# In-silico assessment of airway deposition using functional respiratory imaging for mono, dual, and triple combination Co-Suspension<sup>™</sup> metered dose inhaler formulations

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# Introduction

- Co-Suspension<sup>™</sup> Technology for metered dose inhalers (MDIs) is a promising new platform with the potential to deliver single or multiple active agent particles consistently and uniformly throughout the lung using phospholipid porous particles as suspension and aerosolizing agents.
- Adequate deposition of medicinal aerosols to the airways is important for achieving the intended therapeutic benefits in patients with chronic obstructive pulmonary disease (COPD).<sup>1</sup>
- Inconsistent drug delivery, either due to formulation issues or improper device use, may lead to inadequate drug delivery to the airways.
- Robust formulations containing single or multiple active agents, with similar *in-vitro* performance for each active agent within and across formulations, can be made using the Co-Suspension<sup>™</sup> Technology.<sup>2</sup>
- In this computer simulation (*in-silico*) study, the deposition of different active agents from their Co-Suspension<sup>™</sup> Technology formulations, and the impact of extrathoracic airway geometries, inhalation profiles, and actuation conditions on lung deposition, were assessed using functional respiratory imaging (FRI).

# Methods

- Computerized tomography scans of 20 patients with COPD with a range of disease severity were selected.
- COPD severity was based on the forced expiratory volume in 1 second (FEV,), and included mild  $(n = 5, FEV_1 = 89.8 \pm 6.8\%$  predicted), moderate  $(n = 5, FEV_1 = 59.9 \pm 11.6\%$  predicted), severe  $(n = 5, FEV_1 = 33.3 \pm 6.7\%$  predicted), and very severe  $(n = 5, FEV_1 = 27.5 \pm 9.5\%$  predicted) COPD patients.
- Using the FRI workflow, three-dimensional (3D) computer models of the intrathoracic airways, lungs, and lobes were extracted. Five 3D models of extrathoracic upper airways were selected based on their minimal cross-sectional area (smallest, 25th percentile, median, 75th percentile, largest) and the geometry of the MDI was added to these models.
- Every extrathoracic geometry was combined with one intrathoracic geometry of every disease severity
- FRI was used to simulate the lung deposition of different formulations made by Co-Suspension<sup>™</sup> Technology, using *in-silico* computational flow simulations, incorporating several drug- (measured by next-generation impactor) and device-specific parameters:
- Delivered dose (µg) Fine particle fraction (% of delivered dose)
- Mass mean aerodynamic diameter (µm) Geometric standard deviation
- Plume velocity
- Plume angle
- The above-mentioned drug delivery attributes of glycopyrrolate (GP) or formoterol fumarate (FF) monocomponents, GP and FF dual combination (GFF), and two strengths of budesonide/GP/FF triple combination (BGF) Co-Suspension<sup>™</sup> Technology MDI formulations were used.
- The relative lobar expansion, as obtained from the subject-specific inspiratory and expiratory scans, were used as boundary conditions at the terminal airways. Sinusoidal inhalation maneuvers with flow rates of 15, 30, 60, 90, and 120 L/min were simulated. Aerosol injection was performed at two different timepoints: at the start of inhalation and when the flow rate was maximal.
- The influence of the different parameters on lung deposition was assessed using linear mixedeffect models.
- Equivalence of the various Co-Suspension<sup>™</sup> Technology formulations was assessed using two one-sided tests.

