

Assessing Renal Microvascular Reactivity by Laser Speckle-Contrast Imaging in Angiotensin-II-Treated Mice

This article was published in the following Dove Press journal:
International Journal of Nephrology and Renovascular Disease

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Introduction: The kidney is one of the main organs affected by microvascular damage wrought by hypertension. We developed an approach to investigate renal microcirculatory disturbance in live mice by measuring post-occlusive reactive hyperemia (PORH), a reactivity test exploring endothelial and neuro-microvascular functioning. Laser speckle-contrast analysis (LASCA) assesses microvascular blood flow; it provides real-time images of spatial and temporal blood flow dynamics. We compared basal blood flow and PORH test between control and angiotensin-II-treated mice (Ang-II) to validate the model.

Objective: The study objective was to develop an approach to investigate renal microcirculation, and then to compare microvascular reactivity assessed on LASCA in control versus Ang-II mice.

Methods: Thirty 7-week-old wild-type C57BL/6J mice were allocated into two groups. One received angiotensin-II via osmotic minipumps (Ang-II; n=15); the other served as control (n=15). Basal blood flow was measured on LASCA. The PORH test was then performed in the two groups.

Results: Control mice had significantly lower basal renal microcirculatory flow, expressed in perfusion units (PU), than Ang-II-treated mice (1448 ± 96 vs 1703 ± 185 PU, respectively; $P < 0.05$). Peak flow was lower in controls than in Ang-II mice (1617 ± 104 vs 1724 ± 205 PU, respectively; $P=0.21$). Control mice had significantly higher kidney PORH than Ang-II mice (8 ± 3 vs $1 \pm 4\%$, respectively; $P < 0.05$).

Conclusion: We developed an innovative technique to study renal microcirculation in mice. Ang-II-treated mice showed significantly higher basal blood flow than controls, while PORH was significantly higher in controls than in Ang-II mice.

Keywords: microvascular reactivity, laser speckle-contrast analysis, hypertension, renal microcirculation

Introduction

Hypertension is a significant stimulus for arteriolar remodeling and microvascular rarefaction.¹ Under physiological conditions, the fraction of non-perfused vessels constitutes a useful reserve in various pathophysiological conditions.² There is a dissociation between microvascular damage in hypertension and hemodynamic parameters:³⁻⁵ experimental studies showed distinct trajectories for macro- and micro-circulatory damage. Various organs may sustain microvascular damage induced by hypertension.⁶ In humans, cutaneous circulation is easily accessible, and robust minimally invasive techniques are available to investigate skin microcirculation,⁷ and this has often been used as a surrogate to evaluate microvascular damage in human subjects.

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Specifically, previous studies examined post-occlusive reactive hyperemia (PORH) as a means of assessing microvascular reactivity,⁸ exploring endothelial and neuro-microvascular functioning.^{8,9} PORH can detect recruitment of initially non-perfused capillaries, and reflects both functional and structural parameters.¹⁰ In essential hypertension, this recruitment is impaired.²

Laser speckle-contrast analysis (LASCA) is a real-time non-contact technique with good spatiotemporal accuracy and good reproducibility for the assessment of PORH.¹¹

However, cutaneous microcirculation has certain anatomical and physiological specificities⁸ that are distinct from the renal vascular bed. Specifically, the kidney is perfused with high blood flow and its self-regulating properties are distinct from those of the skin. The kidney is particularly exposed to microvascular damage, as high blood pressure induces early onset of microvascular impairment.¹² Thus, deficits in cutaneous circulation may not faithfully recapitulate renal damage. Consequently, it is of interest to develop techniques to study renal blood flow, which very few studies have examined.^{13–15} Moreover, the development of a robust approach to studying renal microcirculation in the mouse model will facilitate mechanistic studies of the pathways responsible for microvascular rarefaction in response to hypertension, by enabling use of genetically modified mice and experimental hypertension models.

