

# Surfactin-based nanoparticles loaded with doxorubicin to overcome multidrug resistance in cancers

Wenjing Huang<sup>1</sup>Yan Lang<sup>1</sup>Abdul Hakeem<sup>1</sup>Yan Lei<sup>2</sup>Lu Gan<sup>1</sup>Xiangliang Yang<sup>1</sup>

<sup>1</sup>Department of Nanomedicine and Biopharmaceuticals, National Engineering Research Center for Nanomedicine, College of Life Science and Technology, Huazhong University of Science and Technology, Wuhan 430074, China; <sup>2</sup>Pharmacy of School Hospital, Huazhong University of Science and Technology, Wuhan 430074, China

**Background:** Multidrug resistance (MDR) is one of the major obstacles to successful cancer chemotherapy. Developing efficient strategies to reverse MDR remains a major challenge. Surfactin (SUR), a cyclic lipopeptide biosurfactant, has been found to display anticancer activity.

**Methods:** In this paper, SUR was assembled by solvent-emulsion method to load the anticancer drug doxorubicin (DOX). The cytotoxicity of DOX-loaded SUR nanoparticles (DOX@SUR) against DOX-resistant human breast cancer MCF-7/ADR is measured by MTT assay. The cellular uptake and intracellular retention of DOX@SUR are determined by flow cytometry. The tumor accumulation and anticancer activity of DOX@SUR are evaluated in MCF-7/ADR-bearing nude mice.

**Results:** DOX@SUR induce stronger cytotoxicity against DOX-resistant human breast cancer MCF-7/ADR cells compared to free DOX. DOX@SUR nanoparticles exhibit enhanced cellular uptake and decreased cellular efflux, which might be associated with reduced P-glycoprotein expression. After internalization into MCF-7/ADR cells by macropinocytosis- and caveolin-mediated endocytosis, DOX@SUR nanoparticles are colocalized with the lysosomes and translocated to the nucleus to exert cytotoxicity. Furthermore, in vivo animal experiment shows that the DOX@SUR nanoparticles are accumulated more efficiently in tumors than free DOX. Meanwhile, DOX@SUR nanoparticles display stronger tumor inhibition activity and fewer side effects in MCF-7/ADR-bearing nude mice.

**Conclusion:** This study indicates that SUR-based nanocarrier might present a promising platform to reverse MDR in cancer chemotherapy.

**Keywords:** multidrug resistance, cellular uptake, cellular efflux, biodistribution

## Introduction

Breast cancer is the leading cause of cancer mortality in women worldwide.<sup>1</sup> Doxorubicin (DOX) is widely used as a chemotherapeutic agent in the clinical therapy of breast cancer patients.<sup>2-4</sup> Unfortunately, multidrug resistance (MDR) is considered as one of the primary impediments to successful cancer chemotherapy.<sup>5</sup> Therefore, exploring how to overcome MDR is extremely crucial for breast cancer treatment. The most common mechanism of MDR is correlated with overexpression of ATP-binding cassette transporters, particularly P-glycoprotein (P-gp), leading to the efflux of many anticancer drugs.<sup>6</sup> Nanoparticle-based therapeutics have been considered as one of the most prospective platforms in drug delivery applications due to increased drug accumulation in solid tumor by enhanced permeability and retention (EPR) and MDR reversal through bypassing or inhibiting P-gp activity.<sup>7-9</sup>

Correspondence: Lu Gan  
National Engineering Research Center for Nanomedicine, College of Life Science and Technology, Huazhong University of Science and Technology, Wuhan 430074, China  
Tel +86 278 779 2147  
Fax +86 278 779 2234  
Email lugan@mail.hust.edu.cn

Surfactin (SUR) is a cyclic lipopeptide biosurfactant containing heptapeptide (LLDLLDL) and a beta-hydroxy fatty acid produced by *Bacillus subtilis*.<sup>10</sup> In addition to functioning as a biosurfactant owing to its amphipathic property, SUR has been found to exhibit versatile bioactive features including antibacterial,<sup>11,12</sup> antiviral,<sup>13</sup> anti-inflammatory,<sup>14,15</sup> antiproliferative,<sup>16</sup> adjuvant for immunization and antitumor properties.<sup>17–22</sup> Recently, SUR has been found to inhibit the proliferation of MCF-7 cells by inducing apoptosis through a ROS/JNK-mediated mitochondrial/caspase pathway and decrease the drug efflux capacity of P-gp by reducing the function of ATP.<sup>18</sup> Based on the unique amphipathic properties, SUR has the potential to self-assemble into nanoparticles at a certain condition to function as a drug carrier for loading hydrophobic drugs.<sup>23</sup> Combining the anticancer activity of SUR and the characteristics of nanoparticles such as EPR effects and MDR reversal, it might be promising to improve cancer chemotherapy by designing SUR as a carrier to load anticancer drugs.

Herein, we explore the unique ability of SUR nanoparticles as an anticancer drug carrier to overcome MDR. DOX-loaded SUR nanoparticles (DOX@SUR) were synthesized by a solvent-emulsion method. The in vitro cytotoxicity and related mechanism to overcome MDR were studied in DOX-sensitive human breast cancer MCF-7 and DOX-resistant MCF-7/ADR. The therapeutic outcomes were further examined in MCF-7/ADR xenograft model. The rational design of drug carriers based on SUR might have great significance in achieving efficient cancer therapy.

## Materials and methods

### Materials

Doxorubicin hydrochloride (DOX•HCl) was provided by Beijing Huafeng United Technology (Beijing, China). SUR was purchased from Sigma Aldrich (St Louis, MO, USA). RPMI 1640 medium, penicillin–streptomycin and trypsin without EDTA were obtained from Thermo Fisher Scientific (Waltham, MA, USA). Fetal bovine serum was procured from Thermo Fisher Scientific. 4,6-Diamidino-2-phenylindole and MTT were purchased from Biosharp (Anhui, China). LysoTracker Green was obtained from Thermo Fisher Scientific. All other reagents were of analytical grade and used without further purification.

### Synthesis of DOX@SUR nanoparticles

DOX@SUR nanoparticles were synthesized by a solvent-emulsion method. Briefly, DOX•HCl aqueous solution (1.0 mg/mL) was mixed with excess triethylamine (15 µL/mL solution) in chloroform for 40 min to obtain hydrophobic

DOX. Then, this mixture was dropped into SUR aqueous solution (2 mg/mL) under ultrasonic emulsification for 5 min, followed by constant stirring at 40°C overnight to volatilize chloroform. DOX@SUR nanoparticles were purified in an ultrafilter tube (cutoff molecular weight 3000; EMD Millipore) by centrifugation at 4,000 rpm for 20 min to remove free DOX. The blank SUR nanoparticles were formed by the same method, except that no DOX was added. The drug loading capacity of SUR nanoparticles was calculated using the equation: drug loading capacity =  $(W_{\text{administered dose}} - W_{\text{residual dose in solution}})/W_{\text{SUR}} \times 100\%$ . The size distribution and zeta potential of the nanoparticles were determined by dynamic light scattering (Zetasizer Nano ZS90; Malvern Instruments Ltd, Worcestershire, UK). The surface morphology of nanoparticles was observed with a transmission electron microscope (Tecnai G2-20; FEI Corp., Eindhoven, the Netherlands).

### In vitro drug release from DOX@SUR nanoparticles

The release of DOX from DOX@SUR nanoparticles was investigated by the dialysis bag method.<sup>24</sup> Briefly, 1 mL of 200 µg/mL DOX@SUR nanoparticles was placed in a dialysis bag (the cutoff molecular weight was 3000) and submerged fully into 25 mL of PBS, followed by stirring at 100 rpm speed at 37°C. Then, 1 mL of the release medium was taken out at the designated time points and replenished with the same volume of fresh PBS. The amount of DOX released was determined with a fluorescence spectrometer at Ex 488 nm/Em 560 nm using a DOX calibration curve.

