to dendritic cells (DCs) more efficiently and specifically, we designed and synthesized a low-molecular-weight polyethyleneimine and triethylene glycol polymer (PEI–TEG) and a series of its mannosylated derivatives.

Methods: PEI–TEG was synthesized from PEI2000 and PEI600 with TEG as the cross-linker. PEI–TEG was then linked to mannose via a phenylisothiocyanate bridge to obtain man-PEI–TEG conjugates. The DNA conveyance abilities of PEI–TEG, man-PEI–TEG, as well as control PEI25k were evaluated by measuring their zeta potential, particle size, and DNA-binding abilities. The in vitro cytotoxicity, cell uptake, and transfection efficiency of these PEI/DNA complexes were examined on the DC2.4 cell line. Finally, a maturation experiment evaluated the effect of costimulatory molecules CD40, CD80, and CD86 on murine bone marrow-derived DCs (BMDCs) using flow cytometry.

Results: PEI–TEG and man-PEI–TEG were successfully synthesized and were shown to retain the excellent properties of PEI25k for condensing DNA. Compared with PEI–TEG, PEI25k, the man-PEI–TEG had less cytotoxicity and performed better in both cellular uptake and transfection assays in vitro. The results of the maturation experiment showed that the PEI complexes induced an adequate upregulation of surface markers for DC maturation.

Conclusion: These results demonstrated that man-PEI–TEG can be employed as a DC-targeting gene-delivery system.

Keywords: dendritic cells, DCs, mannose, polyethyleneimine, PEI, gene delivery

Introduction
Over the last decade, there has been a lot of interest in DNA vaccines due to their ability to achieve potent immune responses without the limitations of many conventional vaccines. DNA vaccines offer a promising new approach for generating a wide range of desired immune responses, including cytolytic T lymphocytes (CTL), T helper cells, and antibodies, while being easy to administer and safe.

One of the keys to developing DNA vaccines is the establishment of an efficient and specific gene-delivery system that will allow the expression of antigenic protein and subsequent activation of T-cell immunity. A number of DNA delivery systems have been developed that utilize a variety of materials such as polymers, liposomes, and cationic polymers. Among these, the cationic polymer polyethyleneimine (PEI), which was introduced by Boussif et al has been widely studied due to its ability to deliver DNA with high efficiency. Because of its excellent performance as a vehicle for gene delivery, branched PEI25k has been used in a variety of materials such as polymers, liposomes, and cationic polymers. Among these, the cationic polymer polyethyleneimine (PEI), which was introduced by Boussif et al has been widely studied due to its ability to deliver DNA with high efficiency. Because of its excellent performance as a vehicle for gene delivery, branched PEI25k has been used.
as a standard reference for other new polymers. However, this system is significantly limited by its cytotoxicity. Recent reports have demonstrated that, compared with low-
molecular-weight PEI (LMW-PEI, such as PEI2000), high-
molecular-weight PEI (HMW-PEI, such as PEI25k) exhibits higher transfection efficiency and higher cytotoxicity. In our previous study, a biodegradable LMW-PEI polymer (PEI–TEG) was synthesized by cross-linking LMW-PEI through biscardamate linkages. It was shown that this was a promising and applicable gene-delivery carrier due to its lower cytotoxicity and higher gene transfection efficiency than commercial PEI25k.

Another major drawback of PEI-mediated gene-delivery systems is its nonspecific interaction with cells, which is especially important in DNA vaccine treatments that demand highly efficient delivery of antigen-encoded DNA to specific cells. A key point in the development of DNA vaccines is finding suitable target cells. Dendritic cells (DCs), which are the most effective antigen-presenting cells (APCs) of the immune system, are a key component for the regulation of both innate and adaptive immune responses as well as the maintenance of immunological tolerance. Due to their unique ability to efficiently present antigens to T cells, many researchers have focused on their application in DNA vaccines in recent years, and there is tremendous potential in developing DNA vaccines that target DCs with a DNA delivery system.

To enhance the specificity of our delivery system to DCs, a specific ligand is required. It has been demonstrated that there is an abundant expression of mannose receptor (MR) on the surface of APCs, including DCs. The MR has been shown to select ligands carrying terminal sugars such as mannose and N-acetylglucosamine, and to transport these into cells through receptor-mediated endocytosis, which results in major histocompatibility complex (MHC) presentation and subsequent T cell activation. This suggests that the mannosylation of a drug- or gene-delivery system may improve their DC specificity and, as expected, some mannosylated proteins have been shown to enhance MHC-I and -II restricted antigen presentation as well as T cell stimulation compared with non-mannosylated proteins. Furthermore, many mannosylated drug or gene-delivery systems such as mannosylated chitosan microspheres, mannosylated lipopolyplexes, mannosylated PEI, mannosylated PEI-coupled mesoporous silica nanoparticles, and mannosylated chitosan-graft-PEI have been reported to augment transfection efficiency and immunogenicity by targeting the MR on APCs. Therefore, in this study, mannose ligand was employed to provide selective DC targeting for the delivery of a DNA vaccine.