The aim of the present study was therefore to develop a reliable technique to assess renal microvascular reactivity. We then compared 2 mouse populations to validate the model and its feasibility and to evaluate the difference in vascular perfusion. We used the well-established angiotensin-II-induced hypertensive mouse model¹⁶ and normotensive controls to compare renal microcirculation and microvascular reactivity between control and Ang-II-mice on LASCA. To our knowledge, renal microvascular reactivity in mouse has not previously been analyzed on LASCA.

Materials and Methods

Animal models: All animals were maintained in the Johns Hopkins University School of Medicine animal care facility according to the recommendations of the Animal Care and Use Committee, which approved all experimental procedures. Thirty wild-type C57BL/6J mice (Jackson Labs) were used. The 7-week-old mice were distributed 1:1 between 2 groups: one group received angiotensin II (Ang-II; 1 mg/kg/day n=15) via osmotic mini-pumps (Alzet model 1004, Durect Corp, Cupertino, CA) for 21 days, and the other, which did not, served as controls (n=15).

Osmotic pump implantation: Animals were anesthetized with 1.5% isoflurane, and the upper back and neck area were depilated. Under sterile conditions, a dorsal midline incision was made just below the neck and a subcutaneous pocket was created. The minipump containing Ang-II was inserted with its cap facing away from the incision. Local anesthetic was then injected in the suture area (bupivacaine 0.25%, up to 0.3mL); animals were provided with acetaminophen, and their recovery was monitored.

Renal hyperemic response on Laser Speckle Doppler: Mice were anesthetized with 2% isoflurane, positioned in right lateral decubitus on a heated pad, and maintained at 2% isoflurane. The left kidney was exposed through a small flank incision. The connective tissue anterior to the kidney and left renal artery was gently broken by blunt dissection, under binocular magnification. The kidney was externalized and carefully removed from the connective tissue, avoiding the adrenal gland and vessels. Next, the kidney was turned ventral side down into a lucite cup (Klaus Effenberger Med.-Techn. Gerätebau, Pfaffing, Germany) for imaging and to prevent image distortion due to respiratory movement, without exerting tension on the renal vessels (Figure 1).

LASCA is a technique based on speckle-contrast analysis that provides an index of blood flow. The laser light illuminates the kidney and the diffusely backscattered light is collected on the screen. This interference pattern is called “speckle”. If the object, such as red blood cells, moves, the pattern will be dynamic. This is caused by the Doppler shift of the light interacting with the moving particles.

Cortical blood flow in the left kidney was then measured by a MoorFLPI-2 Laser Speckle Contrast Imager (Moor Instruments Inc., Wilmington, DE), with the following settings: camera gain: 93; exposure time: 20 ms; time constant: 0.3 sec; mode: temporal; filter: 25 frames (1 sec/frame); sample interval: 1000 ms; image resolution: 752 x 580. The laser was positioned 12 cm above the region of interest, and zoom and focus were adjusted to acquire high-resolution images of the left kidney.

Blood-flow measurements: Basal blood-flow was first imaged for 15 sec. The PORH test was then performed by carefully clamping the left renal artery for 6 sec with iris forceps (Kent Scientific Corporation, Torrington, CT). The choice of 6 sec occlusion duration was guided by prior studies¹⁷ and based on successful ischemia confirmed visually by a marked decline in blood-flow (Figure 2). Clamping the renal vein was avoided, as it could lead to venous congestion and increased capillary density.¹⁰

Laser Speckle-Contrast Analysis: The following data were recorded and stored, using PeriSoft software for Windows: 1) basal renal blood-flow; 2) peak renal blood-flow (ie, highest value recorded after ischemia); and 3) PORH, expressed as percentage change in peak flow above baseline: $(\text{peak flow} - \text{basal flow}) \times 100/\text{basal flow}$. Flux vs time was analyzed offline by moorFLPI Review software (V3; Moor Instruments, Devon, UK). The region of interest (ROI) was set to correspond to

kidney shape, avoiding proximity to any large blood vessels (Figure 1).