### Cell culture and animals

Sensitive human breast cancer MCF-7 cells and adriamycin-resistant human breast cancer MCF-7 cells (MCF-7/ADR) were kindly provided by Dr Zhiping Zhang from the School of Pharmacy, Huazhong University of Science and Technology, Wuhan, China. MCF-7 and MCF-7/ADR cells were cultivated in RPMI 1640 medium containing 10% fetal bovine serum, 100 U/mL penicillin G sodium and 100 µg/mL streptomycin sulfate at 37°C in a humidified 5% CO<sub>2</sub> incubator, except that 1 mg/mL DOX was added during MCF-7/MDR culture. We obtained the approval of the ethical committee of Huazhong University of Science and Technology for conducting research using these cells.

Female nude mice were purchased from HUAUFUKANG Bioscience Co., Ltd (Beijing, China). All animals received care following the guidelines outlined in the “Guide for the Care and Use of Laboratory Animals”. The mice were subcutaneously injected with 100 µL of cell suspension ( $2 \times 10^6$

MCF-7/ADR cells per mouse) to initiate the formation of breast tumor. All animal experiments were approved and executed under the directions of the ethical committee of Huazhong University of Science and Technology.

### In vitro cytotoxicity of DOX@SUR nanoparticles

The in vitro cytotoxicity of DOX@SUR nanoparticles was determined by MTT assay. Briefly, MCF-7 or MCF-7/ADR cells were initially cultured in complete RPMI 1640 medium for 24 h. After rinsing with PBS, cells were incubated with blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at different concentrations of DOX. At the designated time points, cells were washed with PBS and then further incubated in a medium containing MTT solution (5 mg/mL) at 37°C for another 4 h. Subsequently, the MTT solution containing medium was discarded and 150  $\mu$ L dimethyl sulfoxide was added to liquefy formazan crystals. The absorbance of formazan at 492 nm was measured using an iEMS microplate reader (LabSystems, Helsinki, Finland).<sup>25–27</sup>

### Ki-67, Bax and Bcl-2 expression in MCF-7/ADR cells

MCF-7/ADR cells were treated with blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at a DOX concentration of 5  $\mu$ g/mL. At 12 h after treatment, the cells were harvested and total RNAs were extracted by using Trizol® reagent (Thermo Fisher Scientific). Total RNA content was detected using a NanoDrop spectrophotometer (Thermo Fisher Scientific). cDNAs were generated by reverse transcription-polymerase chain reaction (PCR) method with the total RNA (1  $\mu$ g) from each sample. cDNA (1  $\mu$ g) was added to mixture containing ultrapure water (4  $\mu$ L), SYBR Green (4  $\mu$ L; Takara, Tokyo, Japan), 10  $\mu$ M forward primer (0.5  $\mu$ L) and 10  $\mu$ M reverse primer (0.5  $\mu$ L). Sequences of Bcl-2, Bax, Ki-67 and glyceraldehyde 3-phosphate dehydrogenase primers used for real-time PCR are shown in Table S1. Quantitative real-time PCR was performed by using StepOnePlus™ Real-Time PCR (Thermo Fisher Scientific). Glyceraldehyde 3-phosphate dehydrogenase was considered as the internal reference, and  $2^{-\Delta\Delta C_t}$  was used to calculate the relative expression of target genes.<sup>26</sup>

### Cellular uptake of DOX@SUR nanoparticles

MCF-7/ADR cells were cultured in 12-well plates at a density of  $2 \times 10^5$  cells per well. After 24 h of incubation, the cells were treated with free DOX or DOX@SUR nanoparticles at 5  $\mu$ g/mL DOX concentration for various time

periods. Subsequently, the cells were washed twice with PBS, trypsinized and then resuspended in 400  $\mu$ L PBS for DOX fluorescence intensity measurement by flow cytometry (FC500; Beckman Coulter, Fullerton, CA, USA).

### Intracellular retention of DOX@SUR nanoparticles

MCF-7/ADR cells were incubated in six-well plates at  $1 \times 10^5$  cells per well. The cells were washed twice with PBS and incubated with free DOX or DOX@SUR nanoparticles at 5  $\mu$ g/mL DOX concentration for 12 h. Subsequently, the cells were washed twice with PBS and further incubated in blank medium for different time periods at 37°C. The cells were washed twice with PBS, trypsinized and then resuspended in 400  $\mu$ L PBS for DOX fluorescence intensity measurement by flow cytometry.

### P-gp expression

MCF-7/ADR cells were cultured in 12-well plates at a density of  $2 \times 10^5$  cells per well. After 12 h of incubation, the cells were treated with free DOX or DOX@SUR nanoparticles at 5  $\mu$ g/mL DOX concentration for various time periods. Subsequently, the cells were washed twice with PBS, resuspended in 400  $\mu$ L PBS and then incubated with 20  $\mu$ L fluorescein isothiocyanate-conjugated mouse anti-human P-gp antibody (Becton, Dickinson and Company, Franklin Lakes, NJ, USA) for 15 min. The fluorescence intensity of fluorescein isothiocyanate was measured by flow cytometry.

### Endocytic pathway of DOX@SUR nanoparticles

MCF-7/ADR cells were preincubated in serum-free RPMI 1640 medium containing 2 mM amiloride, 10  $\mu$ g/mL chlorpromazine, 10  $\mu$ g/mL filipin, 20  $\mu$ g/mL nystatin or 5 mM methyl- $\beta$ -cyclodextrin (M $\beta$ CD) for 30 min, respectively.<sup>25</sup> The media were then changed to fresh serum-free medium containing the inhibitors and DOX@SUR nanoparticles at 5  $\mu$ g/mL DOX concentration and incubated for another 1 h. The cells were washed with PBS, harvested and then intracellular DOX fluorescence was determined by flow cytometry.

### Intracellular distribution of DOX@SUR nanoparticles

MCF-7 or MCF-7/ADR cells were treated with DOX@SUR nanoparticles at 5  $\mu$ g/mL DOX concentration. At the designated time points, the cells were washed with PBS and then labeled with 5  $\mu$ g/mL 4,6-diamidino-2-phenylindole or

200 nM LysoTracker Green at 37°C for 20 min. The cells were washed with PBS, fixed with 4% paraformaldehyde and then visualized by FV 1000 confocal microscope (Olympus Corporation, Tokyo, Japan).

## In vivo biodistribution of DOX@SUR nanoparticles

MCF-7/ADR tumor-bearing nude mice were intravenously administered free DOX or DOX@SUR nanoparticles at 5 mg DOX/kg dose. After 24 and 48 h injection, major organs including heart, liver, spleen, lung, kidney and tumor were resected and then imaged to assess ex vivo biodistribution of DOX@SUR in mice by in vivo fluorescence imaging (Thermo Fisher Scientific). These tissues were then washed with saline and homogenized with methanol. DOX content was measured by fluorescence spectrometer at Ex 488 nm/Em 560 nm.

## In vivo antitumor efficacy of DOX@SUR nanoparticles

MCF-7/ADR tumor-bearing nude mice were intravenously administered saline, blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at a DOX dose of 5 mg/kg on day 1, 5 and 9. Tumor sizes were monitored with a digital caliper

every day and calculated based on the formula:  $(L \times W^2)/2$ , where L and W are the length and width of the tumor, respectively. On day 12, the mice were sacrificed, and the major organs were excised, fixed and sliced for H&E staining.