In the current study, a gene-delivery system based on a mannosylated, biodegradable LMW-PEI polymer (man-PEI–TEG) was designed and synthesized for the purpose of improving DC specificity, increasing transfection efficiency, and reducing cytotoxicity. Physiochemical properties of the carrier and its complexes prepared with plasmid DNA were analyzed. The in vitro cytotoxicity, transfection efficiency, and DC maturation abilities were also investigated.

**Materials and methods**

**Materials**

Branched PEI 25k, branched PEI 2k, 3-((4,5-dimethylthiazole-2-y))-2,5-diphenyl tetrazolium bromide (MTT), agarose, and HEPES were purchased from Sigma-Aldrich (St Louis, MO). PEI600 (Alfa Aesar, Ward Hill, MA) was used after vacuum drying at 70°C for 1 hour. Triethyleneglycol (TEG) was purchased from Kelong (Chengdu, China). The pH4.10(luc2) (4242 bp) plasmid DNA was isolated and purified from DH5-α. *Escherichia coli* using the Qiagen Giga Endo-free plasmid purification kit (Germantown, MD). Cell culture medium RPMI-1640 and fetal bovine serum (FBS) were obtained from Gibco Co (Life Technologies, Grand Island, NY). Luciferase assay system was procured from Promega (Madison, WI). BCA protein assay kit was obtained from KeyGEN. DC2.4 cell line was kindly provided by Dr Ying Wan of Third Military Medical University, China. All the other chemicals and solvents were obtained commercially and used without further purification.

**Synthesis and characterization of mannosylated PEI–TEG (man-PEI–TEG)**

**Synthesis of mannopyranosylphenyl isothiocyanate**

Mannopyranosylphenyl isothiocyanate was synthesized according to the methods of Munch et al and Shi et al. Briefly, 180 mL Ac₂O and 210 mL C₅H₅N were added to a three-necked bottle and cooled to −5°C, after which 20 g D-mannose was gradually added. The mixture was stirred for 5 hours at room temperature and then poured into 2 L of icy water. As a result, a crude acetylated mannose precipitate was obtained. BF₃·Et₂O was added slowly to 11.7 g of the solution of the crude acetylated mannose precipitate and 8.4 g p-nitrophenol in 100 mL CH₂Cl₂. After this was stirred at 25°C for 24 hours, the solvent was removed and then purified by silica gel chromatography to yield p-nitrophenol-1-acetylated mannose. Then 5.5 g of the p-nitrophenol-1-acetylated mannose was dissolved in 50 mL absolute MeOH and a small amount of MeONa was added and stirred at room temperature for 1 hour, then cation
Synthesis of PEI polymer with triethylene glycol (TEG) as the cross-linker (PEI–TEG)
The synthesis method of the PEI derivate with TEG as the cross-linker was presented by Zhao et al. Briefly, 1.5 g anhydrous triethylene glycol (TEG, 10.0 mmol) was dissolved in 250 mL anhydrous ethylene dichloride and then 6.04 g 4-nitrophenyl chloroformate (NPC, 30.0 mmol) was added. The solution was stirred and 4.15 mL EtN3 (30.0 mmol) was added. The reaction mixture was stirred at room temperature for 6 hours, and was subsequently washed with saturated NaCl solution and the organic phase was collected and dried over anhydrous Na2SO4. After this, the solvent was added dropwise to 20.0 g of the mixture of PEI600 and PEI2000, which was dissolved in ethylene dichloride, and the weight ratio of PEI600:PEI2000 (1:3) employed was optimized in a previous study (data not shown). After stirring for another 16 hours, the solution was evaporated to remove the solvent. The viscous residue was dissolved again in double-distilled water and dialyzed through a cellulose membrane with a molecular weight cut off of 3500 Da.

Characterization of man-PEI conjugates
Nuclear magnetic resonance (NMR) was used to confirm the structure of products. For proton NMR (1H-NMR) experiments, the mannosylated phenyl isothiocyanate and PEI derivatives were dissolved in CD2OD and D2O (purchased from Sigma-Aldrich) respectively. The samples were analyzed in a Varian UNITY INOVA 400 NMR Spectrometer (Varian Inc., Palo Alto, CA) at 400 MHz.