Statistical analysis: Data were reported as mean \pm standard deviation or box-and-whisker plots. The three horizontal lines shown in the boxes are the 25th, 50th and 75th percentiles; the two lines above and below each box are the highest and lowest values, respectively. The Wilcoxon rank-sum test was used to compare means between Ang-II-treated and control mice. All statistical analyses were performed

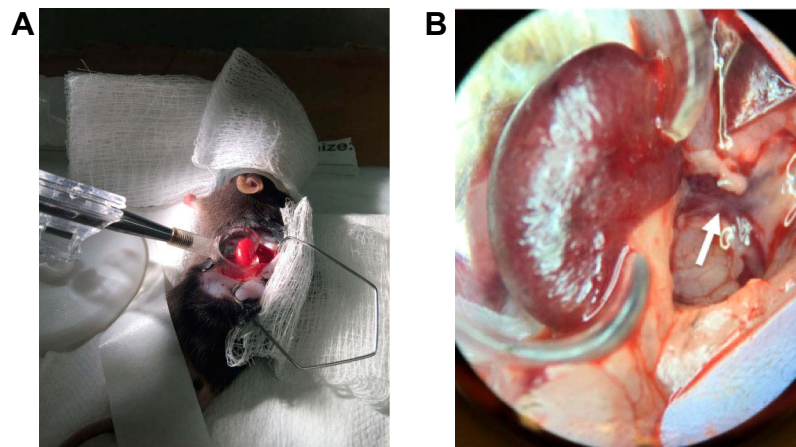


Figure 1 Set-up before measurement. (A) Mouse is placed in right lateral decubitus and the kidney is externalized and placed in a kidney cup. (B) Ventral face of left kidney and left renal artery (white arrow), which divides in two and travels above the renal vein.

