

Injectable Nanosponge-Loaded Pluronic F127 Hydrogel for Pore-Forming Toxin Neutralization

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Purpose: Pore-forming toxins (PFTs) perform important functions during bacterial infections. Among various virulence-targeting therapies, nanosponges (NSs) have excellent neutralization effects on multiple PFTs. To enhance treatment efficacy, NSs tend to be incorporated into other biomaterials, such as hydrogels.

Methods: In the present work, red blood cell (RBC) vesicles were harvested to wrap polymer nanoparticles, leading to the formation of NSs, and the optimal Pluronic F127 hydrogel concentration was determined for gelation. Then, a novel detoxification system was constructed by incorporating NSs into an optimized Pluronic F127 hydrogel (NS-pGel). Next, the system was characterized by rheological and sustained release behavior as well as micromorphology. Then, the in vitro neutralization effect of NS-pGel on various PFTs was examined by a hemolysis protocol. Finally, therapeutic and prophylactic detoxification efficiency was evaluated in a mouse subcutaneous infection model in vivo.

Results: A thermosensitive, injectable detoxification system was successfully constructed by loading NSs into a 30% Pluronic F127 hydrogel. Characterization results demonstrated that the NS-pGel hybrid system sustained an ideal fluidity and viscosity at lower temperatures but exhibited a quick sol-gel transition capacity near body temperature. In addition, this hybrid system had a sustained release behavior accompanied by good biocompatibility and biodegradability. Finally, the NS-pGel system showed neutralization effects similar to those of NSs both in vitro and in vivo, indicating a good preservation of NS functionality.

Conclusion: In conclusion, we constructed a novel temperature-sensitive detoxification system with good biocompatibility and biodegradability, which may be applied to the clinical treatment of PFT-induced local lesions and infections.

Keywords: nanosponges, pore-forming toxins, detoxification, thermosensitive hydrogel, Pluronic F127

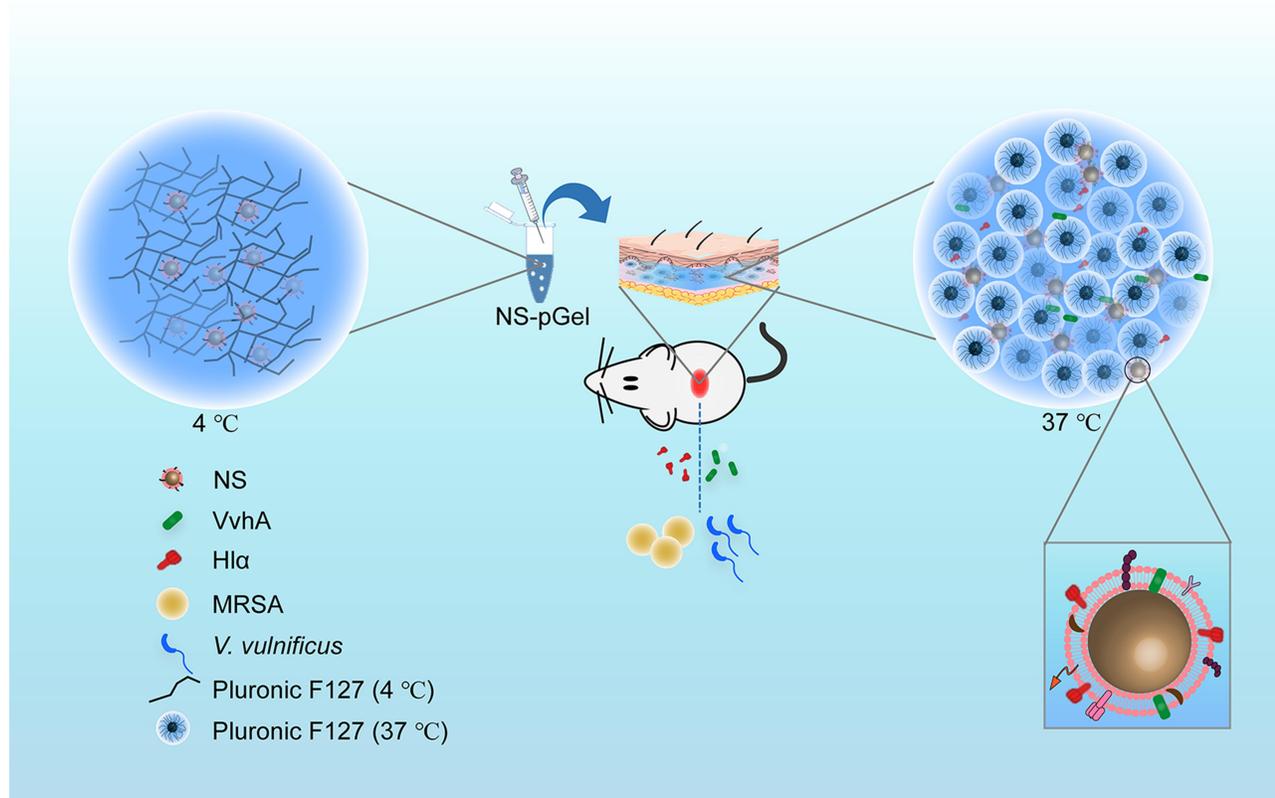
Introduction

Antibiotic-resistant bacterial infections have become a global health crisis due to high morbidity and mortality.^{1,2} In 2019, the World Health Organization (WHO) estimated that globally, at least 700,000 patients die from drug-resistant infections annually. Without any action, the figure might soar to 10 million by 2050.³ Thus, there is an urgent need to actively develop new strategies against antibiotic-resistant bacteria.

