

Transferrin-Decorated Protein-Lipid Hybrid Nanoparticle Efficiently Delivers Cisplatin and Docetaxel for Targeted Lung Cancer Treatment

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Purpose: Non-small cell lung cancer (NSCLC) therapy faces the barriers including drug resistance. A transferrin-functionalized protein-lipid hybrid nanoparticle (PLHN) was designed loading both cisplatin (CIS) and docetaxel (DTX) for the lung cancer treatment.

Methods: CIS and DTX were loaded into the hybrid nanoparticle and then decorated with transferrin (Tf). The Tf-functionalized protein-lipid hybrid nanoparticle (Tf-CIS/DTX-PLHN) was investigated by determining the release behavior, cytotoxicity in vitro, and anticancer efficiency in vivo.

Results: Tf-CIS/DTX-PLHN showed a nano-size of 189.5 ± 5.9 nm, and a surface tested to be -16.9 ± 2.1 mV. Tf-CIS/DTX-PLHN exhibited obviously better antitumor ability in vitro and in vivo compared with the non Tf contained CIS and DTX co-loaded lipid nanoparticles (CIS/DTX-LN), single drug loaded nanoparticles, and free drugs.

Conclusion: Since remarkable enhanced efficiency of Tf and synergistic effect of the drugs, it could inhibit the lung tumor growth and help with the lung cancer treatment.

Keywords: lung cancer, hybrid nanoparticles, nanostructured lipid nanoparticles, protein nanoparticles, transferrin

Introduction

Lung cancer causes the most amount of cancer death among people worldwide.¹ Non-small cell lung cancer (NSCLC) accounts for over 80% of lung cancer, and the majority of patients (about 80%) are diagnosed with advanced or metastatic NSCLC (stage IV disease) and are not suitable for surgery.^{2,3} Among various chemotherapies, platinum-based treatments were the gold standard for the first-line therapy of patients with stage IV disease.^{4,5} Phase 3 randomized trials have proven that many of the platinum-contained combinations (cisplatin and docetaxel, cisplatin and paclitaxel, cisplatin and gemcitabine, carboplatin and paclitaxel, etc) exhibit no remarkable difference in objective response rates, survival and toxicity.^{6,7} Based on phase 3 trials, nanoparticle albumin-bound paclitaxel (Abraxane[®]) with less neurotoxicity and improved response rate has been approved by the US FDA for patients with advanced NSCLC.⁸ Therefore, the combined application of nanotechnology and two or more therapeutic agents has been the research hotspot recently.

Nano-sized drug delivery systems (Nano-DDS) have been explored for cancer therapy because of its advantages: lower toxicity, high efficacy from their capacity

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to accumulate at tumor zone, sustained release and extended bioavailability.⁹ Recently, continuous efforts have been devoted to exploit functional lipid-based nanoparticles to deliver two or more anti-tumor compounds, that include liposomes, solid lipid nanoparticles, and nanostructured lipid carriers.^{10–12} Despite the success of their co-loading hydrophilic and hydrophobic drugs, all lipid-based nanoparticles suffer from some disadvantages, such as lower drug loading, instability in serum, increased reticuloendothelial system (RES) clearance, decreased blood circulation times and efficacy.^{13,14} Therefore, protein-lipid hybrid nanoparticles (PLHN), a new generation of lipid-based nanoparticles have arisen to bring fruitful outcomes, reducing RES clearance, enhancing cellular uptake, and facilitating conjugation of drug or targeting ligand.^{15–18} In our study, we designed a multifunctional PLHN, consist of protein decorated nanostructured lipid carriers to deliver both cisplatin (CIS) and docetaxel (DTX).

Transferrin (Tf) is a polypeptide glycoprotein.¹⁹ Due to overexpression of transferrin receptor (TfR) in various malignant tumor cells such as lung cancer, brain cancer, breast cancer and colorectal cancer, it has been used as a tumor targeting motif in various delivery systems. So Tf was used as part of the lung cancer targeted delivery systems in some studies.^{20–22} In the present study, a multifunctional PLHN, modified by Tf and carried CIS and DTX (Tf-CIS/DTX-PLHN) was developed and evaluated.

Materials and Methods

Materials

Soya lecithin (SL, injectable) was provided by Lipoid GmbH (Ludwigshafen, Germany). Compritol[®] 888 ATO (ATO) was a gift from Gattefossé (Saint-Priest, Lyon, France). DSPE-PEG₂₀₀₀-COOH was produced by Seebio Biotech (Shanghai) Co., Ltd. (Shanghai, China). Transferrin, 1-ethyl-3-(3-dimethylaminopropyl) carbodiimide (EDC), N-Hydroxysuccinimide (NHS), and 3-(4,5-dimethyl-2-thiazolyl)-2,5-diphenyl-2-H-tetrazolium bromide (MTT) were bought from Sigma Aldrich (St. Louis, MO). The CIS resistant NSCLC cell line (A549/CIS cells), another NSCLC cell line (H1975 cells), and human normal lung epithelial cells (BEAS-2B cells) were obtained from American Type Culture Collection (ATCC, Manassas, VA, USA) and cultured in RPMI Medium 1640 supplemented with 10% (v/v) FBS

and 1% (v/v) penicillin–streptomycin at 37°C in an atmosphere of 5% CO₂.

Preparation of CIS and DTX Contained Lipid Nanoparticles

CIS and DTX contained lipid nanoparticles (CIS/DTX-LN) was prepared by the lipid emulsify and solvent injection method.²³ CIS (30 mg), DTX (50 mg), 100 mg of SL and 100 mg of ATO were mixed and warmed to 70–75°C (1), 100 mg of DSPE-PEG₂₀₀₀-COOH and 1% of polysorbate 80 (v/v) were dissolved in 50 mL of distilled water and heated to 70–75°C (2). (1) was injected to (2) rapidly under stirring (400 rpm, 30 min) to get CIS/DTX-LN. CIS/DTX-LN was washed and filtered by microporous membrane (0.45 µm pore size), then stored at 4°C.