The molecular weight and polydispersity index (PDI) of the PEI–TEG and man-PEI–TEG conjugates were determined by gel permeation chromatography (GPC) relative to PEG standards (Polymer Labs, Amherst, MA). Compared to PEI–TEG, the molecular weights of mannosylated PEI–TEG A, B, and C were increasingly affected by an increase in mannose residues. The formula below can be used to calculate the weight ratio of mannose residues in man-PEI–TEG conjugates A, B, and C:

\[
\text{Mannose} \% = \frac{\text{Mw man-PEI–TEG} - \text{Mw PEI–TEG}}{\text{Mw man-PEI–TEG}} \times 100\%
\]

Table 1: Characteristics of the PEI–TEG and man-PEI–TEG derivates: feed ratio, weight-average molecular weight (Mw), polydispersity index (PDI), and mannose content

<table>
<thead>
<tr>
<th>Polymers</th>
<th>PEI:mannose (weight ratio)</th>
<th>Mw (kDa)</th>
<th>PDI</th>
<th>Theoretical mannose %</th>
<th>Experimental mannose %</th>
</tr>
</thead>
<tbody>
<tr>
<td>PEI–TEG</td>
<td></td>
<td>26.02</td>
<td>1.53</td>
<td></td>
<td></td>
</tr>
<tr>
<td>A</td>
<td>1:1</td>
<td>40.05</td>
<td>1.94</td>
<td>50.0%</td>
<td>35.0%</td>
</tr>
<tr>
<td>B</td>
<td>2:1</td>
<td>38.73</td>
<td>1.94</td>
<td>33.3%</td>
<td>32.8%</td>
</tr>
<tr>
<td>C</td>
<td>3:1</td>
<td>34.40</td>
<td>1.89</td>
<td>25.0%</td>
<td>24.4%</td>
</tr>
</tbody>
</table>

Abbreviations: PEI, polyethyleneimine; TEG, triethylene glycol; PEI–TEG, polyethyleneimine and triethylene glycol polymer; man-PEI–TEG, mannosylated PEI–TEG; A, man-PEI–TEG derivative A; B, man-PEI–TEG derivative B; C, man-PEI–TEG derivative C; Mw, molecular weight; PDI, polydispersity index.
man-PEI/DNA complex preparation
The preparation of the man-PEI–TEG/DNA complex was performed according to the delineation published by Kloeckner et al. DNA plasmid (pGL4.10 (luc2)) was diluted in 5% glucose solution to a final concentration of 80 µg/mL, and the indicated amounts of man-PEI–TEG derivates were also diluted to the same volume with 5% glucose solution (pH 4.0). Following this, the DNA solution was added into the PEI solution and was vortexed for 10 seconds, then incubated at room temperature for 20 minutes. To obtain complexes of different carrier: DNA ratios, DNA was condensed by man-PEI–TEG derivates at various mass ratios. In this work, PEI derivates to DNA ratios were expressed by both weight ratios and N/P ratios, and the following formula can be used to convert the weight ratios to N/P ratios:

\[ N/P = \frac{W_{PEI}}{W_{DNA}} \times \frac{E_{DNA}}{E_{WPEI}} \]

where N is the equivalent of ionizable nitrogen, P is the equivalent of ionizable phosphorous, W refers to weight, and EW refers to equivalent weight.

Particle size and zeta potential analysis
The mean particle size and zeta potential of the DNA/PEI complexes were determined at 25°C using photon correlation spectroscopy (PCS) (Zetasizer Nano ZS90; Malvern Instruments Ltd, Worcestershire, UK). Before measurement, the PEI/DNA complexes of N/P ratios ranging from 5:1 to 40:1 were prepared as described above. Each complex sample contained 10 µg plasmid DNA and was diluted to a final volume of 1 mL in 5% glucose solution.

Gel retardation assays
Electrophoresis was employed to confirm the DNA binding ability of the man-PEI–TEG derivates. The PEI/DNA complexes were prepared at PEI:DNA mass ratios of 2:1 and 3:1, then mixed with 6x loading buffer (Generay Biotech, Shanghai, China) and analyzed by gel electrophoresis on a 1.0% agarose gel containing 0.006% Goldview nucleic acid stain (Viswagen Biotech Pvt. Ltd, Kerala, India). After electrophoresis at 80 V for 45 minutes, the bands of plasmid DNA were visualized and photographed by molecular imager (ChemiDoc™ XRS system; Bio-Rad, Hercules, CA).