Virulence factor-targeting therapies have become alternative treatments for antibiotic-resistant infections,⁴⁻⁶ among which biomimetic red blood cell (RBC) membrane-derived “nanosponges (NSs)” provide a novel and promising opportunity.⁷⁻¹⁰ In 2013, Hu and colleagues¹⁰ reported for the first time that NSs

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Graphical Abstract



could effectively transfer pore-forming toxins (PFTs) away from their natural cellular targets and save normal cells. PFTs serve as important and abundant virulence factors from both gram-positive (G^+) and gram-negative (G^-) bacterial pathogens and are well known for their ability to perforate target cells such as RBCs;^{5,11} thus, the NS platform with broad-spectrum absorption of PFTs is logically an effective detoxification therapy. Currently, the NS platform has been reported to inhibit the cytotoxicity of multiple PFTs, such as α -hemolysin (Hla), streptolysin O (SLO) and listeriolysin O (LLO).¹² However, certain drawbacks of NSs limit their further development. For example, for systemic detoxification, NSs may accumulate in the liver and cause secondary injury, especially for patients with liver failure.^{13,14} Further, for local application, NSs show an apparent diffusivity, thus leading to a reduction in drug levels and detoxification efficiency.¹⁵

To improve the stability and therapeutic index of NSs, incorporating NSs into hydrogels has recently gained

much attention.¹⁶ Hydrogels are hydrophilic 3D cross-linked networks that can preserve the structural integrity and functions of incorporated materials.¹⁷ As advanced drug delivery reservoirs, they also have the characteristics of reduced irritation, decreased adverse effects and sustained release.^{18–22} Wang et al¹⁵ demonstrated the potential of nanosponge-loaded hydrogel (NS-gel) as a novel and effective detoxification strategy to treat localized methicillin-resistant *Staphylococcus aureus* (MRSA) infections. However, the preparation of this acrylamide-based, chemical cross-linking hydrogel requires toxic reagents, such as N,N,N',N'-Tetramethylethylenediamine (TEMED) and ammonium persulfate (APS), which compromise biocompatibility and limit its translational applications. In addition, the gel is not suitable for preservation because its gelation time is short, and it can only be injected when freshly prepared.

“Smart” thermosensitive hydrogels are materials displaying a sol-gel phase transition in response to

temperature, which are superior for NS loading.^{23,24} Thermosensitive hydrogels maintain good liquidity and low viscosity at lower temperatures and transform into an immobile gel state immediately at body temperature. The easy injection and sustained drug release make thermosensitive hydrogels potentially useful for local drug loading and delivery.^{25–27} Recently, a variety of thermosensitive hydrogels have been developed, such as Pluronic F127, poly(N-isopropylacrylamide) and methylcellulose.^{28,29} Pluronic F127, also named Poloxamer 407, is an FDA-approved novel temperature-sensitive hydrogel material that has been used for drug delivery and wound healing.^{30–32} Compared to chemical cross-linking hydrogels, the pharmaceutical formulation of the Pluronic F127 hydrogel is simple and completely relies on physical methods without requiring chemical cross-linking agents, thus improving safety and reducing production costs.³³ In addition, the premixed solution can sustain an aqueous state upon injection at a lower temperature with no need for fresh preparation, so it is easier to preserve. Once stimulated by near-physiological temperatures, the amphiphilic triblock copolymers in water can spontaneously form a network by physical cross-linking. These multiple advantages make the Pluronic F127 hydrogel suitable for NS incorporation.

In this study, we first incorporated NSs into FDA-approved biocompatible and thermally responsive Pluronic F127 hydrogels (denoted as NS-pGel). We then selected two representative PFTs, *V. vulnificus* hemolysin (VvhA) from G^- *V. vulnificus* and Hla from G^+ *Staphylococcus aureus* for an examination of the ability for NS-pGel to absorb and neutralize these toxins. We quantified the toxin binding capacity of NS-pGel by an in vitro hemolytic assay and further confirmed the retention of NSs and the local detoxification efficiency of the NS-pGel in vivo. Overall, this study provides an injectable and novel NS-pGel as a broad-spectrum detoxification platform against different types of PFTs.

Materials and Methods

Cells, Animals and Reagents

Male ICR mice (18–20 g) were purchased from Shanghai Lab Animal Research Center. All animal experiments were performed according to the Guide for the Care and Use of Laboratory Animals and approved by Committee on Ethics of Medicine, Navy Medical University, PLA (81974496).

Carboxyl-terminated 50:50 poly (DL-lactide-co-glycolide) (PLGA, Mw 48,000, 0.67 dL/g) was purchased from Lactel Co (USA). 1,1'-Diocetadecyl-3,3',3'-tetramethylindodicarbocyanine, 4-chlorobenzenesulfonate salt (DiD) dye was purchased from Invitrogen (USA). Pluronic F127 was obtained from Beyotime Co (Shanghai, China). Hla from *Staphylococcus aureus* was purchased from Sigma-Aldrich (USA). Recombinant VvhA (rVvhA) was expressed in our lab. Cell Counting Kit-8 (CCK-8) was purchased from Dojindo Molecular Technologies, Inc (Japan). All other reagents were of analytical grade, commercially available and used as received.

Preparation and Characterization of NSs

NSs were prepared by coating RBC vesicles onto PLGA nanoparticles (NPs) with reference to previous studies.^{7,34} Briefly, there were three steps involved in NS construction: (i) Whole blood withdrawn from male ICR mice (20–25 g) was centrifuged at 1000 rpm for 15 min at 4 °C and then washed 3 times until the plasma and buffy coat were completely removed. Next, the resulting RBCs were lysed by a hemolytic protocol followed by high-speed centrifugation at 12,000 rpm for 20 min. The sediment was washed repeatedly to harvest a white pellet. The resulting RBC ghosts were then serially extruded through 400 and 200 nm polycarbonate porous membranes to obtain RBC vesicles. (ii) PLGA NPs were prepared by the nanoprecipitation method.⁷ PLGA polymers (5 mg/mL) dissolved in acetone (1 mL) were poured into distilled water (3 mL) and stirred until the acetone was completely evaporated. A similar method was used to prepare DiD-labelled PLGA NPs, except that 0.1% (w/w) DiD fluorescence dye was added to the PLGA acetone solution. (iii) The RBC vesicles were mixed with PLGA NPs at a protein-to-polymer weight ratio of 1:1, and then NSs were constructed by the coextrusion method.⁷

The hydrodynamic size and zeta potential of prepared RBC vesicles, PLGA NPs and NSs were measured by dynamic light scattering (DLS) at room temperature. The structure of the NSs was examined using transmission electron microscopy (TEM) (JEOL JEM-2010, Japan) by negative staining with 1% uranyl acetate. The cell membrane proteins retained on the NSs were characterized by sodium dodecyl sulfate-polyacrylamide gel electrophoresis (SDS-PAGE), and RBC ghosts and vesicles were used as controls. First, the protein concentration of all samples was determined by the bicinchoninic acid (BCA) protein assay

kit (Thermo Scientific, Pierce, Shanghai). Then, all the samples were heated to 100 °C for 15 min, and 20 µL of samples with equal protein amounts were added and run on a 6% stacking gel at 80 V for 25 min and separation gel at 120 V for another 1 h using a BIO-RAD® Electrophoresis System. Finally, the resulting gel was stained with Coomassie Blue (Sangon, China) for imaging.