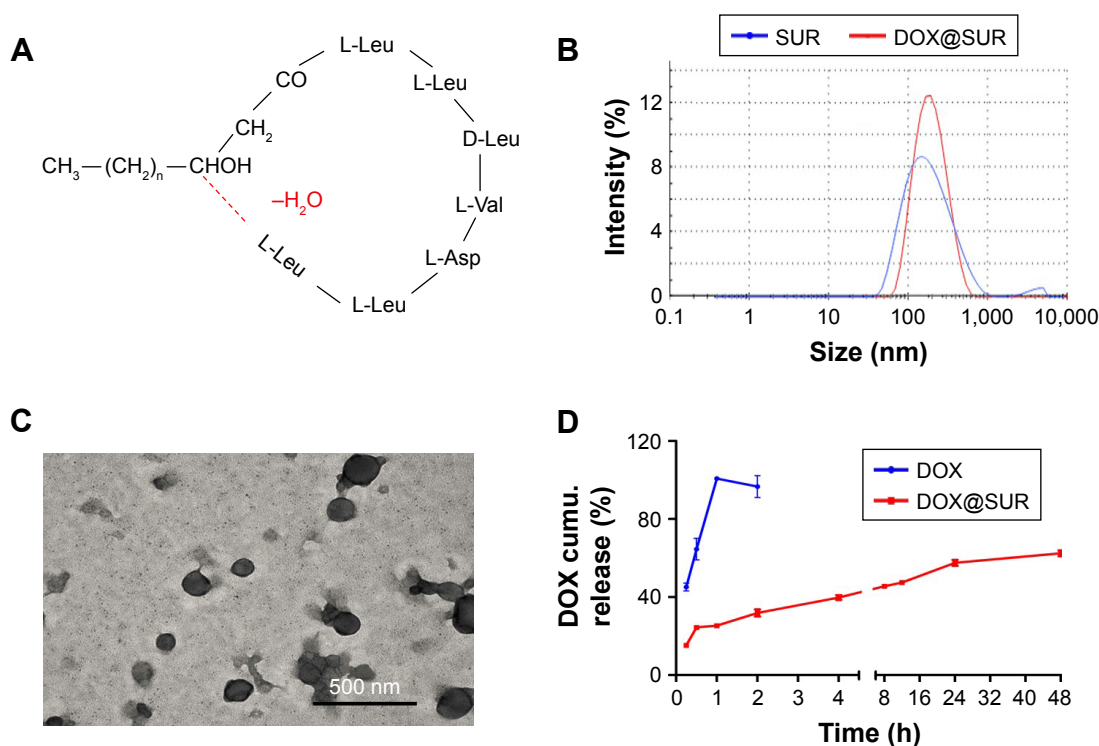
## Statistical analysis

All experiments were performed with at least three replicates. Student's *t*-test was used to carry out statistical analyses. Only  $P < 0.05$  was considered significant.

## Results and discussion

### Synthesis and characterization of DOX@SUR nanoparticles

SUR is an attractive and powerful biosurfactant because of its special amphiphilic character (Figure 1A). When a hydrophobic organic solution of DOX (an anticancer drug model) was mixed with an aqueous solution of SUR, an unstable polymer emulsion was formed. With the evaporation of organic solvents, DOX was forced into the hydrophobic core of SUR nanoparticles, which resulted in the formation of a core-shell structure termed as DOX@SUR nanoparticles. Different feeding ratios of SUR and DOX were used to optimize the conditions of forming DOX@SUR nanoparticles (Table 1). The drug loading efficiency of SUR nanoparticles



**Figure 1** Characterization of DOX@SUR nanoparticles.

**Notes:** (A) Chemical structures of SUR. (B) Hydrodynamic diameter of blank SUR nanoparticles and DOX@SUR nanoparticles by DLS. (C) TEM image of DOX@SUR nanoparticles. (D) Drug release profiles of free DOX and DOX@SUR nanoparticles in PBS buffer (pH 7.4).

**Abbreviations:** DLS, dynamic light scattering; DOX, doxorubicin; SUR, surfactin; TEM, transmission electron microscope; DOX@SUR, DOX-loaded surfactin.



**Table 1** Characterization of DOX@SUR nanoparticles at different DOX/SUR feeding ratios

SUR:DOX (mass ratio)	Diameter (nm)	Zeta (mV)	PDI	Drug-loading rate (%)
5:1	249.5±49.5	-32.5 (0.4)	0.133	10.6±0.5
2:1	217.1±10.8	-35.7 (0.6)	0.152	22.4±0.6
1:1	160.2±10.2	-36.1 (0.5)	0.138	25.8±0.5
1:2	207.1±00.4	-36.6 (0.6)	0.221	27.6±7.8

**Abbreviations:** DOX, doxorubicin; PDI, polydispersity index; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

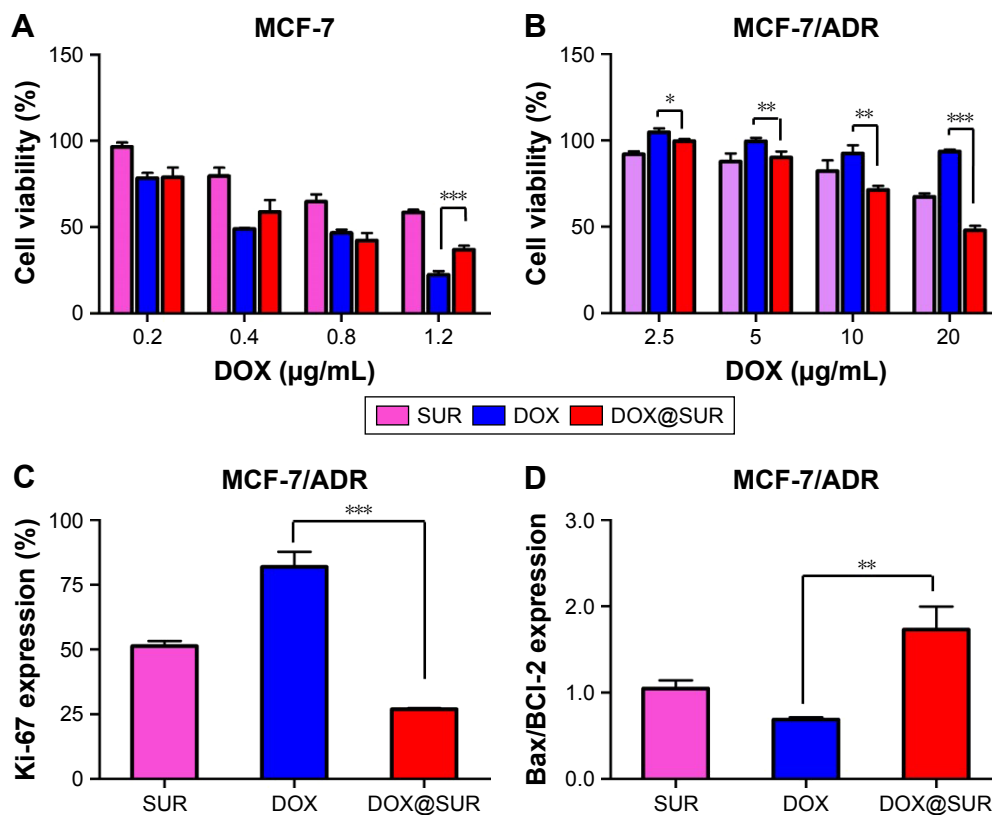
increased with increasing amounts of DOX input and reached 25.8% at the SUR/DOX feeding ratio of 1. The size of the DOX@SUR nanoparticles formed became smaller at a certain range of feeding ratio (SUR:DOX≤1:1). The size of DOX@SUR nanoparticles was the smallest at the SUR/DOX feeding ratio of 1. Considering that the drug loading efficiency increased slowly when the SUR/DOX feeding ratio was <1, we formed DOX@SUR nanoparticles at the feeding ratio of 1 in further experiments.