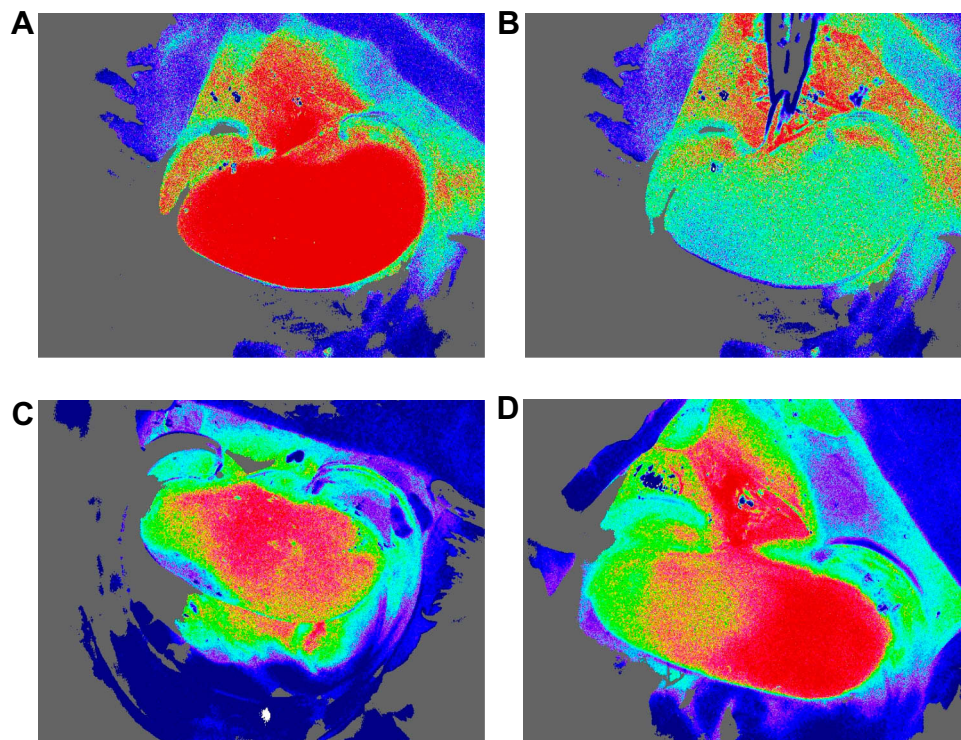


Figure 2 Laser speckle-contrast imaging of the kidney. (A) Kidney before occlusion. (B) Drop in blood-flow during occlusion. (C) Example of degraded outflow. (D) Hemi-kidney not vascularized.

with SPSS Statistics[®] software (IBM, NY). The significance threshold was set at $P < 0.05$.

Results

In the Ang-II cohort, 2 mice died 1 day after osmotic pump insertion. One Ang-II mouse presented immediate poor-quality blood-flow and was removed from analysis. Four mice (3 controls and 1 Ang-II) with severely degraded images after the occlusion test were also removed from analysis, including 2 control mice with non-vascularized hemi-kidney after releasing occlusion (Figure 2). Analysis thus concerned 23 mice: 12 control and 11 Ang-II. Results are summarized in Table 1. Control mice had significantly lower basal renal microcirculatory flow than Ang-II-treated mice (1448 ± 96 vs 1703 ± 185 PU, respectively; $P < 0.05$) (Figure 3). Peak flow was lower in controls than Ang-II mice (1617 ± 104 vs 1724 ± 205 PU, respectively; $P = 0.21$). Control mice had significantly higher kidney PORH than Ang-II mice (8 ± 3 vs $1 \pm 4\%$, respectively; $P < 0.05$).

Discussion

The present study describes a methodology to assess renal microvascular reactivity in mice. Results showed

Table 1 Results of Laser Speckle-Contrast Analysis Measurements, in All 23 Mice, and in Control and Ang-II-Treated Mice. Data are Mean and Standard Deviation

	Total (n=23)	Control (n=12)	Ang-II Treated (n=11)
Basal Flow (PU)	1570 \pm 193	1448 \pm 96	1703 \pm 185*
Peak Flow (PU)	1668 \pm 167	1617 \pm 104	1724 \pm 205
PORH (%)	5 \pm 5	8 \pm 3	1 \pm 4*

Abbreviations: PORH, post-occlusive reactive hyperemia (Peak Flow – Basal Flow) \times 100/Basal Flow; PU, perfusion unit. *Significant differences at $p < 0.05$ level between control and Ang-II-treated mice.

significantly higher renal basal microcirculatory flow in Ang-II-treated mice than in control mice, with higher PORH in controls than in Ang-II-treated mice. Renal microcirculation was studied as microvascular damage in the kidney is well known to occur with hypertension.

The cutaneous microcirculation is readily accessible and provides a powerful model to study human hypertension. Several vascular anatomical and physiological variables, however, differ between organs. Microcirculatory disturbance, for example, develops earlier in the skin than in skeletal muscle.⁶ The skin has a higher density of nerve fibers than other tissues, which explains the major influence of