Preparation of Pluronic F127 Hydrogel, NS-pGel and the Sol-Gel Transition

For bare hydrogel preparation, Pluronic F127 solutions of different concentrations (10%, 15%, 20%, 25%, 30%) were prepared by dissolving Pluronic F127 powder into cold distilled water. The mixture was then magnetically stirred at 4 °C for complete dissolution, and the bubbles were removed overnight. For NS-pGel preparation, NSs at a final concentration of 1 mg/mL were added to 30% Pluronic F127 precursor solution at 4 °C followed by moderate stirring and bubble removal. At 37 °C, the NS-pGel composite was formed in situ due to the temperature-induced sol-gel transition. Samples of Pluronic F127 hydrogel and NS-pGel were examined and photographed after gel formation.

Characterization of the Pluronic F127 Hydrogel and NS-pGel

The NS-pGel and Pluronic F127 hydrogel were characterized with dynamic rheological measurements on a rheometer (Anton Paar, Germany). The storage modulus (G') and loss modulus (G'') were measured as a function of temperature sweeping from 10 °C to 65 °C at an angular frequency of 1 rad/s to determine the phase transition temperature of the NS-pGel. Then, G' and G'' were measured as a function of frequency ranging from 0.1 Hz to 10 Hz at 25 °C to examine the gel formation. In addition, the viscosity of the NS-pGel was tested to determine the injectability at lower temperatures.

To test the release rate of NSs in the hydrogel, 0.5 mL of DiD-labelled NS-pGel was immersed in 5 mL of PBS buffer and incubated at 37 °C. At a predetermined time (0, 1, 2, 4, 8, 12, 24, 48 h), all the buffer was withdrawn and replaced with 5 mL of fresh buffer solution. Then, the fluorescence intensity of DiD was measured by a Varioskan Flash Multimode Reader (Thermo Scientific Company, USA), and the ratio of released NSs was calculated.

To examine the morphology, NS-pGel was lyophilized and coated with a thin layer of gold before observation under a scanning electron microscope (SEM).

For biocompatibility examination, L929 cells grown in 96-well plates were treated with leaching liquor (25%, 50% and 100%) from NS-pGel for 24 and 48 h, and cell viability was determined by a CCK-8 kit.

PFT Neutralization Study of NS-pGel in vitro

Initially, the activities of rVvhA and H1 α were determined by a hemolysis protocol in a 2% murine RBC suspension. Then, the in vitro toxin neutralization ability of NSs was examined by mixing NSs of various concentrations (0.016~2 mg/mL, a final volume of 0.5 mL) with rVvhA (15 µg/mL) or H1 α (1 µg/mL). Next, an equal volume of the 2% RBC suspension was added and incubated at 37 °C for 30 min. Subsequently, the samples were centrifuged at 1000 rpm for 5 min, and the released hemoglobin was quantified at 540 nm to determine the degree of hemolysis using a Varioskan Flash Multimode Reader. Furthermore, a similar hemolysis protocol was used to evaluate the toxin neutralization ability of NS-pGel (containing 1 mg/mL of NSs). Briefly, rVvhA (15 µg/mL) or H1 α (1 µg/mL) was added to NS-pGel, gel, NS and PBS, respectively (a final volume of 0.5 mL). After incubation for gelation at 37 °C, an equal volume of the 2% RBC suspension was added and incubated at 37 °C for 30 min. Each sample was then carefully centrifuged for hemolysis examination.

Live Imaging for NS Retention in vivo

Prior to the study, the back of the male ICR mice (18–20 g) was carefully shaved. Then, 50 µL of DiD-labelled NS-pGel was injected subcutaneously into the left flank of the mice. As a control, 50 µL of DiD-labelled NSs was injected subcutaneously into the right flank of the same mice. At the designated time points (0, 12, 24, 48 h), the mice were anesthetized with sevoflurane and imaged with a QuickView3000 (Bio-Real) system. Fluorescence intensities were then quantified.

PFT Neutralization Study of NS-pGel in vivo

The experiment was performed as previously described.¹⁵ First, 30 µg of rVvhA or 2 µg of H1 α solution (50 µL) was injected into the flanks of male ICR mice (18–20 g). Then, 100 µL samples of NS, NS-pGel or saline were injected into the same wound site. After treatment for 72 h, the lesions were imaged and measured, and then the mice were anesthetized for harvesting skin and muscle samples.

The samples were immobilized and stained with hematoxylin and eosin (H&E staining) for pathological examination under a microscope.

We further explored the prophylactic detoxification efficiency of NS-pGel in vivo. NS or NS-pGel samples were injected into the flank subcutaneously 24 h prior to 30 μ g of rVvhA or 2 μ g of H1 α exposure. The remaining steps were repeated as described above.

Statistical Analysis

All the measurements were performed in triplicate. The results were expressed as the mean \pm standard error (SE). Data were analyzed by one-way ANOVA. Differences were considered statistically significant at $P < 0.05$ (*).

Results

Characterization of NS

To characterize the hydrodynamic size and zeta potential, the PLGA NPs and RBC-derived NSs were measured by DLS. The results revealed an increase (~ 15 nm) in the average hydrodynamic diameters of NPs, which corresponded to RBC membrane wrapping on NPs (Figure 1A). Meanwhile, the zeta potential of the PLGA NPs increased from -37.5 ± 2.3 to -24.1 ± 1.9 mV, which was close to the surface potential of the RBC membrane (Figure 1B). Together, these results demonstrated fusion between NP cores and RBC membranes.

To characterize the nanostructures, the resulting NS sample was dried and examined by TEM. The ultrastructure exhibited a typical core-shell structure with a polymer core coated by a membrane shell, revealing the formation of NSs (Figure 1C).

To further characterize the protein content retained on the NSs, the resulting NS sample was analyzed by SDS-PAGE. The gel image indicated that most of the membrane proteins were retained on the NSs after preparation, which was consistent with those of RBC ghosts and vesicles (Figure 1D).

Overall, the results of physiological characterization and protein retention examination collectively suggested the successful construction of NSs.