DNase I protection assay
The ability of man-PEI–TEG derivates to protect and release DNA in complex was ascertained by gel electrophoresis. In short, 2 µL DNase I (1 unit) or phosphate-buffered saline (PBS; as a negative control) were added to 10 µL naked plasmid DNA solution (0.5 µg) or DNA/PEI complex solutions (with the mass ratio of PEI:DNA 3:1), and this was shaken at 100 rpm at 37°C for 1 hour. Following this, all of the samples were treated with 4 µL EDTA (250 mM) for 10 minute and then mixed with 10 µL sodium dodecyl sulfate (SDS) (1% in 0.1 M NaOH) for the purpose of DNase I inactivation and DNA release, respectively. The samples were incubated at room temperature for 1 hour, and then electrophoresis was performed under the same conditions described above.

Cytotoxicity assay
The cytotoxicity of man-PEI–TEG derivates was evaluated by 3-(4,5-dimethylthiazol-2-yl)-2, 5-diphenyltetrazolium bromide (MTT) assay according to the method of Mosmann et al. The PEI/DNA complexes of each PEI derivate that was prepared at N/P ratios ranging from 5 to 50 were added to DC2.4 cells in 96-well plates. After incubation for 24 hours, MTT (5 mg/mL, 20 µL) was added and reacted for 4 hours at 37°C. Following this, the medium of each well was replaced with 150 µL dimethylsulfoxide (DMSO) to dissolve the formazan crystals. The absorbance at 570 nm of each well was measured using a Varioskan Flash multimode reader (Thermo Fisher Scientific, Waltham, MA). Cell viability was calculated by absorbance of cells pulsed with PEI, and absorbance of untreated cells x 100%. All values presented below represent means of multiple measurements with SD values indicated.

In vitro uptakes by DC2.4
Twenty-four hours prior to the experiments, DC2.4 cells were seeded in 6-wells plates in which each well had been covered by sterile coverslips at 4 x 105 cells/well. The fluorescence-labeled complexes were prepared by mixing fluorescein isothiocyanate (FITC)-labeled PEI derivates with DNA plasmid at the optimal N/P ratio of each derivate. After vortexing and incubating the complex solutions at room temperature for 20 minutes, these were added to the DC2.4 cells adhered to the coverslips in the 6-well plates. Cells were then incubated for 1 hour at 37°C; control cells were processed similarly but incubated at 4°C. Coverslips were then washed by dipping in PBS prior to fixation with 4% paraformaldehyde (5 minutes, RT) and subsequent staining with 2 µg/mL diamidino phenylindole (DAPI). After washing the coverslips three times with PBS, they were then mounted on glass slides with 50% glycerol in 0.2 M Tris-HCl (pH 8.0) containing 2% n-propyl gallate to retard
quenching of the fluorescence signal. Confocal microscopy was performed using a LSM510 confocal microscopy system (Carl Zeiss SMT GmBH, Heidelberg, Germany). All images were collected using the same values for photomultiplier gain, aperture diaphragm, and black levels.

**In vitro competition assay**

For competition assays, cells and fluorescence-labeled complexes were prepared as described above. To block the binding of man-PEI–TEG to MR, cells were pre-incubated for 20 minutes with 0.125 mg/mL mannan dissolved in RPMI-1640 or, as a control, with free RPMI-1640. Following this, FITC labeled complexes were added and cells were incubated for 1 hour at 37°C. After washing the cells three times with PBS, these were removed from wells using 0.25% trypsin and resuspended in FACS buffer. The level of FITC fluorescence of cells was analyzed by flow cytometry using a FC500 flow cytometer (Beckman Coulter Inc, Brea, CA). Data analysis was performed using the Kaluza* software (Beckman Coulter Inc).

**In vitro DC2.4 transfection assay**

The transfection assay was performed on the DC2.4 cell line with the pGL4.10 (luc2) plasmid encoding luciferase as the reporter gene. DC2.4 cells cultured in RPMI-1640 and supplemented with 10% FBS were seeded onto 24-well plates at 1 × 105 cells/well 24 hours before transfection. When approximately 70% confluence was reached, the cells were gently washed twice with PBS and the medium of each well was replaced with 200 µL serum-free culture medium. Following this, 25 µL DNA/PEI complex solutions containing 1 µg plasmid DNA at different N/P ratios was added to each well. After 4 hours of incubation, the transfection medium was removed and 1 mL fresh complete culture medium was added to each well and left to continue culturing for a further 20 hours at 37°C in a 5% CO2 incubator. Luciferase expression was measured using a luciferase assay system (Promega Corporation, Madison, WI) following the manufacturer’s instructions. The total protein concentration of transfected cells was determined by a BCA protein assay (KeyGEN, Nanjing, China). The luciferase expression level was calculated as relative lights units (RLU)/mg total protein.