CIS or DTX loaded lipid nanoparticles (CIS-LN or DTX-LN) were prepared using CIS (100 mg) or DTX (100 mg), respectively. Blank lipid nanoparticles (Blank LN) was prepared using no drug.

Preparation of Tf-CIS/DTX-PLHN

The preparation of Tf modified nanoparticles was conducted by conjugating the amido group of Tf with the DSPE-PEG₂₀₀₀-COOH of lipid nanoparticles.²⁴ Briefly, CIS/DTX-LN suspension (200 mg of CIS/DTX-LN) was incubated with EDC (50 mg) and NHS (30 mg) for 10 min, then Tf (100 mg) were added and stirred (4°C, 12 h) to form an amide linkage between Tf and DSPE-PEG₂₀₀₀-COOH. The density of Tf on the particles was measured using a BCA assay kit by recording the absorbance at 595 nm and determining the protein concentration by comparison to a standard curve.

Characterization of Tf-CIS/DTX-PLHN

The size and size distribution of particles, as well as zeta potential were tested by a Zetasizer (Malvern Instruments Ltd., Malvern, UK).²⁵ The morphology of Tf-CIS/DTX-PLHN and CIS/DTX-LN was observed under a TEM (JEOL, Tokyo, Japan). Encapsulation efficiency (EE) and drug loading (DL): The concentration of CIS was measured using ICP-MS.²⁶ High performance liquid chromatography (HPLC) method was used to determine the amount of DTX using a UV detector at 230 nm.²⁷ The stability of nanoparticles was evaluated cell culture medium (as stated in Materials section) and 50% FBS at 37 °C.

In vitro Drug Release

The drug release patterns of nanoparticles were analyzed using dialysis method.²⁸ Drugs loaded nanoparticles (3 mL) were sealed in dialysis bags (MWCO 8–14 kDa) and incubated in PBS (100 mL, pH 7.4) containing 0.1% (w/v) Tween 80 at 37°C. At different time points, 300 µL of release medium was replaced by 300 µL of fresh PBS. The CIS and DTX content were determined by the method described in the above section.

Cytotoxicity Assay

MTT assay was applied to evaluate the cell viability of drugs loaded nanoparticles and free drugs.²⁹ 96-well plates were used to culture A549/CIS, H1975 or BEAS-2B cells at a density of 1×10^4 cells per well. DMEM medium (100 µL) was added to the wells, incubating for 24 h. 200 µL of fresh medium was utilized to replace the culture medium containing Tf-CIS/DTX-PLHN, CIS/DTX-LN, CIS-LN, DTX-LN, blank LN, free CIS/DTX, free CIS, and free DTX. MTT assay was carried out after incubating the cells for another 24 h. The cell viability was calculated compared with the untreated cells at the absorbance at 490 nm.

Synergistic Effect

Combination index (CI) was calculated to evaluate the synergistic effects of drugs loaded in CIS/DTX-LN system when administrated to A549/CIS cells.³⁰ CI when the drug concentration causing 50% inhibition (CI_{50}) was achieved by the equation: $CI_{50} = (D)_{CIS}/(D_{50})_{CIS} + (D)_{DTX}/(D_{50})_{DTX}$. $(D)_{CIS}$ and $(D)_{DTX}$ means CIS and DTX in combination exhibited 50% of cytotoxicity; $(D_{50})_{CIS}$ and $(D_{50})_{DTX}$ means one drug (CIS or DTX) exhibited 50% of cytotoxicity, respectively. CI_{50} smaller and larger than show synergism and antagonism, respectively.

Cellular Uptake

Cellular uptake of were analyzed using coumarin-6 (C6) loaded nanoparticles, which were prepared by adding C6 (20 mg) along with drugs to get mixture (1) in the “Preparation of CIS and DTX contained lipid nanoparticles” section.³⁰ C6 loaded nanoparticles were added to A549/CIS cells that were seeded at 24-well black plates and incubated for 4 h. Then, the cells were washed three times with D-Hank’s solution, collected and centrifuged and the cell uptake efficiency was quantified using a BD FACSCalibur flow cytometer.

Apoptosis Assay

The levels of apoptosis induced by Tf-CIS/DTX-PLHN, CIS/DTX-LN, CIS-LN, DTX-LN and free CIS/DTX were determined by Annexin V-FITC binding assay was performed using the Annexin V-FITC detection kit I according to the manufacturer’s instructions.^{31,32} The cells were cultured and treated with Tf-CIS/DTX-PLHN, CIS/DTX-LN or free CIS/DTX or 48 h, the cells were trypsinized and collected by centrifugation at 1500 rpm for 5 min. The cell pellet was resuspended with 100 µM binding buffer and incubated with 5 µL of FITC-conjugated Annexin V and 5 µL of propidium iodide (PI) for 15 min at room temperature in the dark. The samples were immediately analyzed by a flow cytometer (FACSCalibur, BD Biosciences, San Diego, CA).

Xenograft Tumor Model and Biodistribution

All animal experiments were approved by the Institutional Animal Care and Use Committee of the Second Affiliated Hospital of Qingdao University and operated following the Guide of the National Institutes of Health for the care and use of experimental animals. Tumor-bearing BALB/C nude mice (5 weeks old, weighing 18–20 g) were established by subcutaneous injecting A549/CIS cells (3×10^6) into the right flanks of the mice and waited for the tumor grew to around 100 mm³.³³ The mice were then injected with Tf-CIS/DTX-PLHN, CIS/DTX-LN, and free CIS/DTX via tail vein (10 mice each group). At 2, 24 and 96 h, tumor, heart, kidney, lung, liver, and spleen samples were excised and homogenized in lysis buffer, mixed with methanol, and then centrifuged for 30 min. The CIS and DTX content were determined the same as “Characterization of nanoparticles” part.