Optimization of Hydrogel and NS-pGel Preparation

To achieve optimal gel formation, Pluronic F127 solutions of various concentrations were screened. As shown in Figure 2A, each group of Pluronic F127 solutions

maintained good fluidity at 4 $^{\circ}$ C, and as the concentration of Pluronic F127 solution increased, the gelation capacity was enhanced at 37 $^{\circ}$ C. The Pluronic F127 solution with a concentration below 25% was not capable of forming hydrogels at body temperature, while the 30% gel solution showed an optimal gel state. Thus, we chose 30% gel solution to load NS (1 mg/mL). Notably, NS-pGel showed a muddy appearance because of the addition of NS suspension, but the fluidity at 4 $^{\circ}$ C and gelation at 37 $^{\circ}$ C were not influenced after mixing (Figure 2B). The above results indicate that the NS-pGel hybrid detoxification system is convenient for storage thanks to everlasting fluidity at lower temperatures, and it permits quick gelation at body temperature.

Characterization of the Pluronic F127 Hydrogel and NS-pGel

The NS-pGel was characterized with dynamic rheological measurements of the storage modulus (G') and the loss modulus (G'') as a function of temperature. As shown in Figure 3A, G' and G'' dramatically increased at approximately 25 $^{\circ}$ C, ie, gelation could quickly occur at this temperature. In addition, G' exceeded G'' over the entire frequency range at 37 $^{\circ}$ C, indicating typical viscoelastic behavior and the stability of the formed hydrogel system (Figure 3B). Viscosity examination results revealed that the viscosity of NS-pGel fluctuated approximately 0 Pa·s below 15 $^{\circ}$ C but increased with heating and reached a plateau at approximately 30 $^{\circ}$ C, indicating that the NS-pGel is easily injected by syringe at lower temperatures and can sustain a high-viscosity gel state for NS retention at body temperature (Figure 3C).

Next, we used fluorescence detection to verify the NS release properties of NS-pGel. As shown in Figure 3D, the release of NSs and the degradation of the hydrogel were time-dependent. Specifically, the release rate of NSs at 1 h was approximately 10%, which gradually increased to 90% at 48 h. Similarly, gel degradation was lower than 5% at 1 h and gradually increased to 70% at 48 h. These results revealed that the NS-pGel hybrid system showed a sustained release behavior accompanied by slow degradation of the Pluronic F127 hydrogel.

To further characterize the nanostructure, freeze-dried NS-pGel and blank hydrogel samples were observed by SEM. The images showed typical porous sponge-like structures of gel materials, further revealing the formation of a hybrid hydrogel system. Notably, at a higher

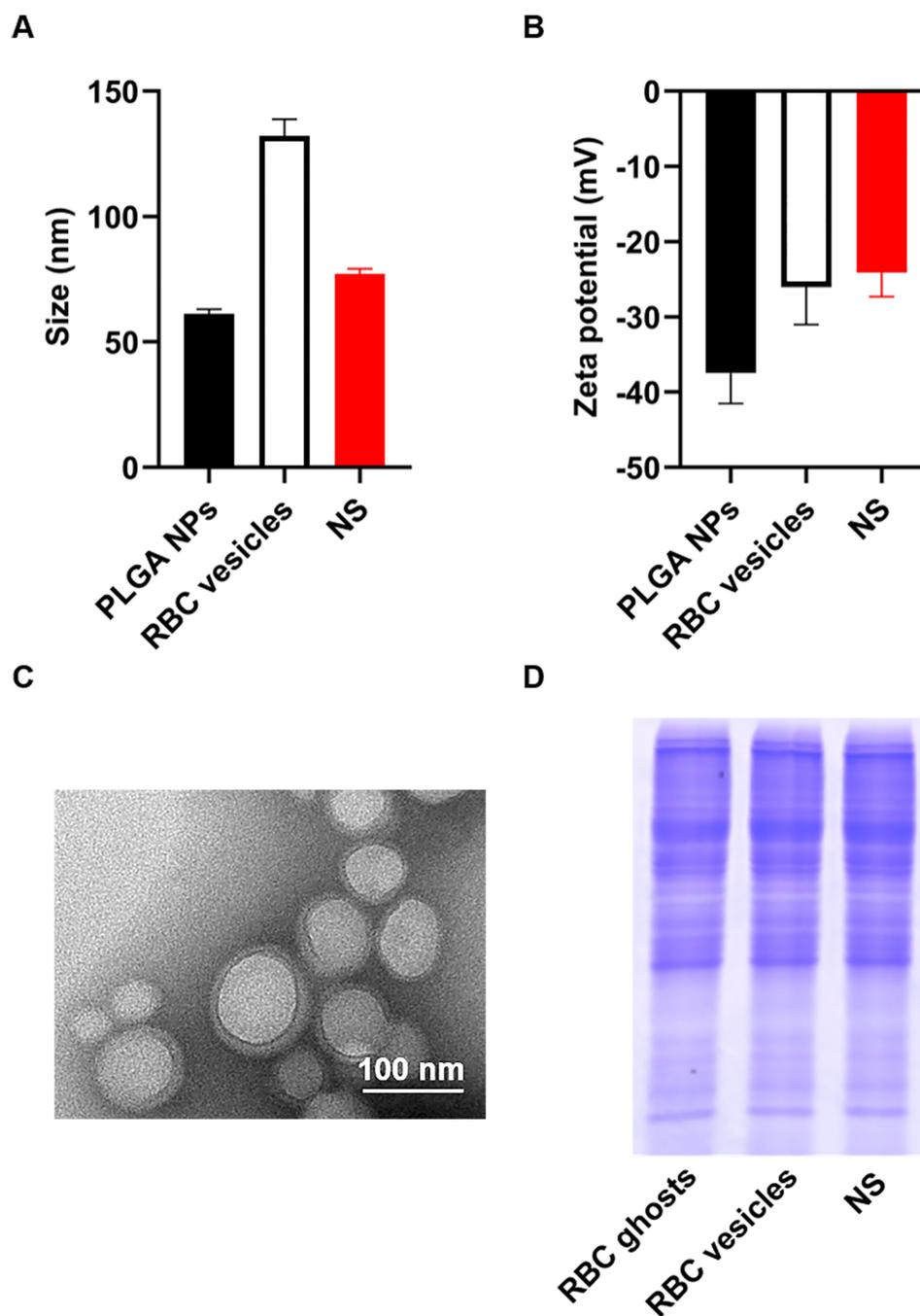


Figure 1 Characterization of NSs. (A–B) Hydrodynamic size and zeta potential of PLGA NPs, RBC vesicles and NSs detected by DLS. (C) A representative TEM image demonstrates the core-shell structure of NSs with RBC membrane shells wrapped onto core NPs. (D) Proteins on RBC ghosts, RBC vesicles, and NSs resolved on a polyacrylamide gel were examined by SDS-PAGE.

magnification, nanosponges loaded in hydrogel were also observed (Figure 3E).