**In vitro BMDCs maturation assay**

**BMDCs culture**

Murine bone marrow-derived DCs (BMDCs) used in this experiment were derived as described by Inaba et al.28 The bone marrow progenitor cells were harvested from 6-week-old C57BL/6 male mice that were purchased from West China Experimental Animal Center of Sichuan University (China). Ten mice were sacrificed and sterilized with 75% ethanol. Femurs were gently removed from mice and the muscles adhered on bones were removed with sterilized gauze. The bones were then immersed in 75% ethanol for 2 minutes for sterilization, then washed twice with ice-cold PBS (pH 7.2), and cultured in a petri dish containing ice-cold RPMI-1640 medium. Both ends (epiphyses) of each bone were cut off and each hollow of the bones was flushed with 2 mL RPMI-1640 medium by inserting a needle into the hollow to obtain as many cells as possible. The cell suspension was filtered through a 70 µm cell strainer (BD, Franklin Lakes, NJ) to remove tissue before centrifugation at 1000 rpm for 10 minutes to collect cells. These were then washed with RPMI-1640 containing 10% FBS (1640-10F) and cultured in petri dishes with R5 medium (RPMI-1640 medium supplemented with 20 ng/mL GM-CSF (R&D Systems, Minneapolis, MN), 10 mM HEPES, 50 µM 2-mercaptoethanol, 10% FBS, and antibiotic) at a total volume of 10 mL medium per dish. Cells were then washed and fed every 2 days. On day 4, aggregates of growing DC were observed attaching to the adherent stroma. These aggregates raised above the monolayer, in contrast to the flattened dispersed macrophage colonies. Spiky processes (dendrites) were also seen extending from the periphery of the aggregates, giving them a hairy or thistle-like appearance. On day 6, the aggregates were harvested by gently pipetting over the adherent stroma. The cells were pooled and centrifuged before being resuspended with RPMI-1640 containing 50% FBS (1640-50F), and incubated at 37°C for 30 minutes to dissociate the residual granulocytes. Following this, the cells were washed twice with 1640-10F medium and resuspended with R5 medium. They were then seeded into 6-well plate at a cell density of 5 × 106 cells/well and a total volume of 2 mL/well.

To determine the purity of BMDCs (the percentage of CD11c+ cells), the FITC-labeled mouse CD11c antibody (eBiosience, San Diego, CA) was used to stain cells, which were then analyzed by flow cytometry. The percentage of CD11c+ cells in cultures was approximately 80%–90%.

**BMDCs maturation in vitro**

The DNA/PEI complexes were prepared with their optimal N/P ratios determined in the in vitro transfection experiment, and were added to BMDCs 6-well plates at 4 µg DNA per well. PBS and 2 µg/mL lipopolysaccharide (LPS) were also added as the negative and positive control, respectively. After
24 hours’ incubation, cells were washed and stained with PE-Cy5/FITC/PE-labeled mouse CD80/CD86/CD40 antibody (eBiosience) at 4°C for 1 hour, then cells were determined by flow cytometry. The isotype control antibodies (eBiosience) for each type of the specific monoclonal antibody were employed to eliminate the autofluorescence of samples.

**Results**

**Synthesis and characterization of man-PEI–TEG**

The low molecular weight PEI polymers (PEI–TEG) and mannosylated PEI–TEG (man-PEI–TEG) were synthesized successfully. Figure 1 shows a simplified flowchart illustrating the method of synthesis. The composition of the synthesized copolymers was analyzed by 1H-NMR, and the chemical shift of each proton peak is showed in Figure 2.

The proton peak of the phenylisothiocyanate in mannosylphenyl isothiocyanate (–CH–) appeared at 7.4–7.0 ppm, and the proton peaks of PEI (–NHCH2CH2-) appeared at 3.3–2.5 ppm, confirming that mannose had successfully been linked to PEI–TEG.

Gel permeation chromatography (GPC) analysis determined that the average molecular weights (Mw) of PEI–TEG and three mannosylated derivates (A, B, and C) were 26.02, 40.05, 38.73, and 34.40 kDa, respectively. The weight ratios of mannose residues in man-PEI–TEG (A, B, 

![Figure 1](https://www.dovepress.com/150x36.png)
and C) were calculated to be 35.0%, 32.8%, and 24.4%, respectively, which were consistent with the theoretical values (Table 1).