In vivo Anti-Cancer Efficacy

Tumor-bearing BALB/C mice were administered with physiological saline, Tf-CIS/DTX-PLHN, CIS/DTX-LN, CIS-LN, DTX-LN, blank LN, free CIS/DTX, free CIS, and free DTX via tail vein injection every 2 days for 16 consecutive days (10 mice each group).³⁴ Mice were killed on day 18, the sizes of the tumor were measured using calipers before every injection. Tumor volumes (V) were achieved by the equation: $V = \frac{\text{the longest axis} \times \text{the perpendicular shorter tumor axis}^2}{2} \times 0.5$ and tumor growth curves were presented after treatment. The tumor images (before and after treatment) and changes of body weight of mice were also recorded.

TUNEL Assay of Tumor Tissue

Tumor tissue was embedded in paraffin, sliced to 5 micron and detected by TUNEL assay using in situ cell death assay kit to evaluate the apoptotic cells in tumor tissue.³⁵ Apoptotic cells were photographed under fluorescence microscope and TUNEL-positive cells were measured with Image J Software.

Statistical Analysis

Student's *t*-test and one-way analysis of variance (ANOVA) was used for the statistical analysis. The parametric variables were expressed as means $\pm$ standard deviation (SD). Differences were considered statistically significant at $P < 0.05$ (*).

Results

Characterization of Nanoparticles

The characterization of nanoparticles in terms of particle size, polydispersity index (PDI), zeta potential, EE, DL and Tf coupling density were summarized in Table 1. Differences were found between Tf-CIS/DTX-PLHN and CIS/DTX-LN in terms of size and surface charge. In particular, the size of Tf-CIS/DTX-PLHN was 189.5 ± 5.9 nm while CIS/DTX-LN exhibit a diameter of 156.3 ± 4.9 nm. The zeta potential of Tf-CIS/DTX-PLHN and CIS/DTX-LN was -16.9 ± 2.1 and -25.3 ± 2.6 mV, respectively. The PDIs of the nanoparticles were below 0.2. The Tf density was found to be $56.3 \pm 3.2\%$. As can be seen from the TEM images, CIS/DTX-LN appeared as uniform nanosized particles, while Tf-CIS/DTX-PLHN showed double layered particles (Figure 1). The size of the nanoparticles tested showed no significant changes during 72 h of study in both cell culture medium and 50% FBS, illustrated the fine stability of the systems.

In vitro Drug Release

Figure 2 shows the accumulated drug release behaviors of nanoparticles wherein. The result revealed no burst release for all formulations, suggested the stability of these particles at the physiological condition. All the drugs contained nanoparticles showed sustained release patterns. Notably, Tf-CIS/DTX-PLHN showed a slower drugs release kinetics compared with CIS/DTX-LN.

Cytotoxicity and Synergistic Effect

Blank nanoparticles showed no obvious cytotoxicity, which may prove its biocompatibility (Figure 3A). At the equivalent drug concentrations, drugs loaded nanoparticles showed higher cell inhibition efficiency than the drugs without nanoparticle loading ($P < 0.05$). The combination treatment using CIS and DTX together (CIS/DTX-LN) synergistically decreases the viability of cells than the single drug loaded DTX-LN and CIS-LN. When evaluated on H1975 cells, Tf-CIS/DTX-PLHN exhibited higher cell inhibition ability compared with CIS/DTX-LN (Figure 3B). However, drugs loaded LN showed no obvious influence on human normal lung epithelial cells (BEAS-2B cells) compared with free drugs (Figure 3C). Whether the dual drugs showed synergistic effect when loaded in one system was further evaluated by CI_{50} values (Figure 3D). The effect of drug combinations of different ratios (from 1:5 to 5:1, CIS: DTX) in CIS/DTX-LN was compared with the effect of treatment with either agent alone. Result showed that the drug ratio of 3:5 had the best synergistic effect with CI values less than 1 at the Fa values from 0.2 to 0.8, so this ratio was used for the nanoparticles preparation.

Cellular Uptake

The cellular uptake efficiency of Tf-CIS/DTX-PLHN showed higher uptake efficiency compared to CIS/DTX-LN and other nanoparticles that not contained Tf (Figure 4, $P < 0.05$), which may be explained by the

Table 1 Characterization of Nanoparticles

Formulations	Tf-CIS/DTX-PLHN	CIS/DTX-LN	CIS-LN	DTX-LN	Blank LN
Particle size (nm)	189.5 ± 5.9	156.3 ± 4.9	161.2 ± 4.5	154.9 ± 4.1	152.3 ± 5.1
PDI	0.18 ± 0.02	0.16 ± 0.02	0.15 ± 0.02	0.14 ± 0.01	0.15 ± 0.02
Zeta potential (mV)	-16.9 ± 2.1	-25.3 ± 2.6	-26.1 ± 1.9	-24.3 ± 2.1	-15.2 ± 2.4
CIS EE (%)	88.5 ± 3.2	85.9 ± 3.5	86.4 ± 3.1	N/A	N/A
DTX EE (%)	86.3 ± 2.9	89.5 ± 3.3	N/A	87.9 ± 3.1	N/A
CIS DL (%)	8.4 ± 0.6	10.3 ± 0.8	N/A	11.1 ± 0.9	N/A
DTX DL (%)	7.9 ± 0.7	9.8 ± 0.9	N/A	9.5 ± 0.8	N/A
Tf density (%)	56.3 ± 3.2	N/A	N/A	N/A	N/A