To test the safety of NS-pGel, L929 cells were treated with various doses of NS-pGel for 24 and 48 h. As shown in Figure 3F, the cell survival rates of all the samples were over 80%, revealing the nonpoisonous and compatible characteristics of NS-pGel.

PFT Neutralization of NSs and NS-pGel in vitro

Hemolysis experiments were performed to determine the optimal dose of PFTs for subsequent study. As shown in Figure 4A and D, the ratio of hemolysis enhanced in an “S” shape with increasing concentrations of PFT toxins (rVvhA and H1 α), which reached peaks at doses of 15 μ g/mL (rVvhA) and 1

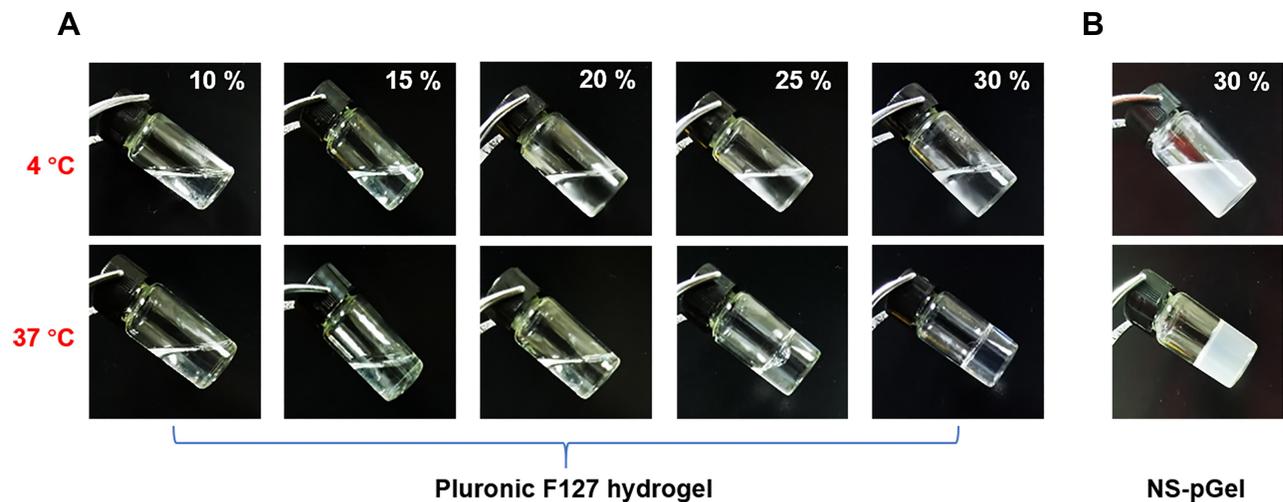


Figure 2 Optimization of Pluronic F127 hydrogel and NS-pGel. **(A)** Gel resolution of different concentrations (10%, 15%, 20%, 25% and 30%) at 4 °C (upper image) and gel formation of Pluronic F127 at 37 °C (lower image). **(B)** NS-pGel resolution at 4 °C (upper image) and gel formation at 37 °C (lower image).

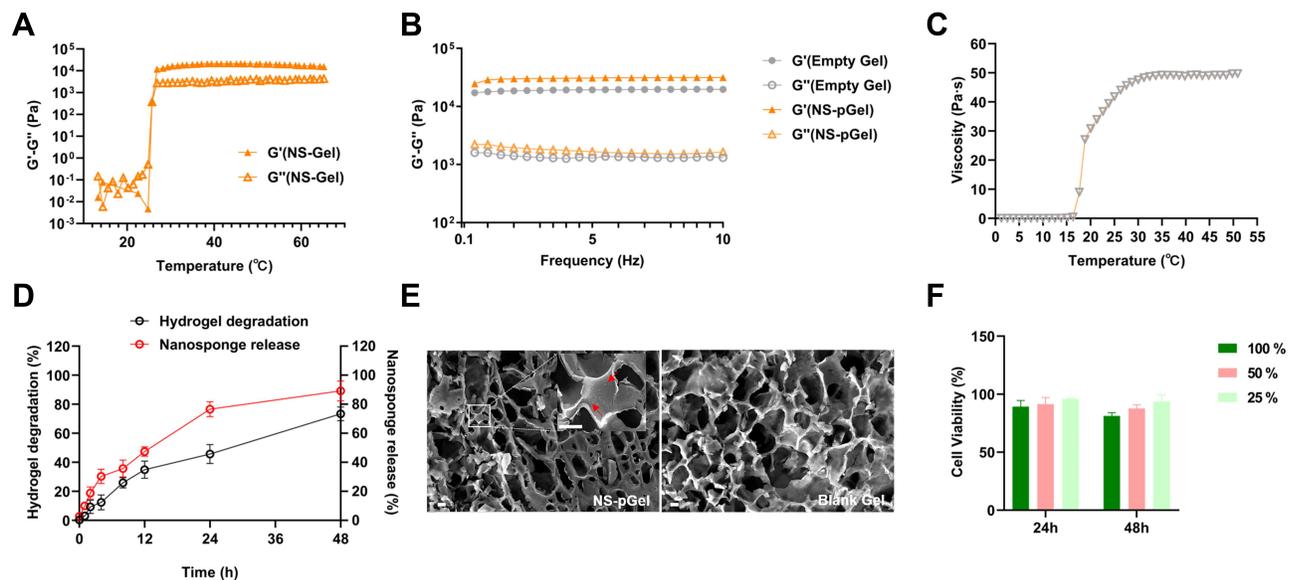


Figure 3 Characterization of the Pluronic F127 hydrogel and NS-pGel. **(A)** Rheological characterization of the Pluronic F127 hydrogel (30%) loaded with 1 mg/mL NS. The storage modulus G' and loss modulus G'' were plotted logarithmically against temperature (10–70 °C). **(B)** Rheological characterization of NS-pGel as a function of frequency (0.1–10 Hz) at 37 °C. **(C)** Viscosity of NS-pGel determined against temperatures between 0 and 55 °C. **(D)** Degradation and NS release kinetics of NS-pGel detected over a period of 120 h. **(E)** Representative SEM images of NS-pGel (left image, red arrows refer to NS) and blank hydrogel (right image) (Scale bar: 2 μ m). **(F)** Cytotoxic effect of NS-pGel on L929 cells. Cells were pretreated with leaching liquor (100%, 50% and 25%) for 24 h or 48 h. Cell viability was determined by a CCK-8 kit. (n=3).