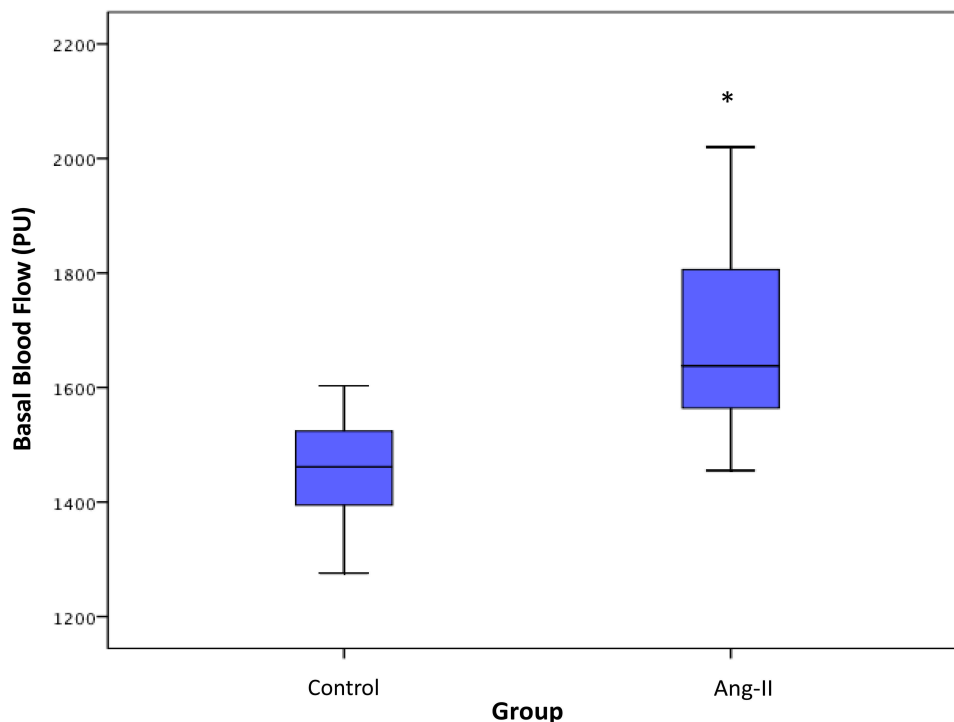


Figure 3 Basal blood-flow in control and Ang-II-treated mice. Data are presented as box plots. The three horizontal lines in the boxes are the 25th, 50th and 75th percentiles. The two lines outside the boxes represent the highest and lowest values. PU: perfusion unit. Asterisk indicates significant blood-flow differences at $p < 0.05$ level between control and Ang-II-treated mice.

neural control on skin microvascular reactivity.⁸ Therefore, it is important to know whether findings in the skin can be directly extrapolated to other vascular beds. Some similarities in response and signaling mechanisms despite kinetic differences were revealed in a previous study, where renal vasodilatory response was evaluated using local pressure application and compared with cutaneous response.¹⁵ Coulon et al demonstrated a correlation between renal resistive index (interlobular arteries) and skin PORH parameters on laser Doppler flowmetry (LDF) in hypertensive and normotensive subjects.¹⁴ While it is clear that changes in microcirculation in both organs occur in parallel under hypertension, further studies are required to directly investigate renal microcirculation in hypertension, in order to determine whether the underlying cellular and molecular causal mechanisms in microvascular dysfunction are the same in these distinct vascular beds. Directly detecting renal microvascular damage is important for another reason: the link between blood pressure and microvascular damage is not well established. Capillary recruitment during post-occlusive reactive hyperemia has been found to correlate inversely with blood pressure.¹⁸ However, blood pressure measurement does not exhaustively track kidney microvascular damage. Structural alterations occur before blood pressure rises in spontaneously hypertensive rats (SHR).⁴ Rizzoni et al showed significant persistent regression of vascular hypertrophy after short calcium entry blocker treatment in SHRs, while blood pressure progressively increased.⁵ ACE (angiotensin-converting enzyme) inhibitors can also limit microvascular changes in mesenteric small arteries, without any statistically significant hemodynamic effects being induced.¹⁹