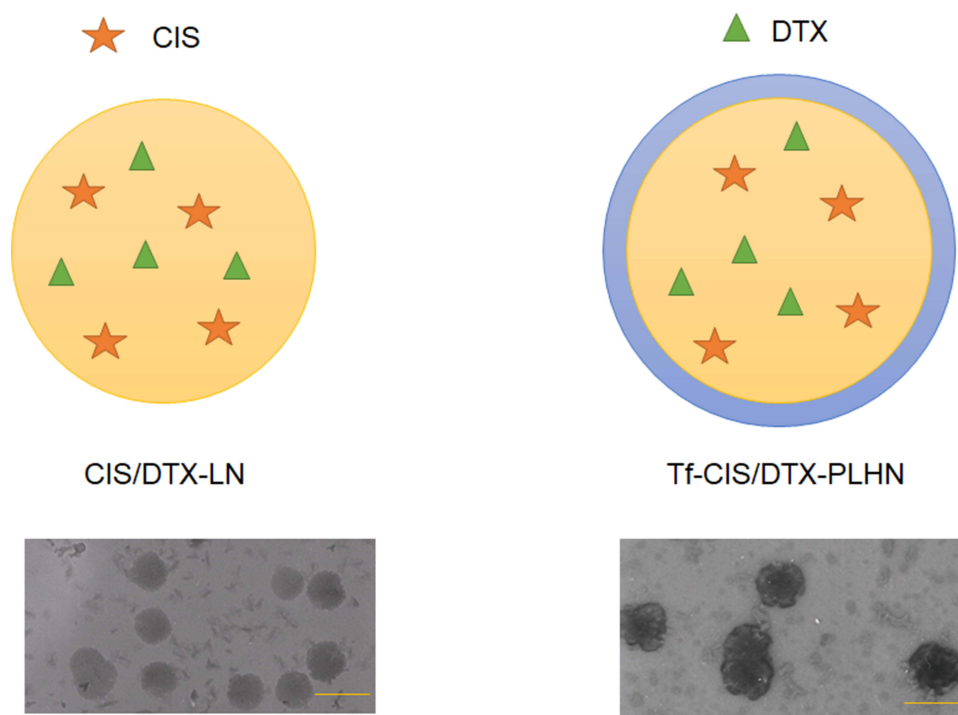


Figure 1 The schematic illustration and TEM images of Tf-CIS/DTX-PLHN and CIS/DTX-LN (scale bar showed 200 nm).

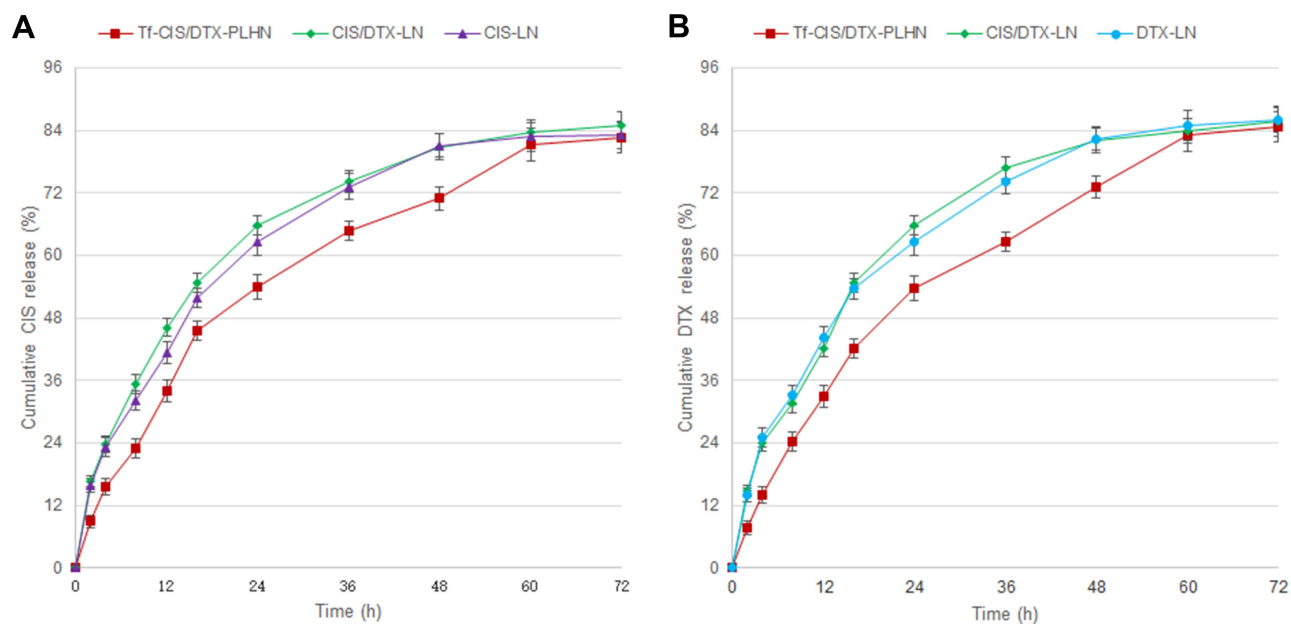


Figure 2 In vitro CIS (A) and DTX (B) release profiles of Tf-CIS/DTX-PLHN, CIS/DTX-LN, CIS-LN, and DTX-LN. Data presented as mean $\pm$ SD.

targeting effect of transferrin to the cancer cells that could improve the uptake of the nanoparticles.

Apoptosis Assay

The level of apoptosis induced by CIS and DTX combined CIS/DTX-LN was higher than CIS-LN and DTX-LN

(Figure 5), indicating that the combination treatment induced cell death more effectively than the individual drug treatments. Tf-CIS/DTX-PLHN exhibited a considerable increase in the apoptotic cell population than that of CIS/DTX-LN, which may be concluded as the targeted efficiency of Tf.