μ g/mL (H1 α), respectively. When treated with NSs, the detoxification capacity was enhanced with the increase in these antidotes. The 0.5 mg/mL concentration of NSs almost completely inhibited hemolysis induced by 15 μ g/mL of rVvhA (Figure 4B). Similarly, the hemolysis induced by 1 μ g/mL of H1 α was almost completely reversed by the 1 mg/mL of NS sample (Figure 4E). Next, the hemolysis-inhibition effect of NS-pGel (loaded with 1 mg/mL of NS) was examined. Our results showed that when compared to NSs, NS-pGel inhibited

hemolysis caused by PFTs (rVvhA, H1 α) to a similar extent, but the hydrogel failed to show a protective effect alone (Figure 4C and F). These results indicate that gel formulation preserves the critical biological functionality of NSs.

The Pluronic F127 Hydrogel Retained NSs Locally in vivo

We then evaluated the retention of NSs by the Pluronic F127 hydrogel in vivo. Within 48 h, the fluorescence

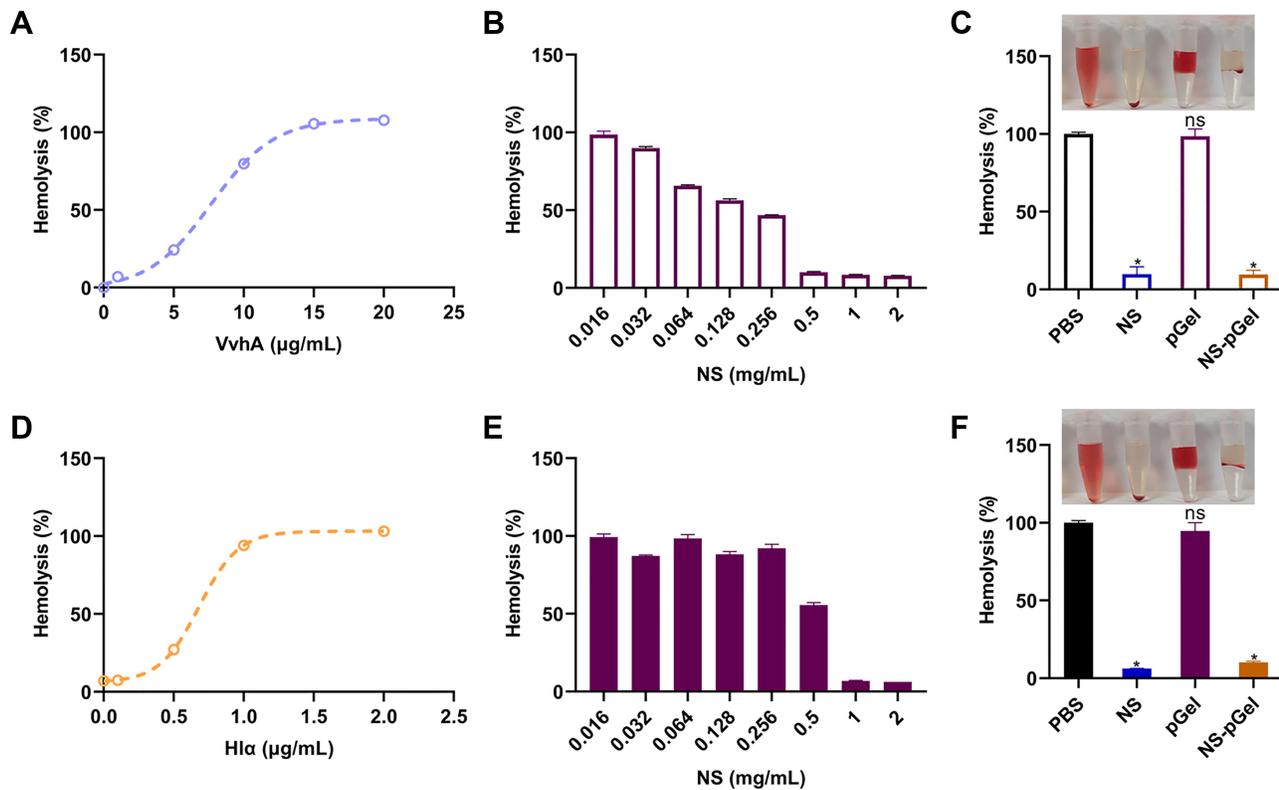


Figure 4 PFT neutralization of NSs and NS-pGel in vitro. **(A)** Activity of rVvhA toxin for hemolysis in vitro. **(B)** Hemolytic activity of rVvhA (15 μg/mL) mixed with NSs at different concentrations. **(C)** Centrifuged RBCs and hemolysis quantification after incubation with rVvhA (15 μg/mL) mixed with PBS, NSs (1 mg/mL), empty gel and NS-pGel (containing 1 mg/mL NS). **(D)** Hemolytic activity of Hla toxin in vitro. **(E)** Hemolysis caused by Hla (1 μg/mL) mixed with NSs at different concentrations. **(F)** Centrifuged RBCs and hemolysis quantification after incubation with Hla mixed with PBS, NSs, empty gel and NS-pGel. (Data represent the mean ± SE, n = 3, *P < 0.05, ns: no significance).

intensity of the NS group showed a more rapid decay than that of the NS-pGel group (Figure 5A). Quantification analysis revealed that over 90% of the NSs diffused over a period of 48 h, while only approximately 40% of the NSs were lost in the NS-pGel group (Figure 5B), indicating good NS retention in the hydrogel.