## Results

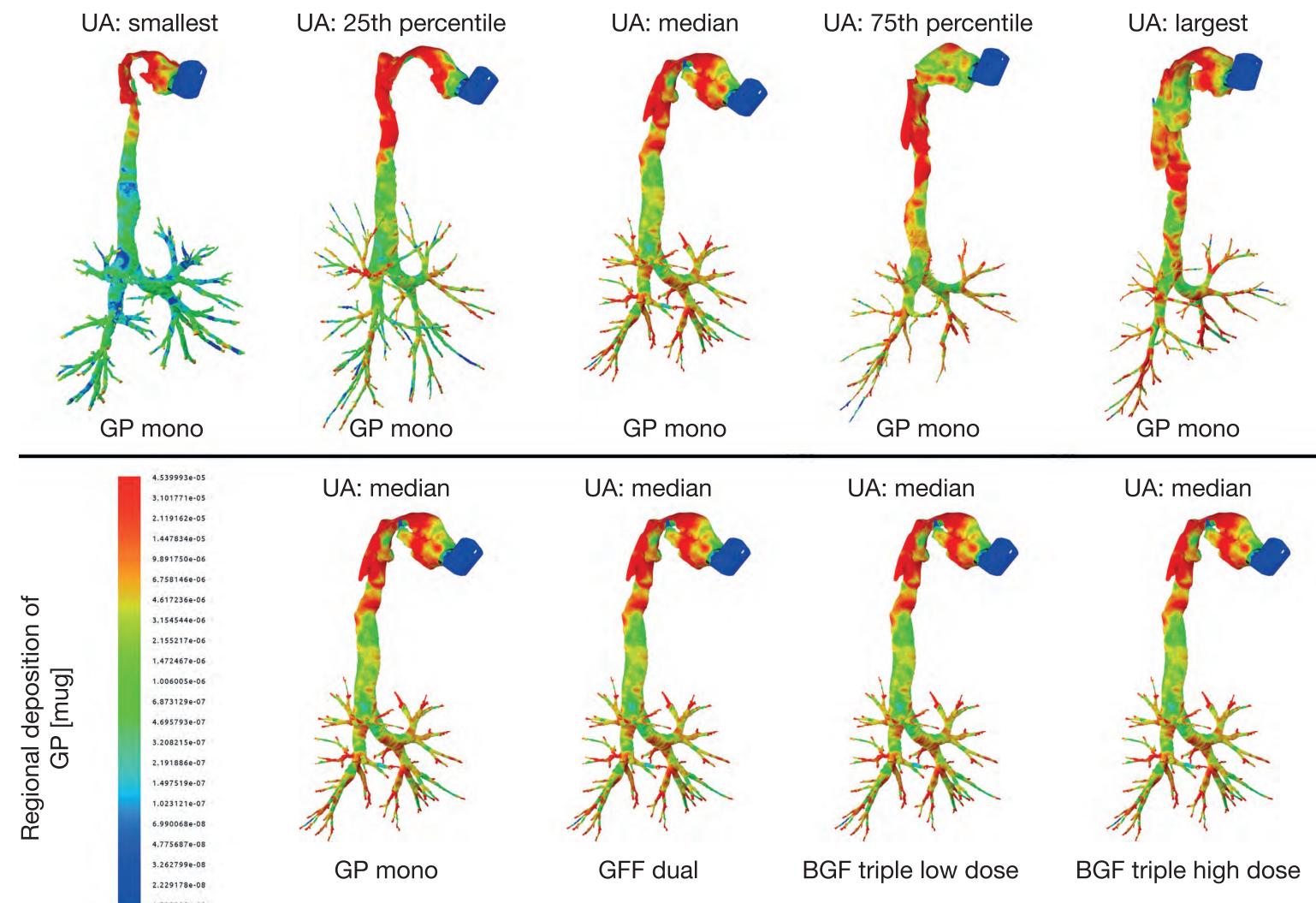
- Extrathoracic upper airway geometry has a large influence on deposition (Figures 1 and 2). Larger cross-sectional areas result in higher lung doses.
- For a given flow rate and disease severity, consistent lung deposition was obtained across mono, dual, and triple Co-Suspension<sup>™</sup> Technology formulations (Table 1).
- The total lung deposition did not significantly change across the multiple formulation types (Figures 2 and 3).
- The total lung dose of both GP (Figure 2) and FF (Figure 3) was equivalent when delivered in mono, dual, and triple combinations.
- The influence of BGF MDI dose on the lung dose of budesonide is shown in Figure 4.

#### Figure 1. Influence of extrathoracic UA geometry on FF lung deposition \_\_\_\_\_ \_\_\_\_\_I 0.5 – \_\_\_\_\_ Smallest 25th percentile 75th percentile Median Largest UA cross-sectional area