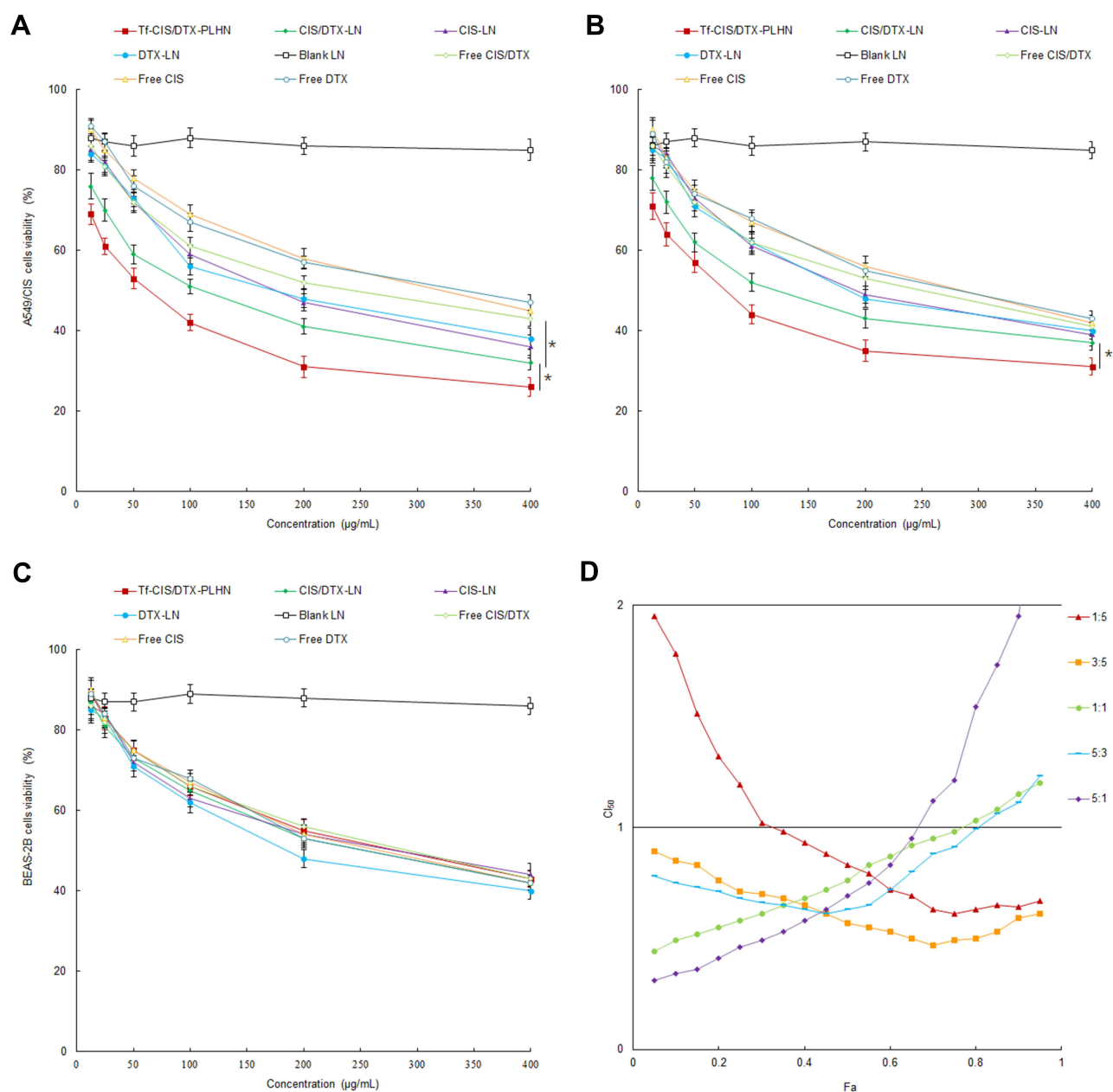


Figure 3 Cytotoxicity of Tf-CIS/DTX-PLHN, CIS/DTX-LN, CIS-LN, DTX-LN, blank LN, free CIS/DTX, free CIS, and free DTX evaluated by MTT assay on A549/CIS (A), H1975 (B) or BEAS-2B (C) cells and combination index (CI) measured on A549/CIS cells to study the synergy effects in the drugs combination system (D). Data presented as mean $\pm$ SD. * $P < 0.05$.

In vivo Biodistribution

Tf-CIS/DTX-PLHN showed higher drug distribution in tumor than non Tf involved CIS/DTX-LN and free drugs at 24 h and 96 h post injection ($P < 0.05$) (Figure 6). At both 2 and 24 h, Tf-CIS/DTX-PLHN and CIS/DTX-LN distributed less in the heart and kidney ($P < 0.05$). At 96 h, drug distribution in tumor decreased obviously, which may suggest another injection of formulations.

In vivo Antitumor Efficacy and Systemic Toxicity

Figure 7A reveals that Tf-CIS/DTX-PLHN had the most significant in vivo tumor inhibition ability, which was better than that of other drugs loaded nanoparticles, free drugs and saline control groups ($P < 0.05$). CIS/DTX-LN presented better tumor suppression ability compared to CIS-LN and DTX-LN ($P < 0.05$). More remarkable