Inhibition Effects of NS-pGel on PFTs in vivo

The efficiency of NS-pGel in neutralizing PFTs in vivo was further examined by subcutaneous injection of various PFTs (rVvhA, Hla) in mice. After 72 h, mice exposed to rVvhA (30 μg) or Hla (2 μg) and treated with saline showed obvious

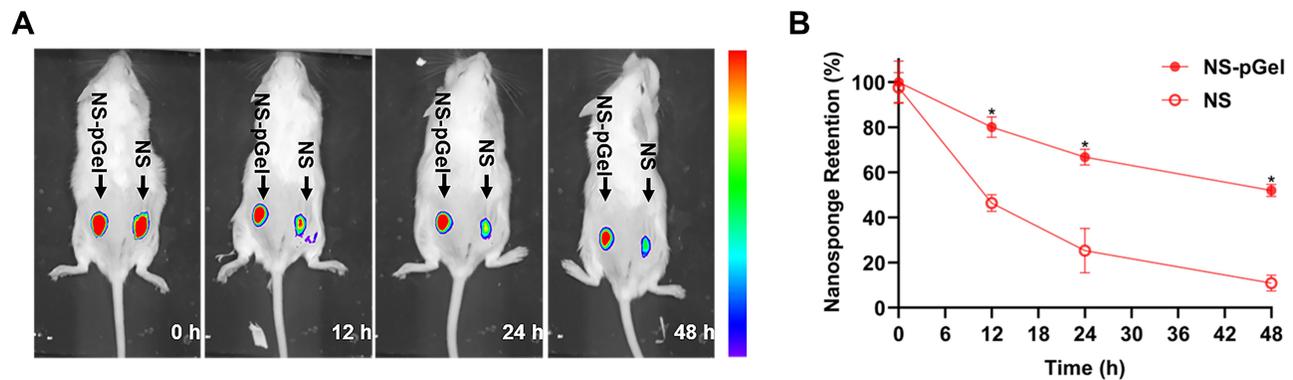


Figure 5 Local NS retention by Pluronic F127 hydrogel. DiD-labelled NSs were injected subcutaneously over the right flanks of mice. DiD-labelled NSs retained by hydrogel (NS-pGel) were injected into the left flanks of the same mice. **(A)** Fluorescence images were taken at certain time points to determine the NS retention in vivo. **(B)** Relevant quantification of the fluorescence intensity. (Data represent the mean ± SE, n = 3, *P < 0.05).

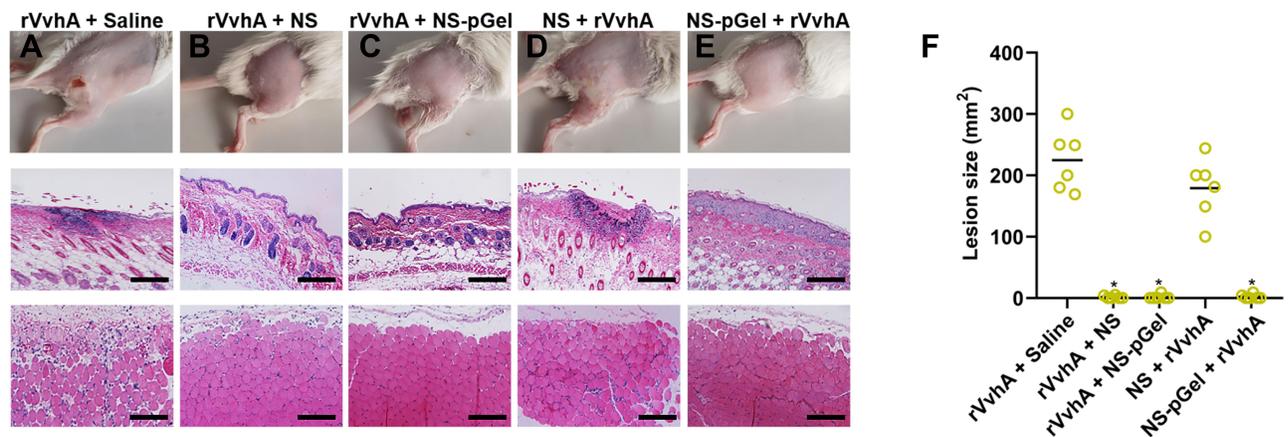


Figure 6 rVvhA neutralization efficiency of NS-pGel in vivo. (A–C) Mice were injected with rVvhA into the flank region immediately followed by saline, NSs or NS-pGel. The local lesions were photographed after 72 h, and then the skin and muscle were harvested for H&E staining and histological examination. (D–E) Mice were injected with saline, NSs or NS-pGel subcutaneously into the flanks 24 h before rVvhA exposure. Images of lesions and H&E-stained tissues were obtained after 72 h. (scale bar: 50 μ m). (F) Skin lesions of each group were measured after treatment. (Data represent the mean \pm SE, n = 6, *P < 0.05 versus group treated with saline).

skin lesions with reddish ecchymosis and inflammation. Histological changes also appeared in the skins and muscles, including apparent oedema, cell death, as well as neutrophil accumulation (Figures 6A, F and 7A, F). However, both the NS (2 mg) and NS-pGel (equal to 2 mg of NS) markedly diminished PFT-induced tissue damage and inflammatory reactions (Figures 6B, C, F and 7B, C, F). Furthermore, the mice pretreated with NS-pGel suffered milder local lesions than those pretreated with NS alone (Figures 6D–F and 7D–F). Therefore, it can be concluded that NS-pGel possesses both therapeutic and preventive effects.

Discussion

Recently, therapeutic biomimetic nanosponges have been increasingly combined with other biomaterials to form

stable structures to improve the therapeutic effects against infectious diseases. In this study, we successfully used RBC-derived NSs and Pluronic F127 hydrogel to construct a novel biocompatible and biodegradable detoxification system denoted “NS-pGel”, which is formed entirely based on physical cross-linking instead of chemical cross-linking. NS-pGel not only preserves the toxin neutralization capability of the incorporated NSs but also achieves a significantly prolonged retention of NSs in both biological buffers and mouse subcutaneous tissues. More importantly, this hybrid hydrogel system has typical temperature-sensitive characteristics with injectable ability at lower temperatures and quick gelation near body temperature and is thus suitable for local wounds with various shapes. Together, these multiple advantages make this