Dynamic light scattering showed the size and zeta potential of DOX@SUR nanoparticles to be about 160 nm (Figure 1B) and -36.0 mV, respectively. Transmission

electron microscopic imaging showed that DOX@SUR was monodisperse and nearly spherical (Figure 1C). DOX release profile analysis from DOX@SUR nanoparticles showed that about 66.5% DOX was released from DOX@SUR even after 48 h of incubation in PBS (Figure 1D). However, free DOX exhibited a burst release during 1 h of incubation. These results indicated that DOX@SUR nanoparticles displayed a slow drug release capacity.

## In vitro cytotoxicity of DOX@SUR nanoparticles

To determine the biological function of DOX@SUR nanoparticles, the in vitro cytotoxicity against MCF-7 and MCF-7/ADR cells was explored by MTT assay. As expected, blank SUR nanoparticles, free DOX and DOX@SUR nanoparticles displayed a dose-dependent cytotoxicity against both MCF-7 cells and MCF-7/ADR cells. However, no obvious difference in cytotoxicity of free DOX and DOX@SUR nanoparticles at a low DOX concentration was observed in MCF-7 cells, and the cytotoxicity of free DOX at 1.2 µg/mL concentration was stronger than that of DOX@SUR (Figure 2A).

**Figure 2** MDR reversal capacity of DOX@SUR nanoparticles.

**Notes:** (A, B) Cytotoxicity against (A) MCF-7 and (B) MCF-7/ADR cells after treatment with blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at different DOX concentrations for 48 h by MTT assay. (C, D) The mRNA expression of (C) Ki-67 and (D) Bax/Bcl-2 in MCF-7/ADR cells treated with blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at a DOX concentration of 5 µg/mL for 12 h by real-time RT-PCR. Data are expressed as mean value ± SD (n=3). \**P*<0.05, \*\**P*<0.01, \*\*\**P*<0.001.

**Abbreviations:** DOX, doxorubicin; MDR, multidrug resistance; RT-PCR, reverse transcription-polymerase chain reaction; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

This could be due to the reason that free DOX was easier to enter the cells than DOX@SUR in MCF-7 cells. However, in DOX-resistant MCF-7/ADR cells, DOX@SUR nanoparticles exhibited stronger cytotoxicity than free DOX (Figure 2B). Furthermore, we examined the  $IC_{50}$  value of free DOX and DOX@SUR nanoparticles (Table S2). The  $IC_{50}$  of free DOX in MCF-7/ADR cells was estimated to be 147  $\mu\text{g/mL}$  after treatment for 48 h, about 420-fold of that in MCF-7 cells, confirming DOX resistance in MCF-7/ADR cells. Consistently, there was no obvious difference in  $IC_{50}$  of free DOX and DOX@SUR nanoparticles in MCF-7 cells. In contrast, the  $IC_{50}$  of DOX@SUR nanoparticles decreased to 15.6  $\mu\text{g/mL}$  in MCF-7/ADR cells, which was about 10.5% of that of free DOX, suggesting that DOX@SUR nanoparticles efficiently reversed the drug resistance in MCF-7/ADR cells. To further confirm this, the expression of proliferation- and apoptosis-related genes was evaluated by real-time PCR. As shown in Figure 2C and D, treatment with DOX@SUR nanoparticles significantly decreased the expression of *Ki-67* and upregulated the ratio of *Bax/Bcl-2* gene expression in MCF-7/ADR cells compared to that with free DOX, suggesting that DOX@SUR nanoparticles had stronger ability to inhibit proliferation and induce apoptosis in MCF-7/ADR cells.

## Cellular uptake and efflux of DOX@SUR nanoparticles

To understand the underlying mechanism of DOX@SUR nanoparticles on MDR reversal in MCF-7/ADR cells, we initially examined their cellular uptake using flow cytometry. Both free DOX and DOX@SUR nanoparticles displayed enhanced cellular uptake by MCF-7 and MCF-7/ADR cells in a dose- and time-dependent manner (Figure 3A and B). Consistent with the stronger cytotoxicity of free DOX against MCF-7 cells (Figure 2A), more free DOX was internalized into MCF-7 cells than DOX@SUR nanoparticles (Figure 3A). In contrast, higher DOX fluorescence was detected in DOX@SUR nanoparticle-treated MCF-7/ADR cells than that in free DOX-treated cells (Figure 3B), suggesting enhanced cellular uptake of DOX@SUR nanoparticles by MCF-7/ADR cells. The increased internalization of DOX@SUR nanoparticles into MCF-7/ADR cells was further confirmed by confocal laser scanning microscopy (Figure S1).

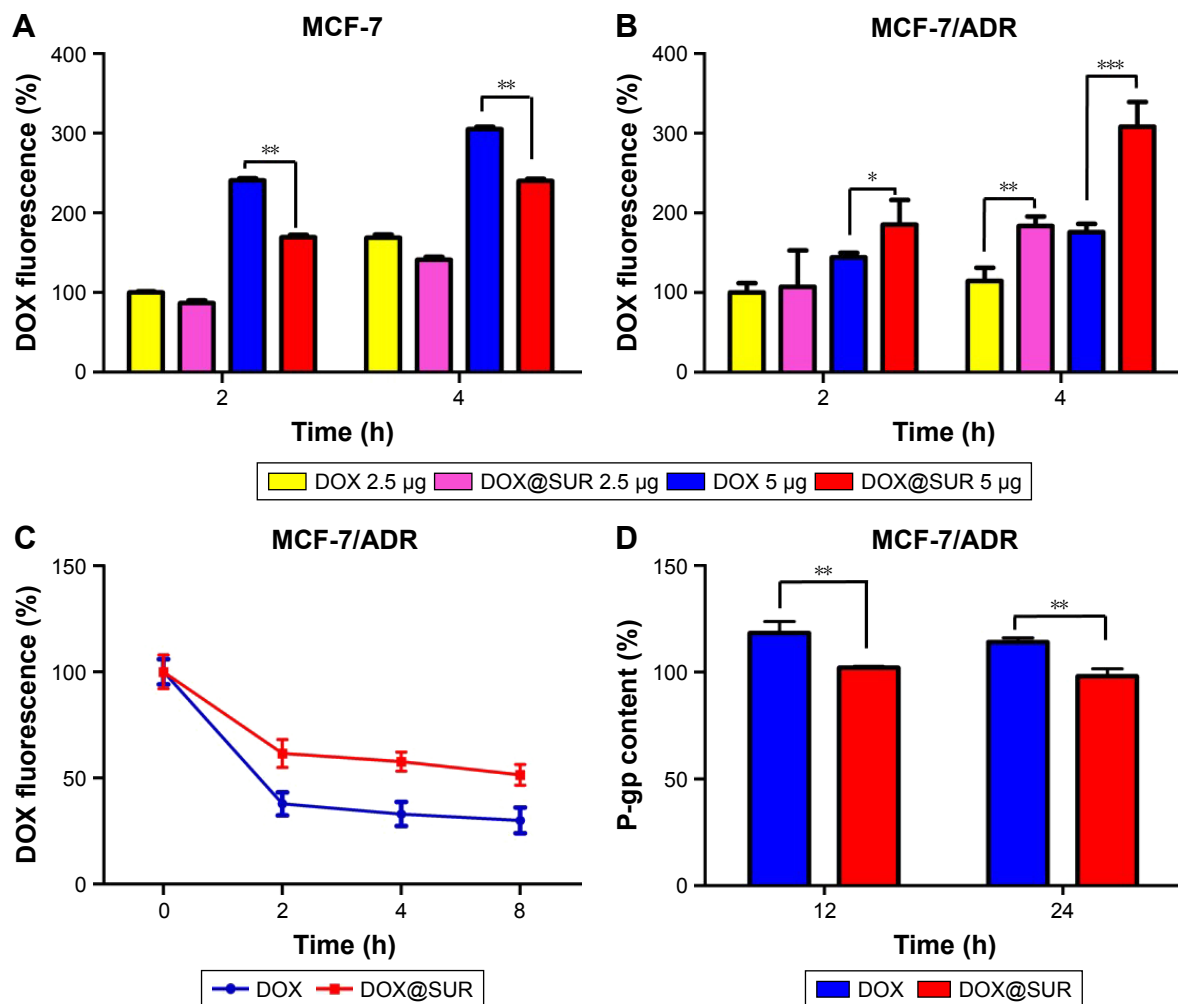
Besides enhanced cellular uptake, it is widely acknowledged that cancer MDR is often allied with drug efflux pumps overexpressed on the cell membrane, such as P-gp, to efflux the intracellular drug.<sup>14</sup> To determine whether DOX@SUR nanoparticles decreased drug efflux, MCF-7/ADR cells were