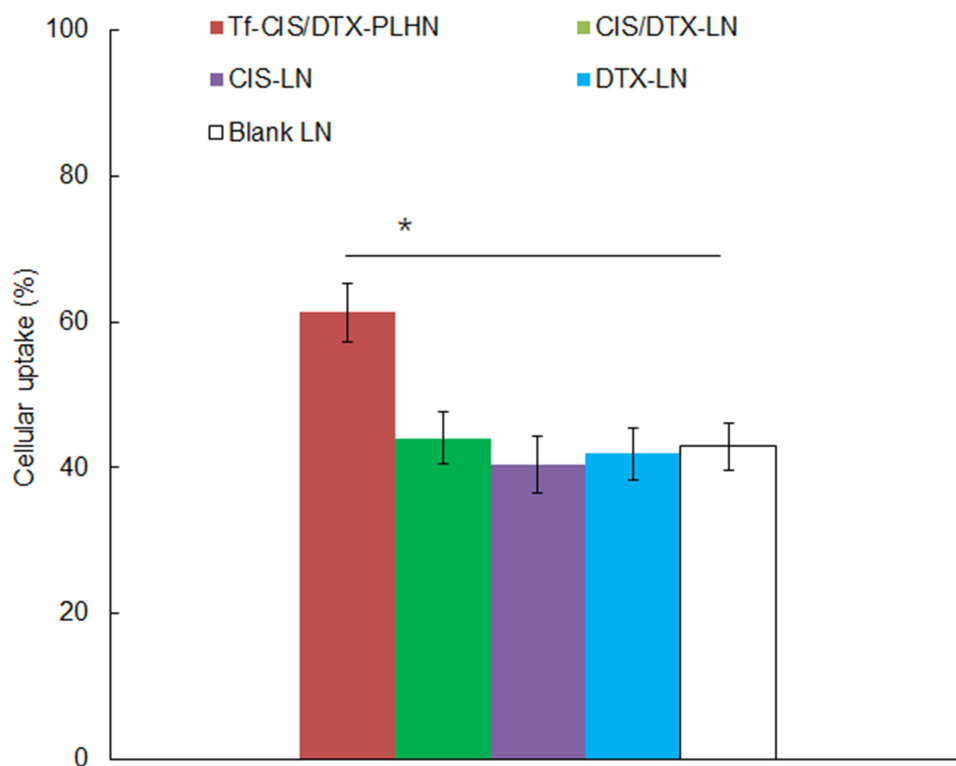


Figure 4 Cellular uptake efficiency quantified by flow cytometry on A549/CIS cells. Data presented as mean $\pm$ SD. * $P < 0.05$.

antitumor efficacy was observed by drugs loaded nanoparticles groups compared with free drugs groups ($P < 0.05$). The body weight changes were summarized in [Figure 7B](#). Obvious body weight lost were found on free drugs administrated groups, in the contrast, nanoparticles groups exhibited no remarkable body weight change. Tumor images (before and after treatment) were applied in [Supplementary Figure 1](#). The effect of nanoparticles on apoptosis of cells in transplanted tumors was examined by the TUNEL assay. TUNEL-positive cells ratio of Tf-CIS/DTX-PLHN group was higher than other groups ([Figure 8](#), $P < 0.05$), which suggested the better efficiency of Tf modified Tf-CIS/DTX-PLHN on the proliferation and apoptosis of cells in vivo. This result was in accordance with the in vitro experiments.

Discussion

Transferrin-decorated protein-lipid hybrid nanoparticle was prepared in this study. CIS/DTX-LN was firstly prepared by the lipid emulsify and solvent injection method. Then Tf was conjugated to nanoparticles surface to obtain Tf-CIS/DTX-PLHN. Tf-CIS/DTX-PLHN exhibited larger particle size (189.5 ± 5.9 nm) compared with CIS/DTX-LN (156.3 ± 4.9 nm), which is also reported by others that

the adding of Tf slightly enlarged the particle sizes.³⁶ Increased surface charge of Tf functionalized nanoparticles may attribute to the positive charged functional groups of Tf. PDIs less than 0.2 indicated the uniform distribution of the nanoparticles.

Scientific rigorous in vitro experiments could help with the evaluating of the in vivo characters of the system. The in vitro release study is a kind of test in the environment of simulated temperature, medium condition and motion state.³⁷ The drug release results showed that the drugs were sustained released from the nanoparticles. Slower drugs release kinetics of Tf-CIS/DTX-PLHN compared with CIS/DTX-LN may attribute to the Tf layer that hindered the drug release.

Drug delivery systems that induce significant cytotoxic effects will provide a valuable pathway for the delivery of antitumor drugs.³⁸ At the equivalent drug concentrations, drugs loaded nanoparticles showed higher cell inhibition efficiency compared with the free drugs ($P < 0.05$). This is because free drugs diffuse through cell membranes but nanoparticles are internalized through the endocytic pathway, resulting in larger amount uptake and higher cytotoxicity than free drugs.³⁹ It is unlikely that such a high concentration of the free drug would persist for such a long