Characterization of PEI/DNA complex

A series of PEI/DNA complexes were successfully obtained, and their pH ranged from 4.3 to 5.2 in 5% glucose solution. The DNA conveyance ability of PEI–TEG and man-PEI–TEG was evaluated by examining properties such as zeta potential, particle size, and their ability to bind and protect DNA from DNase degradation.

The results of the average size and zeta-potential assays are shown in Figure 3, and it can be seen that the average particle size of all the complex samples spanned a range from 110 to 260 nm, with a narrow size distribution (PDI, 0.2). Moreover, all of the DNA/PEI complexes (except those of derivates A and B at the N/P ratio of 5) were positively charged, with the positive charge increasing as the N/P ratio increased from 5 to 40.

In vitro cytotoxicity, cellular uptake, and transfection on DC2.4

DC2.4, a dendritic cell line that expresses moderate MRs, was used to determine the cytotoxicity, cellular uptake, and transfection efficiency of the PEI derivates/DNA complexes in vitro.

As is shown in Figure 5, cytotoxicity increased for all PEI/DNA complexes as the N/P ratio increased, and the viability of cells treated by the three mannosylated derivates (A, B, and C) as well as PEI–TEG was significantly higher than that of commercial PEI25k. As well as this, when the N/P ratio was greater than 30 the relative cell viabilities of PEI–TEG began to decrease quickly, while those of the mannosylated derivates (A, B, and C) remained above 80% even at the highest N/P ratio of 50.

The expression of reporter genes was evaluated using a luciferase assay system, and the data shown...
in Figure 6 indicate that the luciferase expression in cells transfected with the positive control PEI25k/DNA complex was about 100 times greater than the expression of the naked plasmid DNA-treated group ($P < 0.01$), but remained 2–3 times lower than that of the PEI–TEG/DNA complex ($P < 0.03$). In contrast to this, the man-PEI–TEG/DNA complexes exhibited an approximately three-times higher transfection efficiency than the complexes made from the PEI–TEG ($P < 0.01$). Among the three mannosylated PEI–TEG derivates, B (with the mannose weight

Figure 3 Characterization of PEI/DNA complex (n = 3). (A) Average particle size, (B) Zeta-potential.

Note: The PEI/DNA complexes were prepared at an N/P ratio ranging from 5:1 to 40:1, determined using photon correlation spectroscopy.

Abbreviations: PEI, polyethyleneimine; TEG, triethyleneglycol; PEI–TEG, polyethyleneimine and triethyleneglycol polymer; A, mannosylated PEI–TEG derivative A; B, mannosylated PEI–TEG derivative B; C, mannosylated PEI–TEG derivative C; PEI25k, polyethyleneimine with a molecular weight of 25 kD.

Figure 4 DNA retardation and DNase I protection assay. (A) DNA-binding abilities of all PEI derivates were examined by agarose gel electrophoresis, and the examining mass ratios of PEI:DNA were 2:1 and 3:1 respectively. (B) PEI/DNA complexes were prepared at a ratio of 3:1 (w/w) and tested for their abilities to protecting DNA against the DNase I degradation.

Notes: +, samples treated with DNase I; −, samples treated with PBS.

Abbreviations: PEI, polyethyleneimine; TEG, triethyleneglycol; PEI–TEG, polyethyleneimine and triethyleneglycol polymer; A, mannosylated PEI–TEG derivative A; B, mannosylated PEI–TEG derivative B; C, mannosylated PEI–TEG derivative C; PEI25k, polyethyleneimine with a molecular weight of 25 kD.
The introduction of mannose as a ligand into the gene carriers for specific recognition by DC cells may enhance the transfer across the cell membrane, so the cellular uptake of complexes was also determined. Cells were incubated with FITC-labeled PEI derivates/DNA complexes at 37°C/4°C for 1 hour and then photographed by confocal microscopy. As is shown in Figure 7, after being incubated at 37°C for 1 hour the cells treated with man-PEI–TEG-B exhibited significantly more green fluorescence than those treated with PEI25k and PEI–TEG. For man-PEI–TEG-B, almost all of the green fluorescence was observed within the cells. In contrast, for PEI25k and, to an even greater extent, PEI–TEG, a large proportion of the green fluorescence did not enter the cell but only adsorbed onto the surface of the cells, so most of the green fluorescence was observed in rings around the cells. The uptake results of the three groups at 4°C were approximately the same, indicating that almost no complex was taken up by cells.

In order to further investigate the mechanism of internalization of mannosylated complexes, a competition experiment was performed with mannan. As is shown in Figure 8, the mean fluorescence intensity (MFI) of man-PEI–TEG cells pre-incubated with mannan was 4–5-fold lower than that of
control cells. For PEI25k and PEI–TEG, the MFI of the two groups of cells were very similar.