FF, formoterol fumarate; UA, upper airway

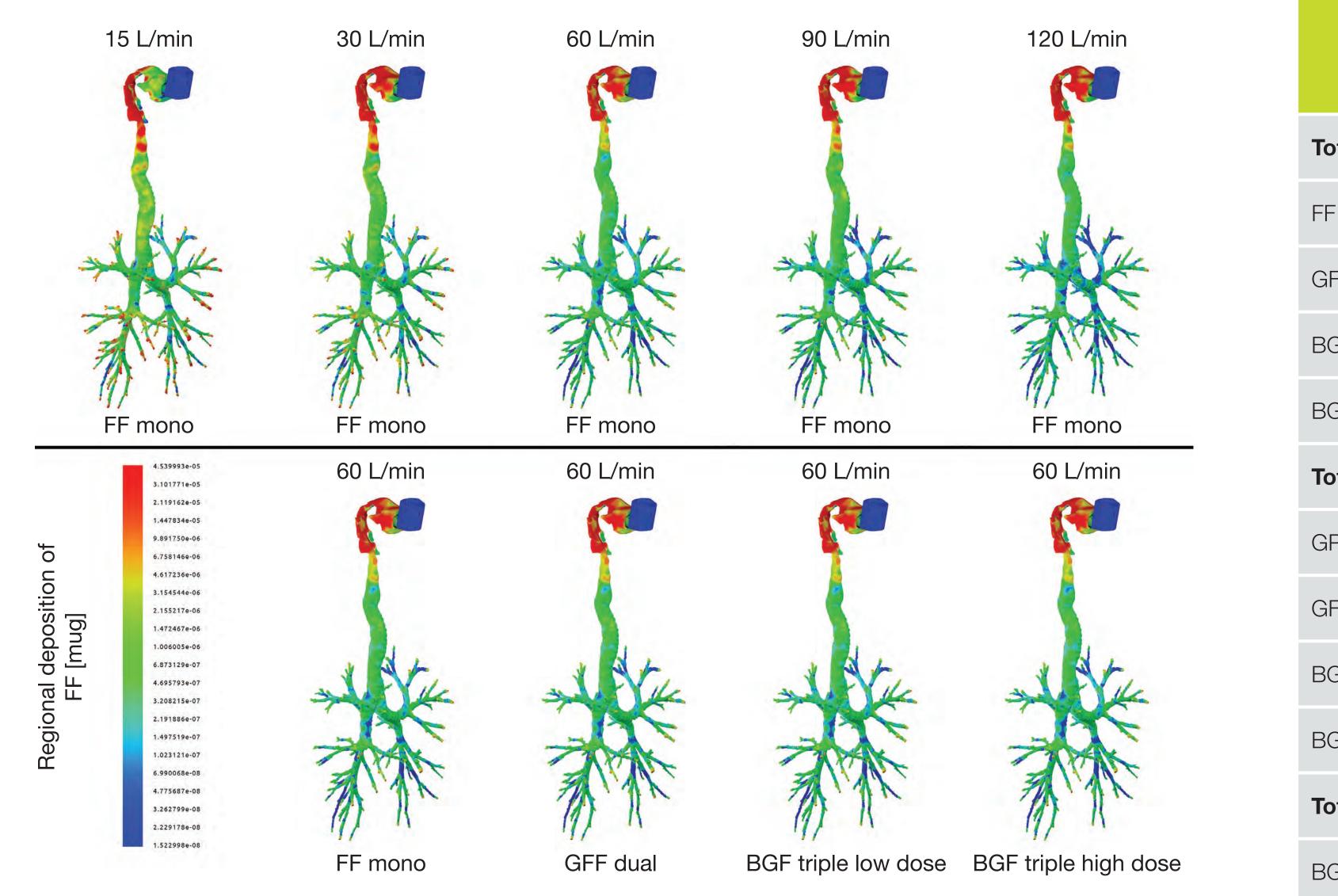
The bottom and top edges of the box represent the first (25th percentile) and bottom (75th percentile) quartiles; the horizontal line within the box represents the median. The vertical lines show the minimum and maximum values, and circles represent extreme values 1.5 times above/below the interguartile range.

Figure 2. Influence of extrathoracic UA geometry on the regional deposition of GP in five patients with moderate COPD (top row); and the consistency when GP is co-administered with other active agents in the patient with the mean extrathoracic airway geometry (bottom row)