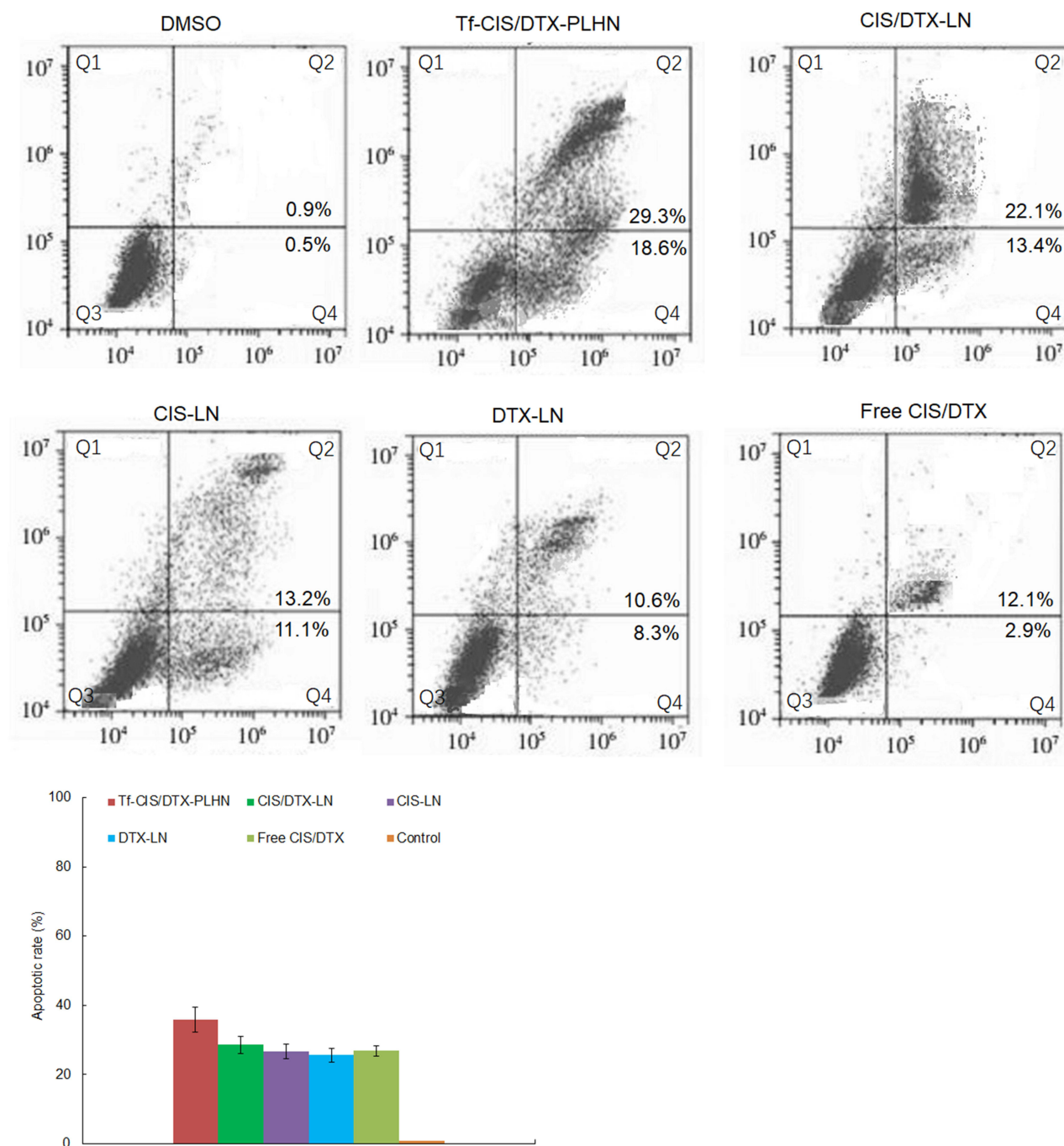


Figure 5 Apoptosis rates analyzed by flow cytometer. Data presented as mean $\pm$ SD.

duration of treatment for in vivo applications; however, drug-loaded nanoparticles may contribute to their passive accumulation in tumor tissue by enhancing the permeability and retention (EPR) effect. Combination index (CI) was raised by Chou and Talalay to evaluate the synergistic effects among drugs.⁴⁰ When the CIS: DTX ratio was 3:5, the most prominent synergistic effect was achieved. Higher cellular uptake efficiency and increased apoptotic cell population of

Tf-CIS/DTX-PLHN than that of CIS/DTX-LN could prove the targeting effect of transferrin to the receptor contained cancer cells. Cell apoptosis results illustrated that CIS and DTX combined CIS/DTX-LN induced cell death more effectively than the individual CIS-LN and DTX-LN.

In vivo tissue biodistribution of Tf-CIS/DTX-PLHN in tumor was higher than non Tf involved CIS/DTX-LN and free drugs at 24 h post injection, and less in the heart

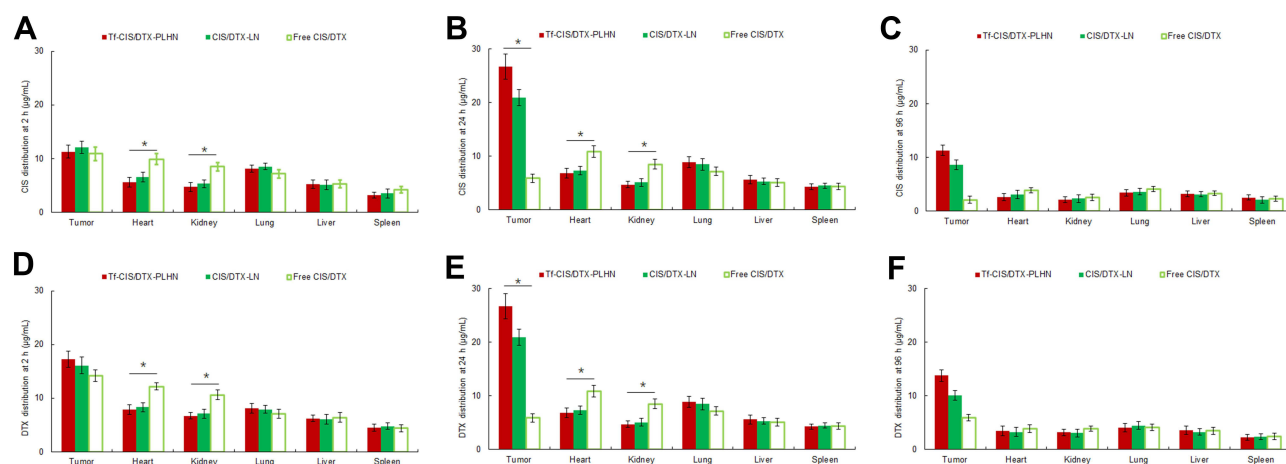


Figure 6 In vivo drugs tissue distribution of Tf-CIS/DTX-PLHN, CIS/DTX-LN, and free CIS/DTX: CIS distribution at 2 h (A), 24 h (B), and 96 h (C); DTX distribution at 2 h (D), 24 h (E), and 96 h (F). Data presented as mean $\pm$ SD. * $P < 0.05$.