first incubated with free DOX or DOX@SUR for 4 h, followed by incubation in fresh medium for various time intervals and then determining the intracellular DOX fluorescent intensity by flow cytometry (Figure 3C). The result showed that 62.2% of free DOX was eliminated from the MCF-7/ADR cells within 2 h, but in contrast, only 38.4% of the DOX carried by DOX@SUR nanoparticles was expelled even after 8 h, revealing that DOX@SUR nanoparticles could more effectively escape from the drug efflux action compared to free DOX. To determine if the reduced drug efflux of DOX@SUR was attributed to P-gp expression change, P-gp protein expression in MCF-7/ADR cells treated with free DOX or DOX@SUR nanoparticles was determined by immunofluorescence staining (Figure 3D). The P-gp expression of MCF-7/ADR cells increased after treatment with DOX, whereas the P-gp expression in DOX@SUR nanoparticle-treated cells was significantly lower than that in free DOX-treated cells, demonstrating that the successful retention of DOX@SUR nanoparticles might be attributed to P-gp suppression.

## Intracellular trafficking of DOX@SUR nanoparticles

In view of the enhanced cellular uptake and decreased drug efflux of DOX@SUR nanoparticles in MCF-7/ADR cells, we further determined their endocytic pathway and intracellular trafficking. MCF-7/ADR cells were pretreated with various endocytic inhibitors, followed by treatment with DOX@SUR nanoparticles for 4 h and then the intracellular fluorescence of DOX@SUR nanoparticles was determined by flow cytometry. As shown in Figure 4A, amiloride (an inhibitor of macropinocytosis-dependent endocytosis) and nystatin, filipin and  $\beta$ -cyclodextrin (caveolin-mediated endocytosis inhibitors) significantly inhibited the internalization of DOX@SUR nanoparticles, whereas chlorpromazine (an inhibitor of clathrin-mediated endocytosis) did not show any notable inhibition on the cellular uptake of DOX@SUR nanoparticles. The data suggested that macropinocytosis- and caveolin-mediated endocytosis might be involved in the cellular uptake of DOX@SUR nanoparticles.

To track the intracellular fate of DOX@SUR nanoparticles after internalization, confocal microscopy was used to determine the colocalization of DOX@SUR nanoparticles with lysosomes and nuclei. As shown in Figure 4B, after the MCF-7/ADR cells were treated with DOX@SUR nanoparticles for 2 h, the DOX@SUR nanoparticles were mostly colocalized with lysosomes and small amounts were found to colocalize with nuclei, demonstrating that the internalized DOX@SUR nanoparticles were mainly transmitted



**Figure 3** Cellular uptake and retention of DOX@SUR nanoparticles.

**Notes:** (A) Relative DOX fluorescence intensity in MCF-7 and (B) MCF-7/ADR cells after treatment with free DOX or DOX@SUR nanoparticles at different DOX concentrations for different time courses. (C) Relative DOX fluorescence intensity in MCF-7/ADR cells after pretreatment with free DOX or DOX@SUR nanoparticles at a DOX concentration of 5 µg/mL for 12 h, followed by incubation in fresh medium for different time courses. (D) Relative P-gp expression in MCF-7/ADR cells after treatment with free DOX or DOX@SUR nanoparticles at a DOX concentration of 5 µg/mL for 12 or 24 h by flow cytometry. Data are expressed as mean value  $\pm$  SD (n=3). \* $P < 0.05$ , \*\* $P < 0.01$ , \*\*\* $P < 0.001$ .

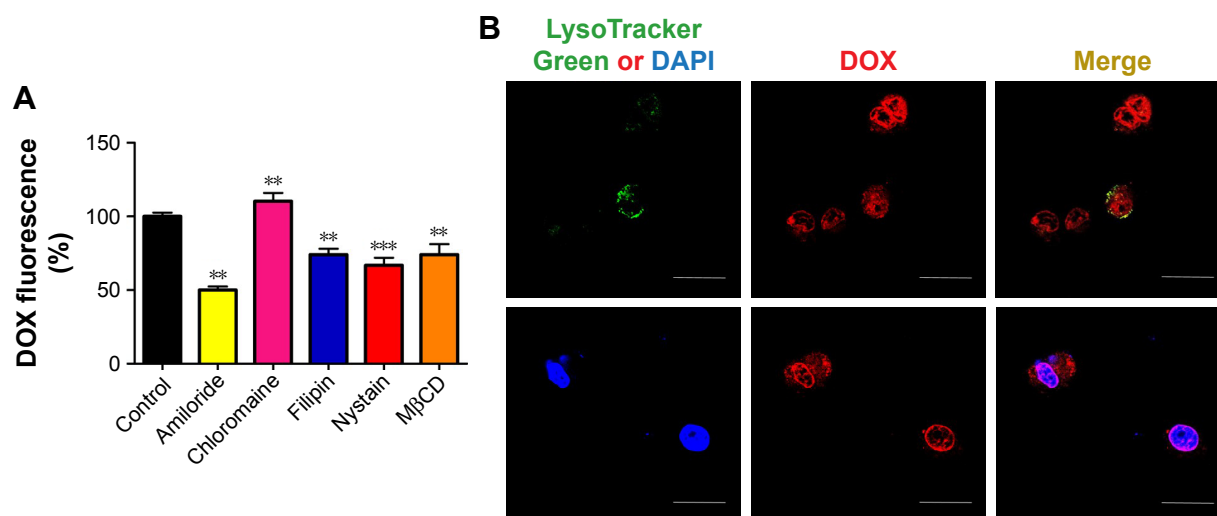
**Abbreviations:** DOX, doxorubicin; P-gp, P-glycoprotein; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

to the lysosomes and released DOX to the nuclei to exert cytotoxicity. To further confirm the nuclear translocation of DOX@SUR nanoparticles, MCF-7/ADR cells were treated with DOX@SUR nanoparticles for different time courses (Figure S2). Consistently, more DOX@SUR nanoparticles were internalized into cells in a time-dependent manner. More importantly, more DOX was detected in the nuclei with increase of incubation time, revealing that DOX was released and translocated to the nuclei after the cellular uptake of DOX@SUR nanoparticles.