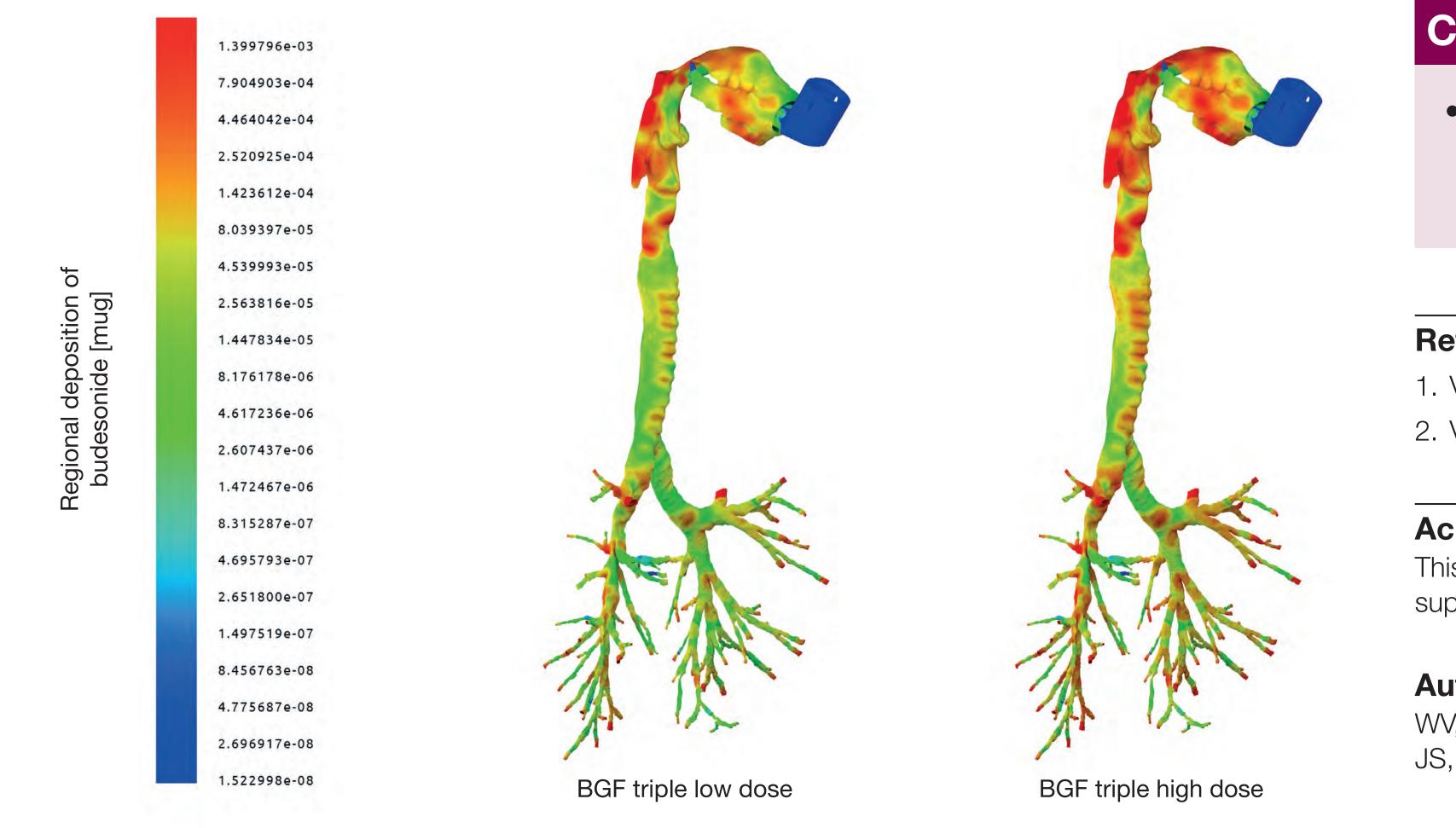
BGF. budesonide/glycopyrrolate/formoterol fumarate; COPD, chronic obstructive pulmonary disease; GFF, glycopyrrolate/formoterol fumarate; GP, glycopyrrolate; UA, upper airway.

Figure 3. Influence of inhalation flow rate on the regional deposition of FF for one patient with mild COPD (top row); and the consistency when FF is co-administered with other active agents at a fixed flow rate of 60 L/min for the same patient (bottom row)



BGF, budesonide/glycopyrrolate/formoterol fumarate; COPD, chronic obstructive pulmonary disease; FF, formoterol fumarate; GFF, glycopyrrolate/formoterol fumarate.

#### Figure 4. Influence of BGF MDI dose on the regional deposition of budesonide for one patient with very severe COPD



BGF, budesonide/glycopyrrolate/formoterol; COPD, chronic obstructive pulmonary disease.

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Table 1. Total lung deposition of FF, GP, and budesonide as % of delivered dose for the different combinations and as a function of the inhalation flow rate

	Flow rate [L/min]				
	15	30	60	90	120
otal lung deposition of FF, % delivered dose					
- mono	53±18	43±19	34±19	30±18	27±17
FF dual	55±19	45±20	36±20	32±19	29±18
GF triple low dose	54±19	45±20	36±19	31±19	28±18
GF triple high dose	53±19	43±20	34±19	30±18	27±17
otal lung deposition of GP, % of delivered dose					
P mono	54±18	44±20	35±19	31±19	28±18
FF dual	55±18	45±20	37±19	32±19	29±18
GF triple low dose	54±18	44±19	36±19	31±19	28±18
GF triple high dose	53±19	43±20	35±19	30±18	27±17
otal lung deposition of budesonide, % of delivered dose					
GF triple low dose	53±18	44±19	35±19	30±18	27±18
GF triple high dose	52±18	42±19	33±19	28±18	25±17

BGF, budesonide/glycopyrrolate/formoterol fumarate; FF, formoterol fumarate; GP, glycopyrrolate; GFF, glycopyrrolate/formoterol fumarate.

### Conclusions

• This computer simulation (*in-silico*) study supports the assertion that the Co-Suspension™ Technology MDI platform can deliver the aerosol consistently throughout the airways, regardless of the number of active agents included in the formulation.

#### References

1. Vos et al. Int J Chron Obstruc Pulmon Dis 2016;11:263–271. 2. Vehring et al. Langmuir 2012;28:15015–15023.

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#### Author disclosures

WV, JDB, and WDB have no relevant conflicts to declare. JS, MS, and SD are employees of Pearl Therapeutics Inc., a member of the AstraZeneca Group.



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