**BMDCs maturation in vitro**

To assess the effect of PEI/DNA complexes on the maturation of mouse BMDCs, levels of the costimulatory molecules CD40, CD80, and CD86 were measured by flow cytometry. As is shown in Figure 9, after 24 hours of culturing with BMDCs, the positive control LPS conspicuously upregulated the expression of the three costimulatory molecules, while PEI25k, PEI–TEG, and man-PEI–TEG all induced remarkable upregulation of the molecules compared to the negative control \((P < 0.01)\), but this was not as strong as that of LPS \((P < 0.01)\), and the upregulation...
intensity of the three carriers were approximately the same ($P > 0.05$).

**Discussion**

In the present study, a series of mannosylated biodegradable LMW-PEI polymers (man-PEI–TEG) were designed and synthesized. The LMW-PEI polymer (PEI–TEG) was synthesized with triethyleneglycol (TEG) as the cross-linker and, to be assigned the DC specificity, the PEI–TEG was mannosylated by the thiourea reaction between the isothiocyanate group of mannopyranosylphenyl isothiocyanate and the primary amine groups of PEI–TEG. Three man-PEI–TEG conjugates (A, B, and C) were obtained, for which the mannose substitution degrees were 35%, 32.8%, and 24.4%, respectively. It appears that this is the first time that this kind of PEI derivate has been reported.

To ensure that the PEI–TEG and its mannosylated derivates that were generated are capable of delivering plasmid DNA, they must be able to bind and condense the plasmid DNA as efficiently as PEI alone. The results of gel electrophoresis to ascertain derivates’ DNA condensation ability suggest that the DNA binding abilities of PEI25k, PEI–TEG, and C were stronger than those of A and B (Figure 4), which may be ascribed to the less positive charge that A and B have due to the mannosylation of the primary amines. This suggests that a higher weight ratio of A/B to DNA is required to completely condense plasmid DNA, while DNA in the gene vehicle should be protected from enzymatic degradation for efficient transfection. The electrophoresis assay also indicated that PEI–TEG and its mannosylated derivates A, B, and C were all able to protect DNA against hydrolysis by nucleases. Furthermore, according to the results of photon correlation spectroscopy, the particle sizes of all PEI/DNA complexes made by these derivates were nano-sized (110–260 nm) with a narrow distribution, which would be favorable for gene delivery. These results indicate that the man-PEI–TEG derivates have retained the excellent properties of PEI for a self-assembled nanoparticle system.

Applicable gene carriers should be non-toxic or minimally toxic, so it was necessary to measure the cytotoxicity of the PEI derivates using a MTT assay. The results (Figure 5) indicate that the cytotoxicity of complexes prepared by PEI–TEG was significantly lower than that of commercial PEI25k, which was consistent with previous studies. When the N/P ratio increased to 30, however, the cytotoxicity of the PEI–TEG/DNA complexes increased, while those of the man-
PEI–TEG/DNA complexes remained low. This indicates that the incorporation of mannose residues played a further role in diminishing the toxicity of carriers.

In the preliminary transfection experiment it was initially found that the transfection efficiency of PEI derivates would be enhanced as the N/P ratio of the PEI/DNA complex was increased. When the N/P ratio was increased too much, however, the transfection efficiency began to drop due to the increasing cytotoxicity of the complexes. As the cytotoxicity of the carriers differed, the optimal transfection N/P ratio for each polymer was selected to ensure that all carriers could obtain an optimal transfection efficiency (data not shown). In the DC2.4 cell line, the optimal N/P ratios of the complex of PEI25k, PEI–TEG, and man-PEI–TEG conjugates A, B, and C were 10, 30, 50, 40, and 30, respectively. Based on the MTT assay, the relative cell viabilities of complexes were all above 80% at their optimal N/P ratio. It was demonstrated in the transfection result (Figure 6) that the biodegradable LMW-PEI polymer PEI–TEG had a better performance in transfection than commercial PEI25k. The most likely reason for this is that the degradable PEI–TEG polymer had a capacity for binding to negatively charged molecules (such as translation-related proteins or mRNA) in the cytoplasm, which would inhibit transfection. Moreover, the mannose residues significantly improved the transfection efficiency of the carrier system. The degree of mannosylation, however, did not simply increase as more mannose was added. In a previous study mannosylated derivates were introduced with different PEI–TEG to mannopyranosylphenyl isothiocyanate feed ratios (1:4, 1:3, 1:2, 4:1, and 8:1), and these had an inferior performance to those in the current study (1:1, 2:1, and 3:1) (data not shown). Moreover, among the three mannosylated derivates reported here, B (32.8% mannose) performed better than A (35% mannose) and C (24.4% mannose). As has been reported previously, the cationic polymer PEI has a strong buffering capacity due to the numerous primary amines in its structure, and this could protect DNA from nuclease degradation and facilitate endosomal escape through the “proton sponge hypothesis,” so becoming highly efficient at delivering DNA. In order to synthesize the man-PEI–TEG conjugate, mannose had to be linked to PEI via a phenylisothiocyanate bridge between the isothiocyanate group of mannopyranosylphenyl isothiocyanate and the primary amine groups of PEI, which meant that the more mannose residues that were linked the weaker buffering capacity the conjugates had. The result of this was that while the mannose residues could offer the carry system the potential to target the MRs expressed on DCs and thus enhance their uptake by receptor-mediated endocytosis, after uptake by cells these residues could slow the further function of PEI. This indicates that it is important to find a balance between those two factors; the current study suggests that man-PEI–TEG-B has optimal mannosylation.