## In vivo biodistribution of DOX@SUR nanoparticles

It is widely acknowledged that the in vivo biodistribution of anticancer drugs affects their therapeutic impact and potential

side reactions. To detect the biodistribution of DOX@SUR nanoparticles, MCF-7/ADR-bearing nude mice were intravenously injected with free DOX or DOX@SUR nanoparticles. At 48 h after injection, DOX fluorescence in the major organs (including heart, liver, spleen, lung and kidney) and tumor was first examined by living fluorescence imaging (Figure 5A). DOX@SUR nanoparticles displayed stronger DOX fluorescence in the tumor than free DOX. In order to further confirm the enhanced tumor accumulation capacity of DOX@SUR nanoparticles, quantitative analysis of DOX in these major organs and tumors was conducted after 24 and 48 h of injection (Figure 5B). DOX content in the tumor tissues of mice treated with DOX@SUR nanoparticles was nearly 2.1-fold that of free DOX at 24 h and it even increased to 3.5-fold after 48 h of injection. Moreover, DOX content in



**Figure 4** Endocytic pathway and intracellular trafficking of DOX@SUR nanoparticles.

**Notes:** (A) Relative DOX fluorescence intensity in MCF-7/ADR cells after pretreatment with 2 mM amiloride, 10  $\mu$ M chlorpromazine, 10  $\mu$ M filipin, 20  $\mu$ M nystatin or 5 mM M $\beta$ CD for 30 min and then treatment with DOX@SUR nanoparticles at a DOX concentration of 5  $\mu$ M for 1 h, respectively. Data are expressed as mean value  $\pm$  SD (n=3). \*\* $P$ <0.01, \*\*\* $P$ <0.001 compared to the control group. (B) Confocal microscopic images of the intracellular localization of DOX@SUR nanoparticles in MCF-7/ADR cells treated with DOX@SUR nanoparticles at a DOX concentration of 5  $\mu$ M for 4 h. Scale bar: 25  $\mu$ m.

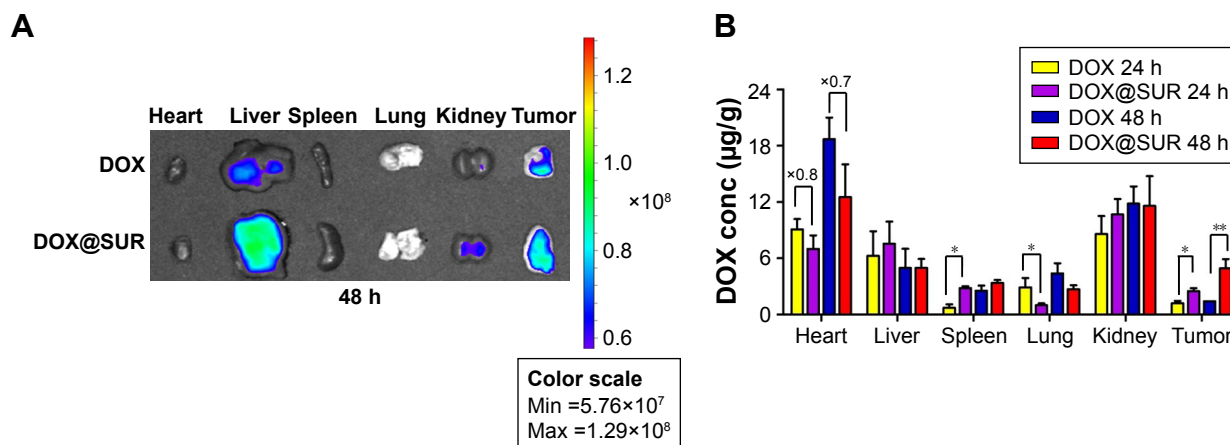
**Abbreviations:** DAPI, 4,6-diamidino-2-phenylindole; DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin; M $\beta$ CD, methyl- $\beta$ -cyclodextrin.

the heart of mice treated with DOX@SUR was slightly lower than that of mice treated with free DOX either after 24 or 48 h, indicating that nanoparticles might have the ability to reduce DOX cardiotoxicity compared to free DOX. These facts consistently suggested that DOX@SUR nanoparticles exhibited good tumor-targeting efficiency, which was mostly due to their enhanced EPR effect.

## Antitumor activity of DOX@SUR nanoparticles

The efficiency of DOX@SUR nanoparticles to overwhelm MDR was further evaluated in a drug-resistant MCF-7/ADR

tumor model. The tumor growth curves (Figure 6A) displayed that blank SUR nanoparticles showed almost similar tumor growth inhibition activity with free DOX. DOX@SUR nanoparticles exhibited the strongest suppression of tumor growth compared to free DOX and blank SUR nanoparticles. Moreover, the weights of excised tumors after treatment also showed a similar trend (Figure 6B and C). These results indicate that DOX@SUR nanoparticles noticeably enhanced the anticancer potential of free DOX and SUR, which might be attributed to the enhanced tumor targeting and reversal MDR of DOX@SUR nanoparticles.

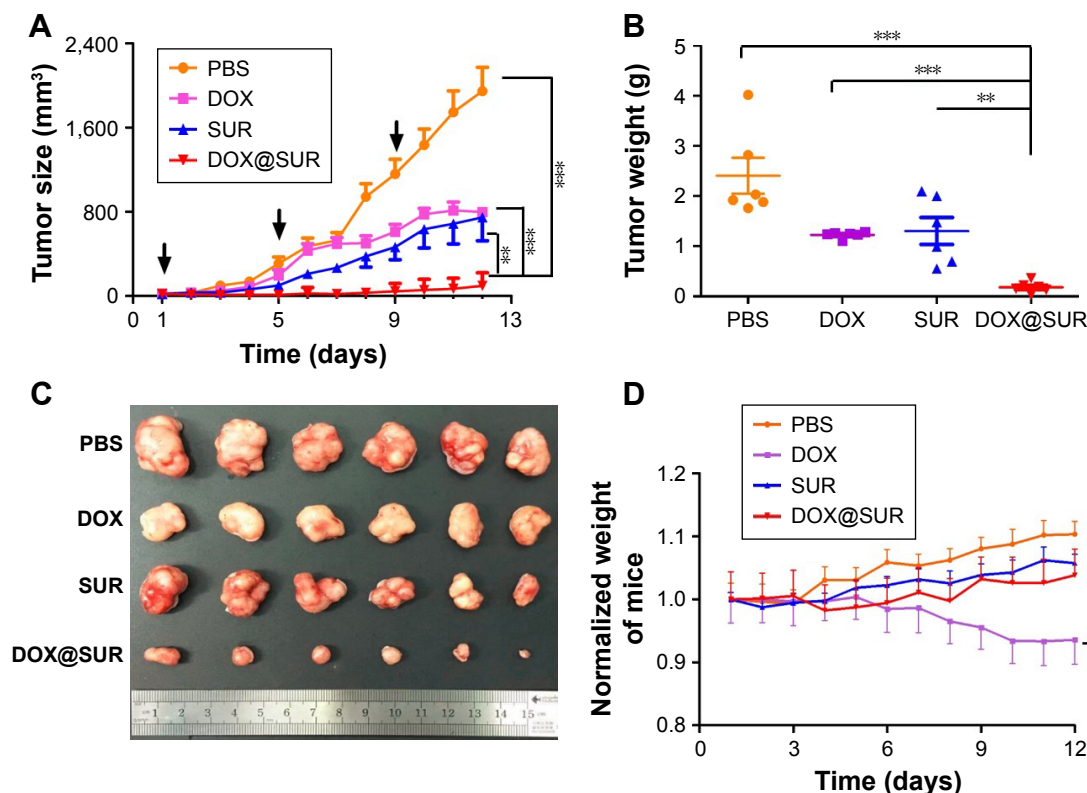


**Figure 5** In vivo biodistribution of DOX@SUR nanoparticles.

**Notes:** (A) Ex vivo fluorescent images of DOX in major organs and tumors at 48 h after intravenous injection of free DOX or DOX@SUR nanoparticles at the DOX dosage of 5 mg/kg, respectively. (B) Quantitative analysis of DOX distribution in the major organs and tumors at 24 and 48 h after intravenous injection of free DOX or DOX@SUR nanoparticles at the DOX dosage of 5 mg/kg. Data are expressed as mean value  $\pm$  SD (n=3). \* $P$ <0.05, \*\* $P$ <0.01.