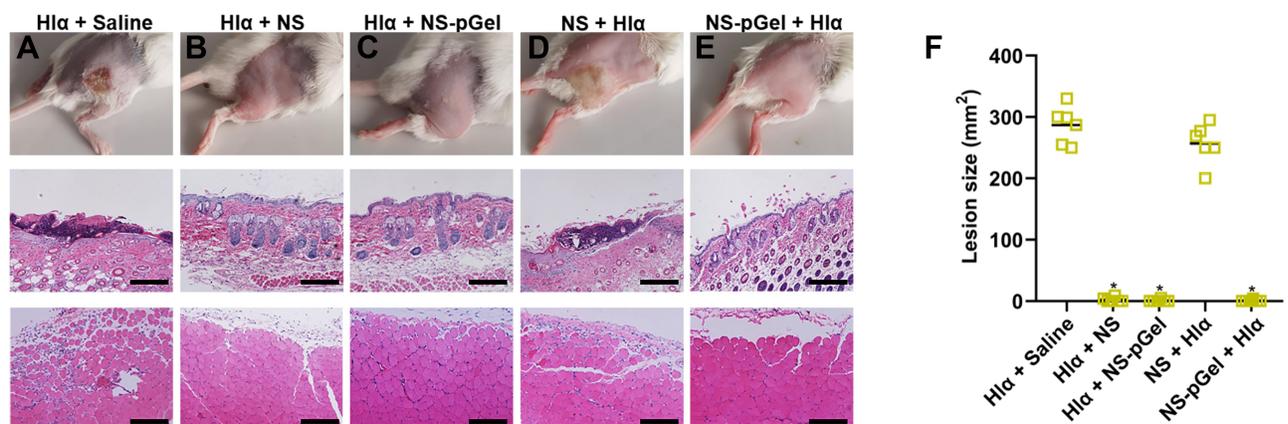


Figure 7 Hla neutralization efficiency of NS-pGel in vivo. (A–C) Mice were injected with Hla into the flank region immediately followed by saline, NSs or NS-pGel. The local lesions were photographed after 72 h, and then the skin and muscle were harvested for H&E staining and histological examination. (D–E) Mice were injected with saline, NSs or NS-pGel subcutaneously into the flanks 24 h before Hla exposure. Images of lesions and H&E-stained tissues were obtained after 72 h. (scale bar: 50 μ m). (F) Skin lesions of each group were measured after treatment. (Data represent the mean \pm SE, n = 6, *P < 0.05 versus group treated with saline).

“NS-pGel” a promising injectable drug reservoir for medical applications, including anti-virulence therapy against localized bacterial infection.

In this study, we employed a Pluronic F127 hydrogel to incorporate NSs for the construction of a nanosponge-hydrogel hybrid system for the first time. As previously mentioned, Pluronic F127 is an FDA-approved thermo-sensitive hydrogel that has been adopted for drug delivery and wound healing. Based on physical cross-linking, the preparation of Pluronic F127 hydrogel is apparently simple and occurs by resolving and stirring, thus providing the possibility for large-scale production and clinical transformation. In the present study, we chose a 30% Pluronic F127 hydrogel solution to construct NS-pGel because the resulting detoxification system had a good fluidity at 4 °C and a stable gel state at body temperature (Figure 2). In addition, viscosity examination also revealed that the viscosity of NS-pGel was significantly low at temperatures below 15 °C but dramatically increased near body temperature. Together, the temperature-sensitive properties of NS-pGel make it easily injectable by syringe, and long-term storage is possible instead of spontaneous gelation at lower temperatures. More importantly, compared to chemical cross-linking, the preparation of NS-pGel is physical, simple, and chemical-free, allowing NS-pGel to retain the functionalities of NSs without affecting the original functions.³⁵

For local administration and treatment, the prolonged retention of NSs by using a hydrogel is desirable. In this study, NS-pGel was formulated with fluorescence-labelled NSs, and the release of NSs was monitored by measuring the fluorescence intensity *in vitro*. NS-pGel released 10% of the total NS amount in 1 h, with the release lasting for nearly 48 h, indicating that the NS-pGel system can effectively immobilize and retain NSs within its network (Figure 3D). We then investigated the retention of NSs within the pGel *in vivo*. Whole-body imaging of the mice and quantification of the fluorescence intensity revealed the confinement and a negligible loss of NSs at sites injected with NS-pGel compared to those injected with free NS (Figure 5), demonstrating that the prolonged retention of NSs was achieved with the NS-pGel formulation. Simultaneously, we also found that the prepared NS-pGel possessed good biocompatibility and safety (Figure 3F), further demonstrating its significant potentials as a local treatment agent to be used on human bodies in the future.

Finally, the NS-pGel system showed a significant detoxification efficiency both *in vitro* and *in vivo*. Since

antibiotic-resistant G⁺/G⁻ bacterial infections pose a threat to humans, we chose two well-characterized PFTs, Hla from G⁺ *Staphylococcus aureus* and VvA from G⁻ *V. vulnificus*, to examine the detoxification ability of the NS-pGel system compared to free NSs. *In vitro* hemolysis examination revealed that NS-pGel samples showed a similar inhibition efficiency compared to that of free NSs (Figure 4C and F), suggesting that the NS-pGel formulation retains the full neutralization capability of its component NSs. Then, neutralization of PFTs by NS-pGel was further tested *in vivo*. Similar toxin neutralization effects were observed in the NS-pGel group compared to the NS group, further confirming that the neutralization function of NSs was well preserved within the NS-pGel formulation. Finally, to demonstrate the prophylactic detoxification potential of NS-pGel, we injected NS-pGel 24 h before toxin exposure. As a result, NS-pGel showed better preventive effects than NSs (Figures 6 and 7). We speculate that the main reason is the sustained release of NSs from the NS-pGel system, which causes retention of NSs in wounds at a high concentration. Overall, the Pluronic F127 hydrogel endows NSs with the possibility of therapeutic and prophylactic application.

Conclusion

In conclusion, the present study developed a novel detoxification system (denoted NS-pGel) with good injectability and temperature sensitivity. Biocompatible Pluronic F127 hydrogel was incorporated with NSs for the first time, and the hydrogel effectively retained NSs within its network without compromising their toxin neutralization capability. *Ex vivo*, NS-pGel exhibited an excellent efficacy on hemolysis inhibition caused by PFTs; in a mouse model of subcutaneous infection, NS-pGel also showed a significant alleviation of skin lesion development in both therapeutic and prophylactic settings. This work may lead to novel clinical treatments for PFT-induced local lesions and infections.

Abbreviations

NS, nanosponge; NS-pGel, nanosponge-loaded Pluronic F127 hydrogel; PFT, pore-forming toxin.

Author Contributions

All authors made substantial contributions to conception and design, acquisition of data, or analysis and interpretation of data; took part in drafting the article or revising it critically for

important intellectual content; agreed to submit to the current journal; gave final approval of the version to be published, and agreed to be accountable for all aspects of the work.

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Disclosure

The authors report no conflicts of interest in this work.

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