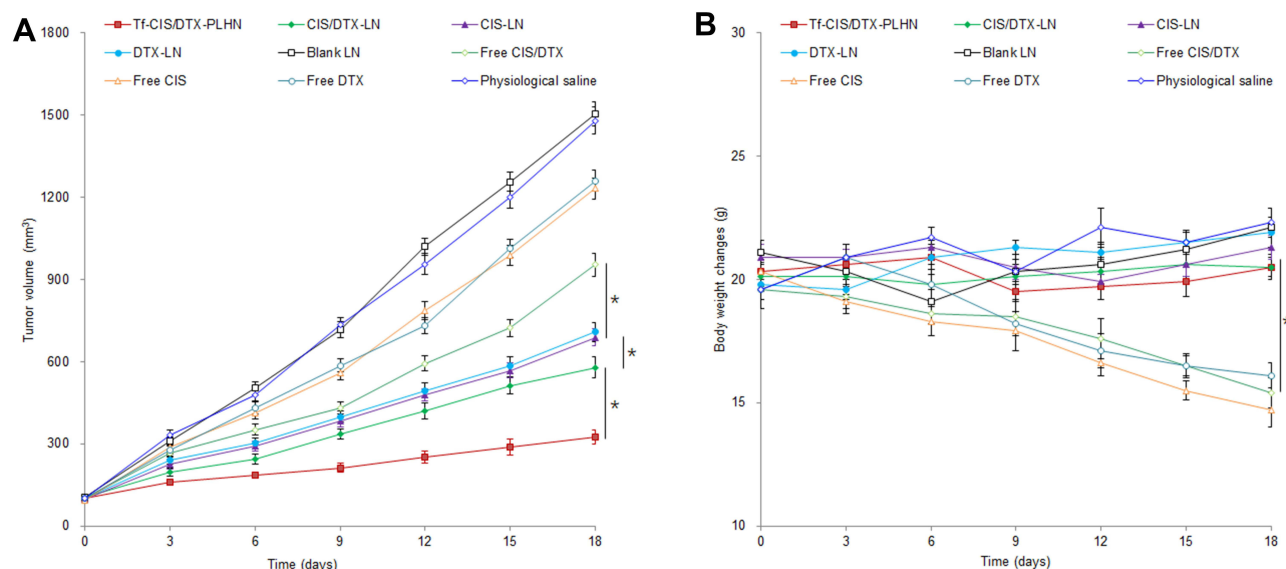


Figure 7 In vivo tumor inhibition effect evaluated by using mice bearing lung carcinoma model: Tumor volume (A); and body weight (B). Data presented as mean $\pm$ SD. * $P < 0.05$.

and kidney, these behaviors may reduce the toxicity of in vivo injection. These results were in line with the research carried by other researchers.^{41,42} They found that the preferential accumulation of nanoparticles in tumor due to the EPR effect.⁴¹ The existence of PEG chain on particle surface plays a stealth role on the system, which is responsible for the long circulating of LPNs. Also coating of Tf could increase the accumulation in the tumor.⁴² The application of this particle might be limited because the biodistribution may be different in a primary or lung metastasis model. We would like to evaluate the anticancer effect in an orthotopic tumor model in the future research.

In vivo anti-tumor nanoparticles have more prominent potential than free drugs, which may be due to enhanced nanoparticle accumulation in tumor sites and effective encapsulation of drugs against leakage in the bloodstream that can promote intracellular release of drugs and contribute to enhanced anti-cancer efficacy.⁴³ CIS/DTX-LN presented more profound anti-tumor capacity than CIS-LN and DTX-LN, which is in line with the synergistic effect evaluation results that the drugs combination could achieve additive effect than the drugs used alone. Tf contained Tf-CIS/DTX-PLHN showed higher tumor suppression ability than that of CIS/DTX-LN, which could prove that the protein-lipid hybrid nanoparticle had a remarkable

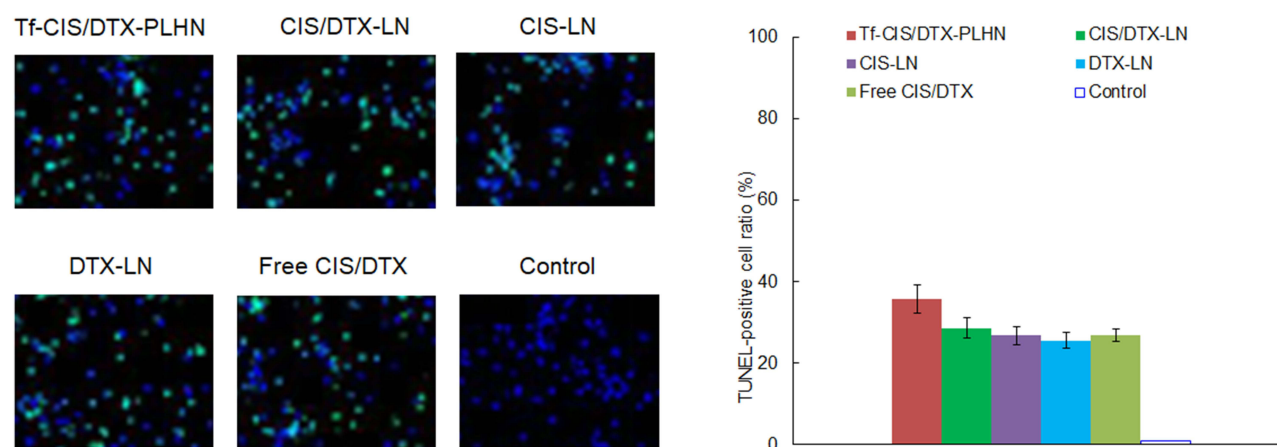


Figure 8 TUNEL assay of tumor tissue: TUNEL-positive cells were measured with Image J Software. Data presented as mean $\pm$ SD. *P < 0.05.

benefit. No significant change of body weight further proved the low systemic toxicity of the nanoparticles, which could be safe when administrated in vivo.

Conclusion

In this study, Tf-functionalized protein-lipid hybrid nanoparticle (Tf-CIS/DTX-PLHN) was developed with a nano-size of 189.5 ± 5.9 nm, and a surface tested to be -16.9 ± 2.1 mV. Tf-CIS/DTX-PLHN exhibited a remarkable tumor cell inhibition ability, outstanding tumor suppression capacity compared with other systems. The results indicated that Tf-CIS/DTX-PLHN it could inhibit the lung tumor growth and help with the lung cancer treatment. No significant change of body weight further proved the low systemic toxicity of the nanoparticles, which could be safe when administrated in vivo.

Disclosure

The authors do not have any conflict of interest for this work to declare.

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