**Abbreviations:** DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.





**Figure 6** In vivo antitumor study of DOX@SUR nanoparticles in Balb/c nude mice implanted with MCF-7/ADR cells.

**Notes:** (A) Tumor growth inhibition profiles in MCF-7/ADR-bearing nude mice after intravenous injection of PBS, blank SUR nanoparticles, free DOX or DOX@SUR nanoparticles at the DOX dose of 5 mg/kg. Black arrows indicate the injection time points. (B) Tumor weight at the end of treatment. (C) Photographs of the tumors at the end of treatment. (D) Body weight change of MCF-7/ADR-bearing nude mice during treatment. Data are expressed as mean value  $\pm$  SD ( $n=6$ ). \* $P<0.05$ , \*\* $P<0.01$ , \*\*\* $P<0.001$ .

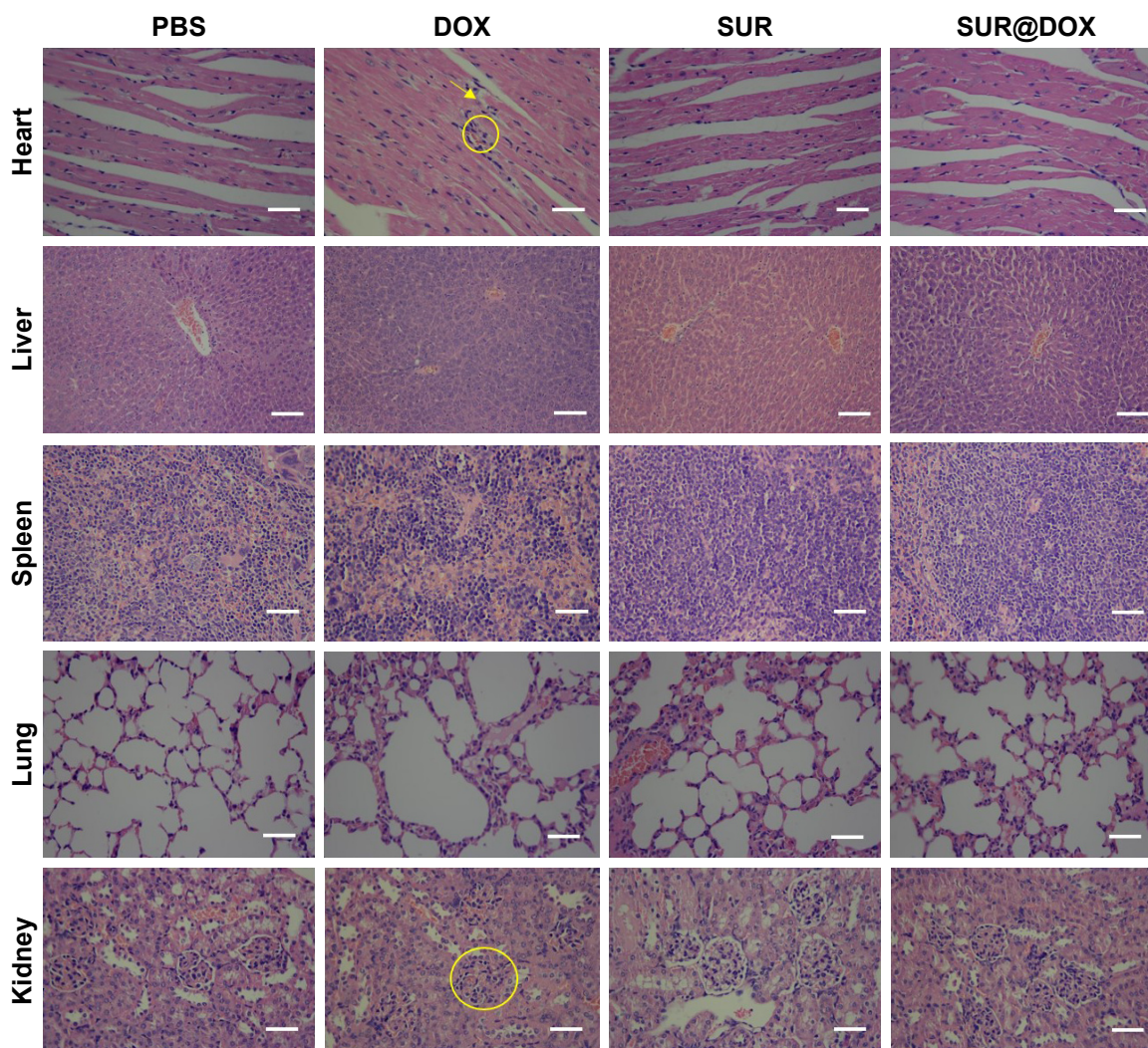
**Abbreviations:** DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

In addition to possessing potential activity of reversing MDR, it is equally important for the nanosized drug delivery systems to be biosafe in vivo.<sup>28</sup> Body weight is considered as an important indicator of general systemic toxicity.<sup>29</sup> The body weight increased in PBS group and decreased in free DOX-treated group (Figure 6D). However, the body weight in DOX@SUR nanoparticle-treated group was substantially unchanged compared to that of PBS group. These findings indicate that the DOX@SUR nanoparticles did not show obvious toxicity, even though free DOX might exhibit systemic toxicity. Furthermore, histopathologic changes of major organs including heart, liver, spleen, lung and kidney were evaluated in MCF-7/ADR xenograft tumor by H&E staining (Figure 7). Cardiotoxicity is the main threat of DOX-based chemotherapy. Noticeable neutrophil accumulation was seen in the heart slices of free DOX-treated group, while DOX-caused cardiocytotoxicity was markedly inhibited in DOX@SUR-treated group. The other tested tissue sections did not show any significant lesion. In addition, serological analysis showed that DOX@SUR nanoparticles did not cause significant toxicity to liver

and kidney function (Figure S3). These fallouts confirmed that DOX@SUR nanoparticles were capable of overcoming MDR and exhibited stronger anticancer activity with reduced adverse effects.

## Conclusion

We have successfully formed DOX-loaded SUR nanoparticles to reverse MDR in cancer therapy. SUR with anticancer activity was self-assembled into nanoparticles to load DOX with a high drug loading efficiency. DOX@SUR nanoparticles exhibited enhanced cellular uptake and decreased cellular efflux in MCF-7/ADR cells due to P-gp inhibition, which resulted in augmented cytotoxicity compared to free DOX. After the DOX@SUR nanoparticles were internalized into MCF-7/ADR cells by macropinocytosis- and caveolin-mediated endocytosis, they were transported to the lysosomes and then translocated to the nucleus to exert cytotoxicity. Moreover, DOX@SUR nanoparticles displayed enhanced tumor accumulation. Therefore, superior in vivo tumor inhibition activity of DOX@SUR nanoparticles was observed in MCF-7/ADR-bearing nude mice with fewer side effects.



**Figure 7** H&E staining assay of major organs and tumors at the end of tumor growth inhibition studies.

**Notes:** Yellow arrows and rings in the heart and kidney sections of free DOX-treated mice indicate severe toxicity. Scale bar: 200  $\mu$ m.

**Abbreviations:** DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

This study demonstrated that SUR-based nanoparticles might be used as potential anticancer drug carriers to reverse MDR in cancer chemotherapy.

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## Disclosure

The authors report no conflicts of interest in this work.