The improved cellular trafficking of synthesized polymers was also confirmed by confocal microscopy. As shown in Figure 7, significantly more fluorescence had been internalized by cells treated with man-PEI–TEG-B and localized in cytoplasm after 60 minutes’ incubation at 37°C than was observed in either PEI25k or PEI–TEG. Additionally, the complexes prepared with PEI–TEG were more likely to be located at the area close to the membrane, while most of the green fluorescence appeared within the cells of the man-PEI–TEG-B-treated group. This indicates that, as expected, incorporation of mannose ligand can facilitate the cellular uptake of the complexes via an alternative pathway that was most likely receptor-mediated endocytosis. However, the correlation between the amount of uptake and the substitution degrees of mannose ligand was not significant in the current study (data not shown).

Furthermore, as was observed in the competition assay (Figure 8), the uptake of man-PEI–TEG/DNA complexes was significantly inhibited in the presence of mannan, while those of PEI25k/DNA and PEI–TEG/DNA were relatively unaffected. This confirmed our hypothesis that the internalization of the mannosylated complexes predominantly occurs via mechanisms dependent on MRs on the cell surface (that is, MR-mediated endocytosis).

It is well known that immature DCs (iDCs) are specialized for antigen capture whereas mature DCs are capable of antigen-presentation and T cell-priming, and the ability of DCs to regulate immunity is dependent on DC maturation stage. This means that when a gene-delivery system targeting DCs is designed, the DC maturation ability of the system is a crucial parameter to consider. A variety of factors can induce maturation following antigen uptake and processing within DCs, including whole bacteria or bacterial-derived antigens (eg, lipopolysaccharide), ligands of certain cell surface receptors (eg, CD40), inflammatory cytokines, and viral products (eg, double-stranded RNA). During their conversion from immature to mature cells, DCs undergo a number of phenotypical and functional changes including a redistribution of major histocompatibility complex molecules from intracellular endocytic compartments to the DC surface, down-regulation of antigen internalization, and upregulation of the surface...
expression of costimulatory molecules such as CD40, CD80, and CD86. With this in mind, the maturation stage of BMDCs through the expressing level of CD40, CD80, and CD86 were examined with PBS and LPS as negative and positive controls, respectively. The results, shown in Figure 9, show that the maturation abilities of complexes based on PEI derivates were not as strong as those of LPS. However, compared to other systems such as poly(lactic-co-glycolic acid) and polyethylene glycol-block-poly(aminooethyl methacrylate), which had been reported to only slightly alter the phenotypes of iBMDCs, the PEI system in the current study could significantly upregulate the expression of the costimulatory molecules. Given that CD40 and CD86 play an important role in the induction of adaptive immunity through activation of CD4+ T cells, this result would be beneficial for the application of DNA vaccines specifically targeting DCs.

**Conclusion**

In this study, a series of man-PEI–TEGs were successfully synthesized and evaluated as a novel gene delivery carrier for DC targeting. The man-PEI–TEG polymers demonstrated the ability to form PEI/DNA complexes with physicochemical properties that would make them suitable as a gene delivery carrier. Furthermore, man-PEI–TEG showed significantly lower cytotoxicity and higher transfection efficiency on the DC2.4 cell line than commercial PEI25k, and demonstrated adequate maturation ability on BMDCs. With further improvement, it appears that these mannosylated PEI polymers will show potential as carriers for targeting DNA vaccines to DCs.

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**Disclosure**

The authors report no conflicts of interest in this work.

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