There are various ways of assessing renal microcirculation. Rodriguez-Porcel et al demonstrated impaired kidney response to vasodilators (acetylcholine and sodium nitroprusside), but they used electron-beam computed tomography, which is difficult to implement routinely.²⁰ LDF has been extensively used to assess renal microcirculation in mice in ischemia-reperfusion,^{21,22} preconditioning,²³ renal cryoinjury²⁴ or other models.²⁵ LASCA and LDF both use laser speckle patterns, but the analysis techniques differ.²⁶ LASCA has been applied to skin, retina, mesenteric microcirculation and to monitor cerebral blood flow.²⁷ In humans, LASCA has been used to assess microcirculation changes in response to treatment²⁸ or other stimuli.²⁹ It has been applied extensively in various mouse models, to assess neurological microcirculation,^{30,31} and for mesenteric³² and liver analysis in rats.³³ LASCA on the kidney surface has been described in

rats.^{34,35} To our knowledge, LASCA has only once been reported for assessment of renal cortical blood flow in a dedicated hypertensive mouse model,³⁶ where a reduction in renal cortical blood flow was induced by Ang-II treatment. LASCA provides an index of blood flow,³⁷ with an arbitrary unit. Since absolute blood flow rates vary with temperature, heart rate and metabolic rate, a normalized approach is needed for measurement. The most relevant value is thus PORH, as it is a ratio, and was therefore used in our study.

Untreated and recently treated hypertensive patients showed significantly higher basal skin blood-flow than controls.^{38,39} Hypertension impairs myogenic tone.¹ Hypertensive patients fail to react by adequate vasodilatation on ischemia test (PORH).^{6,38,40} PORH involves complex mechanosensitive and metabolic mechanisms.⁴¹ Untreated hypertensive patients showed significantly lower skin PORH than controls.³⁸ Our results in the mouse kidney are in good agreement with these prior studies. After treatment, patients did not differ from controls in skin PORH,³⁸ and this remains to be evaluated in mouse models of hypertension.

The duration of ischemia is a critical factor to consider in measuring PORH.

Zatta and Headrick demonstrated that multiple mediators contribute to coronary reactive hyperemia in mouse.¹⁷ Using short (5–10 sec) or long (20–40 sec) occlusion durations, they determined that mechanisms involved in PORH depend on occlusion time. Coronary reactive hyperemia was graded, increasing with occlusion duration from 5 to 40 seconds. We therefore chose a short duration of 6 sec, also to avoid damage to the vessel with longer occlusion times. In humans, occlusion time is much longer.³⁸ Furthermore, PORH amplitude in our experimental set-up was lower than in human skin³⁸ or coronary amplitude.¹⁷ This could be due 1) to arterial dissection (as noted in the vascularized hemi-kidney observed in 2 cases after occlusion test) or 2) to the use of forceps to study PORH amplitude. A model for renal ischemic preconditioning has been developed using a hanging-weight system for isolated renal artery occlusion;⁴² this kind of system should enable precise occlusion and reduce any mechanical damage wrought by the use of forceps.

Conclusion

We described a PORH protocol assessing renal microvascular reactivity using LASCA as an efficient technique to assess renal microcirculation in mice. Ang-II-treated mice were used for comparison and validation

of the model as a method to evaluate differences in vascular perfusion. We observed higher microvascular basal blood-flow but lower PORH in Ang-II-treated than control mice. This method can be combined with the use of various drugs and inhibitors to study specific mechanisms contributing to microvascular damage resulting from hypertension.

Acknowledgments

We would like to warmly thank Sandeep Jandu, Hiroshi Matsushita, and Morgan Elliott of Johns Hopkins University for their technical assistance.

Ethics and Consent Statement

All animal protocols were approved by the Institutional Animal Care and Use Committee at Johns Hopkins University School of Medicine. Animals were maintained in the Johns Hopkins University School of Medicine animal care facility and were handled according to Animal Care and Use Committee recommendations.

Author Contributions

All authors made substantial contributions to conception and design, acquisition of data, or analysis and interpretation of data; took part in drafting the article or revising it critically for important intellectual content; gave final approval of the version to be published; and agree to be accountable for all aspects of the work.

Funding

We acknowledge ACCM StAAR Investigator Award to Dr Lakshmi Santhanam for funding this study. Johns Hopkins University, Baltimore MD, USA.

Disclosure

The authors report no conflicts of interest in this work.

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