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## Supplementary materials

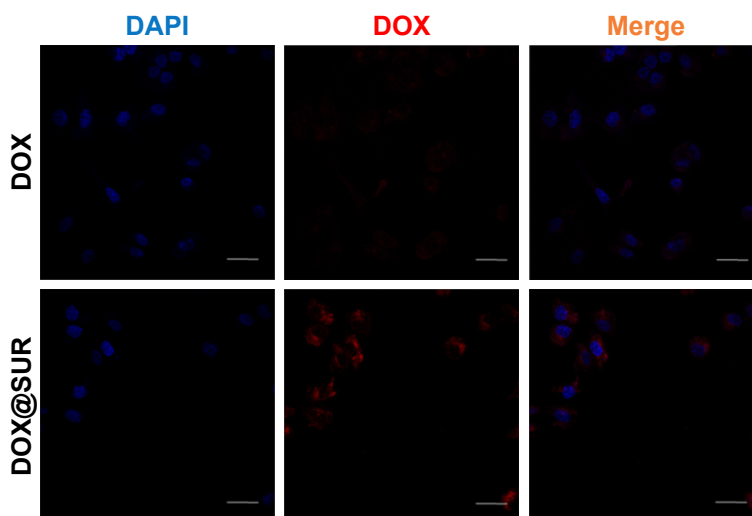
**Table S1** Primer sequences used for real-time RT-PCR

Gene	Primers
GADPH	Forward: GAGAGAAACCCGGGAGGCTA Reverse: GCGCCAATACGACCAAATC
Bcl-2	Forward: GTGAAGTGGGGGAGGATTGTG Reverse: TTCAGAGACAGCCAGGAGAAATC
Bax	Forward: TTTTGCTTCAGGGTTTCATCCA Reverse: TGCCACTCGGAAAAAGACCTC
Ki-67	Forward: ACGCCTGGTTACTATCAAAAGG Reverse: CAGACCCATTACTTGTGTTGGA

**Table S2** IC<sub>50</sub> values of DOX and DOX@SUR against MCF-7 and MCF-7/ADR cells after 48 h of treatment as determined by MTT assay

IC <sub>50</sub> values (μg/mL)			
MCF-7		MCF-7/ADR	
DOX	DOX@SUR	DOX	DOX@SUR
0.35	0.44	147	15.6

**Abbreviations:** DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

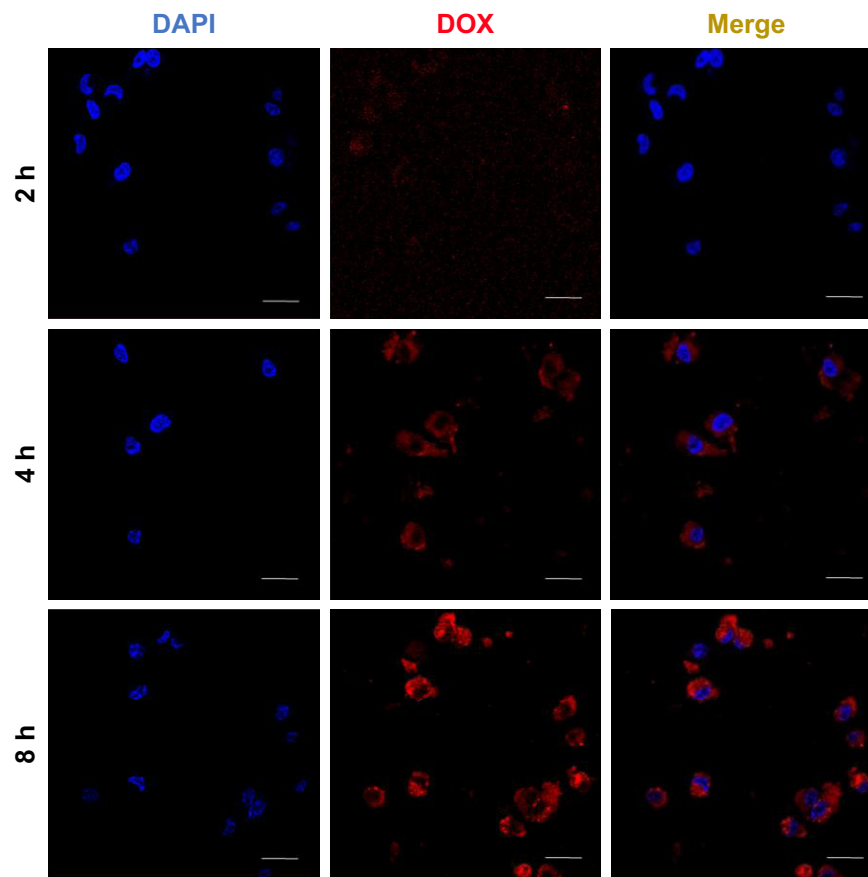


**Figure S1** Confocal microscopic images of the intracellular DOX localization of MCF-7/ADR cells treated with free DOX or DOX@SUR nanoparticles at a DOX concentration of 5 μg/mL for 8 h.

**Note:** Scale bar: 25 μm.

**Abbreviations:** DAPI, 4,6-diamidino-2-phenylindole; DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded SUR.

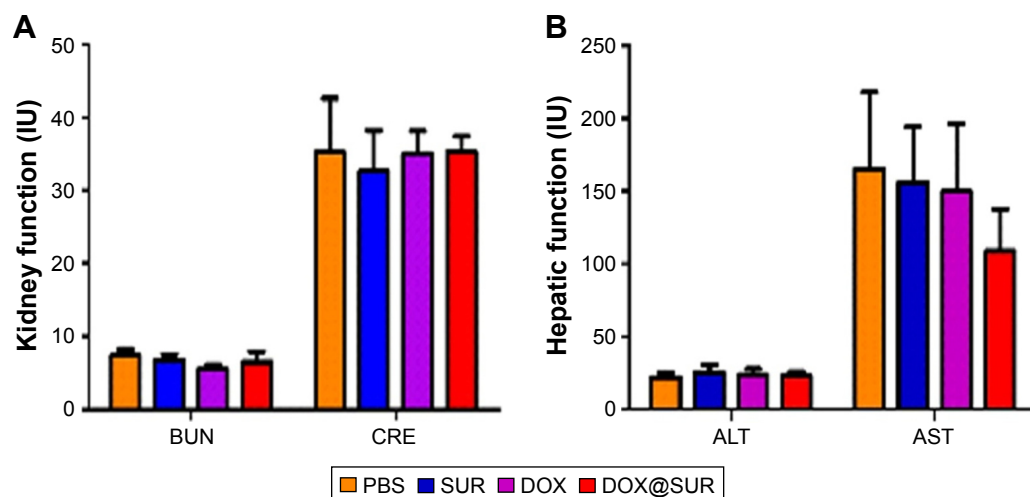




**Figure S2** Confocal microscopic images of the intracellular DOX localization of MCF-7/ADR cells treated with DOX@SUR nanoparticles at a DOX concentration of 5  $\mu\text{g/mL}$  for different time courses.

**Note:** Scale bar: 25  $\mu\text{m}$ .

**Abbreviations:** DAPI, 4,6-diamidino-2-phenylindole; DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.



**Figure S3** Serological analysis of MCF-7/ADR-bearing nude mice at the end of tumor inhibition experiments, including ALT, AST, BUN and CRE.

**Note:** Data are represented as mean value  $\pm$  SD ( $n=6$ ).

**Abbreviations:** ALT, alanine transaminase; AST, aspartate aminotransferase; BUN, blood urea nitrogen; CRE, creatinine; DOX, doxorubicin; SUR, surfactin; DOX@SUR, DOX-loaded surfactin.

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